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Original article

Novel ¹⁸F-labeled dibenzylideneacetone derivatives as potential positron emission tomography probes for *in vivo* imaging of β -amyloid plaques

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ABSTRACT

plaques in the brain.

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1. Introduction

Alzheimer's disease (AD) is devastating the elderly population with dementia, loss of memory, cognitive impairment, and inability to carry out routine activities [1]. It is not only a profound health and emotional influence on affected individuals and their families, but also a substantial economic burden on society. Extraordinary efforts will be spend on both the prevention and the treatment of dementia in the following decades, since this illness is going to affect about 63 million people by 2030, and 114 million by 2050 worldwide [2]. Early treatment depends on early disease diagnosis. However, the clinical diagnosis of AD is based mainly on the examination of mental and cognitive status nowadays [3], and the confirmation of the disease is achieved only by the postmortem examination of brain tissues [4,5]. It has been well established that the major neuropathological characteristics of AD is the presence of

senile plaques (SPs) and neurofibrillary tangles (NFTs). Furthermore, the extra cellular deposition of β -amyloid (A β) as SPs leading to the neuronal pathogenesis is currently considered the major pathological hallmark of AD brains [6,7]. Therefore, recent research efforts have been focused on noninvasive early visualization of A β plaques in living brain tissues to identify and further monitor individuals at risk for AD, as well as to assist in the evaluation of new anti-amyloid therapies currently under development [8–10].

Although several imaging techniques such as magnetic resonance imaging (MRI) [11–13], single photon emission computed tomography (SPECT) [14], and optical imaging [15–18] have been explored for the visualization of A β plaques in the past decade, A β plaque-specific positron emission tomography (PET) imaging remains the most successful noninvasive technique to date, which generated great anticipation and high hopes [10,19,20]. Vast array of PET ligands based on three categories of chemical groups have been reported, the thioflavin-T derivatives, the stilbene derivatives, and the aminonaphthyl derivatives [10,19] (Fig. 1). The first PET tracer specific for A β plaques was [¹¹C]-2-(4-(N-methylamino)phenyl)-6-hydroxybenzothiazol ([¹¹C]PIB) [21,22] through modification of thioflavin-T, but it has certain limitation that requires an on-site cyclotron because of short half-life of ¹¹C. An analogue of PIB, which demonstrates potential utility, [¹⁸F]-2-(3-fluoro-4-(N-

senile plaques (SPs) and neurofibrillary tangles (NFTs). Furthermore, the extra cellular deposition of β -amyloid (A β) as SPs leading to the neuronal pathogenesis is currently considered the major pathological hallmark of AD brains [6,7]. Therefore, recent research

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A series of dibenzylideneacetones were synthesized and evaluated as imaging probes for β -amyloid

plaques. They displayed high binding affinity to $A\beta_{1-42}$ aggregates ($K_i = 6.4$ for **8**, $K_i = 3.0$ for **9**), and the

high binding were confirmed by in vitro autoradiography with AD human and transgenic mouse brain

sections. Two of them were selected for ¹⁸F-labeling directly on the benzene ring. In biodistribution

experiments, $[^{18}F]$ **8** and $[^{18}F]$ **9** displayed high initial uptakes (9.29 ± 0.41 and 5.38 ± 0.68% ID/g) and rapid

washouts from the normal brain (brain_{2 min}/brain_{60 min} ratios of 21.6 and 13.4). These preliminary results suggest that [¹⁸F]**8** and [¹⁸F]**9** may be used as potential PET imaging agents for the detection of $A\beta$







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Fig. 1. Chemical structures of reported ¹⁸F labeled $A\beta$ imaging probes.

methylamino)phenyl)benzo[d]thiazol-6-ol ([¹⁸F]GE-067) [23] has been tested clinically and approved by FDA. The stilbene derivatives include [¹¹C]-4-N-methylamino-4'-hydroxystilbene ([¹¹C]SB-13) [24.25]. ¹⁸F]-4-(N-methylamino)-4'-(2-(2-(2-fluoroethoxy) ethoxy)ethoxy)-stilbene ([¹⁸F]BAY94-9172) [26] and [¹⁸F]-(E)-4-(2-(6-(2-(2-fluoroethoxy)ethoxy)pyridin-3-yl)vinyl)-Nmethylaniline ([¹⁸F]AV-45) [27,28], which are currently under commercial development for the mapping of $A\beta$ plaque burden in living brain tissue. Among them, $[^{18}F]AV-45$ was the first A β tracer approved by FDA. The aminonaphthyl derivative [¹⁸F]-2-(1-(2-(N-(2-fluoroethyl)-N-methylamino)-naphthalene-6-yl)ethylidene) malononitrile ([¹⁸F]FDDNP) was the first PET ligand put into human trials and also reported to bind to NFTs [29–31], whose binding site on A β deposits may differ from those of the prior two categories [10]. However, almost all ¹⁸F-labeled tracers currently in late phases of clinical development have high nonspecific white matter uptakes that give a distinctive white matter pattern in scans of healthy subjects. Furthermore, in PET scan images of AD patients, those ¹⁸Flabeled tracers frequently show the gray matter-white matter demarcation loss, and consequent loss of the normal white matter pattern, which are the predominant evidence of cortical amyloid plaques [32]. In the cortical ribbon typical of a positive [¹¹C]PIB scan, it less often shows the clearly intense binding, too [32]. So, new probes beyond the above three categories with improved properties including higher affinity for A β plaques and less nonspecific binding

in the white matter of the brain are always expected. In 2010, an extensive set of dibenzylideneacetone derivatives was synthesized and screened for affinity toward $A\beta_{1-42}$ aggregates by Cui et al. [33] Structure activity relationships revealed the binding of dibenzylideneacetones at the *para* position was highly tolerant of sterically demanding substitutions (K_i ranging from 0.9 to 7.0 nM). Two of them were labeled with ¹⁸F through a short length of polyethylene glycol chain (PEG). In biodistribution experiments, the radiofluorinated ligands [¹⁸F]**1** and [¹⁸F]**2** exhibited good initial penetration (4.13 and 5.15% ID/g, respectively, at 2 min) of and ordinary clearance from the brain. The brain₂ min/brain₆₀ min ratio of them is acceptable (4.59, and 4.06 for [¹⁸F]**1**, and [¹⁸F]**2**, respectively). These preliminary results suggested that the dibenzylideneacetone structure to be a potential new scaffold for the development of $A\beta$ imaging probes.

Therefore, based on the backbone of dibenzylideneacetones and their known affinities for $A\beta$ aggregates, in the present study we

designed a new type of ¹⁸F-labeled dibenzylideneacetone derivative (Fig. 2) for A β imaging using a novel ¹⁸F-labeling approach in two steps. This pathway labels ¹⁸F atom directly on the benzene ring in order to keep the affinity of dibenzylideneacetone to the greatest extent. Meanwhile, we also expect this innovation could minimize the molecular weight and improve the properties of the tracers, such as high brain uptakes, ineligible defluorination and better brain pharmacokinetics, compared with using the PEG pathway.

2. Results and discussion

2.1. Chemistry

The dibenzylideneacetone derivatives used in the binding assays and characterization of the corresponding ¹⁸F-labeled ligands were produced following the synthetic route shown in Scheme 1. The two substituted (E)-4-phenylbut-3-en-2-one derivatives 4 and 5 were prepared according to the method described previously [33]. The dibenzylideneacetone derivatives were obtained through base-catalyzed Claisen condensation reactions that coupled the substituted (*E*)-4-phenylbut-3-en-2-one suitably with 4flourobenzaldehyde or 2-flourpyridine-5-carboxaldehyde. The unsymmetrically substituted dibenzylideneacetones 7, 8 and 9 were obtained in 85.0–90.5% vields, and their corresponding pyridine substituted compounds 10, 11 and 12 were obtained in 78.3-88.9% vields. It should be mentioned here that we first used ethanol as the solvent for Claisen condensation reaction when preparing the pyridine derivatives **10–12**, but it turned out that the fluorine atom of the aimed product was displaced by ethoxy group (compounds **13–15**) at ambient temperature using K₂CO₃ as base and ethanol as solvent. The aromatic halides usually undergo nucleophilic substitution by various nucleophiles, such as secondary amines and alcoholate ion (e.g. ethanol as nucleophilic reagent at base condition), and the reaction rate will be accelerate when the fluoro atom was substituted at the ortho position of the pyridine ring. Therefore, we tried several different aprotic solvents such as acetonitrile, 1,4dioxane, diethyl ether, DMF and THF to proceed this reaction, and we found DMF is an efficient solvent in this kind of condensation reaction, compound 10-12 were obtained with high yields (78.3–88.9%). It means that we should be very careful to choose the solvent when labeling the pyridine array compounds.



Fig. 2. Chemical structures of the designed ¹⁸F labeled ligands in this work.



Scheme 1. Reagents and conditions: a. SnCl₂·2H₂O, EtOH, HCl, reflux; b. K₂CO₃, CH₃I, r.t.; c. NaOH, EtOH, r.t. for 7–9 and 13–15; NaOH, DMF, r.t. for 10–12.



Fig. 3. In vitro fluorescent staining of compound 7–12 (A, C, E, G, I, K, respectively, with filter set of GFP) on brain sections of a Tg model mouse (C57BL6, APPswe/PSEN1, 11 months old, male), and thioflavin-S on the adjacent sections (B, D, F, H, J, L, respectively, with filter set of DAPI). Stained plaques are indicated by red arrows. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)

2.2. In vitro fluorescent staining

To evaluate the binding affinities of compounds **7–12** to $A\beta$ plaques, *in vitro* fluorescent staining of $A\beta$ plaques on sections of brain tissue from Tg model mice (C57BL6, APPswe/PSEN1, 11 months old) were conducted as stated. As shown in Fig. 3 A, C, E, G, I and K, specific staining of plaques was clearly observed on the brain section of Tg mice for compound **7–12**. The presence and distribution of $A\beta$ plaques were perfectly consistent with the results of staining applying thioflavin-S (a common dye for staining of $A\beta$ plaques) on the adajacent sections (B, D, F, H, J and L).

2.3. In vitro binding studies

The quantitative affinities of these dibenzylideneacetone derivatives (**7**–**15**) for $A\beta_{1-42}$ aggregates were examined in competition binding assays, using [¹²⁵I]-6-iodo-2-(4'-dimethylamino-) phenyl-imidazo[1,2]pyridine ([¹²⁵I]IMPY) as the competing radioligand. IMPY was also screened employing the same system for comparison. As illustrated in Table 1, all compounds inhibited the binding of [¹²⁵I]IMPY in a dose-dependent manner (Fig. 4) and displayed high binding affinities to $A\beta_{1-42}$ aggregates with K_i values varied from 3.0 to 135.2 nM. Consistently to the previously reported findings, the tertiary *N*,*N*-dimethylamino analogues have higher affinities than the corresponding secondary *N*-methylamino analogues [34] (e.g., **8** vs. **9**, **11** vs. **12**). On the basis of the higher binding affinities to $A\beta_{1-42}$ aggregates, compounds **8** ($K_i = 6.4 \pm 3.2$ nM) and **9** ($K_i = 3.0 \pm 0.6$ nM) were selected for ¹⁸F labeling.

2.4. Radiolabeling

As shown in Scheme 2, in the first step of this two-step reaction, the ¹⁸F-labled intermediate $[^{18}F]$ -4-fluorobenzaldehyde ($[^{18}F]$ 17) was prepared with an average radiochemical yield of 40-60% (no decay corrected) after Sep-Pak C18 cartridge (Waters) separation. Then [¹⁸F]**17** was eluted out with ethanol to go through a basecatalyzed Claisen condensation in the ethanol with two corresponding substituted (E)-4-phenylbut-3-en-2-one separately to yield [¹⁸F]**8** and [¹⁸F]**9**. The radiochemical yields of [¹⁸F]**8** and [¹⁸F]**9** in the second step were about 50% (no decay corrected), resulting an average of 25% total yield with radiochemical purity greater than 95% after high performance liquid chromatography (HPLC) purification. The specific activities were estimated at approximately 160 GBg/umol (at the end of synthesis), high enough for the following in vitro and in vivo studies. The chemical identities of the ¹⁸F-labeled tracers were verified by comparison of the retention times with those of the nonradioactive standard compounds (Fig. 5).

 Table 1

 Inhibition constants (K_i , nM) for binding to aggregates of $A\beta_{1-42}$ versus [^{125}I]IMPY.^a

Compound	<i>K</i> _i (nM)	
7	17.1 ± 4.3	
8	6.4 ± 3.2	
9	3.0 ± 0.6	
10	135.2 ± 58.1	
11	36.5 ± 23.9	
12	8.5 ± 2.0	
13	65.8 ± 17.8	
14	14.2 ± 5.2	
15	7.6 ± 3.9	
IMPY	11.5 ± 2.5	

 $^{\rm a}$ Measured in triplicate with results given as the mean \pm SD.



Fig. 4. Inhibition curves for the binding of [¹²⁵I]IMPY to $A\beta_{1-42}$ aggregates.

We have two sound reasons to favor this two-step ¹⁸F labeling strategy. First, the Claisen condensation for coupling was proved to be fast enough for ¹⁸F labeling and a pretty convenient way to label ¹⁸F on a benzene ring, a very important component in the core structure of dibenzylideneacetone. Second, this strategy is ready to be applied when labeling many other different molecules containing one ketone group in the future studies.

2.5. In vitro stability studies

 $[^{18}F]$ **8** and $[^{18}F]$ **9** were found not only stable (>90%) in saline solution after storage for at least 1 h at room temperature during *in vitro* stability study, but also having high *in vitro* stability in mice plasma. After incubating for 60 min with mice plasma at 37 °C, more than 90% of the activity was identified as intact compound $[^{18}F]$ **8** or $[^{18}F]$ **9**, respectively.

2.6. In vitro autoradiography studies

Brain sections of a Tg mouse (C57BL6, APPswe/PSEN1, 11 months old) with A β plaques confirmed as well as an age-matched control mouse (C57BL6, 11 months old) were selected as staining material in the *in vitro* autoradiographic studies. As shown in Figs. 6 and 7, A β plaques of both hippocampus and cortical regions of the Tg mouse were selectively labeled by the ¹⁸F-labeled tracers [¹⁸F]**8** and $[^{18}F]$ **9**, separately, while no notable A β plaques was noticed on the brain of the control mouse. The consistent results of fluorescent staining stained by thioflavin-S further confirmed the distribution and pattern of those A β plaques. Since a previous report suggested that the configuration/folding of A β plaques in Tg mice might be different from the tertiary/quaternary structure of A β plaques in AD brains [35], we consider the binding information of new tracers for A β plaques in human AD brain even more important. As illustrated in Fig. 8, tracer [¹⁸F]9 with a dimethylamino group was tested for autoradiographic studies in sections of human brain tissue, and as we supposed, typical labeling pattern of $A\beta$ plaques was also observed on the AD brain section. For no apparent labeling was observed in normal adult brain section in contrast, this result further proved its affinity to $A\beta$ plaques from AD brain.

2.7. In vivo biodistribution studies

The log *D* values (2.69 \pm 0.19 for [¹⁸F]**8** and 3.89 \pm 0.21 for [¹⁸F]**9**, respectively) indicate that tracer [¹⁸F]**8** and [¹⁸F]**9** have moderate lipophilicity which is suitable for brain imaging. Here, we summarized the time-activity data on the brain permeation as well as the other organ distribution of the ¹⁸F-labeled tracers acquired in



Scheme 2. Reagents and conditions: a. CH₂Cl₂, ice-salt bath; b. K¹⁸F, K₂₂₂, DMSO, 160 °C, 6 min; c. NaOH, EtOH, r.t.



Fig. 5. (A) HPLC profiles of 8 and [18 F]8. (B) HPLC profiles of 9 and [18 F]9. HPLC conditions: Venusil MP C18 column (Agela Technologies, 10 × 250 mm), CH₃CN/H₂O = 70/30, 4 mL/min, UV = 254 nm.

biodistribution study in normal ICR mice in Tables 2 and 3. In this often used test to measure the initial brain uptake and washout kinetics from the normal brain, [¹⁸F]8 and [¹⁸F]9 displayed high uptakes into the brain $(9.29 \pm 0.41 \text{ and } 5.38 \pm 0.68\% \text{ ID/g}, \text{ respec-}$ tively) at 2 min post-injection and fast washout kinetics from the healthy brain (0.43 \pm 0.14 and 0.40 \pm 0.07% ID/g at 60 min, respectively), which are comparable to those reported for the ¹⁸Flabeled dibenzylideneacetone derivatives with PEG chains [33]. The ratio of brain_{2 min}/brain_{60 min} is also considered as an important index to select tracers with appropriate kinetics in vivo. Based on this point, the washout of $[^{18}F]AV-45$ in healthy mice, with a $brain_{2 min}/brain_{60 min}$ ratios of 3.90 (7.33 \pm 1.54% ID/g at 2 min, $1.88 \pm 0.14\%$ ID/g at 60 min) [27], is still not ideal, so as the recently reported ¹⁸F labeled 2-pyridinyl benzoxazole and benzothiazole derivatives [36], with brain_{2 min}/brain_{60 min} ratios ranged from 1.77 to 4.95. However, these two tracers showed brain_{2 min}/brain_{60 min} ratios of 21.6 and 13.4, respectively, indicating that these new type of ¹⁸F-labeled dibenzylideneacetone derivatives without the PEG chain may lower nonspecific white matter uptake. We also observed that in vivo defluorination which is an annoying problem with many ¹⁸F-labeled tracers was very slightly occurring with [¹⁸F] **8** and $[{}^{18}F]$ **9**, because the increase of the bone uptakes with time were minimal, thus the interference of defluorination with the imaging is expected to be relatively minor. Additionally, these ¹⁸Flabeled tracers also distributed to several other organs like the liver and the kidneys, However, their high initial uptakes were followed by moderate washouts. In summary, these two ¹⁸F-labeled derivatives ([¹⁸F]**8** and [¹⁸F]**9**) meet the preliminary requirements for *in vivo* detection of A β plaques as potential PET imaging agents. Compared with the ¹⁸F-labeled dibenzylideneacetone derivatives with PEG chains, the ¹⁸F-labeled dibenzylideneacetone derivatives without PEG chains had greatly improved pharmacokinetics and may lower nonspecific white matter uptake.

3. Conclusions

In conclusion, a series of dibenzylideneacetone derivatives was prepared using straightforward chemistry and evaluated as new PET imaging tracers for $A\beta$ plaques successfully. These dibenzylideneacetone derivatives tracers displayed various binding affinities to A β aggregates varied from 3.0 to 135.2 nM in the binding studies. Among them, two ligands with high affinities ($K_i = 6.4 \pm 3.2$ nM for **8** and $K_i = 3.0 \pm 0.6$ nM for **9**) to the aggregated A β were selected for ¹⁸F labeling and further evaluation. At first, the high affinities of these two tracers were again confirmed in the in vitro autoradiography on sections of postmortem AD brain and Tg mouse brain. Then, in biodistribution experiments, both radiotracers [¹⁸F]**8** and $[^{18}F]$ **9** displayed high initial uptakes into (9.29 ± 0.41 and $5.38 \pm 0.68\%$ ID/g at 2 min, respectively) and very rapid washouts from the brain in normal mice (brain_{2 min}/brain_{60 min} ratios of 21.6 and 13.4, respectively), indicating the pharmacokinetics had been greatly improved by these ¹⁸F-labeled dibenzylideneacetone derivatives without PEG chains. All the above results tell those two components, **8** and **9**, are highly desirable for $A\beta$ imaging because they may have much lower nonspecific white matter uptake. Furthermore, more than 90% of the activity was identified as the



Fig. 6. (A, B) *In vitro* autoradiography of [¹⁸F]**8** on a Tg model mouse (C57BL6, APPswe/PSEN1, 11 months old, male). (C, D) The presence and distribution of plaques were confirmed by fluorescence staining using thioflavin-S on the same section with a filter set for GFP. (E) *In vitro* autoradiography of [¹⁸F]**8** on a brain section of a age matched normal mouse as control. (F) Fluorescence staining using thioflavin-S on the same section of control mouse.

intact tracer respectively after 60 min incubating with either saline solution or mice plasma at 37 °C, indicating that both [¹⁸F]**8** and [¹⁸F]**9** displayed high *in vitro* stability. Overall, [¹⁸F]**8** and [¹⁸F]**9** with ¹⁸F directly labeled on the benzene ring of dibenzylideneacetone derivatives are promising PET agents for imaging cerebral $A\beta$ plaques, and further evaluation in model animal and human subjects with PET would provide valuable data for further $A\beta$ tracer designation and development.

4. Experimental

4.1. General information

All the reagents we used in the synthesis were commercially available and were used without further purification unless otherwise indicated. The ¹H NMR spectra and ¹³C NMR were obtained at a 400 MHz on Bruker spectrometer with samples dissolved in CDCl₃ solutions at room temperature. TMS was used as an internal standard, and all the chemical shifts were reported as δ values relative to the internal TMS. The coupling constants were reported in Hertz. Multiplicity is defined by s (singlet), d (doublet), t (triplet), and m (multiplet). Mass spectrometry was acquired under the Surveyor MSQ Plus (ESI) (Waltham, MA, USA) instrument. The synthesis reactions were carefully monitored by TLC (TLC Silica gel 60 F₂₅₄ aluminum sheets, Merck), because compounds were all visualized when illuminated with a short wavelength UV lamp ($\lambda = 254$ nm). Column chromatography purifications were

performed on silica gel (54–74 µm, Qingdao Haiyang Chemical Co., Ltd.). Radiochemical purity was evaluated by HPLC analysis performed on a Shimadzu system SCL-20 AVP equipped with a SPD-20A UV detector ($\lambda = 254$ nm) as well as a Bioscan Flow Count 3200 NaI/PMT γ -radiation scintillation detector. HPLC separations were achieved on a Venusil MP C18 reverse phase column (Agela Technologies, 5 μ m, 10 mm \times 250 mm) eluted with a binary gradient system at a flow rate of 4.0 mL/min on the Shimadzu HPLC; and HPLC analysis were achieved on a Venusil MP C18 column (Agela Technologies, reverse phase - 5 um. 4.6 mm \times 250 mm) eluted with a binary gradient system at a flow rate of 1.0 mL/min also with the Shimadzu HPLC. Mobile phase A was deionized water while mobile phase B was HPLC grade acetonitrile purchased from Amethyst Chemicals. The purities of the synthesized standard compounds (8 and 9) was determined using analytical HPLC and was found to be higher than 98%. Fluorescent observation was performed on the Observer Z1 (Zeiss. Germany) equipped with a DAPI filter set (excitation, 375 nm) and a GFP filter set (excitation, 488 nm). The normal ICR mice (five weeks, male) we used for biodistribution experiments were purchased from the Department of Laboratory Animal Science, Peking University Health Science Center. The Alzheimer's animal model, a transgenic mouse (C57BL6, APPswe/PSEN1, 11 months old) and an age-matched control mouse (C57BL6, 11 months old) were purchased from the Institute of Laboratory Animal Science, Chinese Academy of Medical Sciences. All protocols in this project requiring the use of mice were under approval by the animal care committee



Fig. 7. (A, B) *In vitro* autoradiography of [¹⁸F]**9** on a Tg model mouse (C57BL6, APPswe/PSEN1, 11 months old, male). (C, D) The presence and distribution of plaques were confirmed by fluorescence staining using thioflavin-S on the same section with a filter set for GFP. (E) *In vitro* autoradiography of [¹⁸F]**9** on a brain section of a age matched normal mouse as control. (F) Fluorescence staining using thioflavin-S on the same section of control mouse.



Fig. 8. (A) In vitro autoradiography of [18F]9 on an AD patient (64 years old, female) and (B) a normal person (74 years old, male) as control.

of Beijing Normal University. Post-mortem brain tissues from an AD case (64 years old, female) and a control case (74 years old, male) were obtained from the Chinese Brain Bank Center.

4.2. (1E, 4E)-1-(4-Aminophenyl)-5-(4-fluorophenyl)penta-1,4dien-3-one (**7**)

Dissolve compound **4** (161 mg, 1 mmol) and 4fluorobenzaldehyde (124 mg, 1 mmol) in 5 mL ethanol and add NaOH (40 mg, 1 mmol). The solution was stirred for 10 min at room temperature, and yellow solids precipitated from the solution. Keep the reaction for another 1 h. Final product was collected by filtration and washing by petroleum ether. The residue was purified by chromatography (ethylacetate/petroleum ether = 1:1, v/v) to afford yellow solid (yield 85.0%). ¹H NMR (CDCl₃, 400 MHz): δ 4.07 (s, 2H), 7.68 (d, *J* = 8.0 Hz, 2H), 6.87 (d, *J* = 15.6 Hz, 1H), 7.00 (d, *J* = 16.0 Hz, 1H), 7.09 (t, *J* = 8.4 Hz, 2H), 7.45 (d, *J* = 8.4 Hz, 2H), 7.59 (dd, *J*₁ = 8.7 Hz, *J*₂ = 2.3 Hz, 2H), 7.67 (d, *J* = 16.0 Hz, 1H), 7.68 (d, *J* = 15.6 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 114.9, 115.9, 116.2, 121.6, 124.9, 125.5, 130.1, 130.5, 141.0, 144.1, 149.2, 162.6, 165.1, 188.7. HRMS (TOF MS ES⁺): *m*/*z* calcd for C₁₇H₁₅NOF⁺ 268.1132 [M+H]⁺; found 268.1139.

4.3. (1E, 4E)-1-(4-Fluorophenyl)-5-(4-(methylamino)phenyl) penta-1,4-dien-3-one (**8**)

Compound **8** was prepared following the procedure used for **7**. The residue was purified by chromatography (ethylacetate/

 Table 2

 Biodistribution of [¹⁸F]8 in male ICR mice.^a

Organ	Time after injection				
	2 min	10 min	30 min	60 min	
Blood	5.08 ± 1.49	3.75 ± 0.81	3.71 ± 1.24	2.53 ± 0.84	
Brain	9.29 ± 0.41	1.65 ± 0.23	0.56 ± 0.06	0.43 ± 0.14	
Heart	8.57 ± 0.67	2.97 ± 0.34	1.77 ± 0.28	1.27 ± 0.31	
Liver	15.72 ± 1.21	21.29 ± 1.90	15.26 ± 1.94	10.74 ± 0.80	
Spleen	4.29 ± 0.72	2.20 ± 0.28	1.64 ± 0.30	1.27 ± 0.38	
Lung	23.90 ± 3.21	12.90 ± 1.63	8.99 ± 1.93	6.32 ± 0.99	
Kidney	17.19 ± 1.11	18.19 ± 4.68	16.07 ± 4.42	12.57 ± 0.58	
Pancreas	9.95 ± 0.39	3.49 ± 0.54	2.12 ± 0.28	1.43 ± 0.39	
Bone	1.87 ± 0.33	0.42 ± 0.08	1.30 ± 0.70	2.20 ± 0.72	
Stomach ^b	2.93 ± 0.48	5.17 ± 0.55	5.22 ± 1.19	2.28 ± 0.63	
Small intestine ^b	9.74 ± 1.01	10.25 ± 5.62	31.22 ± 5.02	55.10 ± 10.58	

 $^a\,$ Expressed as % injected dose per gram. Average for 5 mice \pm standard deviation. $^b\,$ Expressed as % injected dose per organ.

Table 3

Biodistribution of [¹⁸F]**9** in male ICR mice.^a

Organ	Time after injection				
	2 min	10 min	30 min	60 min	
Blood	6.89 ± 1.52	4.44 ± 0.77	5.56 ± 0.91	2.80 ± 0.42	
Brain	5.38 ± 0.68	1.27 ± 0.14	0.55 ± 0.09	0.40 ± 0.07	
Heart	9.86 ± 1.81	2.65 ± 0.23	1.98 ± 0.58	1.16 ± 0.18	
Liver	16.32 ± 4.34	15.37 ± 0.58	6.94 ± 0.89	7.94 ± 0.11	
Spleen	3.32 ± 0.43	1.47 ± 0.19	1.16 ± 0.32	0.61 ± 0.18	
Lung	8.96 ± 1.74	4.82 ± 0.07	3.79 ± 1.00	2.51 ± 0.35	
Kidney	17.02 ± 1.00	13.96 ± 2.38	15.98 ± 3.64	12.23 ± 4.31	
Pancreas	7.16 ± 0.86	2.83 ± 0.48	2.40 ± 0.33	1.08 ± 0.16	
Bone	2.42 ± 0.51	1.23 ± 0.49	0.92 ± 0.46	1.09 ± 0.27	
Stomach ^b	2.04 ± 0.25	2.54 ± 0.46	3.11 ± 0.73	2.28 ± 0.13	
Small intestine ^b	6.52 ± 2.77	7.41 ± 2.83	12.67 ± 1.76	31.18 ± 9.47	

 $^a\,$ Expressed as % injected dose per gram. Average for 5 mice \pm standard deviation. $^b\,$ Expressed as % injected dose per organ.

petroleum ether = 1:2, v/v) to afford yellow solid (yield 87.6%). ¹H NMR (CDCl₃, 400 MHz): δ 2.90 (s, 3H), 6.60 (d, *J* = 8.4 Hz, 2H), 6.85 (d, *J* = 15.6 Hz, 1H), 7.01 (d, *J* = 16.0 Hz, 1H), 7.09 (t, *J* = 8.6 Hz, 2H), 7.48 (d, *J* = 8.8 Hz, 2H), 7.60 (dd, *J*₁ = 8.8 Hz, *J*₂ = 5.6 Hz, 2H), 7.67 (d, *J* = 15.6 Hz, 1H), 7.70 (d, *J* = 15.60 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 30.3, 112.2, 115.9, 116.1, 120.9, 123.5, 125.5, 130.1, 130.6, 140.7, 144.5, 151.5, 162.8, 164.8, 188.7. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₈H₁₇NOF⁺ 282.1289 [M+H]⁺; found 282.1291.

4.4. (1E, 4E)-1-(4-(Dimethylamino)phenyl)-5-(4-fluorophenyl) penta-1,4-dien-3-one (**9**)

Compound **9** was prepared following the procedure used for **7**. The residue was purified by chromatography (ethylacetate/petroleum ether = 1:3, v/v) to afford yellow solid (yield 90.5%). ¹H NMR (CDCl₃, 400 MHz): δ 3.06 (s, 3H), 6.72 (d, *J* = 8.9 Hz, 2H), 6.88 (d, *J* = 15.7 Hz, 1H), 7.04 (d, *J* = 15.9 Hz, 1H), 7.11 (t, *J* = 8.6 Hz, 2H), 7.54 (d, *J* = 8.9 Hz, 2H), 7.62 (dd, *J*₁ = 8.7 Hz, *J*₂ = 5.4 Hz, 2H), 7.69 (d, *J* = 15.9 Hz, 1H), 7.74 (d, *J* = 15.8 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 40.1, 111.9, 115.9, 116.1, 120.9, 122.5, 125.6, 130.1, 130.5, 140.6, 144.4, 152.1, 162.6, 165.1, 188.6. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₉H₁₉NOF⁺ 296.1445 [M+H]⁺; found C₁₉H₁₉NOF⁺ 296.1450.

4.5. (1E, 4E)-1-(4-Aminophenyl)-5-(6-fluoropyridin-3-yl)penta-1,4-dien-3-one (**10**)

Dissolve compound **4** (161 mg, 1 mmol) and 6-fluoropyridine-3carbaldehyde (125 mg, 1 mmol) in 5 mL DMF and add NaOH (40 mg, 1 mmol). The solution was stirred for 1 h at room temperature, and yellow solids precipitated from the solution. Keep the reaction for another 1 h. Final product was collected by filtration and washing by petroleum ether. The residue was purified by silica gel chromatography (ethylacetate/petroleum ether = 1:1, v/v) to afford yellow solid (yield 78.3%). ¹H NMR (CDCl₃, 400 MHz): δ 4.07 (s, 2H), 6.68 (d, *J* = 8.4 Hz, 2H), 6.87 (d, *J* = 15.8 Hz, 1H), 7.00 (dd, *J*₁ = 8.5 Hz, *J*₂ = 2.7 Hz, 1H), 7.07 (d, *J* = 15.9 Hz, 1H), 7.46 (d, *J* = 8.4 Hz, 2H), 7.68 (t, *J* = 15.3 Hz, 2H), 8.01–8.06 (m, 1H), 8.43 (s, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 111.7, 114.9, 121.6, 124.7, 130.5, 130.6, 136.5, 138.8, 144.0, 148.8, 149.2, 165.1, 188.5. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₆H₁₃N₂OF⁺ 269.1085 [M+H]⁺; found 269.1107.

4.6. (1E, 4E)-1-(6-Fluoropyridin-3-yl)-5-(4-(methylamino)phenyl) penta-1,4-dien-3-one (**11**)

Compound **11** was prepared following the procedure used for **10**. The residue was purified by chromatography (ethylacetate/petroleum ether = 1:2, v/v) to afford yellow solid (yield 83.2%). ¹H NMR (CDCl₃, 400 MHz): δ 2.90 (s, 3H), 4.24 (s, 1H), 6.60 (d, *J* = 8.4 Hz, 2H), 6.84 (d, *J* = 15.7 Hz, 1H), 6.99 (dd, *J*₁ = 8.5 Hz, *J*₂ = 2.6 Hz, 1H), 7.08 (d, *J* = 15.9 Hz, 1H), 7.48 (d, *J* = 8.4 Hz, 2H), 7.66 (d, *J* = 15.9 Hz, 1H), 7.72 (d, *J* = 15.8 Hz, 1H), 8.01–8.05 (m, 1H), 8.42 (s, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 30.3, 109.9, 112.3, 123.3, 127.3, 130.3, 130.7, 136.6, 139.4, 145.2, 148.2, 151.7, 165.1, 188.1. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₇H₁₅N₂OF⁺ 283.1241 [M+H]⁺; found 283.1260.

4.7. (1E, 4E)-1-(4-(Dimethylamino)phenyl)-5-(6-fluoropyridin-3yl)penta-1,4-dien-3-one (**12**)

Compound **12** was prepared following the procedure used for **10**. The residue was purified by silica gel chromatography (ethylacetate/petroleum ether = 1:3, v/v) to afford yellow solid (yield 88.9%). ¹H NMR (CDCl₃, 400 MHz): δ 3.07 (s, 6H), 6.73 (d, *J* = 7.9 Hz, 2H), 6.86 (d, *J* = 15.7 Hz, 1H), 7.01 (dd, *J*₁ = 8.5 Hz, *J*₂ = 2.8 Hz, 1H), 7.10 (d, *J* = 15.9 Hz, 1H), 7.54 (d, *J* = 8.8 Hz, 2H), 7.67 (d, *J* = 15.9 Hz, 1H), 7.75 (d, *J* = 15.7 Hz, 1H), 8.03–8.07 (m, 1H), 8.44 (s, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 40.1, 111.6, 111.9, 120.8, 122.5, 124.4, 124.7, 130.4, 136.5, 138.4, 144.3, 148.7, 165.0, 188.4. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₈H₁₇N₂OF⁺ 297.1398 [M+H]⁺; found 297.1431.

4.8. (1E, 4E)-1-(4-aminophenyl)-5-(6-ethoxypyridin-3-yl)penta-1,4-dien-3-one (**13**)

Compound **13** was prepared following the procedure used for **7**. The residue was purified by silica gel chromatography (ethylacetate/petroleum ether = 1:1, v/v) to afford yellow solid (yield 73.6%). ¹H NMR (CDCl₃, 400 MHz): δ 1.41 (t, *J* = 7.1 Hz, 3H), 4.06 (s, 2H), 4.40 (dd, *J*₁ = 14.1 Hz, *J*₂ = 7.0 Hz, 2H), 6.67 (d, *J* = 8.4 Hz, 2H), 6.76 (d, *J* = 8.7 Hz, 1H), 6.87 (d, *J* = 15.8 Hz, 1H), 6.96 (d, *J* = 15.9 Hz, 1H), 7.44 (d, *J* = 8.5 Hz, 2H), 7.65 (d, *J* = 15.8 Hz, 1H), 7.67 (d, *J* = 15.8 Hz, 1H), 7.85 (dd, *J*₁ = 8.7 Hz, *J*₂ = 2.4 Hz, 1H), 8.32 (d, *J* = 2.2 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 14.6, 62.3, 111.7, 114.9, 121.5, 124.7, 130.2, 130.4, 130.5, 136.5, 138.8, 144.1, 148.8, 149.2, 165.0, 188.5. HRMS (TOF MS ES⁺): *m/z* calcd for C₁₈H₁₉N₂O⁺₂ 295.1441 [M+H]⁺; found 295.1436.

4.9. (1E, 4E)-1-(6-ethoxypyridin-3-yl)-5-(4-(methylamino)phenyl) penta-1,4-dien-3-one (**14**)

Compound **14** was prepared following the procedure used for **7**. The residue was purified by silica gel chromatography (ethylacetate/petroleum ether = 1:2, v/v) to afford yellow solid (yield 83.4%). ¹H NMR (CDCl₃, 400 MHz): δ 1.41 (t, *J* = 7.0 Hz, 3H), 2.89 (s, 3H), 4.40 (dd, *J*₁ = 14.1 Hz, *J*₂ = 7.0 Hz, 2H), 6.59 (d, *J* = 8.6 Hz, 2H),

6.76 (d, J = 8.7 Hz, 1H), 6.84 (d, J = 15.8 Hz, 1H), 6.97 (d, J = 15.8 Hz, 1H), 7.47 (d, J = 8.6 Hz, 2H), 7.69 (d, J = 16.0 Hz, 1H), 7.65 (d, J = 16.0 Hz, 1H), 7.84 (dd, $J_1 = 8.6$ Hz, $J_2 = 2.4$ Hz, 1H), 8.32 (d, J = 2.1 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 14.6, 30.3, 62.3, 111.6, 112.2, 120.8, 123.6, 124.3, 124.7, 130.6, 136.5, 138.5, 144.4, 148.7, 151.5, 165.0, 188.5. HRMS (TOF MS ES⁺): m/z calcd for C₁₉H₂₁N₂O⁺₂ 309.1603 [M+H]⁺; found 309.1542.

4.10. (1E, 4E)-1-(4-(dimethylamino)phenyl)-5-(6-ethoxypyridin-3-yl)penta-1,4-dien-3-one (**15**)

Compound **15** was prepared following the procedure used for **7**. The residue was purified by silica gel chromatography (ethylacetate/petroleum ether = 1:3, v/v) to afford yellow solid (yield 85.8%). ¹H NMR (CDCl₃, 400 MHz): δ 1.40 (t, *J* = 7.1 Hz, 3H), 3.02 (s, 6H), 4.40 (dd, *J*₁ = 14.2 Hz, *J*₂ = 7.1 Hz, 2H), 6.67 (d, *J* = 8.8 Hz, 2H), 6.75 (d, *J* = 8.6 Hz, 1H), 6.84 (d, *J* = 15.7 Hz, 1H), 6.97 (d, *J* = 15.8 Hz, 1H), 7.50 (d, *J* = 8.8 Hz, 2H), 7.64 (d, *J* = 15.9 Hz, 1H), 7.70 (d, *J* = 15.7 Hz, 1H), 7.84 (dd, *J*₁ = 8.7 Hz, *J*₂ = 2.3 Hz, 1H), 8.32 (d, *J* = 2.2 Hz, 1H). ¹³C NMR (CDCl₃, 100 MHz): δ 14.6, 40.1, 62.2, 111.6, 111.9, 120.7, 122.4, 124.4, 124.7, 130.4, 136.4, 138.4, 144.3, 148.7, 152.0, 165.0, 188.4. MS (TOF MS ES⁺): *m*/*z* calcd for C₂₀H₂₃N₂O⁺₂ 323.1760 [M+H]⁺; found 323.1804.

4.11. 4-(N, N, N-trimethylamino)benzaldehyde triflate (16)

Dissolve 4-dimethylaminobenzaldehyde (124 mg, 1 mmol) in 5 mL CH₂Cl₂ and add methyl trifluoromethanesulfonate (150 µL, 1.2 mmol) dropwise in ice salt bath. The solution was stirred for 3 h in the ice salt bath, and white solid precipitated from the solution. After filtration, washing with CH₂Cl₂, 75.7 mg white solid was obtained (yield 24.2%). ¹H NMR (D₂O, 400 MHz): δ 3.66 (s, 9H), 8.02 (d, J = 9.0 Hz, 2H), 8.13 (d, J = 9.0 Hz, 2H), 9.99 (s, 1H).

4.12. In vitro fluorescent staining of $A\beta$ plaques on transgenic mouse brain sections

Before use, paraffin-embedded brain sections of Tg mouse (C57BL6, APPswe/PSEN1, 11 months old, male, 6 µm) were deparaffinized according to the following procedure: 2×20 min washes with xylene, 2×5 min washes with 100% ethanol, 5 min washes with 90% ethanol/H₂O, 5 min wash with 80% ethanol/H₂O, 5 min wash with 60% ethanol/H₂O, running tap water for 10 min, and then incubated in PBS buffer (0.2 M, pH = 7.4) for 30 min. The brain sections were then incubated with 10% (v/v) ethanol solution of 7-12 (1 µM) for 10 min at room temperature just before examining by microscope. The localization and patterns of $A\beta$ plaques was confirmed by staining with thioflavin-S on the adjacent sections as contrast. For the staining of thioflavin-S, the deparaffinized sections were immersed in a thioflavin-S solution (0.125%, w/w) containing 10% EtOH (v/v) for 3 min and then washed with 40% EtOH. Finally, before examining by the microscope, the sections were washed again with 40% ethanol and PBS (0.2 M, pH = 7.4) for 10 min. Fluorescent observation was performed by microscope Observer Z1 (Zeiss, Germany) equipped with DAPI (excitation, 375 nm) and GFP filter sets (excitation, 488 nm).

4.13. In vitro binding assay to $A\beta$ aggregates

The trifluoroacetic acid salt forms of peptides $A\beta_{1-42}$ were purchased from Osaka Peptide Institute (Osaka, Japan). Aggregation reaction was carried out by first gently dissolving the peptide (0.56 mg/mL for $A\beta_{1-42}$) in a buffer solution (pH = 7.4) which contained 10 mM sodium phosphate and 1 mM EDTA. The solution was incubated with gentle and constant shaking at 37 °C for 42 h. Inhibition experiments were carried out according to procedures described previously [37] with some modification. To be brief, 100 μ L of aggregated A β fibrils (28 nM in the final assay mixture) was added to a mixture which contains 100 μ L of radioligand ([¹²⁵I] IMPY, 100,000 cpm/100 μ L), 100 μ L of inhibitors (10⁻⁴-10^{-8.5} M in ethanol), and 700 μ L of PBS (0.2 M, pH = 7.4) in a final volume of 1 mL in 12 mm \times 75 mm borosilicate glass tubes. The mixture was incubated at room temperature for 3 h. and then, the bound and free radioactive fractions were separated by vacuum filtration through borosilicate glass fiber filters (Whatman GF/B) performed by a Mp-48T cell harvester (Brandel, Gaithersburg, MD). The radioactivity caught by the filters containing the bound ¹²⁵I-ligand was measured by a γ -counter (WALLAC/Wizard1470, United States) with about 70% efficiency. Under the assay conditions, the specifically bound fraction accounted for about 10% of total radioactivity. Nonspecific binding was defined in the presence of IMPY $(1 \mu M)$ in the same way. The inhibitory concentration (IC_{50}) was determined using Graph Pad Prism 4.0 software. The inhibition constant (K_i) was calculated according to the Cheng-Prusoff inhibition constant equation: $K_i = IC_{50}/(1+[L]/K_d)$.

4.14. Radiolabeling

[¹⁸F]Fluoride trapped on a QMA Light cartridge (Waters) was eluted with 1 mL of Kryptofix₂₂₂/K₂CO₃ solution (13 mg of Kryptofix₂₂₂ and 1.1 mg of K₂CO₃ in CH₃CN/H₂O, 4: 1 (v/v) into a clean glass vial. The solvent was quickly removed by heating at 120 °C under a stream of nitrogen gas. Then, the residue was azeotropically dried with 1 mL of anhydrous acetonitrile by three times (about 0.3 mL for each) at 120 °C under a stream of nitrogen gas. 4-(N, N, N-trimethylamino)benzaldehyde triflate (5.0 mg) dissolved in 1.0 mL of dry DMSO was added to the reaction vessel containing the ¹⁸F[–] activity and heated at 160 °C for 6 min. After the reaction vial was cooled by running cold water to room temperature, 10.0 mL of water were added to this orange solution. We passed the mixture with a syringe through a Sep-Pak C18 cartridge (Agela Technologies). The cartridge was washed with 10 mL of water, and the intermediate [¹⁸F]-4-fluorobenzaldehyde was eluted with 1 mL of EtOH the [¹⁸F]-4-fluorobenzaldehyde was washed out by 1 mL EtOH. The appropriate ketones (5 or 6, 1.0 mg) were added into the EtOH solution containing [¹⁸F]-4-fluorobenzaldehyde, as well as 4.0 mg of NaOH to catalyze the Claisen condensation, the mixture was kept for 30 min with gentle shaking under room temperature. The longer the reaction was, the higher the condensation yields are found. But taking the decay into consideration, 30 min is better. The solvent was evaporated under nitrogen gas and the residue was dissolved in HPLC eluent and neutralized with 6 µL acetic acid before subjecting to HPLC for purification (Agela Technologies, 5 μ m, 10 mm \times 250 mm, CH₃CN/H₂O = 70/30; flow rate = 4 mL/ min). After purification by HPLC, the radiochemical purity of [¹⁸F]**8** and [¹⁸F]**9** was greater than 95%. The retention time of [¹⁸F]**8** and [¹⁸F]**9** were 11.05 and 17.02 min in this HPLC system, respectively. The preparation took 90 min and the total radiochemical yield was about 25% (at the end of synthesis, no decay corrected).

4.15. In vitro autoradiography on brain sections of human and transgenic model mouse

The paraffin-embedded sections of human and transgenic model mouse brain were deparaffinized first with 2 \times 20 min washes in xylene; then 2 \times 5 min washes in 100% ethanol; 5 min wash in 90% ethanol/H₂O; 5 min wash in 80% ethanol/H₂O; 5 min wash in 60% ethanol/H₂O and finally 10 min wash in running tap water before incubating in PBS (0.2 M, pH = 7.4) for 30 min. The sections were then incubated with [¹⁸F]**8** and [¹⁸F]**9** (1.85 MBq/

200 μ L) solution in saline for 1 h at room temperature. After they were rinsed with water for 1 min, washed with 40% EtOH, and dried with blowing air, the sections were exposed to a phosphorus plate (Perkin Elmer, USA) for 2 h in dark. *In vivo* autoradiographic images were obtained by a phosphor imaging system (Cyclone, Packard). After the *in vitro* autoradiographic examination, the same mouse brain sections were stained again by thioflavin-S solution the same way in *in vitro* fluorescent staining to confirm the presence and pattern of A β plaques. The fluorescent observation was performed on the Observer Z1 (Zeiss, Germany) equipped with GFP filter sets (excitation, 488 nm).

4.16. Biodistribution

A saline solution which contains the HPLC-purified ¹⁸F-labled tracer (0.1 mL, 10% ethanol, 185 kBq) was injected via tail veins of the ICR mice (five weeks, male). The mice were then sacrificed by cervical fracture exactly at time points of 2, 10, 30 and 60 min. The samples of blood and interested organs were collected, weighed and counted separately in an automatic γ -counter (Wallac 1470 Wizard, USA). The final results were expressed in terms of the percentage of the injected dose per gram (% ID/g) of blood or organs with decay corrected.

4.17. Partition coefficient determination

The log *D* values of $[^{18}F]$ **8** and $[^{18}F]$ **9** were determined by measuring the distribution of the radiotracer between 1-octanol and PBS buffer (0.05 M) at pH = 7.4. The two phases were presaturated with each other. 1-octanol (3 mL) and PBS (3 mL) were pipetted into a 10 mL plastic centrifuge tube. 10 µL of HPLC-purified $[^{18}F]$ **8** or $[^{18}F]$ **9** (0.74 MBq) in ethanol was then added. The tube was vortexed for 5 min, followed by centrifugation for 15 min (3500 rpm, Anke TDL80-2B, China). Two samples removed from the *n*-octanol (50 µL) and water (500 µL) layers were separately measured by an automatic γ -counter (Wallac 1470 Wizard, USA). The distribution coefficient was determined by calculating the ratio of cpm/mL of 1-octanol layer to that of buffer layer and expressed as log *D*. Samples from the 1-octanol layer were re-distributed until consistent distribution coefficient values were obtained.

4.18. In vitro stability studies

The *in vitro* stability of $[^{18}F]$ **8** and $[^{18}F]$ **9** in saline and mouse plasma were examined by incubating 1.85 MBq purified $[^{18}F]$ **8** or $[^{18}F]$ **9** with 100 µL saline or mouse plasma at 37 °C for 2 min, 10 min, 30 min and 60 min. Proteins were precipitated by adding 200 µL acetonitrile. The supernatant was collected, after centrifugation at 5000 rpm for 5 min at 4 °C. A sample of approximately 0.1 mL of the supernatant solution was removed and subjected to HPLC for analysis.

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Appendix A. Supplementary data

Supplementary data related to this article can be found at http://dx.doi.org/10.1016/j.ejmech.2014.07.070.

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