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Metallostar Assemblies Based on Dithiocarbamates for Use as MRI Contrast Agents

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multimetallic compound compared to clinically approved Dotarem. The gadolinium complexes based on the DOTAGA chelate also performed well at 63.87 MHz, with a relaxivity value of 9.5 $mM^{-1} s^{-1}$ per gadolinium unit being observed for the trigadolinium d-f mixed-metal complex with a ruthenium(III) core. The versatility of dithiocarbamate coordination chemistry thus provides access to a wide range of d-f hybrids with potential for use as high-performance MRI contrast agents.

INTRODUCTION

Magnetic resonance imaging (MRI) is a noninvasive medical imaging technique that provides detailed anatomical images with the highest spatial resolution of all of the nonionizing and noninvasive imaging modalities.¹ Different tissues are characterized by MRI-specific relaxation parameters (longitudinal relaxation time, T_1 ; transverse relaxation time, T_2) and differing proton densities. The intrinsic soft tissue contrast observed enables detailed anatomical images to be acquired using MRI. However, because of the poor contrast often observed between different tissue types (such as healthy and diseased), contrast agents² are often employed in order to alter and accelerate the relaxation of water protons in healthy and diseased tissue, thereby improving the image detail and contrast. This is achieved by the presence of an exogenous paramagnetic species (e.g., trivalent gadolinium), which affects both T_1 recovery and T_2 decay due to its strong local magnetic moment. Higher relaxivity values (in $mM^{-1} s^{-1}$) correlate with better contrast enhancement.² The contrast agents currently used in a clinical setting are almost all based on paramagnetic $(4f^7)$ trivalent gadolinium ions. Examples of these monogadolinium compounds are Dotarem and Primovist (Figure 1), which are both extracellular probes with a nonspecific biodistribution. Their design features an octadentate chelate, which prevents loss of the toxic gadolinium ion, while still



Figure 1. Two commonly used, clinically approved gadolinium contrast agents, which both have a hydration number (q) of 1.

allowing a single coordination site for a water molecule (q = 1). The release of gadolinium cations into the body leads to the formation of salts with endogenous anions, such as phosphate or carbonate. Upon entering tissues, these species stimulate an inflammatory response, which results in scarring of the tissue. This nephrogenic systemic fibrosis (NSF) can lead to severe

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Scheme 1. Synthesis of Gd-DO3A-DTC and Gd-DOTAGA-DTC



renal impairment in patients and has led to restrictions in the use of contrast agents with acyclic chelates.²

Interactions between the paramagnet and coordinated water as well as the surrounding water molecules lead to an improvement in the relaxation rates of these water protons, enhancing the image contrast and signal-to-noise performance.² Due to the inherent low sensitivity of MRI, very high concentrations (typically 0.1 mmol/kg patient weight) of contrast agent are required, and so efforts have been made to increase the relaxivity performance of each Gd^{3+} ion. This could also reduce the amount of contrast agent that needs to be administered.

The attachment of Gd^{3+} chelates to larger assemblies such as polymers and nanoparticles has been successfully used to dramatically increase the relaxivity per Gd^{3+} ion. This can be explained in terms of the rotational correlation time, which increases when the assembly rotates slowly, leading to enhanced relaxation rates. In addition, the degree to which the relaxation of water protons changes is due to the multimeric effect, which stems from the increased, localized contrast agent concentration.²

Pioneering work by Tóth,³ Helm,⁴ Parac-Vogt,⁵ and Desreux⁶ has focused on the synthesis of molecular multimetallic gadolinium compounds, with either an organic or metal-based core. These assemblies have demonstrated impressive relaxivity in many cases. However, one pitfall common to all polygadolinium approaches is the difficulty in eliminating internal rotation of the individual gadolinium chelates, which undermines the potential for extremely high relaxivity enhancement.

For over a decade, we have focused on the development of a wide range of routes to multimetallic compounds,⁷ with the use of dithiocarbamates ($R_2NCS_2^{-}$) being a recurring feature.⁸ This has been driven partly by the ease of formation of dithiocarbamates from (usually secondary) amines in the presence of base and carbon disulfide.⁹ The fact that dithiocarbamate compounds are known for their ability to coordinate to all of the transition metals in all common

oxidation states (both high and low) indicates the vast potential that dithiocarbamates with additional functionality could promise. 9,10

In 2014, we reported for the first time how dithiocarbamates could be used to incorporate gadolinium units into multimetallic assemblies or onto the surface of gold nanoparticles.¹¹ These materials showed promising relaxivity behavior; however, the hexacoordinate coordination of the Gd³⁺ ion (q = 3) raised concerns over the potential loss of this toxic ion under physiological conditions. This led to new designs based on an octadentate coordination environment, such as that found in Dotarem (Figure 1).¹² The present work describes how these improved and highly stable gadolinium chelates can be employed in the generation of multimetallic compounds based on both d- and f-block metals, along with an assessment of their performance in MRI contrast enhancement.

RESULTS AND DISCUSSION

Two polydentate chelates designed for the immobilization of gadolinium on the surface of gold nanoparticles,^{13,14} **Gd-DO3A-DTC** and **Gd-DOTAGA-DTC**, were used to provide gadolinium chelates with either an overall neutral or anionic environment for the gadolinium ion. It was expected that charge on this part of the molecule would have a significant impact on the interaction of water with the paramagnetic ion and hence modify the relaxivity observed.

The Gd-DO3A-NH₂ and Gd-DOTAGA-NH₂ precursors were prepared by a straightforward multistep route starting from commercially available cyclen, as reported previously (Scheme 1).^{13,14} The corresponding dithiocarbamates, Gd-DO3A-DTC and Gd-DOTAGA-DTC, were prepared and isolated shortly before use as the ammonium precursors are more suitable for long-term storage than these reactive species.

Synthesis of Multimetallic d–f Hybrids. The benefit of using reliable linkers, such as pyridyl donors, to form multimetallic d–f hybrids for use in imaging applications has been demonstrated by Faulkner and co-workers.¹⁵ While less frequently employed than nitrogen-based donors, the depend-



Scheme 2. Synthesis of Mono-, Bi-, and Trigadolinium Compounds Based on Ln-DO3A-DTC (Ln = La, Gd)

able reactivity and versatility of dithiocarbamate ligands⁹ make them ideally suited to the construction of multimetallic assemblies.⁸ Accordingly, the dithiocarbamate **Gd-DO3A-DTC** was used to prepare a series of multimeric molecular gadolinium compounds through the addition of suitable transition-metal precursors (Scheme 2). In order to enable characterization by NMR spectroscopy, the lanthanum analogues of the compounds were also prepared. The synthesis of **La-DO3A-NH₂** and **La-DO3A-DTC** is described in the Supporting Information.

Dithiocarbamate complexes of gold are well-known,⁹ particularly of gold(I), in which this 1,1'-dithio ligand typically bonds in an anisobidentate manner. The versatile starting material, [AuCl(PPh₃)], was chosen for reaction with the lanthanum complex La-DO3A-DTC (Scheme 2). After stirring at room temperature in the dark for 1 h, the precipitated KCl salt was removed by filtration and the product was isolated and analyzed by ³¹P{¹H} NMR spectroscopy. This revealed a shift of the PPh₃ resonance from 33.2 ppm in the starting material to 37.3 ppm in the product. The ¹³C{¹H} NMR spectrum

displayed a resonance at 213.3 ppm for the CS₂ carbon nucleus,⁹ while the ¹H NMR spectrum showed broadened peaks attributed to the DO3A-piperazine chelate in addition to aromatic resonances for the phosphine ligand. The IR spectrum revealed an absorption at 1599 cm^{-1} (C=O stretch) as well as a feature at 1430 cm⁻¹ attributed to the C–N stretch and a band at 999 cm⁻¹ assigned as the ν (C–S) absorption of the dithiocarbamate ligand.⁹ Along with a molecular ion for [M $- H_2O^{\dagger}$ at m/z 1142 in the mass spectrum (matrix-assisted laser desorption/ionization, positive mode), these data confirmed the formulation of the product as La-DO3A-DTC-AuPPh₃. The gadolinium analogue was then synthesized from Gd-DO3A-DTC using the same protocol to yield an offwhite powder, Gd-DO3A-DTC-AuPPh₃. IR analysis supported the preparation of this analogous product with typical bands for the PPh₃ ligand along with absorptions at 1679 cm⁻¹ $[\nu C=N]$, 1603 cm⁻¹ $[\nu (C=O)]$, 1396 cm⁻¹ $[\nu (C-N)]$, and 994 cm⁻¹ [ν (C–S)]. These features are consistent with the anisobidentate binding mode for the dithiocarbamate ligand, which is typical for gold(I) complexes."

Scheme 3. Synthesis of Mono-, Di-, and Trigadolinium Compounds Based on Gd-DOTAGA-DTC^a



^{*a*}All countercations are potassium ions.

Compound La-DO3A-DTC was added to nickel nitrate hydrate, causing a rapid change in color of the solution from pale-blue to bright yellow. This solution was then stirred for 1 h at room temperature (Scheme 2) to give Ni(La-DO3A-DTC)₂ as a pale-green powder. The solid-state IR spectrum of Ni(La-DO3A-DTC)₂ indicated the presence of the DO3Adithiocarbamate ligand with characteristic features at 1671 cm⁻¹ [ν (C=N)], 1599 cm⁻¹ [ν (C=O)], 1403 cm⁻¹ [ν (C-N)], and 1003 cm⁻¹ [ν (C=S)]. The corresponding reaction between Gd-DO3A-DTC and Ni(NO₃)₂·6H₂O followed the same pathway to afford a pale-green powder, Ni(Gd-DO3A-DTC)₂. The IR spectrum of this compound confirmed the presence of the dithiocarbamate ligand with absorptions at values similar to those found for Ni(La-DO3A-DTC)₂. Mass spectrometry was used to further characterize Ni(La-DO3A-DTC)₂ and Ni(Gd-DO3A-DTC)₂.

Following the successful preparation of bimetallic monogadolinium and trimetallic digadolinium complexes, attention then turned to the synthesis of tetrametallic trilanthanide complexes (Scheme 2). Compound La-DO3A-DTC was added to CoCl₂·6H₂O, leading to a rapid change in the solution color from pale pink to dark green. After stirring for 1 h at room temperature and filtration through Celite, all solvent was removed to afford a dark-green solid, formulated as Co(La-DO3A-DTC)₃. The IR spectrum of this compound confirmed the presence of the DO3A-dithiocarbamate ligand with absorptions similar to those found for the other complexes. The gadolinium analogue Co(Gd-DO3A-DTC)₃

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was prepared in the same manner. In common with many literature examples,⁹ the reaction of a divalent cobalt precursor leads to the isolation of a trivalent diamagnetic tris-(dithiocarbamate) product. **Ru(La-DO3A-DTC)**₃ and **Ru-(Gd-DO3A-DTC)**₃ were synthesized following a procedure similar to that used for their cobalt analogues using RuCl₃· $3H_2O$. Formation of these RuLn₃ complexes was accompanied by a color change from black to dark green. IR spectroscopy and mass spectrometry confirmed the successful synthesis of the desired tetrametallic trigadolinium complexes. An investigation of the magnetic properties through both the Evans NMR method and measurement using a magnetic susceptibility balance led to $\mu_{\rm eff}$ values between 1.92 and 2.10 $\mu_{\rm B}$, strongly suggesting only one unpaired electron and a low-spin $(t_{2g})^{\rm S}(e_g)^0$ configuration for the trivalent ruthenium center.

In a similar manner, the dianionic **Gd-DOTAGA-DTC** complex was added to various transition-metal salts to form anionic multimeric gadolinium compounds (Scheme 3). As expected, the spectroscopic data for these compounds were found to be similar to those described above. Characterization details for these compounds can be found in the Supporting Information.

Macrocyclic chelates with carboxylate arms, such as **Gd-DOTAGA-DTC**, often have faster water exchange rates (contributing to higher relaxivity) than macrocyclic chelates with amide arms (like **Gd-DO3A-DTC**).¹² The coordination environment of **Gd-DOTAGA-DTC** mimics that found in the leading, clinically used contrast agent, Dotarem, which is known for its high stability (log K_{GdL} of 25.3).¹ This fact provides reassurance (particularly in the context of NSF) that the toxic gadolinium(III) ion will not be released under biological conditions.

The synthesis described above resulted in a series of analogous multimetallic complexes bearing the **Gd-DO3A-DTC** and **Gd-DOTAGA-DTC** units. This allowed their relaxivity to be evaluated and their potential as MRI contrast agents to be determined.

Relaxivity Measurements. Using a 0.01-10 MHz fast field-cycling NMR relaxometer (0.25 T SMARtracer, Stelar), the relaxivity performance of the polygadolinium compounds was established and compared to Gd-DO3A-NH₂ and Gd-DOTAGA-NH₂ (chosen in preference to the corresponding dithiocarbamates because of their greater stability) as well as the clinically approved standard, Dotarem. The data point at 63.87 MHz was acquired using a 1.5 T clinical MRI scanner, which operates only at room temperature (25 $^{\circ}$ C). Fluorescence lifetime measurements reported in previous studies 13,14 for the europium analogues Eu-DO3A-NH₂ and Eu-DOTAGA-NH₂ confirmed the expected hydration value of q = 1 for the octadentate chelates. Both **Gd-DO3A-NH**₂ and Gd-DOTAGA-NH₂ were found to possess a higher relaxivity than Dotarem, likely because of the slightly higher molecular mass, which is known to enhance the relaxivity.² The nuclear magnetic relaxation dispersion (NMRD) profiles of these chelates are shown in Figure 2. The presence of an amide arm, such as that found in Gd-DO3A-NH₂, has been reported to have a potentially negative impact on the relaxivity;¹⁶ however, this does not seem to be a significant factor in the performance of the chelate design reported here.

The relaxivity of the various multimetallic assemblies was also measured at 25 and 37 °C in water, and the NMRD profiles were determined. It is known that an increase in mass of the gadolinium-containing unit results in an enhancement of



Figure 2. NMRD profiles of Dotarem, Gd-DO3A-NH₂, and Gd-DOTAGA-NH₂ at 25 and 37 °C.

the relaxivity^{17,18} due to slow tumbling and a reduction in the rotational freedom experienced by each individual gadolinium unit. However, it was anticipated that a particularly pronounced enhancement would be observed for the materials prepared in this study. In addition to the increased mass, the rigidity of the piperazine rings and the multiple-bond character of the dithiocarbamate and amide bonds also limit rotational freedom and thus enhance relaxivity. Previous designs based on an organic or a metal core often allow rotation about the axis of the tether, and this can have a detrimental effect on the relaxivity.³⁻⁶

Using the Evans method to determine the gadolinium concentration,¹⁹ the relaxivity of **Gd-DO3A-DTC-AuPPh**₃ at 0.01 MHz was found to be 11.3 and 10.3 mM⁻¹ s⁻¹ at 25 and 37 °C, respectively (Figure 3). As the temperature increases,



Figure 3. NMRD profiles of Gd-DO3A-DTC-AuPPh₃ at 25 and 37 $^\circ\text{C}.$

the rate of internal rotation increases, and this results in a reduction in the relaxivity of the complex. Although the relaxivity maintained a constant value at Larmor frequencies between 0.01 and 1 MHz, at Larmor frequencies beyond 1 MHz, the relaxivity of the complex decreased with increasing frequency, a typical effect seen in small-molecule contrast agents.²⁰ The relaxivity of **Gd-DO3A-DTC-AuPPh**₃ at 10 MHz was found to be 6.4 and 5.6 mM⁻¹ s⁻¹ at 25 and 37 °C, respectively.

This represents a modest improvement in the r_1 value of **Gd-DO3A-NH**₂ at 10 MHz (5.2 mM⁻¹ s⁻¹ at 25 °C and 4.5 mM⁻¹ s⁻¹ at 37 °C), and this enhancement can be attributed to the additional mass provided by the AuPPh₃ unit slowing the rotational correlation time. The trimetallic (digadolinium) complex, **Ni(Gd-DO3A-DTC)**₂, was found to display r_1 values (at 10 MHz) per Gd³⁺ ion of 6.1 and 5.5 mM⁻¹ s⁻¹ at 25 and

37 °C, respectively (Figure 4). Again, this represents an increase over the relaxivity of Gd-DO3A-NH, and is a value



Figure 4. Relaxivity values per Gd $^{3+}$ ion for Ni(Gd-DO3A-DTC)2 at 25 and 37 $^{\circ}C.$

similar to that measured for Gd-DO3A-DTC-AuPPh₃. This is not surprising given their similar masses. The overall relaxivity (at 10 MHz) of Ni(Gd-DO3A-DTC)₂ was found to be 12.2 and 10.9 mM⁻¹ s⁻¹ at 25 and 37 °C, demonstrating the benefits of an increased gadolinium payload.

NMRD studies performed on $Co(Gd-DO3A-DTC)_3$ revealed this trigadolinium compound to display relaxivity values per gadolinium ion (at 10 MHz) of 10.5 mM⁻¹ s⁻¹ (25 °C) and 9.7 mM⁻¹ s⁻¹ (37 °C) (Figure 5). This is almost double the value obtained for monometallic Gd-DO3A-NH₂ and also a significant improvement with respect to the digadolinium complex Ni(Gd-DO3A-DTC)₂.



Figure 5. Relaxivity values per Gd³⁺ ion for Co(Gd-DO3A-DTC)₃ at 25 and 37 $^{\circ}$ C.

The rigidity of the dithiocarbamate—piperazine linker, due to multiple-bond character in both the amide and dithiocarbamate units, decreases the internal rotation in the complexes, thus increasing the relaxivity. However, in the mono- and digadolinium complexes, this boost in relaxivity is limited by the rapid overall rotation of the complexes. It appears that the mass of Co(Gd-DO3A-DTC)₃ causes the overall rotation to decrease sufficiently to allow the gains in relaxivity from the reduced internal motion to be observed. This results in a reduced temperature dependence; the difference between the r_1 values recorded at 25 and 37 °C is significantly smaller than that found in the complexes of lower mass. As the molecular mass increases, this reduction will continue until the increase in temperature leads to a situation in which the rotational correlation time is no longer a limiting factor. Figure 5 also shows an increase in relaxivity as the frequency approaches 10 MHz, which is a trend typical of macromolecular structures.^{20,21} With three Gd^{3+} ions in the same molecular assembly, the high payload of gadolinium ions per complex gives an overall relaxivity for Co(Gd-DO3A-DTC)₃ of 31.4 mM⁻¹ s⁻¹ (25 °C) and 29.0 mM⁻¹ s⁻¹ (37 °C). This is almost 6 times the r_1 value of Gd-DO3A-NH₂ and is comparable to the trigadolinium species synthesized by Desreux and coworkers.⁶

A second trigadolinium complex based on Gd-DO3A-DTC was prepared using a ruthenium core, $Ru(Gd-DO3A-DTC)_3$. It performed similarly to $Co(Gd-DO3A-DTC)_3$, with relaxivity values at 10 MHz of 9.2 mM⁻¹ s⁻¹ and 8.5 mM⁻¹ s⁻¹ at 25 and 37 °C, respectively (Figure 6). These values



Figure 6. Relaxivity values per Gd³⁺ ion for $Ru(Gd-DO3A-DTC)_3$ at 25 and 37 °C.

increase to 27.6 and 25.6 mM⁻¹ s⁻¹ when considering the overall relaxivity of the trigadolinium complex. The same trend in relaxivity, with an "upswing" between 7 and 10 MHz, was observed with $Ru(Gd-DO3A-DTC)_3$, just as it had been with $Co(Gd-DO3A-DTC)_3$.

A comparison of the complexes in this study based on **Gd-DO3A-DTC** at 25 °C is provided in Figure 7. The DOTAGAbased complexes displayed trends in relaxivity similar to those of their DO3A-based analogues, with the gold and nickel complexes achieving relaxivity values of 6.9 and 7.2 mM⁻¹ s⁻¹, respectively, and the cobalt and ruthenium complexes performing better with relaxivity values of 10.8 and 9.9 mM⁻¹ s⁻¹, respectively (10 MHz, 25 °C). The overall



Figure 7. Summary of the relaxivity per Gd^{3+} ion of Dotarem, Gd-DO3A-NH₂, Gd-DO3A-DTC-AuPPh₃, Ni(Gd-DO3A-DTC)₃, Co-(Gd-DO3A-DTC)₃, and Ru(Gd-DO3A-DTC)₃ at 25 °C.



Figure 8. Overall relaxivity values of the DO3A-based (left) and DOTAGA-based (right) metallostars at 25 °C. The central metal ion is distinguished by color: cobalt, light blue; ruthenium, green; nickel, yellow; gold, gray. Also displayed are Gd-DO3A-NH₂ (orange circles), Gd-DOTAGA-NH₂ (orange squares), and Dotarem (dark blue). Note that the traces for Gd-DO3A-NH₂ and Dotarem are superimposed.

relaxivities of the DOTAGA-based complexes are displayed in Figure 8 to emphasize the benefit of incorporating multiple gadolinium chelates into a single assembly. The individual NMRD profiles of the DOTAGA-based complexes at 25 and 37 °C can be found in the Supporting Information, where the same characteristic upswing in the relaxivity that was seen with $Co(Gd-DO3A-DTC)_3$ and $Ru(Gd-DO3A-DTC)_3$ is replicated for $Co(Gd-DOTAGA-DTC)_3$ and $Ru(Gd-DOTAGA-DTC)_3$.

In order to provide a convenient numerical comparison, the r_1 values (10 MHz) at 25 and 37 °C for each complex are shown in Table 1, both per Gd³⁺ ion and overall. Upon an

Table 1. Summary of the Relaxivity Values $(mM^{-1} s^{-1})$ for the Multimetallic Complexes Measured at 25 and 37 °C (10 MHz)

	25 °C		37 °C	
	r1 per Gd	r ₁ overall	r1 per Gd	r ₁ overall
Dotarem	5.4	5.4	4.0	4.0
Gd-DO3A-NH ₂	5.2	5.2	4.5	4.5
Gd-DO3A-DTC-AuPPh ₃	6.4	6.4	5.6	5.6
Ni(Gd-DO3A-DTC) ₂	6.1	12.2	5.5	10.9
Co(Gd-DO3A-DTC) ₃	10.5	31.4	9.7	29.0
Ru(Gd-DO3A-DTC) ₃	9.2	27.6	8.5	25.6
Gd-DOTAGA-NH ₂	6.4	6.4	5.0	5.0
$Gd\text{-}DOTAGA\text{-}DTC\text{-}AuPPh_3$	6.9	6.9	5.9	5.9
Ni(Gd-DOTAGA-DTC) ₂	7.2	14.4	5.9	11.9
Co(Gd-DOTAGA-DTC) ₃	10.8	32.4	9.8	29.5
$Ru(Gd-DOTAGA-DTC)_3$	9.9	29.7	9.6	28.7

increase in the temperature of the Dotarem solution, the relaxivity decreased from 5.4 to 4.0 mM^{-1} s⁻¹, which represented a 26% decrease. The relaxivity of **Ru(Gd-DOTAGA-DTC)**₃, on the other hand, decreased by only 3%, from 9.9 to 9.6 mM^{-1} s⁻¹. In fact, all of the multimetallic complexes were far less affected by the temperature change than Dotarem. This can be traced to their larger size, compared to Dotarem, and the internal rigidity present in their structures. As the temperature was increased, the rotational motion of the smaller Dotarem chelates increased more significantly than was the case for the multimetallic complexes. This led to the relaxivity values for the multimetallic complexes being less

affected by the temperature change than the relaxivity of Dotarem.

The T_1 -weighted MRI images of the compounds (Figure 9) were measured using a clinical scanner at 63.87 MHz (1.5 T)



Figure 9. T_1 -weighted MRI images (shown in "16 colors", *ImageJ*) of the multimetallic complexes (DO3A-based, above, and DOTAGA-based, below) and Dotarem at 25 °C and 63.87 MHz. [Gd³⁺] = 0.2 mM in all cases.

and compared to Dotarem. This revealed that, for the same concentration of Gd^{3+} ions (0.2 mM), significantly greater contrast can be achieved per Gd^{3+} unit in **Gd-DO3A-DTC**-AuPPh₃ ($r_1 = 5.0 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$), Ni(Gd-DO3A-DTC)₂ ($r_1 = 5.7 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$), Co(Gd-DO3A-DTC)₃ ($r_1 = 7.2 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$), and Ru(Gd-DO3A-DTC)₃ ($r_1 = 8.2 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$) compared to Dotarem ($r_1 = 4.4 \pm 0.2 \text{ mM}^{-1} \text{ s}^{-1}$) at clinical field strength.

The multimetallic complexes based on the DOTAGA chelate consistently showed greater relaxivity values than their equivalent DO3A complexes, demonstrating the importance of the gadolinium chelate design. This is despite the short alkyl chain that features in the DOTAGA linker, which could facilitate undesirable internal flexibility. It appears that, in this case at least, the additional flexibility generated by this unsaturated linkage is not sufficiently significant to affect the relaxivity noticeably. It is also likely that other factors associated with the DOTAGA chelate, such as an increased water exchange rate at the metal center, provide a greater contribution to the observed relaxivity. The relaxivity values measured for the DOTAGA compounds at a clinical magnetic



Figure 10. Uptake of Gd-DOTAGA-DTC-AuPPh₃ (A), Ni(Gd-DOTAGA-DTC)₂ (B), Co(Gd-DOTAGA-DTC)₃ (C), Ru(Gd-DOTAGA-DTC)₃ (D), and Dotarem by HeLa cells following 24 h of incubation.

field strength were particularly impressive, with greater contrast being achieved by **Gd-DOTAGA-DTC-AuPPh**₃ ($r_1 = 5.9 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$), **Ni(Gd-DOTAGA-DTC)**₂ ($r_1 = 6.2 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$), **Co(Gd-DOTAGA-DTC)**₃ ($r_1 = 9.0 \pm 0.2 \text{ mM}^{-1} \text{ s}^{-1}$), and **Ru(Gd-DOTAGA-DTC)**₃ ($r_1 = 9.5 \pm 0.1 \text{ mM}^{-1} \text{ s}^{-1}$) compared to Dotarem ($r_1 = 4.4 \pm 0.2 \text{ mM}^{-1} \text{ s}^{-1}$). Most noteworthy were the relaxivity values for the trigadolinium complexes, **Co(Gd-DOTAGA-DTC)**₃ and **Ru(Gd-DOTAGA-DTC)**₃ at 1.5 T, which were at least twice that of Dotarem.

Stability and Toxicity Studies. The designs of the chelates used to complex the gadolinium ion are intentionally closely based on that of Dotarem, one of the leading clinically approved contrast agents. The stability of the chelate toward the loss of gadolinium ions (and, hence, its toxicity) has been probed in previous studies.^{13,14} This revealed that the addition of excess Zn^{2+} ions to **Gd-DO3A-NH**₂ and **Gd-DOTAGA-NH**₂ led to no change in the relaxivity values obtained, indicating that no displacement of Gd^{3+} ions occurred.²²

Stability studies were repeated for the multimetallic complexes, again in the presence and absence of excess Zn^{2+} ions. When the multimetallic complexes were dissolved only in phosphate-buffered saline (pH 7.4), there was no change in relaxivity for at least 72 h, indicating that the multimetallic complexes had remained intact and not degraded in this time. When the multimetallic complexes were in the presence of 10 equiv of Zn^{2+} ions, the relaxivity once again remained constant, confirming that no transmetalation had occurred between the Zn^{2+} and Gd^{3+} ions. These results were crucial for their potential use as clinical contrast agents as unchelated Gd^{3+} is known to be highly toxic, whereas chelated Gd^{3+} is generally well tolerated by the body.

In earlier studies, cytotoxicity assessment of the **Gd-DO3A-NH**₂ and **Gd-DOTAGA-NH**₂ gadolinium units revealed no toxicity to MCF-7 (breast cancer) or HeLa (cervical cancer) cells, even at concentrations of 250 μ M.^{13,14} In order to ascertain whether the multimetallic compounds described in this contribution had any adverse effects on the cell viability, the same 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) assay as previously reported^{13,14} was carried out in human embryonic kidney (HEK) and HeLa cell lines (Supporting Information). The multimetallic complexes all demonstrated low or no toxicity at concentrations up to 250 μ M. In the HEK cell line, the cell viability at 250 μ M ranged from 82 ± 4% for Co(Gd-DOTAGA-DTC)₃ (showing low

toxicity) up to $106 \pm 4\%$ for Ni(Gd-DO3A-DTC)₂ (showing no toxicity). In the HeLa cell line, the cell viability at 250 μ M ranged from 88 $\pm 2\%$ for Ru(Gd-DO3A-DTC)₃ to $103 \pm 2\%$ for Co(Gd-DO3A-DTC)₃.

The MTT cell viability assay was also performed on an additional complex, Gd-DO3A-DTC-AuPPh₂C₆H₄COOH (Supporting Information). This multimetallic compound was prepared based on work by Bodio et al.,²³ who demonstrated the antiproliferative properties of a number of gold(I) phosphine dithiocarbamate complexes featuring a central cyclam motif. The empty cyclam in the previous design was replaced with the Gd-DO3A chelate with the aim of creating a theranostic complex for combined MRI and cancer therapy. Unfortunately, no evidence of a therapeutic effect was observed following 24 h of incubation of Gd-DO3A-DTC-AuPPh₂C₆H₄COOH with HeLa (cervical cancer) cells as the cell viability remained at 89%, even at a concentration of 250 μ M. The addition of a carboxylic acid group to one of the phenyl rings was found to have little effect on the relaxivity of the complex because it performed very similarly to Gd-DO3A-DTC-AuPPh₃ at magnetic field strengths up to 0.25 T (Larmor frequency of 10 MHz).

Cell Uptake Studies. The uptake study was designed to gather further information on the behavior of these multigadolinium systems in a biological environment. Because of the superior relaxivity performance of the DOTAGA-based contrast agents, compared to the equivalent DO3A-based complexes, only the DOTAGA-based agents were taken forward to the uptake studies. Additionally, the negative charge on the DOTAGA chelates and lack of amide arm render them closer in structure to Dotarem, which allows an easier comparison to be made. By focusing on the DOTAGA-based agents, the charge density and lipophilicity were maintained (DOTAGA and Dotarem both have a negative charge, whereas DO3A is neutral), which ensured that the uptake of gadolinium depended principally on changes in the structure of the agent (i.e., number of Gd³⁺ units per complex).

The uptake of the DOTAGA-based multimetallic complexes by HeLa cells (Figure 10) was determined after incubation with the complexes for 24 h. The gadolinium concentration, not the complex concentration, was kept constant for each of the contrast agents, and the results showed that the uptake of gadolinium per cell increased as the number of gadolinium chelates per complex increased. The mass of gadolinium delivered to each cell increased from 1.2 ± 0.1 pg [Gd-DOTAGA-DTC-AuPPh₃] to 2.6 ± 0.2 pg [Co(Gd-DOTAGA-DTC)₃], which represents an uptake similar in mass to that achieved by other polygadolinium systems.^{13,14} This supported our hypothesis that incorporating multiple gadolinium chelates into the same assembly results in a more efficient delivery of gadolinium into cells. Extrapolation of this procedure from a cellular scale to a larger "tissue scale" would lead to an uptake of micrograms or even milligrams, which is adequate for MRI, as has already been observed with small-molecule gadolinium complexes both in vitro²⁴ and in vivo.²⁵

By keeping the concentration of gadolinium constant, it is possible to deduce that the increase in delivery of gadolinium is due to the design of the tetrametallic complexes and not simply because the cells were incubated with more gadolinium. Furthermore, the assessment of the ratio of gadolinium ions to central metal ions before and after uptake (Supporting Information) revealed no significant change, indicating that the complexes were entering the cells as a whole unit and therefore were stable toward degradation, even under biological conditions.

CONCLUSIONS

A series of bi-, tri-, and tetrametallic d-f mixed-metal complexes have been synthesized using either DO3A- or DOTAGA-based gadolinium chelates to generate potential MRI contrast agents with consistently greater relaxivity values than Dotarem, a clinically approved MRI contrast agent. Most remarkable were Co(Gd-DOTAGA-DTC)₃ and Ru(Gd-DOTAGA-DTC)₃, which achieved relaxivity values (per Gd³⁺ ion) of more than twice the value of Dotarem at a clinical magnetic field strength. This can be partly attributed to the larger mass of the multimetallic complexes compared to Dotarem, which leads to slower rotational motion and consequently greater relaxivity. However, a significant factor is also the rigidity of the piperazine-based dithiocarbamate linkers, which reduce the internal flexibility of the chelates and further enhance the relaxivity.

A number of tests were performed to probe the stability, toxicity, and cellular uptake of the multimetallic complexes. The stability tests revealed that the complexes were stable toward degradation and transmetalation, and an assessment of the gadolinium to central metal ion ratio before and after uptake by cells revealed that this stability toward degradation was maintained, even under biological conditions. MTT cell viability assays showed no evidence of toxicity, even at concentrations up to 250 μ M, and cell uptake studies demonstrated the improved delivery of gadolinium into cells when using a multigadolinium system.

The metallostar assemblies described here display significant potential as multigadolinium MRI contrast agents. Given the versatility of dithiocarbamate coordination chemistry, there is a wealth of opportunity to further develop these multimetallic complexes into targeted, multimodal or theranostic agents by exchanging a gadolinium chelate for an appropriate dithiocarbamate-linked ligand. Such a modification would improve the clinical appeal of these assemblies while avoiding a significant adjustment to an already straightforward synthetic route.

ASSOCIATED CONTENT

1 Supporting Information

The Supporting Information is available free of charge at https://pubs.acs.org/doi/10.1021/acs.inorgchem.0c01318.

Additional details on characterization of the compounds described here along with details of relaxivity, cytotoxicity, and cell uptake studies (PDF)

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Notes

The authors declare no competing financial interest.

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