

Communication

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An Optical/Photoacoustic Dual Modality Probe: Ratiometric in/ex Vivo Imaging for Stimulated H₂S Upregulation in Mice

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Supporting Information Placeholder

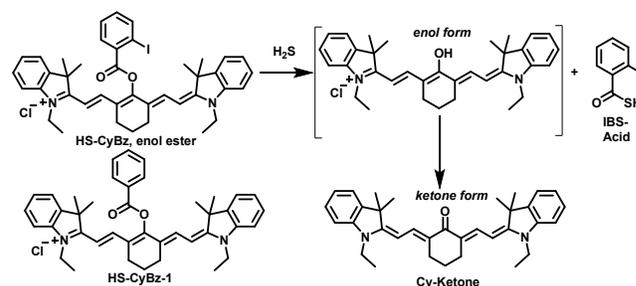
ABSTRACT: Tracking signaling H₂S in live mice demands responsive imaging with fine tissue imaging depth and low interferences from tissue scattering/autofluorescence and probe concentration. With complementary advantages of fluorescence and photoacoustic (PA) imaging, optical/PA dual modality imaging was suggested for in/ex vivo H₂S imaging. Therefore, a *meso*-benzoyloxytricarboheptamethine cyanine, **HS-CyBz**, was prepared as the first ratiometric optical/PA dual modality probe for H₂S, profiting from a keto-enol transition sensing mechanism. Tail intravenous injection of this probe leads to probe accumulation in the liver of mice, and the endogenous H₂S upregulation triggered by S-adenosyl-L-methionine has been verified by ratiometric optical/PA imaging, suggesting the promising potential of this ratiometric dual modality imaging.

Many small molecule species including metal cations, reactive oxygen species, and gasotransmitters are essentially involved in signaling pathways and pathogenesis.^{1,2} Beyond intracellular fluorescence imaging of signaling small molecules (SSMs),³ in/ex vivo SSMs tracking in animal model especially in mice is appealed in pathological and clinical study. To evaluate the signaling behavior and pathology, in/ex vivo SSMs imaging is required to track SSM fluctuation besides offering SSM distribution pattern. Therefore imaging technique showing deep tissue imaging depth and SSM response is demanded. PET and SPECT are incapable to provide SSMs fluctuation information due to their irresponsive probe. Although MRI responsive probes have been reported,⁴ optical imaging is more attractive for its quick response and high sensitivity.⁵ However, the limited tissue penetration depth of fluorescence (<1 mm) makes optical imaging visualize only superficial SSMs. This disadvantages can be overcome by photoacoustic (PA) imaging with imaging depth of several centimeters in tissues,⁶ although the sensitivity and resolution of PA imaging are lower. Therefore, fluorescence/PA dual modality imaging, which possesses the advantages of both modalities, is expected to improve SSMs imaging efficacy in mice.⁷ As fluorescence and PA signals can be interfered by tissue scattering/autofluorescence and probe concentration, single channel optical and PA imaging is not reliable for tracking stimulated SSM fluctuation. Considering the advantage of

ratiometric imaging in overcoming these interferences,⁸ NIR ratiometric optical/PA dual modality probe is required for in/ex vivo SSM imaging.

As the third gaseous signaling molecule, H₂S is involved in vasodilation, angiogenesis, anti-oxidation, anti-inflammation, and central nervous regulation.⁹ Many fluorescence probes have been developed for intracellular H₂S imaging,¹⁰ in vivo optical or PA imaging for H₂S is still not satisfying since most of them are based on turn-on probes.¹¹ In this study, the first optical/PA dual modality probe showing ratiometric response to H₂S, **HS-CyBz**, was developed (Scheme 1), and in/ex vivo ratiometric optical and PA imaging for endogenous H₂S upregulation stimulated by the cystathionase activator S-adenosyl-L-methionine (SAM) was realized in mice with this probe.

Scheme 1. H₂S sensing mechanism of HS-CyBz and chemical structure of HS-CyBz-1.



As benzoic esters of a *meso*-hydroxytricarboheptamethine cyanine, both probe **HS-CyBz** and its analogue without ortho-iodo substituent, **HS-CyBz-1** were prepared in this study. Their cyanine moiety was adopted to provide NIR absorption and emission.¹² It is expected that nucleophilic substitution of the ester by HS⁻ would release enolic heptamethine cyanine, which undergoes keto-enol tautomerization to form **Cy-ketone** (Scheme 1). This tautomerization would shift emission and absorption distinctly, showing ratiometric fluorescent and photoacoustic response to HS⁻. Both compounds were prepared via reacting the corresponding benzoic chloride with *meso*-hydroxytricarboheptamethine cyanine.

Emission spectrum of **HS-CyBz** exhibits a main emission band centered at 805 nm and a minor broad band centered at 630 nm (λ_{ex} , 595 nm). Na₂S addition resulted in the drop of

former band and drastic enhancement of the latter one (Figure 1a). The large hypsochromic emission shift of ~ 175 nm and well separated dual emission bands indicated the excellent ratiometric response behavior of **HS-CyBz** toward H_2S . A linear enhancement of emission ratio (F_{630}/F_{805}) was observed upon Na_2S titration from 0 to 1 mM (Figure S7), and the H_2S detection limit of this probe was determined to be $0.5 \mu\text{M}$. This showed the potential of **HS-CyBz** for endogenous H_2S detection (10 – $600 \mu\text{M}$ in human brain, 10 – $100 \mu\text{M}$ in human blood^{10a,13}). **HS-CyBz-1** possesses a similar emission spectrum. Temporal tracking of ratio F_{630}/F_{805} after Na_2S addition revealed that **HS-CyBz** reacted with HS^- rapidly and attained equilibrium in 10 min, while **HS-CyBz-1** reacted with HS^- much more slowly and reaction equilibrium could not be attained even after 0.5 h. Moreover, the HS^- -induced ratio enhancement factor of **HS-CyBz** is much higher than that of **HS-CyBz-1** (Figure S8c). Therefore **HS-CyBz** is more suitable for H_2S sensing due to its high sensitivity and rapid response, and the electron withdrawing iodo group favoring ester cleavage via HS^- nucleophilic attacking might be the origin.

Absorption spectrum of **HS-CyBz** shows a sharp absorption band at 775 nm ($\epsilon \sim 1.8 \times 10^5 \text{ M}^{-1} \text{ cm}^{-1}$) and a shoulder band (708 nm). Probe reaction with Na_2S at pH 7.4 led to the distinct decrease of the sharp band and a minor increase at 850 nm, resulting in an isobestic point at 825 nm (Figures 1b, S8b and S9). This colorimetric sensing behavior suggested that this probe might be a ratiometric PA probe for HS^- .

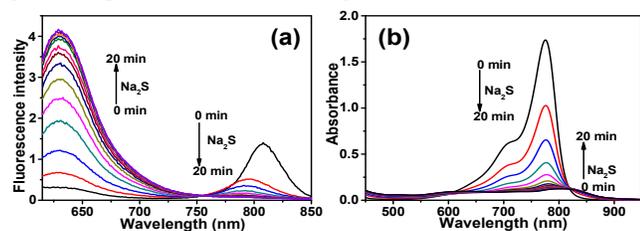


Figure 1. Emission (a, λ_{ex} 595 nm) and absorption (b) spectra of **HS-CyBz** ($10 \mu\text{M}$) in HEPES buffer (pH 7.4) determined after the addition of Na_2S (1 mM).

ESI mass determination of **HS-CyBz** solution mixed with Na_2S displayed a signal of m/z 493.25 in positive mode spectrum and a signal of m/z 262.80 in negative mode spectrum. The two signals were assigned as $[\text{Cy-ketone}+\text{H}]^+$ and $[\text{IBS-Acid-H}]^-$, respectively (Figure S10). **Cy-Ketone** has been separated from the reaction mixture in a medium yield. All these indicated that HS^- nucleophilic substitution of benzoic ester would release enolic *meso*-hydroxyltricarboheptamethine cyanine and trigger keto-enol transition, which is responsible for the HS^- -induced spectroscopic response. The quantum yield of **HS-CyBz** and **Cy-Ketone** were determined as 0.02 and 0.17. The emission ratio F_{630}/F_{805} for **HS-CyBz** increased from 0.3 to 54.9 (183-fold) after 100 equiv Na_2S being added.

Investigating sensing behavior of **HS-CyBz** for biochemical species of interest revealed that only Na_2S led to a distinct enhancement of emission ratio F_{630}/F_{805} (~ 32 -fold, 30 equiv HS^-), while other species such as cations (K^+ , Na^+ , Ca^{2+} , Mg^{2+} , 1 mM), anions (S_n^{2-} , 300 μM ; Ac^- , HCO_3^- , NO_3^- , NO_2^- , SO_4^{2-} , SO_3^{2-} , H_2PO_4^- , SCN^- , $\text{S}_2\text{O}_3^{2-}$, 1 mM), reactive oxygen species (H_2O_2 , ClO^- , 1 mM), biothiols (GSH, Cys, 1 mM; Hcy 200 μM), and carboxylesterase (0.5 U/mL) triggered minor change in F_{630}/F_{805} . The presence of biothiols GSH, Cys and Hcy showed no obvious interference with the HS^- -induced ratio enhancement (Figure S12a). Moreover, the emission ratio F_{630}/F_{805} of **HS-CyBz** showed no distinct pH-dependence from

pH 5.0 to pH 8.5 (Figure S13). The colorimetric sensing behavior suggested that this probe might enable ratiometric photoacoustic sensing for HS^- . PA imaging of **HS-CyBz** solutions revealed that the PA signal upon excitation at 825 nm (isobestic point) was weak and stable upon HS^- titration, while the signal upon excitation at 775 nm decreased distinctly in the process (Figure 2c), and the ratio $\text{PA}_{825}/\text{PA}_{775}$ increased almost linearly from ~ 0.2 to ~ 0.7 with $[\text{HS}^-]_{\text{total}}$ increasing from 0 to 1 mM (Figure S12c). Moreover, other tested biochemical species did not induce obvious change of $\text{PA}_{825}/\text{PA}_{775}$, and the presence of biothiols such as GSH, Hcy and Cys did not interfere with the HS^- -induced $\text{PA}_{825}/\text{PA}_{775}$ ratio enhancement (Figures 2b and S12b), showing the ratiometric photoacoustic sensing ability for H_2S .

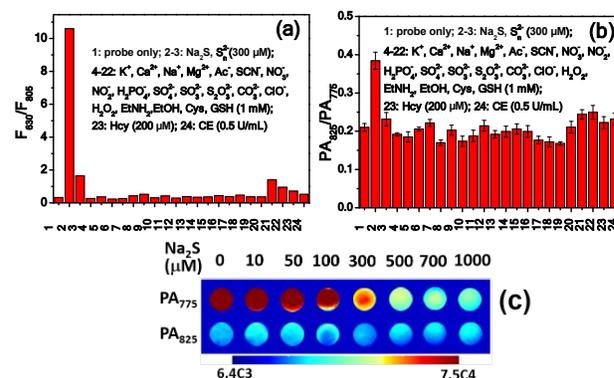


Figure 2. Emission ratio F_{630}/F_{805} (a) and PA ratio $\text{PA}_{825}/\text{PA}_{775}$ (b) of **HS-CyBz** ($10 \mu\text{M}$) in HEPES buffer in the presence of different analytes. (c) PA image of probe ($10 \mu\text{M}$) solutions upon Na_2S titration (dual channel mode: λ_{ex} 775 and 825 nm).

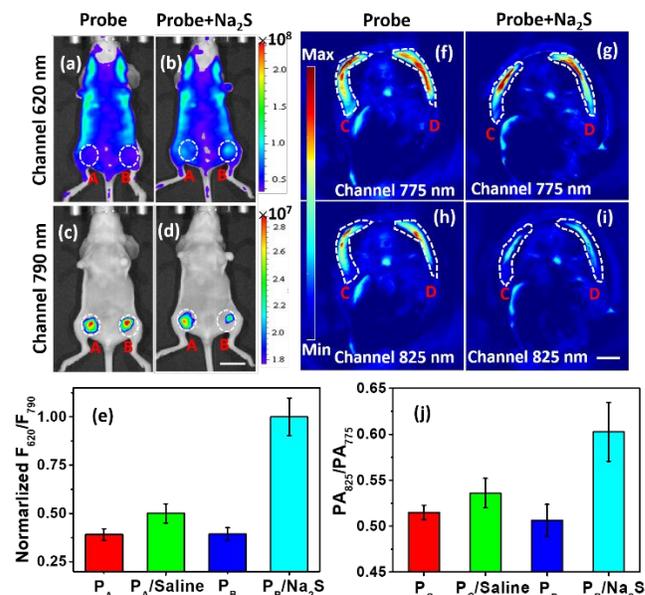


Figure 3. *In vivo* ratiometric optical (a-e, Ch 1: 620 ± 20 nm, Ch 2: 790 ± 20 nm, λ_{ex} 560 nm) and PA (f-i, Ch 3: 775 nm, Ch 4: 825 nm) imaging for H_2S in mice injected subcutaneously with **HS-CyBz** (P, 100 μL , 20 μM) in region of interests (A, B on the hind limbs; C, D on the back). (a, c) Images of probe-injected mouse; (b, d) images of mouse in (a, c) 30 min post saline (ROI A) and Na_2S (ROI B) injection (100 μL , 1 mM); (e) normalized F_{620}/F_{790} of ROIs A and B determined in (a-d). Scale bar: 1 cm. (f, h) PA images of probe-injected mouse; (g, i) PA images of mouse in (f, h) 30 mins post injection with saline (ROI C) and Na_2S (ROI D); (j) $\text{PA}_{825}/\text{PA}_{775}$ ratios for ROIs C and D. Scale bar: 3 mm.

Without commercial available apparatus uniting optical and PA imaging, ratiometric optical and PA imaging ability of **HS-CyBz** for H_2S were investigated in mice, respectively. In vivo ratiometric optical imaging was realized initially in a 6-week-old mouse with the hind limbs being injected with probe subcutaneously (ROIs A and B). The image from channel 1 (620 ± 20 nm) showed that the weak fluorescence of free probe in ROIs A and B was almost concealed by tissue autofluorescence. The subsequent Na_2S injection in ROI B led to the fluorescence enhancement (~ 1.60 -fold, Figures 3b and S14a), which was still interfered by tissue autofluorescence. The control (ROI A) injected with saline showed a less enhancement factor of ~ 1.21 -fold. Images from Channel 2 (790 ± 20 nm) showed no obvious autofluorescence interference, and Na_2S injection led to fluorescence decrease with a factor of ~ 0.63 -fold, and that for control (ROI A) was ~ 0.94 -fold. Therefore, Na_2S injection in ROI B made fluorescence ratio F_{620}/F_{790} increase with a factor of ~ 2.54 -fold, indicating the enhanced HS^- concentration. The control in ROI A showed a minor ratio enhancement factor of ~ 1.28 -fold (Figure 3e). The Na_2S -induced F_{620}/F_{790} change in ROI B is more distinct than the single channel signal change (F_{620}). This result indicated that in vivo ratiometric optical imaging is more reliable and sensitive than single channel turn-on imaging, and the interference from autofluorescence and deviated probe concentration is effectively reduced.

The dual channel photoacoustic imaging was carried out on the back of mouse with ROIs C and D injected subcutaneously with the probe. The distinct photoacoustic signals of the probe were observed in both channels (Figures 3f and 3h, ROIs C and D) with Channel 4 showing the lower signal. The signal ratio $\text{PA}_{825}/\text{PA}_{775}$ for both ROIs C and D with only probe injection is similar (~ 0.51 , Figures S14b and 3j). The subsequent Na_2S injection in ROI D made the signal in both channels decrease (Figures 3g and 3i), which is different from the expected signal decrease in Channel 3 and stable signal in Channel 4. The local probe concentration decrease caused by diffusion and the injection-induced dilution may be the origin. However, ratio $\text{PA}_{825}/\text{PA}_{775}$ of ROI D was enhanced to 0.60 upon Na_2S injection (Figure 3j), while that for control in ROI C with saline injection was 0.53. This confirmed that the HS^- level in ROI D was enhanced. All results revealed that the ratiometric PA imaging is more reliable than single channel PA imaging in reducing interference from the deviated local probe concentration.

12 h post SAM injection. (a) Fluorescence image of mice injected with SAM and saline. Bandpath 790 ± 20 nm, λ_{ex} 720 nm; (b) ex vivo fluorescence images of isolated livers from mouse in (a) acquired at 620 (left) and 790 (middle) nm, and ratiometric image (right), λ_{ex} 560 nm; Scale bar, 1 cm. (c-d) PA images of livers from the SAM- and saline-injected mice recorded by channel 775 nm (c) and channel 825 nm (d), and the related $\text{PA}_{775}/\text{PA}_{825}$ ratios (e). Scale bar, 6 mm.

In/ex vivo imaging for endogenous H_2S upregulation in mice was explored, and SAM was utilized to upregulate H_2S expression.¹⁴ The mouse was injected intravenously with **HS-CyBz** 12 h post SAM intraperitoneal injection. Optical imaging revealed that the fluorescence in the epigastrium of SAM-injected mouse was much lower than that in mouse with saline injection, implying SAM-injection enhanced H_2S level distinctly (Figure 4a). The ex vivo optical imaging of isolated viscera disclosed the liver accumulation of this probe (Figure S15), and ex vivo ratiometric image revealed that F_{620}/F_{790} ratio in the liver of SAM-injected mouse was distinctly higher than that in mouse with no SAM injection (Figure 4b), confirming SAM-injection inducing endogenous H_2S enhancement in the liver. As shown in single channel PA images of the isolated livers (Figures 4c and 4d), it is difficult to judge whether SAM-injection trigger H_2S upregulation in liver. However, the PA signal ratio $\text{PA}_{825}/\text{PA}_{775}$ was enhanced from 0.59 in the liver of saline-injected mouse to 0.65 in the liver of SAM-injected mouse (Figure 4e). This result indicated that SAM injection caused H_2S upregulation, confirming the advantage of dual channel ratiometric PA imaging.

In summary, the first ratiometric optical/PA dual modality probe for H_2S was prepared, profiting from the HS^- -induced keto-enol tautomerization of *meso*-hydroxytricarboheptamethine cyanine. With NIR absorption/emission, **HS-CyBz** enables the optical/photoacoustic dual modality imaging for subcutaneous H_2S in mice, and the ratiometric imaging for both modes favors the alleviation of interferences from tissue autofluorescence and the deviated probe concentration. Tail intravenous injection of probe resulted in accumulation in mice liver, and the SAM-stimulated endogenous H_2S enhancement in the liver was confirmed by optical/PA dual modality imaging. This study indicates that ratiometric optical/PA dual modality imaging was an effective approach to tracking SSM upregulation in live mice and tissues, and the perspective technique uniting optical and PA imaging should promote SSM biology in the future.

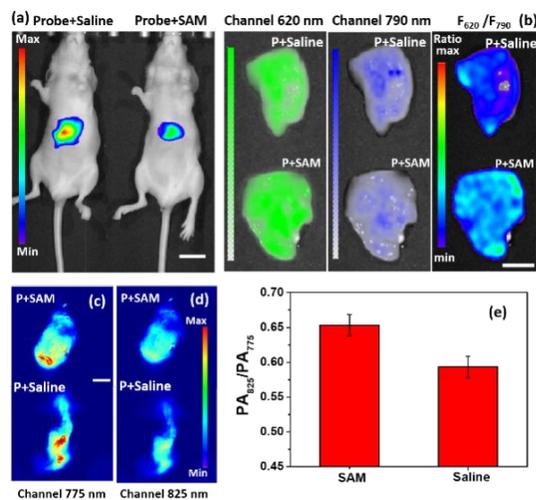


Figure 4. Optical (a-b) and photoacoustic (c-e) imaging for mice injected with SAM. **HS-CyBz** was injected intravenously

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website. Synthesis, characterization of probe and experiment details for spectroscopic and imaging study.

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Notes

The authors declare no competing financial interests.

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