ORIGINAL PAPER

Immobilization of tyrosinase on Fe₃O₄@Au core–shell nanoparticles **as bio‑probe for detection of dopamine, phenol and catechol**

Elham Arkan1 · Changiz Karami1 · Ronak Rafpur2

Received: 30 April 2019 / Accepted: 14 July 2019 © Society for Biological Inorganic Chemistry (SBIC) 2019

Abstract

An optical bio-probe based on the immobilized tyrosinase on the surface of $Fe₃O₄@Au$ was described for the detection of dopamine, phenol and catechol. The prepared bio-probe (Fe₃O₄@Au@tyrosinase) was characterized by means such as TEM, SEM, VSM, DLS and TGA. In the presence of the bio-probe, the phenol, catechol and dopamine were converted to benzoquinone, o-quinone and dopaquinone, and the fuorescence spectra appeared at 308 nm, 329 nm and 336 nm with ex = 270 nm, respectively. However, by increasing the concentration of phenolic compounds in the bio-probe, the amount of products (benzoquinone, o-quinone and dopaquinone) was increased which was the reason for the increase in fuorescence intensity. Using this mechanism, a bio-probe was designed such that the intensity of the fuorescence spectra increased proportionally with the increase of the substrate concentrations after different time periods. The 0.003 mg/mL of tyrosinase was loaded on 1.65 mg/mL of the Fe₃O₄@Au. The highest performance for a bio-probe was demonstrated at room temperature and pH 6.8. By investigating the characteristics of the response of the bio-probe to diferent phenolic compounds, it was found that the bio-probe had a linear response in the concentration range 5.0–75.0 μ M, 10.0–100.0 μ M for phenol and dopamine and 50.0–500.0 M for catechol. The Michaelis–Menten constant (K_m) of the bio-probe was calculated as $0.6 \mu M$. Finally, the bio-probe seems to be stable and efficient even after about 2 months.

Graphic abstract

A novel and easy method for the detection of dopamine, phenol and catechol by forescence that uses oxide capability to identify the phenolic compounds was introduced.

Keywords $Fe₃O₄@Au \cdot Optical sensor \cdot Core-shell \cdot Tyrosinase immobilization \cdot Bio-probe \cdot Dopamine \cdot Phenol and$ catechol

Electronic supplementary material The online version of this article [\(https://doi.org/10.1007/s00775-019-01691-0\)](https://doi.org/10.1007/s00775-019-01691-0) contains supplementary material, which is available to authorized users.

Extended author information available on the last page of the article

Introduction

One of the most critical constituents of hormones and neurotransmitters is the dopamine (DA) composition, which is a family of catecholamine and phenethylamine. Motivation, emotion, endocrine regulation, and locomotion are the essential roles of dopamine in the human body [[1\]](#page-6-0). Regarding the usefulness of dopamine, the abnormal amount of dopamine causes a series of diseases, including schizophrenia and anorexia Parkinson's disease [\[2](#page-6-1)]. However, the amount of this compound in living organisms is between 0.1 and 10.0 mM, which is very low [\[3](#page-6-2), [4](#page-6-3)]. Therefore, the measuring of dopamine amount for researchers is still interesting [\[5\]](#page-6-4). Catechol is another compound that causes a series of diseases in humans, animals, and plants, and its toxicity is dangerous because the skin quickly absorbs it [\[6](#page-6-5), [7](#page-6-6)].

Another compound that is considered by researchers is phenol [[8\]](#page-6-7). Phenol is one of the most common compounds that cause environmental contamination, and this compound as a corrosive compound is easily absorbed by contact with skin or by ingestion and inhalation. One of the disadvantages of phenol is that the amount of 21 μ M is very toxic and dangerous to fsh and the concentration between 106 and 1062 µM causes the death of the entire aquatic ecosystem [[9,](#page-6-8) [10\]](#page-6-9). It is considering that the wide variety of sources are available for the production of phenol, including the refneries coal processing, coking operations, manufacture of petrochemicals, wood product, plastic, pharmaceutical, and paper industries, etc. However, it can be concluded that a large amount of this composition exists in the environment, including drinking water [[11,](#page-7-0) [12\]](#page-7-1). Besides, the use of drinking water, with phenol, can lead to several diseases including diarrhea, nausea, dark urine, mouth sores, kidney damage and paralysis of the central nervous system [[13](#page-7-2)]. The bioaccumulation of phenol in human and animal tissue and biomagnifcation in food chains can lead to severe contamination and hence is a signifcant concern [[14\]](#page-7-3).

So far, diferent methods for measuring dopamine have been introduced, such as mass spectrometry, high-performance liquid chromatography, and electrochemical techniques [\[15](#page-7-4)–[17\]](#page-7-5). The same techniques, such as gas chromatography, capillary electrophoresis, and spectrophotometry analysis, are used to measure phenol [\[18](#page-7-6), [19](#page-7-7)], but these techniques have a lot of drawbacks. For instance, gas chromatography and HPLC are time consuming, complicated and also involves expensive equipment. Among others, fuorescencebased methods are remarkable for researchers because this technique can detect trace amounts of analytes in various samples. Sensitivity, wide linear dynamic range, rapidity, high accuracy, and selectivity are the advantages of fuorescence methods that make it attractive to researchers [[20](#page-7-8)[–23](#page-7-9)].

In various felds of science, including drug delivery, pharmacy and biotechnology, the $Fe₃O₄$ magnetic nanoparticles are of interest to researchers which attributed to the low toxicity, biocompatibility, strong supermagnetism, catalytic activity, the ease of preparation, the ability to functionalize, and the separation of the product from the external magnetic feld in the reaction [\[24](#page-7-10)[–30](#page-7-11)].

Among different $Fe₃O₄$ magnetic structures, the Fe@Au (core–shell) structure is very important. The Au as an inert element is very suitable for coating magnetic nanoparticles, unique biocompatibility and versatility in surface modifcation [[31\]](#page-7-12). Due to the noticeable advantages of Au nanoparticles, this core–shell ability has made it possible to modify biomolecules such as enzymes and use them as biosensors.

A lot of sensors were used [[32–](#page-7-13)[37\]](#page-7-14). Biosensors are introduced as an ideal system for monitoring phenolic structures due to high selectivity, fast response cost-efectiveness and simplicity of operation and manufacture. Known biomolecules such as tyrosinase [[38\]](#page-7-15), laccase [[39](#page-7-16)] and horseradish peroxidase are used as biosensors and bio-probe to the detection of phenolic compounds [\[40](#page-7-17)]. The tyrosinase enzymes can catalyze reactions: the hydroxylation of monophenols to benzoquinone and the oxidation of o-diphenols to o-quinones [\[41](#page-7-18)]. However, due to limitations on the use of enzymes, the design of biosensors based on the immobilization of the tyrosinase enzyme is very much considered [[42\]](#page-7-19). Several examples of immobilization methods such as incorporation within carbon paste [\[43\]](#page-7-20), physical adsorption [[44\]](#page-7-21), immobilization in polymer flms [[45](#page-7-22)], and covalent cross-linking [[46\]](#page-7-23) have been reported. These methods had problems such as complicated synthesis, low stability, weak bioactivity maintenance, etc. Thus, the immobilization of the tyrosinase that does not have the issues listed above is a special challenge for researchers.

By considering the advantages of using the core–shell of iron–gold structure, in this research, the bio-probe of $Fe₃O₄$ @tyrosinase was synthesized and characterized by several techniques such as TEM, FT-IR, SEM, TGA, VSM, and DLS. Proposed mechanism for this bio-probe, the compounds such as phenol, catechol and dopamine was oxidation and convert to benzoquinone, o-quinone and dopaquinone, respectively, in the presence of tyrosinase, and a new fuorescence spectrum at 308 nm, 329 nm and 336 nm, respectively, was appeared. By increasing the concentration of each of these compounds into the specifed amount of $Fe₃O₄$ @tyrosinase, the fluorescence spectrum increased. Thus, by linking the spectrum of fuorescence to the phenol concentration of 308 nm, catechol at 329 nm and dopamine at 336 nm, a bio-probe can be designed to detect phenol, catechol and dopamine. Finally, to evaluate the best conditions, the parameters such as time, temperature and pH of the reaction were also investigated.

Experimental

Reagents

The chemical materials such as tyrosinase (from mushroom 2067 units/mg), glutaraldehyde (2.5%), *N*-hydroxysuccinimide (NHS), FeCl₂ 4H₂O, 99%, and FeCl₃ 6H₂O, 99% EDC (1-ethyl-3-(3-dimethylaminopropyl)carbodiimide) were purchased from Sigma-Aldrich. Trisodium citrate dehydrates, ammonium hydroxide, $HAuCl₄.4H₂O$ (99.99%) and glutaraldehyde (25% water solution) were purchased from Merck.

Apparatus and measurements

For the functional group properties of the bio-probe, the FT-IR spectra were recorded in the wavenumber range 400–4000 cm−1 [Thermo (AVATAR)]; the surface morphology of nanoparticle was studied by scanning electron microscope (SEM) (TESCAN, MIRA III). The particles were measured by the TEM (JEOL-JEM 2010). The value of the magnetic properties was studied using the vibrating sample magnetometer (VSM, LakeShore 7073). The dynamic light scattering (DLS) was used for hydrodynamic diameter (DLS, Malvern, and ZEN3600). Thermal gravimetric analysis (TGA–DTA) was another technique used to characterize the thermal stability of compounds (Germany, Bahr, STA504).

Immobilization of tyrosinase

For immobilization of the tyrosinase on the $Fe₃O₄@Au@$ cysteine, the Fe₃O₄@Au@cysteine was modified using glutaraldehyde as a cross-linking reagent. $Fe₃O₄@Au@cysteine$ (20 mg) was added to 1.0 ml of glutaraldehyde (2.5%) under the agitation at room temperature for 3 h, and the mixture was centrifuged and the product was washed with PBS four times. Then the tyrosinase (5.0 mg mL⁻¹⁾ was added to $Fe₃O₄@Au@cysteine with 5.0 ml of PBS (pH 6.8), and$ the mixture was agitated for 24 h at 4 °C. The precipitates were washed by PBS for the removal of excess tyrosinase. The formed magnetic bio-nanoparticles were stored at 4 °C in a refrigerator. The synthesis of the Fe₃O₄ and Fe₃O₄[@] Au@cysteine was described in the supporting information (SI) [[47\]](#page-7-24).

Detection of DA, phenol and catechol

1.65 mg/mL of freshly prepared bio-nanoparticles was mixed with diferent concentrations (10.0–100 µM) of DA solutions, $(5.0-75.0 \mu M)$ phenol solutions and $(50.0-500 \mu M)$ catechol. Then with PBS (pH 6.8) the solution was diluted to 1.0 mL and incubated for 15 min for DA, 5 min for phenol and 10 min for catechol at ambient temperature. In the excitation wavelength at 270 nm, the fuorescence spectra were recorded at 308 nm for phenol, 329 nm for catechol and 336 nm for dopamine. The slit widths were 5 nm and 15 nm for ex/em.

Activity assays of tyrosinase

The Bradford method was used to calculate the amount of immobilized tyrosinase on the $Fe₃O₄@Au@tyrosinase$, The concentration of bovine albumin as a protein standard was measured using the Bradford method. This testing was carried out at ambient temperature. The optimum enzyme loading on 1.65 mg/mL of the $Fe₃O₄@Au$ core–shell was found to be 0.003 mg/mL [\[48](#page-8-0)].

Results and discussion

Characterization of bio‑nanoparticles

The TEM and SEM were used for the characterization of particle size and surface morphology of $Fe₃O₄@Au@$ tyrosinase, the FT-IR was used for functional groups, the DLS, VSM and TGA methods also were used for particle size, magnetic properties and stability of the bio-probe, respectively. The FT-IR spectra of bare Fe₃O₄, Fe₃O₄[@] Au@cysteine and Fe₃O₄@tyrosinase are shown in Fig. [1.](#page-2-0) The peak observed at 585 cm−1 is attributed to the Fe–O bond vibration and the broadband peak at 3300–3500 cm−1 is attributed to the O–H stretching vibrations (Fig. [1a](#page-2-0)). The peak band at approximately 3422 cm−1 is attributed to OH stretching vibration and peak at 2973–2893 cm⁻¹ is related to the stretching vibration of C–H bond. In Fe₃O₄@Au@ cysteine, the peak at 3423 cm^{-1} is attributed to the N–H

Fig. 1 The FT-IR spectra of *a* the Fe₃O₄ nanoparticles, *b* Fe₃O₄[@] Au@cysteine, and *c* Fe₃O₄@tyrosinase

stretching vibrations of amine group $NH₂$ and signals at 2924 and 2968 cm−1 are related to the symmetric and asymmetric vibrations of the C–H bond, and 16,354 cm⁻¹ corresponds to the stretching vibration of the carbonyl group (Fig. [1](#page-2-0)b). To show the presence of enzymes on the surface of the Fe₃O₄@ Au@cysteine, the main peaks at 1571 cm⁻¹, 1405 cm−1 and 3295 cm−1 related to secondary amide and hydroxyl groups, respectively. Therefore, the FT-IR results provide evidential component information of diferently modified $Fe₃O₄$.

The SEM image of bio-nanoparticles is shown in Fig. [2a](#page-3-0) which shows the particles have a spherical shape with 30 nm diameter. Also, the TEM image shows the spherical shape and diameter of the particle (30 nm) (Fig. [2b](#page-3-0)) and shows the thickness of the Au around the core which is about 0.8 nm. The magnetic properties of the bio-probe are shown in Fig. [3.](#page-3-1) Figure [3](#page-3-1)a, b shows the values of the saturation magnetization of the Fe₃O₄ and Fe₃O₄@Au@tyrosinase which are 63.5 and 48.5 emu/g, respectively. A signifcant decrease in the magnetic property of $Fe₃O₄@Au@tyrosinase$ in comparison to the $Fe₃O₄$ state is due to layers such as cysteine, tyrosinase and diamagnetic Au. Anyway, Fig. [3c](#page-3-1), is shown, the Fe₃O₄@Au@tyrosinase is separated with an external magnet at 5 min, and this decreases the magnetic strength does not have much effect on the separation of the bio-probe from the solution. The TGA of the $Fe₃O₄$ and $Fe₃O₄@Au@$ tyrosinase at 15 °C/min under nitrogen atmosphere was done (Fig. [4](#page-4-0)). The TGA curve (a) is related to the as-prepared Fe₃O₄; at 225–250 °C, it loses significant weight (5%) which is due to the dehydroxylation of Fe–O in the $Fe₃O₄$

Fig. 3 Magnetization curves of *a* Fe₃O₄ and *b* Fe₃O₄@Au@ cysteine. *c* The photographs of $Fe₃O₄@Au@tyrosinase$ dispersed in solution (left), and separated from water solution under an external magnetic feld (right)

Applied Magnetic Field (Oe)

Fig. 2 a SEM image of Fe₃O₄ $@$ Au@tyrosinase and **b** TEM image of Fe₃O₄@Au@tyrosinase

Fig. 4 The TGA curves of *a* Fe₃O₄ and *b* Fe₃O₄@Au@cysteine

Fig. 5 The particle size by DLS with $PI = 0.313$

structure [[49](#page-8-1)]. In curve (b), weight loss occurs in several steps, the frst step until 100 ℃ is about 10% weight that is related to the adsorbed physical and chemical water. In the next step that starts at 100 °C until 225 °C is related to the

de-hydroxylation of Fe–O structure, it is losing about 20% of its weight. The last step that starts at 225 °C until 600 °C is due to the decomposition of other functional groups such as carboxyl and hydroxyl of tyrosinase. The TGA curves of $Fe₃O₄@Au@tyrosinase pointed that coated layer of Fe₃O₄ is$ about 58%. Figure [5](#page-4-1) shows the particle size of $Fe₃O₄@Au@$ tyrosinase by a DLS, the particle size in a DLS is 100 nm which is larger than the TEM in comparison. In the explanation of the diference of particle size between DLS and TEM, the TEM image is related to the metal core (Fe and Au) while the DLS contains a metallic core plus the layers of the organic ligand such as glutaraldehyde, cysteine and tyrosinase.

Possible mechanism of the bio‑sensing

The basic principle of $Fe₃O₄@Au@tyrosinase detection of$ DA, phenol and catechol is illustrated in Scheme [1](#page-4-2). Considering that the tyrosinase on the surface of bio-probe was used, and due to the high ability of this enzyme to oxidize phenolic compounds, the basis for detection was based on the ability to oxidize phenolic compounds by tyrosinase. In the presence of the bio-probe, dopamine, phenol and catechol converted to dopaquinone, benzoquinone and o-quinone, respectively [[50,](#page-8-2) [51\]](#page-8-3). For each of these products (benzoquinone, dopaquinone, and quinone), a fuorescence spectrum appeared at 308 nm, 336 nm and 329 nm with $ex = 270$ nm. However, by increasing the concentration of dopamine, phenol and catechol to the bio-probe, the amount of dopaquinone, benzoquinone and o-quinone as a product in the solution increases, so the fuorescence intensity was increased. Using these data, a bio-probe can be designed such that the increase in fuorescence intensity related to increasing the concentration of dopamine, phenol and catechol (Fig. [6](#page-5-0)).

Optimization of the experimental conditions

The optimal conditions for this kind of bio-probes are very important. The optimal conditions for this kind of bio-probes are very important because tyrosinase activity is highly dependent on pH. As you well know, various enzymes require diferent times for their reaction as a catalyst. Nonetheless, the efects of diferent pH values (3, 4, 6, 6.5 and 6.8) for the detection of DA, phenol and catechol were investigated, and the fuorescence intensities at 336 nm, 308 nm and 329 nm for these pHs were calculated. Given the highest performance of the bio-probe, the highest amount of DA, phenol and catechol was oxidized. Therefore, the bestoptimized condition was for a situation that the fuorescence spectrum had a low intensity in the spectrum. Therefore, to continue measuring DA, phenol and catechol, the phosphate buffer at pH 6.8 was used (Figs. S1, S2, S3).

As you know, various enzymes require diferent times for their reaction as a catalyst. To obtain the best reaction time in this system, the fuorescence intensity was calculated with a mixture of $Fe₃O₄@Au@tyrosinase$ and the DA, phenol and catechol at diferent times from 1 min to 30 min. In Figs. S3, S4, and S5, it can be seen that by increasing the reaction time to 5 min for phenol, 15 min for DA and 10 min for catechol, the fuorescence intensity decreases, and after this time the fuorescence intensity reduction can be neglected. Nevertheless, the favorable conditions for these reactions were 5 min for phenol, 15 min for DA and 10 min for catechol with a pH 6.8 of phosphate buffer.

Calibration curves and detection limit

The bio-probe performance in the detection of phenolic compounds (DA, phenol and catechol) under the optimized experimental conditions was studied. For this purpose, the wavelengths of 336, 308 and 329 nm were chosen $(ex = 270 \text{ nm})$ for the respective determination of DA, phenol and catechol, respectively. As shown in Fig. [7](#page-5-1), the intensity of the fuorescence spectra with various concentration ranges of phenolic compounds had diferent performances. The fuorescence intensity of concentration of the dopamine (DA) in the presence of bio-probe was linear over the range $10.0-100.0 \mu M$ with a calibration equation of $y = 5.503x + 107.96$ ($r = 0.96$) (Fig. [7a](#page-5-1)), and 5.0–75.0 µM range with a calibration equation of $y = 8.44x + 338.95$ ($r = 0.9805$) for phenol (Fig. [7](#page-5-1)b). For catechol, a wide range $(50.0–500 \mu M)$ with a calibration equation of $y = 1.51x + 235.5$ ($r = 0.99$) was calculated (Fig. [7](#page-5-1)c). The detection limit of 1.00 µM for DA, 5.00 µM for phenol and 20.00 µM for catechol was obtained (*S*/*N*=3).

For activity, the Michaelis–Menten constant (K_m) was calculated from the Lineweaver–Burk equation:

$$
1/V_{\rm ss} = (K_{\rm m}/V_{\rm max}) \times 1/[C] + (1/V_{\rm max}),\tag{1}
$$

Fig. 6 The emission spectrum of DA, phenol and catechol in the presence of magnetic bio-probe in the experiment $(ex = 270 \text{ nm})$

Fig. 7 The response curve of the biosensor towards **a** DA, **b** phenol and **c** catechol in the diferent range, pH 6.8, **b** Increase in the relative sensitivity of the detection system concerning the concentration of the DA, phenol and catechol

where V_{ss} is the steady-state current, K_m is the Michaelis–Menten constant, V_{max} is the maximum current of the reaction and *C* is the concentration of the substrate. K_m was 0.6 μ M, and V_{max} was 6.8 μ M/min. The calculated K_{m} was lower than previous research [\[7,](#page-6-6) [42\]](#page-7-19) which indicates that this enzyme has higher phenolic compound affinity.

Selectivity and interferences

The oxidation products of phenol, dopamine and catechol had specific wavelength at $ex = 270$ nm; however, the selectivity of the technique was examined with other molecules such as uric acid (UA), glucose (Glc), inositol (Ins), amino acids such as Ala, Gln, Cys, Arg, Glu, Leu, Ile, Trp and Lys), and some ions such as Mg^{2+} , Na^{+} , Ca^{2+} , and K^{+}). In Fig. S6, it is seen that the fluorescence spectrum at $ex = 270$ nm does not appear; therefore, this system is not selective for the above materials. For the study of interferences, Fig. S7 clearly shows phenolic compounds (phenol, dopamine and catechol) with the compounds mentioned above not interfering with the results of the proposed method even if they were present at 100-fold higher concentrations.

Real sample analysis

To evaluate the real sample analysis of the proposed method, the human serum samples were collected from healthy volunteers and diluted tenfold by PBS (pH 6.8) before. The known concentrations of DA, phenol or catechol were spiked to diluted human serums and detected under the optimum conditions. As shown in Table [1,](#page-6-10) the results fully agree with the spiked values. These results suggest that matrix efects from the diluted serum did not afect the substantial detection.

Conclusion

A favorable method of immobilized tyrosinase in a Fe₃O₄[@] Au core–shell for the development of an optical bio-probe of dopamine, phenol and catechol has been described based on the oxidation of the phenolic compounds in the presence of tyrosinase. By increasing the substrate concentration, the fuorescence intensity was increased proportionally. The bio-probe permits good sensitivity and stability. The LOD towards DA, phenol and catechol was observed to be 1.00 μ M for DA, 5.00 μ M for phenol and 20.00 μ M (*S*/*N*=3). Eventually, the developed bio-probe has good potential for determining the amount of dopamine, phenol and catechol in human serum.

Table 1 Determination of concentration amounts of DA, phenol or catechol in serum samples $(n=3)$

Sample		Added (μM)	Found (μM)	Recovery $(\%)$	RSD%
DA	1	Ω			
	$\overline{2}$	10	9.9	99	5.1
	3	20	21	105	4.76
	$\overline{4}$	50	54.3	108	2.8
Phenol	1	0			
	\overline{c}	10	10.4	104	5.7
	3	20	19.8	99	5.2
	$\overline{4}$	50	53.6	101.2	3.87
Catechol	1	0			
	$\overline{2}$	50	52.1	100.2	1.4
	3	100	103	103	4.2

Acknowledgements The authors gratefully acknowledge the Research Council of Kermanshah University of Medical Sciences (Grant number: 97708) for the fnancial support.

References

- 1. Liggett SB (2000) Pharmacogenetics of beta-1-and beta-2-adrenergic receptors. Pharmacology 61(3):167
- 2. Jaber M, Robinson SW, Missale C, Caron MG (1996) Dopamine receptors and brain function. Neuropharmacology 35(11):1503–1519
- 3. Ali SR, Ma Y, Parajuli RR, Balogun Y, Lai WY-C, He H (2007) A nonoxidative sensor based on a self-doped polyaniline/carbon nanotube composite for sensitive and selective detection of the neurotransmitter dopamine. Anal Chem 79(6):2583–2587
- 4. Ankireddy SR, Kim J (2015) Selective detection of dopamine in the presence of ascorbic acid via fuorescence quenching of InP/ ZnS quantum dots. Int J Nanomed 10(1):113
- 5. He Y-S, Pan C-G, Cao H-X, Yue M-Z, Wang L, Liang G-X (2018) Highly sensitive and selective dual-emission ratiometric fuorescence detection of dopamine based on carbon dots-gold nanoclusters hybrid. Sens Actuators B Chem 265:371–377
- 6. Freire RS, Durán N, Kubota LT (2002) Electrochemical biosensorbased devices for continuous phenols monitoring in environmental matrices. J Braz Chem Soc 13(4):456–462
- 7. Leboukh S, Gouzi H, Coradin T, Yahia H (2018) An optical catechol biosensor based on a desert truffle tyrosinase extract immobilized into a sol–gel silica layered matrix. J Sol-Gel Sci Technol 86(3):675–681
- 8. Gupta VK, Karimi-Maleh H, Sadegh R (2015) Simultaneous determination of hydroxylamine, phenol and sulfte in water and waste water samples using a voltammetric nanosensor. Int J Electrochem Sci 10:303–316
- 9. Huang J, Wang X, Jin Q, Liu Y, Wang Y (2007) Removal of phenol from aqueous solution by adsorption onto OTMAC-modifed attapulgite. J Environ Manag 84(2):229–236
- 10. Contreras EM, Albertario ME, Bertola NC, Zaritzky NE (2008) Modelling phenol biodegradation by activated sludges evaluated through respirometric techniques. J Hazard Mater 158(2–3):366–374
- 11. Busca G, Berardinelli S, Resini C, Arrighi L (2008) Technologies for the removal of phenol from fuid streams: a short review of recent developments. J Hazard Mater 160(2–3):265–288
- 12. Wei G, Yu J, Zhu Y, Chen W, Wang L (2008) Characterization of phenol degradation by Rhizobium sp. CCNWTB 701 isolated from *Astragalus chrysopteru* in mining tailing region. J Hazard Mater 151(1):111–117
- 13. Senturk HB, Ozdes D, Gundogdu A, Duran C, Soylak M (2009) Removal of phenol from aqueous solutions by adsorption onto organomodifed Tirebolu bentonite: equilibrium, kinetic and thermodynamic study. J Hazard Mater 172(1):353–362
- 14. dos Santos VL, de Souza Monteiro A, Braga DT, Santoro MM (2009) Phenol degradation by *Aureobasidium pullu*lans FE13 isolated from industrial effluents. J Hazard Mater 161(2–3):1413–1420
- 15. van de Merbel NC, Hendriks G, Imbos R, Tuunainen J, Rouru J, Nikkanen H (2011) Quantitative determination of free and total dopamine in human plasma by LC–MS/MS: the importance of sample preparation. Bioanalysis 3(17):1949–1961
- 16. Perry M, Li Q, Kennedy RT (2009) Review of recent advances in analytical techniques for the determination of neurotransmitters. Anal Chim Acta 653(1):1–22
- 17. Mao Y, Bao Y, Gan S, Li F, Niu L (2011) Electrochemical sensor for dopamine based on a novel graphene-molecular imprinted polymers composite recognition element. Biosens Bioelectron 28(1):291–297
- 18. Wang C, Wu C, Zhang L, Zhang J (2016) Ultraperformance liquid chromatography–tandem mass spectrometry method for profling ketolic and phenolic sex steroids using an automated injection program combined with diverter valve switch and step analysis. Anal Chem 88(16):7878–7884
- 19. Quynh BTP, Byun JY, Kim SH (2015) Non-enzymatic amperometric detection of phenol and catechol using nanoporous gold. Sens Actuators B Chem 221:191–200
- 20. Gupta VK, Mergu N, Kumawat LK, Singh AK (2015) Selective naked-eye detection of magnesium (II) ions using a coumarinderived fuorescent probe. Sens Actuators B Chem 207:216–223
- 21. Gupta VK, Mergu N, Kumawat LK, Singh AK (2015) A reversible fluorescence "off-on-off" sensor for sequential detection of aluminum and acetate/fuoride ions. Talanta 144:80–89
- 22. Yola ML, Gupta VK, Eren T, Şen AE, Atar N (2014) A novel electro analytical nanosensor based on graphene oxide/silver nanoparticles for simultaneous determination of quercetin and morin. Electrochim Acta 120:204–211
- 23. Gupta VK, Singh AK, Kumawat LK (2014) Thiazole Schif base turn-on fuorescent chemosensor for Al3+ion. Sens Actuators B Chem 195:98–108
- 24. Xing Y, Jin Y-Y, Si J-C, Peng M-L, Wang X-F, Chen C, Cui Y-L (2015) Controllable synthesis and characterization of Fe3O4/Au composite nanoparticles. J Magn Magn Mater 380:150–156
- 25. Zhang T, Wang W, Zhang D, Zhang X, Ma Y, Zhou Y, Qi L (2010) Biotemplated synthesis of gold nanoparticle–bacteria cellulose nanofber nanocomposites and their application in biosensing. Adv Funct Mater 20(7):1152–1160
- 26. Lai G-S, Zhang H-L, Han D-Y (2009) Amperometric hydrogen peroxide biosensor based on the immobilization of horseradish peroxidase by carbon-coated iron nanoparticles in combination with chitosan and cross-linking of glutaraldehyde. Microchim Acta 165(1–2):159–165
- 27. Guo S, Li D, Zhang L, Li J, Wang E (2009) Monodisperse mesoporous superparamagnetic single-crystal magnetite nanoparticles for drug delivery. Biomaterials 30(10):1881–1889
- 28. Pham TTH, Cao C, Sim SJ (2008) Application of citrate-stabilized gold-coated ferric oxide composite nanoparticles for biological separations. J Magn Magn Mater 320(15):2049–2055
- 29. Kim J, Park S, Lee JE, Jin SM, Lee JH, Lee IS, Yang I, Kim JS, Kim SK, Cho MH (2006) Designed fabrication of multifunctional magnetic gold nanoshells and their application to magnetic resonance imaging and photothermal therapy. Angew Chem 118(46):7918–7922
- 30. Baby TT, Ramaprabhu S (2010) SiO2 coated Fe3O4 magnetic nanoparticle dispersed multiwalled carbon nanotubes based amperometric glucose biosensor. Talanta 80(5):2016–2022
- 31. Grabar KC, Freeman RG, Hommer MB, Natan MJ (1995) Preparation and characterization of Au colloid monolayers. Anal Chem 67(4):735–743
- 32. Dehghani MH, Sanaei D, Ali I, Bhatnagar A (2016) Removal of chromium (VI) from aqueous solution using treated waste newspaper as a low-cost adsorbent: kinetic modeling and isotherm studies. J Mol Liq 215:671–679
- 33. Karimi-Maleh H, Tahernejad-Javazmi F, Atar N, Yola ML, Gupta VK, Ensafi AA (2015) A novel DNA biosensor based on a pencil graphite electrode modifed with polypyrrole/functionalized multiwalled carbon nanotubes for determination of 6-mercaptopurine anticancer drug. Ind Eng Chem Res 54(14):3634–3639
- 34. Asfaram A, Ghaedi M, Agarwal S, Tyagi I, Gupta VK (2015) Removal of basic dye Auramine-O by ZnS: Cu nanoparticles loaded on activated carbon: optimization of parameters using response surface methodology with central composite design. RSC Adv 5(24):18438–18450
- 35. Gupta KV, Nayak A, Agarwal S, Singhal B (2011) Recent advances on potentiometric membrane sensors for pharmaceutical analysis. Comb Chem High Throughput Screening 14(4):284–302
- 36. Vinod K (1995) Determination of lead using a poly (vinyl chloride)-based crown ether membrane. Analyst 120(2):495–498
- 37. Jain AK, Gupta VK, Sahoo BB, Singh LP (1995) Copper (II) selective electrodes based on macrocyclic compounds. Analytical proceedings including analytical communications, vol 3. Royal Society of Chemistry, UK, pp 99–101
- 38. Yang L, Xiong H, Zhang X, Wang S (2012) A novel tyrosinase biosensor based on chitosan-carbon-coated nickel nanocomposite flm. Bioelectrochemistry 84:44–48
- 39. Quan D, Kim Y, Shin W (2004) Characterization of an amperometric laccase electrode covalently immobilized on platinum surface. J Electroanal Chem 561:181–189
- 40. Kaf A, Chen A (2009) A novel amperometric biosensor for the detection of nitrophenol. Talanta 79(1):97–102
- 41. Chen X, Cheng G, Dong S (2001) Amperometric tyrosinase biosensor based on a sol–gel-derived titanium oxide–copolymer composite matrix for detection of phenolic compounds. Analyst 126(10):1728–1732
- 42. Abdullah J, Ahmad M, Karuppiah N, Heng LY, Sidek H (2006) Immobilization of tyrosinase in chitosan flm for an optical detection of phenol. Sens Actuators B Chem 114(2):604–609
- 43. Wang J, Fang L, Lopez D (1994) Amperometric biosensor for phenols based on a tyrosinase–graphite–epoxy biocomposite. Analyst 119(3):455–458
- 44. Hall GF, Best DJ, Turner AP (1988) Amperometric enzyme electrode for the determination of phenols in chloroform. Enzym Microb Technol 10(9):543–546
- 45. Cosnier S, Innocent C (1993) A new strategy for the construction of a tyrosinase-based amperometric phenol and o-diphenol sensor. Bioelectrochem Bioenerg 31(2):147–160
- 46. Önnerford P, Emnéus J, Marko-Varga G, Gorton L, Ortega F, Domínguez E (1995) Tyrosinase graphite-epoxy based composite electrodes for detection of phenols. Biosens Bioelectron 10(6–7):607–619
- 47. Karami C, Taher MA (2019) A catechol biosensor based on immobilizing laccase to Fe3O4@ Au core-shell nanoparticles. Int J Biol Macromol 129:84–90
- 48. Karagoz B, Bayramoglu G, Altintas B, Bicak N, Arica MY (2011) Amine functional monodisperse microbeads via precipitation polymerization of *N*-vinyl formamide: immobilized laccase for benzidine based dyes degradation. Bioresour Technol 102(13):6783–6790
- 49. Xie J, Xu C, Kohler N, Hou Y, Sun S (2007) Controlled PEGylation of monodisperse Fe3O4 nanoparticles for reduced non-specifc uptake by macrophage cells. Adv Mater 19(20):3163–3166
- 50. Park S-A, Jang E, Koh W-G, Kim B (2010) Fabrication and characterization of optical biosensors using polymer hydrogel

Afliations

Elham Arkan1 · Changiz Karami1 · Ronak Rafpur2

- \boxtimes Changiz Karami Changiz.karami@gmail.com
- ¹ Nano Drug Delivery Research Center, Kermanshah University of Medical Sciences, Kermanshah, Iran

microparticles and enzyme–quantum dot conjugates. Sens Actuators B Chem 150(1):120–125

51. Chai L, Zhou J, Feng H, Tang C, Huang Y, Qian Z (2015) Functionalized carbon quantum dots with dopamine for tyrosinase activity monitoring and inhibitor screening: in vitro and intracellular investigation. ACS Appl Mater Interfaces 7(42):23564–23574

Publisher's Note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

² Department of Chemistry, Faculty of Sciences, Azad University of Kermanshah, Kermanshah, Iran