

Fast Indirect Fluorine-18 Labeling of Protein/Peptide using the useful 6-Fluoronicotinic acid-2,3,5,6-Tetrafluorophenyl prosthetic group: A Method Comparable to direct Fluorination

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Abstract

Fluorine-18 labeling of biomolecules are mostly performed by an indirect labeling method using a prosthetic group. Fluorine-18 labeled 6-fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester is a useful prosthetic group to radiolabel a protein. Recently we reported an improved preparation of this prosthetic group. To test the conjugation efficiency of the labeled ester prepared by this method we have performed conjugation reactions with two different peptides and a protein. Prostate-specific membrane antigen (PSMA) targeting peptide [^{18}F]DCFPyL, $\alpha\text{v}\beta\text{3}$ integrin receptors targeting peptide [^{18}F]c(RGDfK) and [^{18}F]albumin were prepared in good radiochemical yields. The conjugation reactions were completed at 40 - 50 °C in 10 min. The overall radiochemical yield was 25-43 % in 30-45 min.

1. Introduction

An increasing number of peptide and protein based drugs have been developed for clinical use due to their therapeutic efficacy *in vivo*.¹⁻⁴ This has prompted researchers to develop corresponding radiolabeled peptides and proteins for diagnosis and therapy.⁵⁻⁸ Among the clinically established non-invasive imaging techniques, positron emission tomography (PET) is the most sensitive imaging modality which provides a specific view of normal or abnormal biological processes or conditions.⁹⁻¹¹ The functional information provided by PET imaging allows an earlier diagnosis and clear visualization of the disease state, which is crucial to provide reliable prognosis and therapeutic intervention. Among the many available PET radionuclides, fluorine-18 is the most commonly used positron emitter for routine imaging due to ease of production and appropriate half-life ($t_{1/2} = 110$ min) to allow syntheses, transportation, and imaging procedures.¹²⁻¹⁸

Fluorine-18 incorporation into the large biomolecules can be achieved by either direct or an indirect labeling approach. However, labeling of biomolecules such as peptides or proteins is difficult due to the number and diversity of the functional groups present. Conventional nucleophilic fluorine-18 labeling to form C-¹⁸F bond often requires base and high temperature. Although there are a few examples of direct fluorine-18 labeling of peptide,¹⁹⁻²² protein labeling is typically performed using an indirect labeling method. In this approach a small molecule containing a suitable functional group is radiolabeled by conventional nucleophilic substitution chemistry using [¹⁸F]fluoride and conjugated with proteins of interest. The most widely used prosthetic group is N-succinimidyl-4-[¹⁸F]fluorobenzoate ([¹⁸F]SFB)²³⁻²⁷ for conjugation with amine functionalities. Other commonly used prosthetic groups include 4-[¹⁸F]fluorobenzaldehyde ([¹⁸F]FBA)²⁸⁻³³ for reaction with amine functionalities and ¹⁸F-N-[2-(4-Fluorobenzamido)ethyl]maleimide [¹⁸F]FBEM³⁴⁻³⁶ for conjugation with thiols on cysteine residues. Click chemistry, widely applied in many fields of chemical sciences, has also been applied to radiolabel peptides/proteins.^{37, 38} However, while each of these synthesis methods has certain advantages, other complications have limited their applications for clinical purposes. Therefore, there is a continuing effort to develop a rapid, clean and mild synthesis technique for the radiolabeling of peptides/proteins.

Several very useful aqueous based fluorine-18 labeling methods such as [¹⁸F]AlF₆^{39, 40} B-¹⁸F^{41, 42} and Si-¹⁸F^{43, 44} have been developed to radiolabel biomolecules. Fluorine-18 labeling was usually achieved at elevated temperature, therefore direct fluorination was restricted to only thermally stable peptides. Recently room temperature fluorination using [¹⁸F]AlF was achieved by modifying the chelate.⁴⁰ In all approaches, the precursor cannot be separated from the labeled product. Hence there is a fine balance between the amount of precursor used

and specific activity (SA) of the tracers. Large amounts of starting fluorine-18 are often required to produce tracers with high SA.

In 2010, Olberg et al. reported synthesis of fluorine-18 labeled 6-fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester for radiolabeling peptides.⁴⁵ The radiolabeling method is straight forward (one-step) in comparison with multi-step synthesis of [¹⁸F]SFB.²³⁻²⁷ The synthesis time is significantly shorter as there is no need of time consuming HPLC purification. Moreover, stability of tetrafluorophenyl ester is better at higher pH. This prosthetic group has been used by us and others to radiolabel peptides/proteins.^{46, 47} Recently, we reported a simple preparation of 6-[¹⁸F]fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester on an anion-exchange cartridge (Chromafix 30-PS-HCO₃) without azeotropic drying of fluorine-18.⁴⁸ Purification of the labeled product was done by Oasis MCX Plus cartridge. The overall synthesis time is only 5 min, similar to the catch and release of the fluorine-18 on the anion exchange cartridge. Herein we report the rapid conjugation of this 6-[¹⁸F]fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester prepared by our new technique with peptide (RGD), protein (albumin) and a small molecule (PSMA targeting) in short synthesis time.

2. Materials and Methods

PSMA precursor, di-tert-butyl (((S)-6-amino-1-(tert-butoxy)-1-oxohexan-2-yl)carbamoyl)-L-glutamate formate salt, and cold standard were prepared according to the literature method.⁴⁹

Cyclic peptide c(RGDfK) was obtained from Peptides International Inc. (Louisville, KY, USA). PBS 1X buffer (Gibco) was obtained from Life Technologies (Carlsbad, CA, USA).

Normal saline was obtained from Quality Biological (Gaithersburg, MD, USA). PD10 MiniTrapTM columns were obtained from GE Healthcare Bioscience (Pittsburg, PA, USA).

All other chemicals and solvents were received from Sigma-Aldrich (St. Louis, MO, USA)

and used without further purification. The precursor N,N,N-trimethyl-5-((2,3,5,6-tetrafluorophenoxy)carbonyl)pyridin-2-aminium fluoromethanesulfonate (**1**) and cold standard 6-fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester were prepared as previously described.^{45, 46} Fluorine-18 was obtained from National Institutes of Health cyclotron facility (Bethesda, MD, USA). Chromafix 30-PS-HCO₃ anion-exchange cartridge was purchased from Macherey-Nagel (Düren, Germany). Columns and all other Sep-Pak cartridges used in this synthesis were obtained from Agilent Technologies (Santa Clara, CA, USA) and Waters (Milford, MA, USA), respectively. tC18 environmental cartridge was activated by passing 5 mL ethanol followed by 10 mL water. Oasis MCX Plus cartridge was conditioned with 5 mL anhydrous acetonitrile. Semi-prep HPLC purification and analytical HPLC analyses for radiochemical work were performed on an Agilent 1200 Series instrument equipped with multi-wavelength detectors. Mass spectrometry (MS) was performed on a 6130 Quadrupole LC/MS Agilent Technologies instrument equipped with a diode array detector.

2.1. Preparation of ¹⁹F standard of c(RGDfK)

To a solution of c(RGDfK) (10 mg, 0.016 mmol) in acetonitrile (1 mL) and water (1 mL) was added 6-fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester (4.67 mg, 0.016 mmol) and N,N-diisopropylethylamine (6.2 mg, 0.048 mmol). The reaction mixture was stirred at 50 °C for 1 h. The product was purified by semi-preparative HPLC (conditions: Agilent Eclipse plus C18 column (9.4 × 250 mm, 5 μm), mobile phase: 5 - 50% acetonitrile in water (0.1% TFA), with a flow rate of 4.0 mL/min.) The product peak was collected and freeze-dried to obtain the ¹⁹F cold standard of c(RGDfK). (3 mg, 27% yield). LC/MS calculated for C₃₃H₄₃FN₁₀O₈, 726.32, found 727.20 (M + H)⁺.

2.2. Radiosynthesis of 6-¹⁸F]fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester (**3**)⁴⁸

Fluorine-18 labeled target water (10-25 mCi) was diluted with 2 mL water and passed through an anion-exchange cartridge (Chromafix 30-PS-HCO₃). The cartridge was washed with anhydrous acetonitrile (6 mL) and dried for 1 min under vacuum. The [¹⁸F]fluoride from the Sep-Pak was eluted with quaternary ammonium triflate precursor (5-7 mg, **1**) in 0.5 mL 1:4, acetonitrile : *t*-butanol through a conditioned Oasis MCX Plus cartridge. The cartridge was flushed with 1 mL acetonitrile and collected in the same vial for small molecule and peptide labeling. The cartridges were flushed with 2 mL diethyl ether for protein labeling.

2.3. Radiosynthesis and stability test of [¹⁸F]c(RGDfK)

To the solution of **3** (1.5 mL) was added a mixture of c(RGDfK) (3-5 mg) and sodium bicarbonate (10-15 mg) in 1 mL water. The solution was stirred for 10 min at 50 °C. The product was purified by either Sep-Pak or semi-prep HPLC. For Sep-Pak purification, the mixture was diluted with 30 mL of water and passed through tC18 environmental cartridge. The cartridge was washed with water (10 mL) followed by 10% ethanol in water (10 mL). The product was eluted with 3 mL 30% ethanol in water. For semi-prep HPLC purification, the crude reaction mixture was diluted with 2 mL HPLC buffer and injected to the HPLC (conditions: Phenomenex Luna (2) C18 column (10 × 250 mm, 5 μm), mobile phase: 25% ethanol in 50 mM o-phosphoric acid, with a flow rate of 4 mL/min). The identity and purity of the product was confirmed by analytical HPLC.

To test the serum stability, 2 mCi of [¹⁸F]c(RGDfK) was added to whole human serum (2 mL) and kept at room temperature. At different time interval (0, 1, 2 and 4h), 20 μL of the incubated sample was directly injected to the analytical HPLC (supporting information, **Figure S3**) without further processing.

2.4. Radiosynthesis of [¹⁸F]DCFPyL

To the solution of **3** (1.5 mL) was added an acetonitrile solution (300 μL) of di-tert-butyl (((S)-6-amino-1-(tert-butoxy)-1-oxohexan-2-yl)carbamoyl)-L-glutamate formate salt (3-5 mg)⁴⁹ with triethylamine (5 μL). The solution was stirred for 10 min at 50 °C. Solvent was evaporated under N₂ and vacuum, and TFA (400 μL) was added. The mixture was stirred for 10 min at 50 °C. TFA was removed under N₂ and vacuum. Ethanol in 50 mM phosphoric acid (10%, 3 mL) was added to the crude mixture, which was purified by semi-prep HPLC (conditions: Agilent Eclipse plus C18 column (9.4 × 250 mm, 5 μm), mobile phase: 12% ethanol in 50 mM phosphoric acid, with a flow rate of 4 mL/min). The identity and purity of the product was confirmed by analytical HPLC.

2.5. Radiosynthesis of [¹⁸F]albumin

The solvent from **3** was removed under nitrogen at 40 °C. The conjugation reaction with albumin was performed according to the literature method.⁴⁶ Briefly, to the vial containing **3** was added albumin (20 mg in 450 μL of phosphate buffer of pH 9 + 50 μL dimethylsulfoxide) and incubated for 15 min at 40 °C. The product was purified by PD10 Minitrap size exclusion column using phosphate buffer (pH 7.4) as an eluent. The product fraction was collected in 0.8 mL. Formation of the product was confirmed by analytical HPLC.

3. Results and Discussion

Fluorine-18 labeled 6-fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester (**3**), first reported by Olberg et al., is a useful prosthetic group for radiolabeling of biomolecules.⁴⁵⁻⁴⁷ Compound **3** for this study was prepared according to the literature method⁴⁸ recently reported by us and purified by passing through an activated Oasis MCX Plus cartridge. In this

method, **3** is formed directly by passing the precursor solution (**1**) through the anion-exchange cartridge (Chromafix 30-PS-HCO₃). The use of anhydrous acetonitrile, DMSO or mixture of acetonitrile/ *t*-butanol is necessary for nucleophilic displacement to form the product (**3**). Aqueous acetonitrile, methanol or ethanol solution of **1** only elutes the fluorine-18 from the anion-exchange cartridge as a fluoride salt (supporting information, **Figure S1**). Compound **3** was purified by passing through the activated Oasis MCX Plus cartridge. The activated ester (**3**) was eluted from the cartridge by flushing with either acetonitrile for peptide labeling (**Figure 1**) or diethyl ether for protein labeling. In this work, our main focus is to develop a simple and straightforward labeling method to synthesize fluorine-18 labeled peptides and proteins containing a C-¹⁸F bond using fluorine-18 labeling prosthetic group **3**. We chose to radiolabel cyclic RGD peptide c(RGDfK), PSMA inhibitor (DCFpyL) and albumin (**Figure 1**) due to their current interests in nuclear imaging research.

3.1. [¹⁸F]c(RGDfK)

Integrin $\alpha_v\beta_3$ is a potential molecular marker for angiogenesis during imaging and therapy due to its significant up-regulation on activated endothelial cells.⁵⁰⁻⁵² The tripeptide Arg-Gly-Asp (RGD) has been extensively used as imaging tracer for integrin $\alpha_v\beta_3$ because of its high affinity and specificity. In a recent review Chen et al. compared the radiosynthesis, dosimetry, pharmacokinetics and clinical efficacy of clinically available RGD-based PET tracers.⁵³ [¹⁸F]Glacto-RGD, radiolabeled by an indirect approach using 4-nitrophenyl-2-[¹⁸F]fluoropropionate, was the first fluorine-18 labeled PET tracer of this class tested clinically.^{54, 55} There are other conventional C-¹⁸F bond containing RGD-based tracers.^{28, 56-60} These tracers are prepared in multi-step syntheses with several HPLC purifications, thus requiring a long synthesis time.

Reaction of **3** with c(RGDfK) in the presence of base (sodium carbonate) proceeded with over 80% radiochemical conversion to the product (**Figure S2b**) by analytical HPLC. The compound was purified by Sep-Pak to produce > 98% radio-chemically pure (**Figure 1a**) product with a SA of 1000-2200 Ci/mmol (end of synthesis, n = 12). The overall radiochemical yield was 32-43% (uncorrected, n = 6) in a 30 min synthesis time. A minor UV impurity peak at ~5 min was observed in analytical HPLC chromatogram (**Figure 1a**). In a typical radiosynthesis starting from 103 mCi of [¹⁸F]F⁻, the amount of impurity was <7 ug/mL in 39 mCi (3 mL) of product. The crude product was also purified by semi-prep HPLC to remove the impurity peak (**Figure 1b**). The identity of the product [¹⁸F]c(RGDfK) was confirmed by comparing its HPLC retention time with co-injected, authentic nonradioactive standard (**Figure 1c**). [¹⁸F]c(RGDfK) showed excellent serum stability up to 4 h post synthesis (**Figure S3**).

3.2. [¹⁸F]DCFPyL

Prostate cancer (PC) is the most common cancer in men in the United States. It is the second leading cause of death from cancer in men.⁶¹ Therefore over the decades, there has been an increasing interest in synthesis and evaluation of PET tracer for PC. [¹⁸F]FDG, the most widely used metabolic radiotracer for PET imaging of tumors, gave mixed results in PC.⁶² Although carbon-11 or fluorine-18 choline PET/CT showed promising results for the detection of bone metastases, this approach has limitations in terms of sensitivity and specificity. Therefore routine clinical use of carbon-11 or fluorine-18 choline PET/CT is debatable.⁶³ This unmet clinical need led to the development of another class of prostate-specific membrane antigen (PSMA) target specific tracers. Over expression of PSMA has been linked to PC and is an important target in patients with negative bone scan who are at high risk of metastatic disease. A recent review by Maurer et al. summarized the current use

of PET tracers such as [^{11}C]choline, [^{18}F]fluorocholine, gallium-68, and fluorine-18 labeled low-molecular weight PSMA inhibitors including DCFBC and DCFPyL in PC management.⁶⁴ The second generation PSMA inhibitor reported by Chen et al. showed high tumor: background ratio and favorable pharmacokinetics compared to other small molecules.^{47, 65, 66} Therefore development of reproducible radiochemical synthesis with high radiochemical yield for this tracer is of interest. Synthesis of [^{18}F]DCFPyL was firstly reported by an indirect method using **3**.⁴⁷ Recently synthesis of [^{18}F]DCFPyL has been reported by a direct fluorination method using a single precursor.^{49, 67} In this report we prepared [^{18}F]DCFPyL by an indirect labeling method. Compound **3** was prepared on a Sep-Pak following the method recently published by our group⁴⁸ and purified by passing through an Oasis MCX plus cartridge. The cartridge efficiently removed unreacted precursor (**1**) from the product **3**. Hence this method of preparation of **3** is comparable to initial anion exchange catch and release of fluorine-18 containing target water (**Table 1**). Final conjugation, de-protection and purification were done according to the literature method.⁴⁷ The overall radiochemical yield was 25-32% (uncorrected, n = 6) in a 45 min synthesis time. Both radiochemical and chemical purity were >98% determined by analytical HPLC (**Figure 2a**) with a SA of 1200-2600 Ci/mmol (end of synthesis, n = 15). The identity of the product was confirmed by comparing its HPLC retention time with co-injected, authentic non-radioactive standard (**Figure 2b**). The total labeling method is comparable with the direct method of radiolabeling (**Table 1**).

3.3. [^{18}F]albumin

Recently fluorine-18 labeling of albumin by conjugation with **3** has been reported by our group.⁴⁶ The labeled albumin showed excellent blood pool imaging property. We therefore set out to further simplify the radiolabeling using the current method. By conjugating **3** to target pendant amine groups, albumin can be radiolabeled in 30 min with moderate

radiochemical yield (**Table 2**). The radiochemical purity (>98%) and chemical purity (>98%) of the labeled albumin were determined by size exclusion chromatography (**Figure 3**).

In summary, the yield and synthesis time of this current method has been compared with the literature reported methods for two known PET tracers ($[^{18}\text{F}]\text{DCFPyL}$ and $[^{18}\text{F}]\text{Albumin}$) in **Table 2**. The RGD peptide (cRGDfK) has not been radiolabeled using **3**, therefore the yield and synthesis time of this tracer is compared with the known C- ^{18}F bonded RGD tracers (**Table 2**). The current method requires much less time with comparable or higher radiochemical yield.

4. Conclusions

We have successfully prepared $[^{18}\text{F}]\text{c(RGDfK)}$, $[^{18}\text{F}]\text{DCFPyL}$ and $[^{18}\text{F}]\text{albumin}$ in short synthesis time (30-50 min) with moderate to high radiochemical yield. For the first time RGD-peptide c(RGDfK) has been radiolabeled with **3**. This method is comparable with direct fluorine-18 labeling approaches. Due to the simplicity of the method, it could easily be automated for routine clinical production.

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References

- [1] Bruno BJ, Miller GD, and Lim CS. Basics and recent advances in peptide and protein drug delivery. *Ther Deliv* 2013;4:1443-1467.
- [2] Craik DJ, Fairlie DP, Liras S, and Price D. The future of peptide-based drugs. *Chem Biol Drug Des* 2013;81:136-147.
- [3] Laakkonen P and Vuorinen K. Homing peptides as targeted delivery vehicles. *Integr Biol* 2010;2:326-337.
- [4] Fosgerau K and Hoffmann T. Peptide therapeutics: current status and future directions. *Drug Discov Today* 2015;20:122-128.
- [5] Richter S and Wuest F. ¹⁸F-Labeled Peptides: The Future Is Bright. *Molecules* 2014;19:20536-20556.
- [6] Fani M and Maecke HR. Radiopharmaceutical development of radiolabelled peptides. *Eur J Nucl Med Mol Imaging* 2012;39 Suppl 1:S11-30.
- [7] E. Olberg D and K. Hjelstuen O. Labeling Strategies of Peptides with ¹⁸F for Positron Emission Tomography. *Curr Top Med Chem* 2010;10:1669-1679.
- [8] Li X-G, Haaparanta M, and Solin O. Oxime formation for fluorine-18 labeling of peptides and proteins for positron emission tomography (PET) imaging: A review. *J Fluorine Chem* 2012;143:49-56.
- [9] Ametamey SM, Honer M, and Schubiger PA. Molecular imaging with PET. *Chem Rev* 2008;108:1501-1516.
- [10] Willmann JK, van Bruggen N, Dinkelborg LM, and Gambhir SS. Molecular imaging in drug development. *Nat Rev Drug Discov* 2008;7:591-607.
- [11] Li ZB and Conti PS. Radiopharmaceutical chemistry for positron emission tomography. *Adv Drug Del Rev* 2010;62:1031-1051.

- [12] Le Bars D. Fluorine-18 and medical imaging: Radiopharmaceuticals for positron emission tomography. *J Fluorine Chem* 2006;127:1488-1493.
- [13] Papash AI and Alenitsky YG. Commercial cyclotrons. Part I: Commercial cyclotrons in the energy range 10–30 MeV for isotope production. *Phys Part Nuclei* 2008;39:597-631.
- [14] Levin CS and Hoffman EJ. Calculation of positron range and its effect on the fundamental limit of positron emission tomography system spatial resolution. *Phys Med Biol* 1999;44:781-799.
- [15] Jacobson O, Kiesewetter DO, and Chen X. Fluorine-18 Radiochemistry, Labeling Strategies and Synthetic Routes. *Bioconjugate Chem* 2015;26:1-18.
- [16] Preshlock S, Tredwell M, and Gouverneur V. ¹⁸F-Labeling of Arenes and Heteroarenes for Applications in Positron Emission Tomography. *Chem Rev* 2016;116:719-766.
- [17] Liang SH and Vasdev N. C(sp³)–¹⁸F Bond Formation by Transition-Metal-Based [¹⁸F]Fluorination. *Angew Chem Int Ed* 2014;53:11416-11418.
- [18] Neumann CN and Ritter T. Late-Stage Fluorination: Fancy Novelty or Useful Tool? *Angew Chem Int Ed* 2015;54:3216-3221.
- [19] Mu L, Höhne A, Schubiger PA, Ametamey SM, Graham K, Cyr JE, et al. Silicon-Based Building Blocks for One-Step ¹⁸F-Radiolabeling of Peptides for PET Imaging. *Angew Chem Int Ed* 2008;47:4922-4925.
- [20] Roehn U, Becaud J, Mu L, Srinivasan A, Stellfeld T, Fitzner A, et al. Nucleophilic ring-opening of activated aziridines: A one-step method for labeling biomolecules with fluorine-18. *J Fluorine Chem* 2009;130:902-912.
- [21] Becaud J, Mu L, Karramkam M, Schubiger PA, Ametamey SM, Graham K, et al. Direct One-Step ¹⁸F-Labeling of Peptides via Nucleophilic Aromatic Substitution. *Bioconjugate Chem* 2009;20:2254-2261.

- [22] Höhne A, Mu L, Honer M, Schubiger PA, Ametamey SM, Graham K, et al. Synthesis, ¹⁸F-Labeling, and in Vitro and in Vivo Studies of Bombesin Peptides Modified with Silicon-Based Building Blocks. *Bioconjugate Chem* 2008;19:1871-1879.
- [23] Wüst F, Hultsch C, Bergmann R, Johannsen B, and Henle T. Radiolabelling of isopeptide N ϵ -(γ -glutamyl)-l-lysine by conjugation with N-succinimidyl-4-¹⁸F]fluorobenzoate. *Appl Radiat Isot* 2003;59:43-48.
- [24] Li Z-B, Wu Z, Chen K, Ryu EK, and Chen X. ¹⁸F-Labeled BBN-RGD Heterodimer for Prostate Cancer Imaging. *J Nucl Med* 2008;49:453-461.
- [25] Vaidyanathan G and Zalutsky MR. Synthesis of N-succinimidyl 4-¹⁸F]fluorobenzoate, an agent for labeling proteins and peptides with ¹⁸F. *Nat Protocols* 2006;1:1655-1661.
- [26] Tang G, Zeng W, Yu M, and Kabalka G. Facile synthesis of N-succinimidyl 4-¹⁸F]fluorobenzoate ([¹⁸F]SFB) for protein labeling. *J Labelled Compd Radiopharm* 2008;51:68-71.
- [27] Zhu J-C, Wang F, Fang W, Hua Z-C, and Wang Z-z. ¹⁸F-annexin V apoptosis imaging for detection of myocardium ischemia and reperfusion injury in a rat model. *J Radioanal Nucl Chem* 2013;298:1733-1738.
- [28] Glaser M, Morrison M, Solbakken M, Arukwe J, Karlsen H, Wiggen U, et al. Radiosynthesis and Biodistribution of Cyclic RGD Peptides Conjugated with Novel ¹⁸F]Fluorinated Aldehyde-Containing Prosthetic Groups. *Bioconjugate Chem* 2008;19:951-957.
- [29] Cheng Z, De Jesus OP, Namavari M, De A, Levi J, Webster JM, et al. Small-Animal PET Imaging of Human Epidermal Growth Factor Receptor Type 2 Expression with Site-Specific ¹⁸F-Labeled Protein Scaffold Molecules. *J Nucl Med* 2008;49:804-813.

- [30] Berndt M, Pietzsch J, and Wuest F. Labeling of low-density lipoproteins using the ¹⁸F-labeled thiol-reactive reagent N-[6-(4-[¹⁸F]fluorobenzylidene)aminoxyhexyl]maleimide. *Nucl Med Biol* 2007;34:5-15.
- [31] Li X, Link JM, Stekhova S, Yagle KJ, Smith C, Krohn KA, et al. Site-Specific Labeling of Annexin V with F-18 for Apoptosis Imaging. *Bioconjugate Chem* 2008;19:1684-1688.
- [32] Poethko T, Schottelius M, Thumshirn G, Hersel U, Herz M, Henriksen G, et al. Two-Step Methodology for High-Yield Routine Radiohalogenation of Peptides: ¹⁸F-Labeled RGD and Octreotide Analogs. *J Nucl Med* 2004;45:892-902.
- [33] Morrison MS, Ricketts S-A, Barnett J, Cuthbertson A, Tessier J, and Wedge SR. Use of a Novel Arg-Gly-Asp Radioligand, ¹⁸F-AH111585, to Determine Changes in Tumor Vascularity After Antitumor Therapy. *J Nucl Med* 2009;50:116-122.
- [34] Gao H, Niu G, Yang M, Quan Q, Ma Y, Murage EN, et al. PET of Insulinoma using (¹⁸F)-FBEM-EM3106B, a New GLP-1 Analog. *Mol Pharm* 2011;8:1775-1782.
- [35] Kiesewetter DO, Jacobson O, Lang L, and Chen X. Automated radiochemical synthesis of [¹⁸F]FBEM: a thiol reactive synthon for radiofluorination of peptides and proteins. *Appl Radiat Isot* 2011;69:410-414.
- [36] Wang H, Gao H, Guo N, Niu G, Ma Y, Kiesewetter DO, et al. Site-Specific Labeling of scVEGF with Fluorine-18 for Positron Emission Tomography Imaging. *Theranostics* 2012;2:607-617.
- [37] Li Z-B, Wu Z, Chen K, Chin FT, and Chen X. Click Chemistry for ¹⁸F-Labeling of RGD Peptides and microPET Imaging of Tumor Integrin $\alpha v \beta 3$ Expression. *Bioconjugate Chem* 2007;18:1987-1994.
- [38] Glaser M and Årstad E. "Click Labeling" with 2-[¹⁸F]Fluoroethylazide for Positron Emission Tomography. *Bioconjugate Chem* 2007;18:989-993.

- [39] Laverman P, McBride WJ, Sharkey RM, Goldenberg DM, and Boerman OC. Al18F labeling of peptides and proteins. *J Labelled Compd Radiopharm* 2014;57:219-223.
- [40] Cleeren F, Lecina J, Billaud EMF, Ahamed M, Verbruggen A, and Bormans GM. New Chelators for Low Temperature Al18F-Labeling of Biomolecules. *Bioconjugate Chem* 2016;27:790-798.
- [41] Liu Z, Pourghiasian M, Radtke MA, Lau J, Pan J, Dias GM, et al. An Organotrifluoroborate for Broadly Applicable One-Step 18F-Labeling. *Angew Chem Int Ed* 2014;53:11876-11880.
- [42] Perrin DM. [18F]-Organotrifluoroborates as Radioprosthetic Groups for PET Imaging: From Design Principles to Preclinical Applications. *Acc Chem Res* 2016;49:1333-1343.
- [43] Wängler B, Quandt G, Iovkova L, Schirmacher E, Wängler C, Boening G, et al. Kit-Like 18F-Labeling of Proteins: Synthesis of 4-(Di-tert-butyl[18F]fluorosilyl)benzenethiol (Si[18F]FA-SH) Labeled Rat Serum Albumin for Blood Pool Imaging with PET. *Bioconjugate Chem* 2009;20:317-321.
- [44] Kostikov AP, Chin J, Orchowski K, Niedermoser S, Kovacevic MM, Aliaga A, et al. Oxalic acid supported Si-18F-radiofluorination: one-step radiosynthesis of N-succinimidyl 3-(di-tert-butyl[18F]fluorosilyl)benzoate ([18F]SiFB) for protein labeling. *Bioconjug Chem* 2012;23:106-114.
- [45] Olberg DE, Arukwe JM, Grace D, Hjelstuen OK, Solbakken M, Kindberg GM, et al. One Step Radiosynthesis of 6-[18F]Fluoronicotinic Acid 2,3,5,6-Tetrafluorophenyl Ester ([18F]F-Py-TFP): A New Prosthetic Group for Efficient Labeling of Biomolecules with Fluorine-18. *J Med Chem* 2010;53:1732-1740.
- [46] Basuli F, Li C, Xu B, Williams M, Wong K, Coble VL, et al. Synthesis of Fluorine-18 Radio-labeled Serum Albumins for PET Blood Pool Imaging. *Nucl Med Biol* 2015;42:219-225.

- [47] Chen Y, Pullambhatla M, Foss CA, Byun Y, Nimmagadda S, Srinivasan S, et al. 2-(3-{1-Carboxy-5-[(6-[(¹⁸F]fluoro-pyridine-3-carbonyl)-amino]-pentyl}-ureido)-pentanedioic acid, [(¹⁸F)DCFPyL, a PSMA-based PET Imaging Agent for Prostate Cancer. *Clin Cancer Res* 2011;17:7645-7653.
- [48] Basuli F, Zhang X, Jagoda EM, Choyke PL, and Swenson RE. Facile room temperature synthesis of fluorine-18 labeled fluoronicotinic acid-2,3,5,6-tetrafluorophenyl ester without azeotropic drying of fluorine-18. *Nucl Med Biol* 2016;43:770-772.
- [49] Bouvet V, Wuest M, Jans H-S, Janzen N, Genady AR, Valliant JF, et al. Automated synthesis of [¹⁸F]DCFPyL via direct radiofluorination and validation in preclinical prostate cancer models. *EJNMMI Research* 2016;6:40.
- [50] Niu G and Chen X. Why integrin as a primary target for imaging and therapy. *Theranostics* 2011;1:30-47.
- [51] Zitzmann S, Ehemann V, and Schwab M. Arginine-glycine-aspartic acid (RGD)-peptide binds to both tumor and tumor-endothelial cells in vivo. *Cancer Res* 2002;62:5139-5143.
- [52] Mondal G, Barui S, and Chaudhuri A. The relationship between the cyclic-RGDfK ligand and alphavbeta3 integrin receptor. *Biomaterials* 2013;34:6249-6260.
- [53] Chen H, Niu G, Wu H, and Chen X. Clinical Application of Radiolabeled RGD Peptides for PET Imaging of Integrin alphavbeta3. *Theranostics* 2016;6:78-92.
- [54] Haubner R, Kuhnast B, Mang C, Weber WA, Kessler H, Wester HJ, et al. [¹⁸F]Galacto-RGD: synthesis, radiolabeling, metabolic stability, and radiation dose estimates. *Bioconjug Chem* 2004;15:61-69.
- [55] Haubner R, Weber WA, Beer AJ, Vabuliene E, Reim D, Sarbia M, et al. Noninvasive Visualization of the Activated $\alpha\beta_3$ Integrin in Cancer Patients by Positron Emission Tomography and [¹⁸F]Galacto-RGD. *PLoS Med* 2005;2:e70.

- [56] Minamimoto R, Jamali M, Barkhodari A, Mosci C, Mittra E, Shen B, et al. Biodistribution of the 18F-FPPRGD2 PET radiopharmaceutical in cancer patients: an atlas of SUV measurements. *Eur J Nucl Med Mol Imag* 2015;42:1850-1858.
- [57] Kenny LM, Coombes RC, Oulie I, Contractor KB, Miller M, Spinks TJ, et al. Phase I Trial of the Positron-Emitting Arg-Gly-Asp (RGD) Peptide Radioligand 18F-AH111585 in Breast Cancer Patients. *J Nucl Med* 2008;49:879-886.
- [58] Liu S, Liu Z, Chen K, Yan Y, Watzlowik P, Wester HJ, et al. 18F-labeled galacto and PEGylated RGD dimers for PET imaging of alphavbeta3 integrin expression. *Mol Imaging Biol* 2010;12:530-538.
- [59] Thompson S, Onega M, Ashworth S, Fleming IN, Passchier J, and O'Hagan D. A two-step fluorinase enzyme mediated 18F labelling of an RGD peptide for positron emission tomography. *Chem Commun* 2015;51:13542-13545.
- [60] Mirfeizi L, Walsh J, Kolb H, Campbell-Verduyn L, Dierckx RA, Feringa BL, et al. Synthesis of [18F]RGD-K5 by catalyzed [3 + 2] cycloaddition for imaging integrin $\alpha\beta_3$ expression in vivo. *Nucl Med Biol* 2013;40:710-716.
- [61] Jemal A, Siegel R, Ward E, Hao Y, Xu J, and Thun MJ. Cancer statistics, 2009. *CA Cancer J Clin* 2009;59:225-249.
- [62] Jadvar H. Molecular imaging of prostate cancer with (18)F-fluorodeoxyglucose PET. *Nat Rev Urol* 2009;6:317-323.
- [63] Mapelli P, Incerti E, Ceci F, Castellucci P, Fanti S, and Picchio M. 11C- or 18F-Choline PET/CT for Imaging Evaluation of Biochemical Recurrence of Prostate Cancer. *J Nucl Med* 2016;57:43S-48S.
- [64] Maurer T, Eiber M, Schwaiger M, and Gschwend JE. Current use of PSMA-PET in prostate cancer management. *Nat Rev Urol* 2016;13:226-235.

[65] Szabo Z, Mena E, Rowe SP, Plyku D, Nidal R, Eisenberger MA, et al. Initial Evaluation of [(18)F]DCFPyL for Prostate-Specific Membrane Antigen (PSMA)-Targeted PET Imaging of Prostate Cancer. *Mol Imaging Biol* 2015;17:565-574.

[66] Dietlein M, Kobe C, Kuhnert G, Stockter S, Fischer T, Schomacker K, et al. Comparison of [(18)F]DCFPyL and [(68)Ga]Ga-PSMA-HBED-CC for PSMA-PET Imaging in Patients with Relapsed Prostate Cancer. *Mol Imaging Biol* 2015;17:575-584.

[67] Ravert HT, Holt DP, Chen Y, Mease RC, Fan H, Pomper MG, et al. An improved synthesis of the radiolabeled prostate-specific membrane antigen inhibitor, [18F]DCFPyL. *J Labelled Compd Radiopharm* 2016;59:439-450.

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Table 1: Key steps of direct labeling method and current indirect labeling method to prepare [¹⁸F]DCFpyL

Direct labeling method (Literature) ^{49, 67}	Indirect radiolabeling method (Current)
F-18 catch on the anion exchange resin	F-18 catch on the anion exchange resin
Wash with water	Wash with anhydrous acetonitrile
Elution with base	Drying under vacuum
Azeotropic drying	Elution with precursor (1) through Oasis MCX
Reaction with precursor	Reaction with second precursor (peptide)
De-protection, purification	De-protection, purification

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Table 2: Comparison of yield, time and SA for literature and current method

Compound	Yield (%)		SA (Ci/mmol)		Time (min)		References
	Literature	Current ^c	Literature	Current	Literature	Current	
[¹⁸ F]RGD ^a	10-35 ^b	39-43	2-2700	1000-2200	90-218	30	28, 54-60
[¹⁸ F]DCFPyL	5-53 ^b	25-32	340- 120000	1200-2600	55-128	45	47, 49, 66
[¹⁸ F]Albumin	18-35 ^c	26-35	n/a	n/a	90	30	46

^aOnly C-¹⁸F bonded tracers are included in this table; ^bdecay corrected; ^cdecay uncorrected

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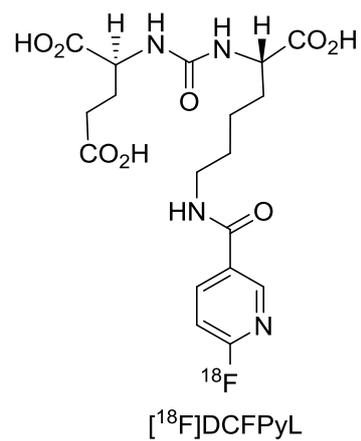
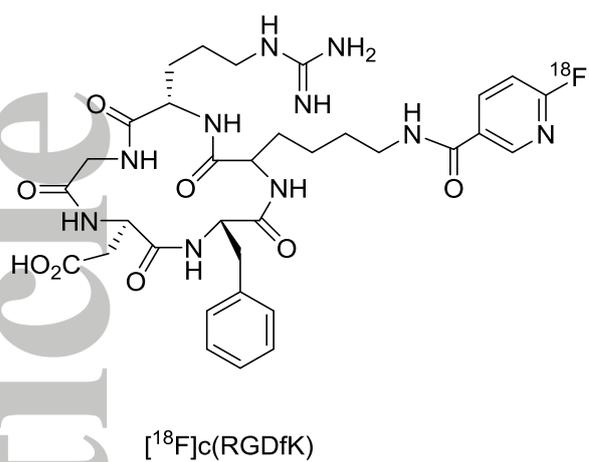
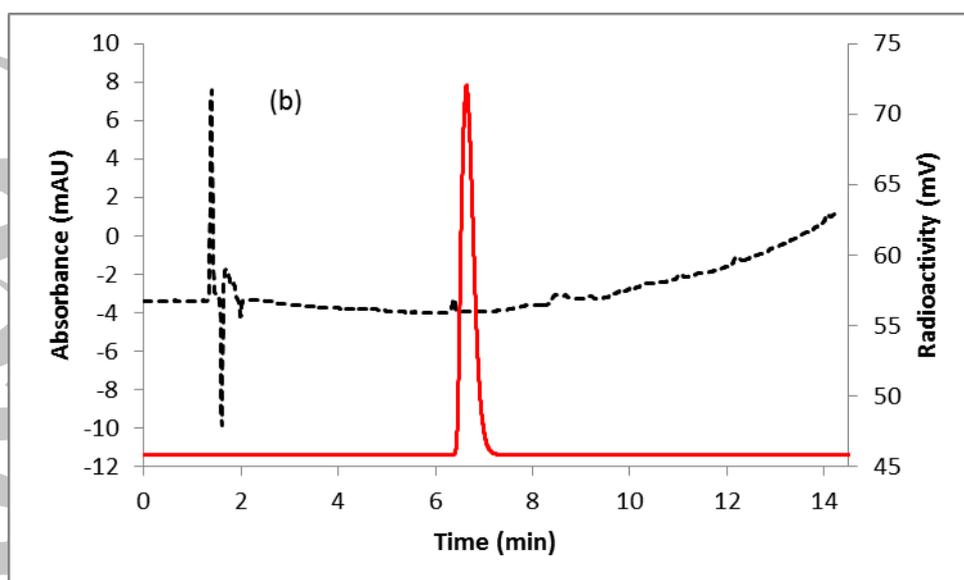
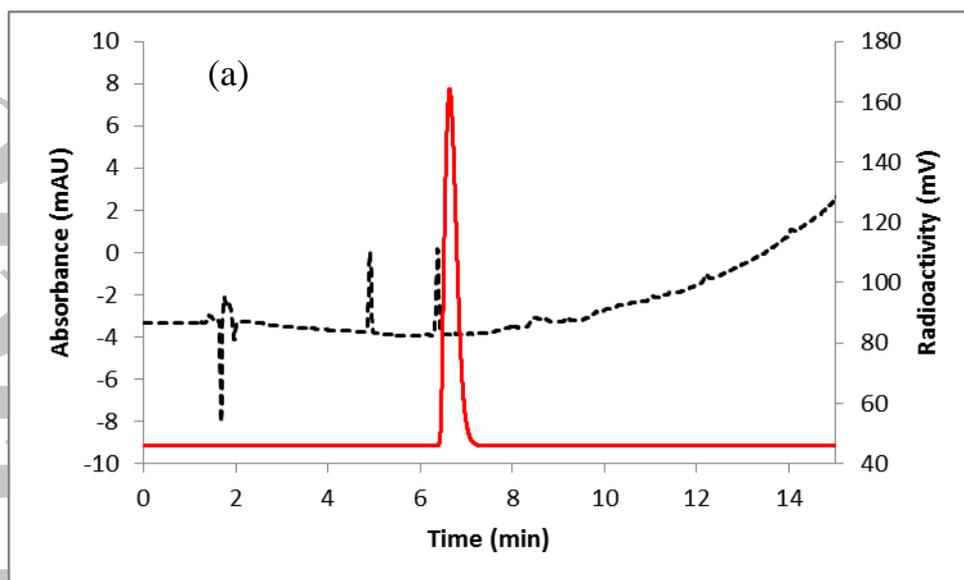


Figure 1: Structures of fluorine-18 labeled cyclic RGD and $[^{18}\text{F}]\text{DCFPyL}$



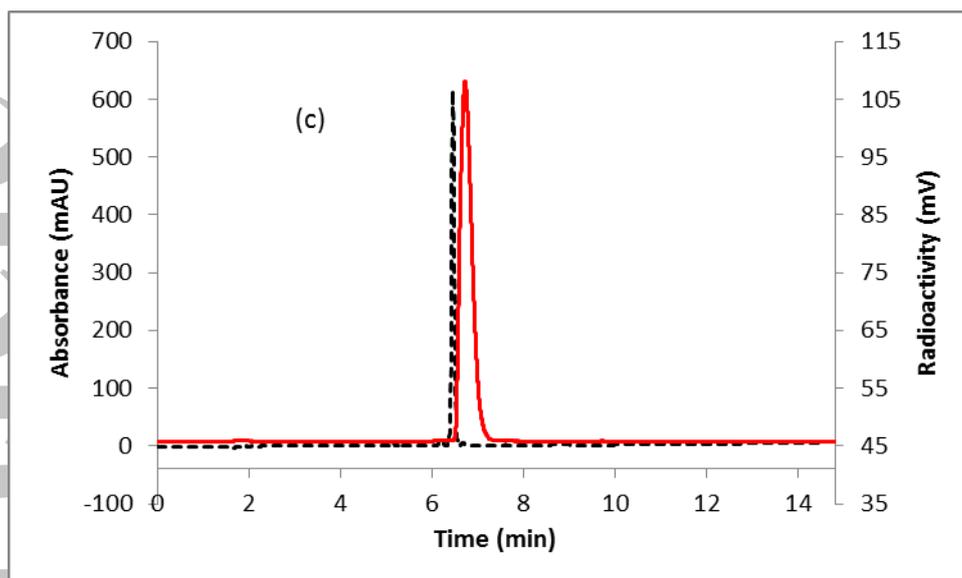


Figure 2. HPLC analysis of a) Sep-Pak purified [^{18}F]c(RGDfK); b) HPLC purified [^{18}F]c(RGDfK); c) [^{18}F]c(RGDfK), co-injected with the non-radioactive standard. HPLC condition: Agilent Eclipse plus C18 column (4.6×150 mm, $3.5 \mu\text{m}$), mobile phase: 10 - 50% A in 8 min, 50 - 90 % A in 15 min. A = acetonitrile (0.1% TFA), B = water (0.1% TFA), with a flow rate of 1.0 mL/min. Solid line, in-line radiodetector; dotted line, UV detector at 254 nm.

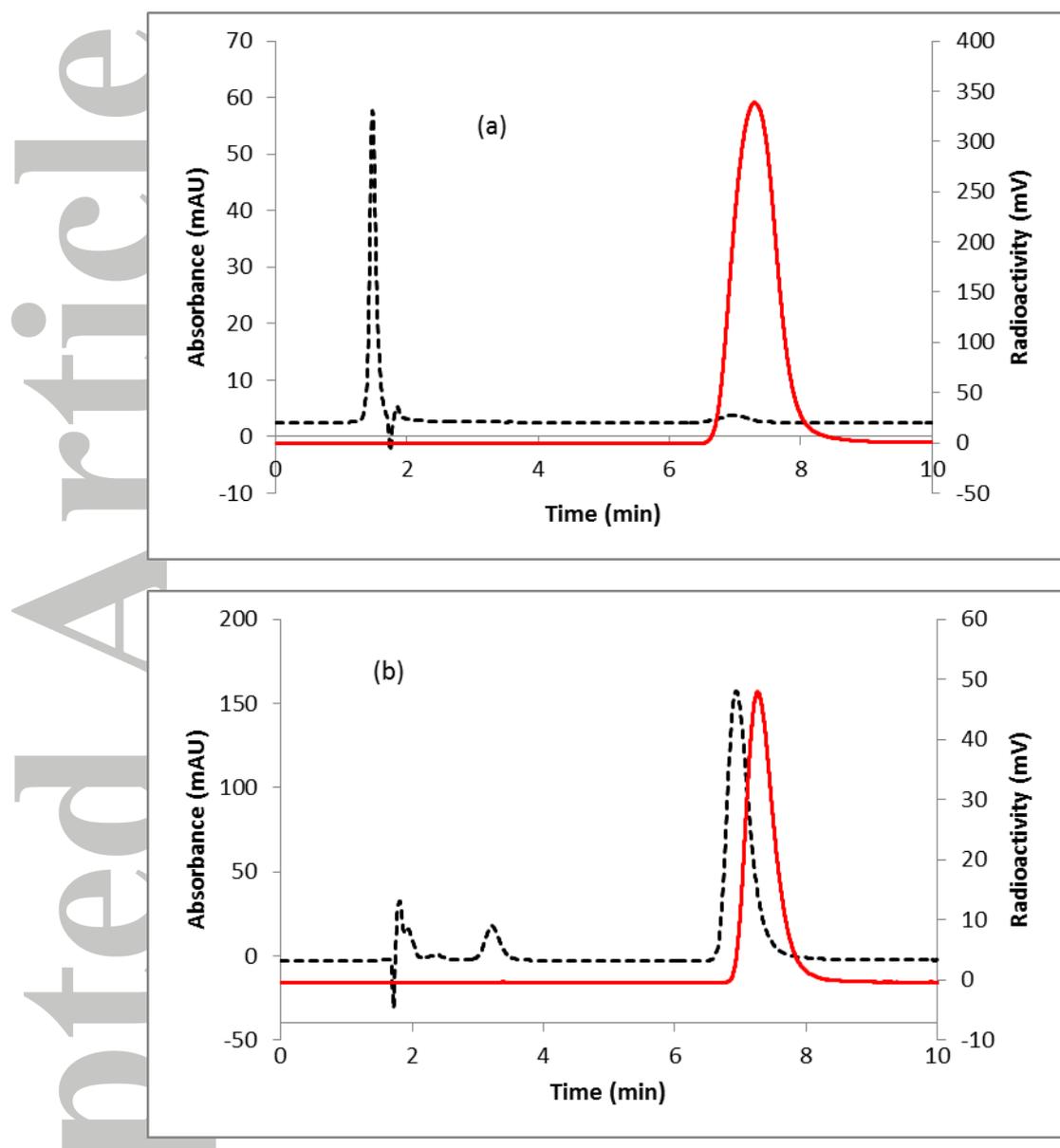


Figure 3: HPLC analysis of a) [^{18}F]DCFPyL; b) [^{18}F]DCFPyL, co-injected with the non-radioactive standard. HPLC condition: Agilent Eclipse plus C18 column (4.6×150 mm, $3.5 \mu\text{m}$), mobile phase: 5% acetonitrile in 0.1 M ammonium formate (pH 3.5), with a flow rate of 1.0 mL/min. Solid line, in-line radiodetector; dotted line, UV detector at 254 nm.

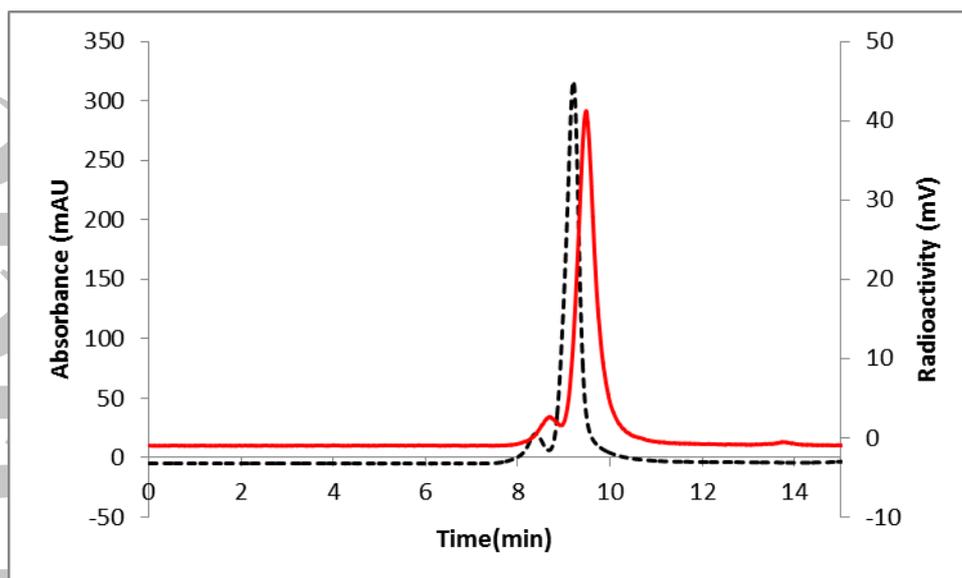
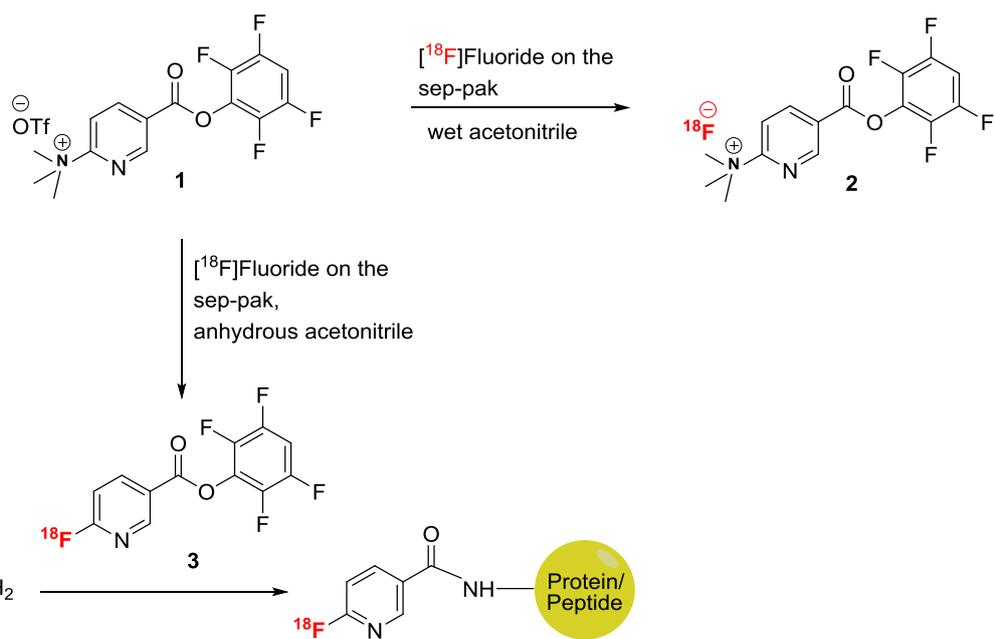


Figure 4. HPLC analysis of [^{18}F]RSA. HPLC condition: Agilent GF250 column (9.4×250 mm, $3.5 \mu\text{m}$), mobile phase: PBX 1X, pH 7.4, with a flow rate of 1.0 mL/min. Solid line, in-line radiodetector; dotted line, UV detector at 254 nm.



Scheme 1: Fluorine-18 labeling of peptide and protein through nicotinic ester approach