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Radiochemical Synthesis and Evaluation of ¹³N-Labeled 5-Aminolevulinic Acid for PET Imaging of Gliomas

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KEYWORDS: 5-ALA, brain tumor, cancer, positron emission tomography, imaging

ABSTRACT: The endogenous amino acid, 5-aminolevulinic acid (5-ALA), has received significant attention as an imaging agent, including on-going clinical trials for image-guided tumor resection due to its selective uptake and subsequent accumulation of the fluorescent protoporphyrin IX in tumor cells. Based on the widely reported selectivity of 5-ALA, a new Positron Emission Tomography imaging probe was developed by reacting methyl 5-bromolevuinate with [¹³N] ammonia. The radiotracer, [¹³N] 5-ALA, was produced in high radiochemical yield (65%) in 10 minutes, and could be purified using only solid phase cartridges. *In vivo* testing in rats bearing intracranial 9L glioblastoma showed peak tumor uptake occurred within 10 minutes of radiotracer administration. Immunohistochemical staining and fluorescent imaging was used to confirm the tumor location and accumulation of the tracer seen from the PET images. The quick synthesis and rapid tumor specific uptake of [¹³N] 5-ALA makes it a potential novel clinical applicable radiotracer for detecting and monitoring tumors non-invasively.

Brain tumors present additional challenges for diagnosis and treatment due to the intracranial location, involvement of the central nervous system and difficult to deliver imaging and therapeutic agents through the blood brain barrier. Gliomas make up 80% of malignant brain tumors and often result in poor prognosis and decreased life expectancy¹. Diagnosing brain tumors heavily depends on invasive procedures of cranial biopsy or after tumor resection. Current first pass diagnostic imaging for brain tumors² such as MRI and CT provide mostly anatomical and morphological details, but lack of molecular and functional information.

The endogenous amino acid, 5-aminolevulinic acid (5-ALA), is the first compound in the biological synthesis of heme in mammals³. It is found that enhanced uptake of 5-ALA in cancerous cells provides an accumulation of a fluorescent porphyrin known as Protoporphyrin IX (PpIX)⁴. While the preferential accumulation of 5-ALA in tumors still remains an area of active investigation, the current proposed mechanisms include: increased 5-ALA entry through a disrupted blood brain barrier⁵, upregulation of beta⁶ and oligopeptide transporters⁷ (PEPT1 and PEPT2), increased expressions of enzymes in the heme biosynthesis pathway and decreased amount of the enzyme ferrochetelase⁸. In particular, 5-ALA is useful for brain tumors because of its selective fluorescence in gilomas⁹. It is widely reported that PpIX is preferentially accumulated in glioblastoma cells with ratios of 20 to 50:1 compared to normal brain cells^{10,11}. Primary transportation through the blood brain barrier occurs through the choroid plexus¹², however, leaky vascular may also be a factor when tumors are present in the brain⁵. Therefore, there are increasing interests and efforts in developing clinical applications of 5-ALA. For example, 5-ALA and its esters¹³ have found use in fluorescence-guided surgery to help visualize tumorous tissue in neurosurgical procedures¹¹. The use of 5-ALA as an intraoperative imaging probe for determining tumor margins during the resection of malignant gliomas has been found to increase the rate of gross total resection to 65% compared to 35% without 5-ALA¹⁴. The progression-free survival rate at 6 months is also increased to 41% when using 5-ALA versus 21% without^{14,15}. In addition, 5-ALA shows promise for future therapeutic applications for cancer using photodynamic therapy (PDT). In this therapy technique, the preferential accumulation of PpIX in tumors provides a substrate which when exposed to UV light, results in reactive oxygen species that can ultimately kill cancer cells¹⁶. While the fluorescence of PpIX can be useful for therapeutic applications, imaging PpIX for diagnostic purposes is limited to superficial tumors or intraoperative procedures due to poor light penetration through the skin^{17,18}.

Using a radiolabled version of 5-ALA for Positron Emission Tomography (PET) not only can overcome the limitations of optical detectability but also can potentially provide a highly tumor specific PET tracer compared to existing $[^{18}F]$ fluorodeoxyglucose (FDG), which often has strong background signals due to the high uptake in brain parenchyma¹⁹. Furthermore, 5-ALA PET scanning would be useful for pre-operative planning in conjunction to surgical resection procedures that use 5-ALA to visualize tumors for fluorescence-guided surgery. Thus, an amino acid-based PET tracer may be more useful for imaging tumors in the brain²⁰⁻²³. Additionally, a 5-ALA based radioligand could also help determine the viability of a candidate for PDT when using 5-ALA as a photosensitizer. There is also evidence that the uptake of 5-ALA is variable in different tumor lines^{24,25}. A PET ligand may be used to quantitate the rate of PpIX synthesis^{26,27}. This information could potentially be used to non-invasively grade or differentiate brain tumors based on the PpIX metabolism. These wide arrays of potential applications lead us to seek a method to develop a radioactive



Scheme 1. Synthesis of the precursor, methyl 5-bromolevulinate 2, and radiochemical synthesis of [¹³N] 5-ALA 1.

version of the naturally occurring amino acid that would be suitable for use with PET imaging.

The molecule 5-ALA lends itself to very few practical installments of a PET radioisotope. Without altering the compound, the only usable PET isotopes are ¹¹C, ¹³N, and ¹⁵O. Ideally, ¹¹C would be the best-suited isotope due to its extensive use in the field of PET imaging and its longer half-life (20 min). Unfortunately, at this time, there are no facile ways of synthesizing a ¹¹C version of 5-ALA in high radiochemical yield. To date, only a ¹¹C derivative of 5-ALA, 5-amino-4oxo-[6-11C]hexanoic acid ([11C] MALA) has been synthesized¹⁷. This novel radiotracer was created by installing a ¹¹C methyl group on an oxime precursor using tetrabutyl ammonium fluoride and [11C] methyl iodide in DMSO. There were several drawbacks to this radiosythesis: the precursor was difficult to purify, the reaction results in a racemic mixture, the synthesis is multiple steps, preparatory HPLC is required, radiochemical yield was low (4.4% uncorrected decay), and the resulting radiotracer is not a natural occurring amino acid. Non-radioactive MALA, was found to be an inhibitor of 5aminolevulinate dehvdratase ($K_i = 0.2$ M), and thus can only be used to estimate the synthesis rate of PpIX^{17,28}. Because of these factors and our previous experience working with the quick decaying ${}^{13}N$ isotope 29 , we sought to produce the naturally occurring $[{}^{13}N]$ 5-ALA radiotracer 1. Herein, we describe the radiochemical synthesis of $[^{13}N]$ 5-ALA 1 and demonstrate its use in tumor imaging in a rat model of glioma using the 9L glioma cell line.

The precursor for [¹³N] 5-ALA 1, methyl 5-bromolevulinate 2, was synthesized by reacting levulinic acid with bromine in methanol (**Scheme 1**). This reaction has been studied at great length in a variety of different solvents including ionic liquids^{30,31}. The reaction of bromine with levulinic acid typically produces a mixture of 3-bromo, 5-bromo, and 3,5-dibromo isomers depending on the solvent used. Using methanol as a solvent, the non-optimized reaction resulted in a 30% yield of the desired isomer after separation using silica column chromatography. The amount of methyl 5-bromolevulinate produced was sufficient for labeling studies.

[¹³N] Ammonia is produced by bombarding water containing ethanol (0.25%) as a reductant³². After eluting the cyclotron product through a QMA cartridge to remove residual [¹⁸F] fluoride, [¹³N] ammonia can be trapped on a CM cartridge in near quantitative recovery. The [¹³N] ammonia can be eluted off the CM cartridge in aqueous form by an increase in ionic strength. In a typical experiment, a 30 minute bombardment (60 $\mu A)$ produced around 250 mCi (9.25 GBq) of $[^{13}N]$ ammonia.

For the production of $[^{13}N]$ 5-ALA 1, the $[^{13}N]$ ammonia was eluted off the cartridge with aqueous sodium acetate (1 mL, 3 M) into a vial containing the precursor 2 (8 mg) dissolved in acetonitrile (250 µL) (Scheme 1). Heating the vial for 3 minutes at 50 °C was sufficient for complete radioisotope incorporation, but to ensure no $[^{13}N]$ ammonia was present, the vial was purged with argon for 2 minutes to remove any volatile unreacted [¹³N] ammonia. Due to time constraints and the lack of side products, the radiotracer was quickly purified using only cartridges to remove any remaining precursor. The crude reaction mixture was loaded by vacuum onto tC18 and HLB cartridges (Waters) into a waste vial. A small amount of ¹³N] 5-ALA 1 (<20 mCi or 0.74 GBg) was detected in the waste vial but the majority of radioactivity was retained on the two cartridges. Eluting 3 mL of an acidic solution through the Sep-Paks provided the radiotracer [¹³N] 5-ALA 1 in high radiochemical yield (65% decay corrected) (Scheme 1). Using acidic phosphate (0.2 M, pH = 5), acetic acid/sodium acetate (0.2 M, pH = 6), or HCl (10 mmol, pH = 2) for elution all provided similar yields (~100 mCi or 3.7 GBq). To ensure no particles were present, the purified solution was pressure filtered through a 0.2 µm filter into a sterile vial and subsequently used immediately in studies. The total time from the end of bombardment to dose was 10 minutes. The dose formulation was intentionally made slightly acidic (pH = 6) to ensure dimerization did not occur. It is well known that when nonradioactive 5-ALA is formulated at neutral or basic pH, it can rapidly dimerize to 2,5-dicarboxyethyl-3,6-dihydropyrazine and further oxidize to produce 2,5-(DHPY) dicarboxyethylpyrazine (PY)³³. In an acidic formulation, the radiotracer shelf-life was longer than its decay.

Due to the short half-life of ¹³N, the quality control on the amino acid was conveniently performed using radio thin layer chromatography. This is the type of analysis routinely used for the quality control of polar radiotracers. For a more in-depth analysis, the polar nature of this amino acid requires the use of hydrophilic interaction chromatography to assay the quality of the dose produced¹⁷. The 5-ALA HCl salt standard lacks a significant chromophore and requires that low wavelengths (210 nm) be used. This also makes determining specific activity difficult. The only source of ammonia should be from the cyclotron target, we estimate the specific activity of [¹³N] 5-ALA **1** is similar to [¹³N] ammonia (> 2 Ci/µmol or 74 GBq/µmol) for the end of synthesis.



Figure 1. HPLC profiles of 5-ALA. (A) UV absorbance (210 nm) of unlabeled 5-ALA. (B) Radioactivity (mV) of $[^{13}N]$ 5-ALA.

Studies reported by Hebeda et al showed 5-ALA was readily taken up in 9L glioma cells implanted in rats by using fluorescence to detect PpIX³⁴. Therefore, we chose to use the 9L cells to prepare the rat intracranial tumor model to test [¹³N] 5-ALA *in vivo* using microPET imaging. The studies were conducted in male rats with 9L cells surgically implanted into the right hemisphere of the brain. After 12 to 14 days, in which the 9L tumors typically grow to 3-5 mm in size, dynamic PET imaging was performed for 60 minutes followed by a CT scan to obtain the anatomic images.

PET images (Figure 2) show that the 9L tumor takes up ¹³N] 5-ALA, resulting in observation of high signal intensity at the tumor region with a signal intensity ratio of 1.5 compared to the symmetrical contralateral normal brain tissue in the left hemisphere (Figure 3). Peak uptake of [¹³N] 5-ALA in the tumor cells occurred within 10 minutes. To confirm and validate the imaging results, the animals were sacrificed immediately after the imaging experiments to collect the whole brains and snap frozen before storing in -80 °C. Each brain was then sectioned to 1 mm thick slices for fluorescent imaging using the wavelength of PpIX to determine the distribution in the brain, followed by the H&E staining for tumor region identification. Figure 4 shows PET, optical images and H&E staining of the brain slice from one of the animals. H&E staining indicate the location of the 9L tumor and corresponding PET image which correlates well with the high signal region in the PpIX fluorescent image.

In conclusion, we have successfully synthesized [¹³N] 5-ALA in high radiochemical yield and purity within 10 minutes. The stability of the radiotracer was high for imaging experiments and no dimerization was observed. This rapid synthesis time and lack of HPLC purification makes the radiotracer [¹³N] 5-ALA suitable for additional imaging experiments of other tumor cell lines.



Figure 2. Summed coronal PET images (0-15 min) of a rat bearing intracranial 9L glioma: (A) $[^{13}N]$ 5-ALA in the brain, (B) coregistered PET-CT, (C) CT template. The arrow indicates the location of the tumor.

[N-13] 5-ALA Tumor/Brain uptake



Figure 3. Ratio of $[^{13}N]$ 5-ALA uptake in the 9L tumor (right hemisphere) vs normal brain tissue (left hemisphere) (n = 3).





Figure 4. (A) Transverse PET summed image (0-15 min) of the brain. (B) Post mortem brain slice. (C) Optical image of the brain slice shown in B. (D) Immunohistochemical (H&E) staining of the brain slice B. The circle indicates the location of the tumor.

ASSOCIATED CONTENT

Supporting Information

Supporting information provides full experimental details and characterization data for organic compounds, and radiochemical procedures. This material is available free of charge via the internet at http://pubs.acs.org

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The manuscript was written through contributions of all authors. / All authors have given approval to the final version of the manuscript. / ‡These authors contributed equally.

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Notes

The authors declare no competing financial interest.

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ABBREVIATIONS

5-ALA, 5-aminolevulinic acid; PPIX, Protoporphyrin IX; MRI, Magnetic Resonance Imaging; PET, Positron Emission Tomography; CT, Computed Tomography; PEPT1, Peptide Transporter 1; PEPT2, Peptide Transporter 2; PDT, Photodynmaic Therapy; FDG, Fluorodeoxyglucose; MALA, methyl aminolevulinic acid; QMA, Quaternary Methyl Amine; CM, Carboxy Methylate.

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Scheme 1. Synthesis of the precursor, methyl 5-bromolevulinate 2, and radiochemical synthesis of [13N] 5- $\,$ ALA 1.

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Figure 1. HPLC profiles of 5-ALA. (A) UV absorbance (210 nm) of unlabeled 5-ALA. (B) Radioactivity (mV) of [13N] 5-ALA.

83x88mm (150 x 150 DPI)





Figure 2. Summed coronal PET images (0-15 min) of a rat bearing intracranial 9L glioma (arrow): (A) [13N] 5-ALA in the brain, (B) coregistered PET-CT, (C) CT template.

83x36mm (150 x 150 DPI)



Figure 3. Ratio of [13N] 5-ALA uptake in the 9L tumor (right hemisphere) vs normal brain tissue (left hemisphere) (n = 3).

83x66mm (122 x 122 DPI)



Figure 4. (A) Transverse PET summed image (0-15 min) of the brain. (B) Post mortem brain slice. (C) Optical image of the brain slice shown in B. (D) Immunohistochemical (H&E) staining of the brain slice B.

84x72mm (150 x 150 DPI)



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