

In vivo ester hydrolysis as a new approach in development of PET tracers for imaging hypoxia

Lifang Zhang, Xinyue Yao, Jianhua Cao, Haiyan Hong, Aili Zhang, Ruiyue Zhao, Yan Zhang, Zhihao Zha, Yajing Liu, Jinping Qiao, Lin Zhu, and Hank F. Kung

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4 **1 In vivo ester hydrolysis as a new approach in development of PET**
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7 **2 tracers for imaging hypoxia**
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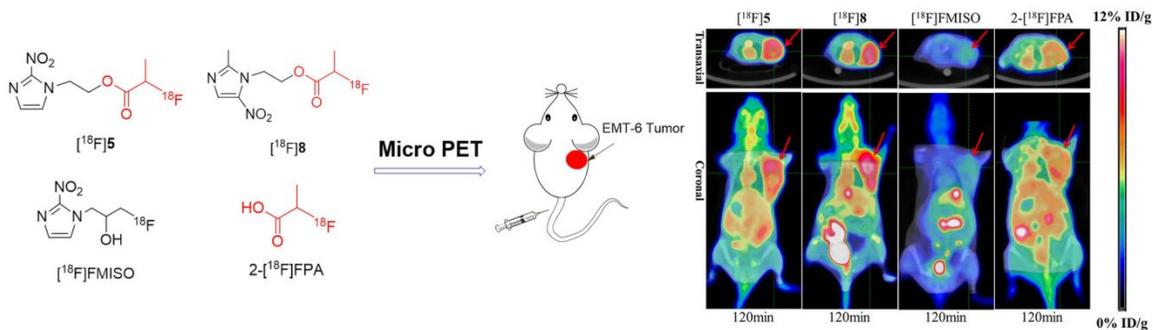
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New PET tracers for imaging hypoxia

1 Table of Contents



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Abstract:

Hypoxia is an important biochemical and physiological condition associated with uncontrolled growth of tumor. Measurement of hypoxia in tumor tissue may be useful in characterization of tumor progression and monitoring drug treatment. [^{18}F]FMISO is the most widely employed radiotracer for imaging of hypoxic tissue with positron emission tomography (PET). However, it showed relatively low uptake in hypoxic tissues, which led to low target-to-background contrast in PET images. To overcome these shortcomings, two novel 2-fluoropropionic acid esters, nitroimidazole derivatives, 2-fluoropropionic acid 2-(2-nitro-imidazol-1-yl)-ethyl ester (FNPFT, [^{19}F]**5**) and 2-fluoropropionic acid 2-(2-methyl-5-nitro-imidazol-1-yl)-ethyl ester (FMNPFT, [^{19}F]**8**), were prepared and tested. Radiolabeling of [^{18}F]**5** and [^{18}F]**8** were accomplished in 45 min (radiochemical purity > 95%, the decay-corrected radiochemical yield of [^{18}F]**5** was $11 \pm 2\%$, and that of [^{18}F]**8** was $13 \pm 2\%$, $n = 5$). In vitro cell uptake studies using EMT-6 tumor cells showed that both radiotracers [^{18}F]**5** and [^{18}F]**8** displayed significantly higher uptake in hypoxic cells than those under normoxic condition, while 2- [^{18}F]fluoropropionic acid (2- [^{18}F]FPA) displayed no difference. Biodistribution studies in mice bearing EMT-6 tumor showed that [^{18}F]**5**, [^{18}F]**8**, and 2- [^{18}F]FPA displayed similar tumor and major organ uptakes. Tumor uptake values for all three agents were higher than those of [^{18}F]FMISO, respectively ($P < 0.05$). This is likely due to a rapid in vivo hydrolysis of [^{18}F]**5** and [^{18}F]**8** to their metabolite, 2- [^{18}F]FPA. Micro PET imaging studies in the same

1 EMT-6 implanted mice tumor model also demonstrated that both [¹⁸F]**5** and [¹⁸F]**8**
2 displayed similar tumor uptake comparable to that of 2-[¹⁸F]FPA.

3 In conclusion, two new fluorine-18 labeled nitroimidazole derivatives, [¹⁸F]**5** and
4 [¹⁸F]**8**, showed good tumor uptakes in mice bearing EMT-6 tumor. However, in vivo
5 biodistribution results suggested that they were more likely reflect the predominance of in
6 vivo produced metabolite, 2-[¹⁸F]FPA, which may not be related to tumor hypoxic
7 condition.

8
9 **Keywords:** Micro PET imaging; in vivo metabolism; EMT-6 tumor; nitroimidazole;
10 hypoxia

11 12 **Abbreviations**

13 PET: Positron Emission Tomography; HPLC: High performance liquid chromatography;
14 TLC: Thin-layer chromatography; [¹⁸F]FMISO: [¹⁸F]Fluoromisonidazole; [¹⁸F]FAZA:
15 [¹⁸F]fluoroazomycin arabinofuranoside; [¹⁸F]FETNIM: [¹⁸F]fluoroerythronitroimidazole;
16 [¹⁸F]FETA: [¹⁸F]fluoroetanidazole; [¹⁸F]EF5: 2-(2-nitro-1*H*-imidazol-1-yl)-*N*-(2, 2, 3, 3,
17 3-[¹⁸F]pentafluoro-propyl)acetamide; 2-[¹⁸F]FPA: 2-[¹⁸F]fluoropropionic acid; NITTP:
18 1-(2-nitro-10-imidazolyl)-2-*O*-tetra-hydropyranyl-3-*O*-toluenesulfonylpropane-diol;
19 [¹⁸F]EF3: 2-(2-nitroimidazol-1-yl)-*N*-(3, 3, 3-[¹⁸F]trifluoropropyl)-acetamide; RCY:

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- 1 Radiochemical yield; RCP: Radiochemical purity; OTBDMS: tert-butyldimethylsilyloxy
- 2 group.

1 Introduction

2 Hypoxia in tumor tissue is an important pathological process that commonly
3 associated with uncontrolled growth of tumor. It is considered to be a factor determining
4 the curability of radiotherapy and chemotherapy.¹⁻⁴ The effect of hypoxia on biological
5 processes depends on tumor type, as well as the degree and duration of oxygen
6 deprivation.^{5, 6} Thus, determining the extent of tumor hypoxia is an important factor for
7 planning of cancer therapy.^{7, 8} There is an urgent need to develop effective approaches for
8 measuring hypoxia in tumor tissue. Currently, oxygen sensitive electrode and
9 immunohistochemistry are gold standards for detecting hypoxic areas in tumor. However,
10 they are not suitable for routine use due to their technical difficulty and invasiveness.⁹⁻¹¹
11 Positron emission tomography (PET) imaging may have certain advantages, which may
12 overcome the difficulties in evaluation of hypoxia tumor tissue non-invasively. In
13 addition, PET imaging has superior global sensitivity and quantification capability
14 making it as one of the most promising technologies for detecting tumor hypoxia.^{7, 11-13}

15 Originally, 2-nitroimidazole compounds, for example, [¹⁸F]fluoromisonidazole
16 ([¹⁸F]FMISO, Figure 1), were developed for detecting tumor hypoxia in 1979.¹⁴ Currently,
17 [¹⁸F]FMISO is still the most commonly used PET agent for imaging hypoxia and it is
18 considered as a gold standard for studying hypoxia by in vivo PET imaging.¹⁵⁻²⁰ However,
19 despite its long history and extensive literature reports, [¹⁸F]FMISO has failed to gain

1 wide acceptance for routine clinical application. This is due to its relatively low uptake in
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4 hypoxic tumor, slow clearance from the blood and normal tissues, which contribute to
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7 low target-to-background contrast in PET images. In the past few decades, significant
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10 efforts have been reported in developing better hypoxia PET imaging agents.^{12, 21-25} New
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13 nitroimidazole PET tracers with different side chains were produced and evaluated
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16 successively for PET imaging of hypoxic tumors, including the introduction of sugars
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19 (¹⁸F)fluoroazomycin arabinofuranoside, [¹⁸F]FAZA),^{9, 26, 27} adding hydroxyl groups
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22 (¹⁸F)fluoroerythronitroimidazole, [¹⁸F]FETNIM),^{28, 29} and adding amide bonds
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25 (¹⁸F)fluoroetanidazole, [¹⁸F]FETA).^{30, 31} (Figure 1) However, these ¹⁸F-labeled
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28 2-nitroimidazoles shared a common feature: they showed a higher hydrophilicity, thus,
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31 reduced lipophilicity for cell membrane penetration than that of [¹⁸F]FMISO. These
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34 radiotracers displayed either low signal/noise ratios due to lower uptake in hypoxic
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37 lesions or slower clearance from normal tissues.^{10, 11, 32} It has been shown that
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40 hydrophilicity facilitates clearance in well oxygenated tissues, while lipophilicity
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43 enhances accumulation in hypoxic tissues. In search of optimal hypoxia imaging agents
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46 achieving a delicate balance between these contrasting properties is critically important.
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49 In recent years, a new series of highly lipophilic derivatives have been studied, such as
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52 2-(2-nitro-1*H*-imidazol-1-yl)-*N*-(2, 2, 3, 3, 3-[¹⁸F]pentafluoropropyl)-acetamide
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55 ([¹⁸F]EF5) and 2-(2-nitroimidazol-1-yl)-*N*-(3, 3, 3-[¹⁸F]trifluoropropyl)-acetamide
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58 ([¹⁸F]EF3).³³⁻³⁷ (Figure 1) In addition, several hypoxia radiotracers based on

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1 metronidazole derivatives (i.e. 5-nitroimidazole derivatives) have been reported, some of
2 which demonstrated very favorable in vivo biodistribution properties.³⁸⁻⁴⁰

3 Earlier reports have pointed out that more lipophilic nitroimidazole analogs would
4 be expected to cross cellular membranes and the blood–brain barrier (BBB) more readily
5 and resulted in a greater initial uptake in the targeted hypoxic tissue than [¹⁸F]FMISO,
6 although there is a concomitant increase of nonspecific uptake.^{21, 41, 42} This is a necessary
7 trade-off between a higher lipophilicity (promoting cellular uptake through diffusion) and
8 a higher liver uptake (due to a higher lipophilicity). The requirement of optimal
9 lipophilicity leading to favorable biodistribution and pharmacokinetics of the radiotracer
10 must be carefully balanced in the course of design an ideal hypoxia imaging agent.
11 Recently, ¹⁸F-acetyl has been conjugated to 2-nitroimidazole to form a ¹⁸F-labeled
12 fluoroacetate of 2-nitroimidazole.⁴³ Results of LC-MS data showed that the hypoxia
13 tracer was hydrolyzed in vivo to hydrophilic ¹⁸F-fluoroacetic acid. Results suggested that
14 it was possible to enhance tumor uptake and speed up non-target clearance in vivo by
15 introducing ¹⁸F-aliphatic ester into nitroimidazole analogues. Additionally, previous
16 studies reported that hydrolysable nitroimidazole aliphatic esters might be useful as
17 radiosensitizers for cancer therapy.^{44, 45} The esters were subject to enzyme-catalyzed
18 hydrolysis in human plasma and in pure buffer solution. The length of the linear carbon
19 chain in the aliphatic esters influences the rate of enzyme catalyzed degradation.
20 Furthermore, studies by Johansen et al⁴⁵ also revealed large differences in chemical

1 stability of the nitroimidazole aliphatic ester derivatives in aqueous solution and in
2 plasma. The hydrolysis rate of the esters was remarkably increased in human plasma, but
3 the rate of hydrolysis was significantly decreased, or none, in buffer solution with
4 increased length of the acyl side chain from the methyl to the pentyl. Thus, it offers
5 flexibility to design hypoxia tracers with optimized physicochemical and
6 pharmacokinetic characteristics using ^{18}F -labeled nitroimidazole aliphatic esters by
7 controlling the hydrolysis rate via regulating length of the acyl side chain. This might
8 maintain a balance between an ester acyl chain length and its hydrolysis rate, which may
9 lead to optimal tracers for hypoxia imaging. In an attempt to control the in vivo
10 hydrolysis and maintain the hypoxic uptake towards tumor cells envision new
11 nitroimidazole ester derivatives may be a reasonable starting point for designing better
12 hypoxic imaging agents.

13 In this work, we have developed two new nitroimidazole derivatives,
14 2-fluoropropionic acid 2-(2-nitro-imidazol-1-yl)-ethyl ester (FNPFT, [^{19}F]**5**), and
15 2-fluoropropionic acid 2-(2-methyl-5-nitro-imidazol-1-yl)-ethyl ester (FMNPFT, [^{19}F]**8**),
16 which containing 2-fluoropropionyl ester group without changing the hypoxia-targeting
17 nitroimidazole group. Reported herein is the synthesis of [^{18}F]NPFT ([^{18}F]**5**) and
18 [^{18}F]MNPFT ([^{18}F]**8**) (Figure 1), and evaluation of their potentiality as hypoxia imaging
19 agents by measuring their stability in vitro, partition coefficient, tumor cell uptake, and
20 biodistribution/Micro PET imaging in EMT-6 tumor-bearing mice.

1 Experimental Section

2 *General*

3 *Reagents and solvents*

4 The precursor used for preparation of [¹⁸F]FMISO,
5 1-(2-nitro-10-imidazolyl)-2-O-tetra-hydropyranyl-3-O-toluenesulfonylpropane-diol
6 (NITTP), was purchased from Huayi Chemicals Co., Ltd. (Changshu, Jiang Su, China).
7 Other reagents and solvents were of analytical reagent grade and purchased from
8 commercial sources (Aldrich, Acros, or Alfa Inc.), and were used without further
9 purification unless otherwise specified.

10 *Instrument and consumables materials*

11 Thin-layer chromatography (TLC) was run on pre-coated plates of silica gel 60
12 F254 (Merck, Darmstadt, Germany). ¹H NMR spectra were recorded on a 400 MHz
13 Bruker Advance spectrophotometer (Bruker Co., Germany), ¹³C NMR spectra were
14 recorded on a 600 MHz JMTC-600/54/JJ (Japan Superconductor Technology, Inc.,
15 Japan), and the chemical shifts were reported as δ values (parts per million) relative to
16 residual protons of deuterated solvent. Coupling constants are reported in Hertz (Hz). The
17 multiplicity is defined by s (singlet), d (doublet), t (triplet), br (broad), and m (multiplet).
18 Melting points were measured on an X-5 melting point apparatus. Mass spectrometric
19 detection was performed in the positive ion mode on a Micromass Quattro micro API

1 mass spectrometer (Waters, Milford, MA) with an electrospray ionization (ESI) source
2 and high-resolution mass spectrometry (HRMS) data was registered by an Agilent (Santa
3 Clara, CA) G3250AA LC/MSD TOF system. Solid-phase extraction cartridges (Oasis
4 HLB (3cc) cartridge, Sep-Pak light QMA cartridge, neutral Al₂O₃ cartridge and Sep-pak
5 C-18 cartridge) were obtained from Waters (Milford, MA, USA). The [¹⁸F]fluoride ion
6 was produced by Peking University Cancer Hospital.

7 *Animals*

8 Animal studies were performed in BALB/c female mice (weight, 18 ± 2 g)
9 bearing EMT-6 tumors (purchased from Cancer Hospital Chinese Academy of Medical
10 Sciences, Beijing, China), which grew to right upper limb diameter of 10–15 mm. Male
11 Sprague–Dawley rats, 6–7 weeks old, 180–220 g, were obtained from Vital River
12 Laboratory Animal Co. Ltd (Beijing, China). All the animals were maintained according
13 as the Chinese government guidelines for care and use of laboratory animals.

14 *Synthesis*

15 *1-(2-(tert-Butyldimethylsilyloxy)ethyl)-2-nitro-1H-imidazole (2)*

16 A mixture of **1** (313 mg, 2.77 mmol), (2-bromoethoxy)(tert-butyl)dimethylsilyl-lane
17 (892 mg, 3.73 mmol) and potassium carbonate (K₂CO₃) (404 mg, 2.92 mmol) in 5 mL N,
18 N-dimethylformamide (DMF) was stirred at 100°C for 4 h. The mixture was then diluted
19 with 15 mL ethyl acetate (EtOAc) and washed by saturated solution of brine (10 mL × 3).

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1 The organic layers were dried by anhydrous Na₂SO₄ and filtered. The filtrate was
2 concentrated, and the residual crude product was purified by flash chromatography
3 (EtOAc/hexane: 3/7) to give 696 mg white solid **2** (yield: 97%): ¹H NMR (400 MHz,
4 CDCl₃) δ: 7.21 (s, 1 H), 7.20 (s, 1 H), 4.61 (t, *J* = 4.9 Hz, 2 H), 4.01 (t, *J* = 4.9 Hz, 2 H),
5 0.89 (s, 9 H), 0.10 (s, 6 H).

6 *2-(2-Nitro-1H-imidazol-1-yl)-ethanol (3)*

7 To a solution of **2** (796 mg, 2.93 mmol) in 5 mL tetrahydrofuran (THF) was
8 added 5 mL HCl solution (0.5 mL 1% HCl in 4.5 mL ethanol) dropwise at room
9 temperature. After 3 h, the mixture was cooled to 0°C and neutralized with 10% Na₂CO₃.
10 The aqueous layer was extracted with dichloromethane (20 mL × 3). The organic layers
11 were dried by anhydrous Na₂SO₄ and filtered. The filtrate was concentrated, and the
12 residual crude product was purified by flash chromatography (EtOAc/hexane: 3/7) to
13 give 356.4 mg yellow solid **3** (yield: 70%): ¹H NMR (400 MHz, DMSO) δ: 7.61 (s, 1 H),
14 7.16 (s, 1 H), 5.01 (t, *J* = 5.4 Hz, 2 H), 3.70 (t, *J* = 5.24 Hz, 2 H), 3.33 (s, 1 H).

15 *2-Fluoropropionic acid 2-(2-nitro-imidazol-1-yl)-ethyl ester ([¹⁹F]**5**)*

16 2-Fluoropropionic acid (0.1 mL, 1.32 mmol) was dissolved in anhydrous DMF (5
17 mL), N,N-Diisopropylethylamine (DIPEA, 0.25 mL, 1.43 mmol),
18 1-Ethyl-(3-dimethylaminopropyl)carbodiimide hydrochloride (EDCI, 250 mg, 1.30
19 mmol), and 1-Hydroxybenzotriazole hydrate (HOBt, 180 mg, 1.33 mmol) were added
20 under ice-water bath conditions, then dropwise with the compound **3** (105 mg, 0.67

1 mmol). After 2 h, the ice-water bath was removed. After stirring overnight, the mixture
2 was diluted with 20 mL dichloromethane (DCM) and washed by saturated solution of
3 brine (10 mL × 3). The organic layers were dried by anhydrous Na₂SO₄ and filtered. The
4 filtrate was concentrated, and the residual crude product was purified by flash
5 chromatography (DCM/Methanol: 100/1) to give 139 mg yellow solid [¹⁹F]**5** (yield:
6 89.7%): Mp: 66.9–67.2°C. ¹H NMR (400 MHz, CDCl₃) δ: 7.18 (s, 1 H), 7.11 (s, 1 H),
7 4.90–5.08 (dq, 1 H), 4.77 (t, *J* = 5.06 Hz, 2 H), 4.60 (t, *J* = 5.04 Hz, 2 H), 1.50–1.58 (dd, 3
8 H). ¹³C NMR (600 MHz, CDCl₃) δ: 170.04, 169.89, 128.70, 126.79, 86.18, 84.96, 63.32,
9 48.77, 18.39, 18.24. HRMS (ESI) calculated for C₈H₁₁FN₃O₄ (M+H⁺), 232.0734; found,
10 232.0732.

11 *2-Bromo-propionic acid 2-(2-nitro-imidazol-1-yl)-ethyl ester (4)*

12 To a mixture of compound **3** (162 mg, 1.03 mmol) and triethylamine (0.4 mL,
13 2.88 mmol) in anhydrous DCM, bromopropionyl bromide (0.2 mL, 2.00 mmol) in
14 anhydrous DCM (2 mL) was added dropwise in 1 h. The reaction solution was then
15 stirred at room temperature overnight. H₂O (10 mL) was added and extracted with DCM
16 (10 mL × 2), and the organic layers were combined and dried over anhydrous Na₂SO₄,
17 filtered, the filtrate was evaporated and purified by flash chromatography (EtOAc/hexane:
18 2/3) to give product **4** (116 mg, yield: 38.7%) as a yellow oily liquid. ¹H NMR (400MHz,
19 CDCl₃) δ: 7.19 (s, 2 H), 4.75 (t, *J* = 7.44 Hz, 2 H), 4.34 (t, *J* = 6.91 Hz, 2 H), 4.10–4.15
20 (m, 1 H), 1.79–1.80 (d, *J* = 6.92 Hz, 3 H). ¹³C NMR (600 MHz, CDCl₃) δ: 169.81, 128.68,

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1 127.07, 63.81, 48.85, 39.32, 21.55. HRMS (ESI) calculated for $C_8H_{11}BrN_3O_4$ ($M+H^+$),
2 291.9933; found, 291.9926.

3 *2-Fluoropropionic acid 2-(2-methyl-5-nitro-imidazol-1-yl)-ethyl ester* ($[^{19}F]8$)

4 Compound $[^{19}F]8$ was prepared from 2-Methyl-5-nitroimidazole-1-ethanol (171
5 mg, 1 mmol), DIPEA (0.35 mL, 2 mmol), HOBt (270 mg, 2 mmol) and 2-fluoropropionic
6 acid (0.15 mL, 2 mmol), with the same procedure described for compound $[^{19}F]5$.
7 Compound $[^{19}F]8$: 146 mg yellow solid (yield: 59.6%); Mp: 71.0–71.5°C. 1H NMR (400
8 MHz, $CDCl_3$) δ : 7.98 (s, 1 H), 4.90–5.07 (dq, 1 H), 4.66 (t, $J = 5.04$ Hz, 2 H), 4.55 (t, $J =$
9 3.49 Hz, 2 H), 2.54 (s, 3 H), 1.49–1.57 (dd, 3 H). ^{13}C NMR (600 MHz, $CDCl_3$) δ : 170.12,
10 169.97, 133.41, 86.29, 85.07, 63.71, 45.06, 18.39, 18.24, 14.45. HRMS (ESI) calculated
11 for $C_9H_{13}FN_3O_4$ ($M+H^+$), 246.0890; found, 246.0885.

12 *2-Bromo-propionic acid 2-(2-methyl-5-nitro-imidazol-1-yl)-ethyl ester* (**7**)

13 To a mixture of 2-Methyl-5-nitroimidazole-1-ethanol (177 mg, 1.01 mmol) and
14 triethylamine (0.4 mL, 2.88 mmol) in anhydrous DCM, bromopropionyl bromide (0.2 mL,
15 2.00 mmol) in anhydrous DCM (2 mL) was added dropwise in 1 h. The reaction solution
16 was then stirred at room temperature overnight. H_2O (10 mL) was added and extracted
17 with DCM (10 mL \times 2), and the organic layers were combined and dried over anhydrous
18 Na_2SO_4 , filtered, the filtrate was evaporated and purified by flash chromatography
19 (EtOAc/Petroleum ether: 2/1) to give product **7** (169 mg, yield: 55.4%) as a yellow oily
20 liquid. 1H NMR (400 MHz, $CDCl_3$) δ : 7.91 (s, 1 H), 4.57 (t, $J = 3.12$ Hz, 2 H), 4.45 (t, J

1 = 4.52 Hz, 2 H), 4.20–4.26 (q, 1 H), 2.50 (s, 3 H), 1.71 (d, $J = 6.92$ Hz, 3 H). ^{13}C NMR (600 MHz, CDCl_3) δ : 169.88, 151.21, 133.45, 64.09, 44.99, 39.12, 21.58, 14.72. HRMS (ESI) calculated for $\text{C}_9\text{H}_{13}\text{BrN}_3\text{O}_4$ ($\text{M}+\text{H}^+$), 306.0089; found, 306.0085.

4 *Radiolabeling*

5 *Preparation of [^{18}F]1-(2-nitro-1-imidazolyl)-3-fluoro-2-propanol ([^{18}F]FMISO)*

6 The aqueous solution of the [^{18}F]fluoride ion produced by the cyclotron was
7 passed through a Sep-Pak light QMA cartridge, The cartridge was previously activated
8 with 10 mL 1 M NaHCO_3 and 10 mL water, as well as dried with argon. Then the ^{18}F
9 activity was eluted with 1.1 mL of Kryptofix 2.2.2 ($\text{K}2.2.2$)/ K_2CO_3 solution (11.0 mg
10 $\text{K}2.2.2$ and 2.0 mg K_2CO_3 in 0.93 mL acetonitrile and 0.17 mL H_2O). The eluent was
11 then evaporated at 100°C under an argon stream. Additionally, the residue was
12 azeotropically dried twice with 1.0 mL anhydrous acetonitrile at 100°C under an argon
13 stream. A solution of 1 mg precursor (NITTP) in 1 mL anhydrous acetonitrile was added
14 to the evaporation residue, and the mixture was heated at 100°C for 10 min, followed by
15 hydrolysis with 2 M HCl (1 mL) at 100°C for 10 min. After cooling down to room
16 temperature, 2 M NaOH (1 mL) was added to neutralize. The crude reaction mixture was
17 subsequently delivered to a neutral Al_2O_3 cartridge and a Sep-pak C-18 cartridge for
18 purification. [^{18}F]FMISO was trapped on the cartridge and eluted with 1 mL ethanol. The
19 pure product was diluted with saline to 10% ethanol solution, and then sterilized by

1 passing through a 0.22 μm sterile membrane. The structure of the purified product was
2 confirmed by HPLC with a gamma ray radio-detector and a UV detector at 320 nm, as
3 well as the radiochemical purity (RCP). The HPLC condition was as follow: Phenomenex
4 Gemini C18 (4.6 mm \times 250 mm, 5 μm), mobile phase: acetonitrile/H₂O 3/7 (V/V), 1
5 mL/min. The RCP was also measured by Radio-TLC, with a mobile phase
6 acetonitrile/H₂O 85/15.

7 *Preparation of [¹⁸F]5 and [¹⁸F]8*

8 [¹⁸F]KF/18-crown-6 complex was prepared as previously described for
9 [¹⁸F]FMISO. A solution of precursor 4 (2 mg) or precursor 7 (2 mg) in 1 mL acetonitrile
10 was added to the dried [¹⁸F]KF/18-crown-6 complex and heated at 80°C for 10 min. After
11 cooling down to room temperature, the reaction mixture was quickly diluted with 5 mL
12 buffer solution (pH = 6.40) containing 0.2 M disodium hydrogen phosphate and 0.1 M
13 citric acid, and subsequently passed through an Oasis HLB cartridge. The cartridge was
14 rinsed with 2 mL 10% ethanol/H₂O (V/V) and then eluted with 1 mL ethanol to obtain
15 [¹⁸F]5 or [¹⁸F]8. The pure product was diluted with saline to 10% ethanol solution, and
16 then sterilized by passing through a 0.22 μm sterile membrane. The structure and RCP of
17 the product was confirmed by HPLC with a gamma ray radio-detector and a UV detector
18 at 320 nm. The HPLC condition was as follow: Column was Phenomenex Gemini C18
19 (4.6 mm \times 250 mm, 5 μm), mobile phase: 0.1% Formic acid solution(A), acetonitrile (B),
20 1 mL/min with a gradient as shown below: from 0 to 3 min, A 99%, B 1%; from 3 to 10

1 min, gradient A 99-5%, B 1-95%; from 10 to 15 min, gradient A 5-80%, B 95-20%; from 15 to 18 min, gradient A 80-99%, B 20-1%. The RCP was also measured by Radio-TLC, with a mobile phase $\text{CH}_2\text{Cl}_2/\text{CH}_3\text{OH} = 9/1$.

4 *Preparation of 2-[^{18}F]FPA*

5 2-[^{18}F]FPA was prepared according to the method previously described.⁴⁶

6 *In vitro stability study*

7 The in vitro stability of [^{18}F]**5** and [^{18}F]**8** were examined by incubating in 1 mL saline for 2 h at room temperature, and the RCP was measured by Radio-TLC and Radio-HPLC using chromatographic conditions as previously described.

10 *In vitro metabolism studies in rat serum*

11 Rat blood was freshly drawn from an anesthetized SD rat into tubes. Centrifugation was performed at 5000 g for 5 min, and the supernatant was taken as rat serum. Incubations were carried out at 37 °C in a water bath. The hydrolysis reactions were initiated by adding [^{18}F]**5** or [^{18}F]**8** (~3 MBq), in 100 μL 10% ethanol solution to preheated blood samples (900 μL) or 10% ethanol solution (as control). Aliquots (100 μL) were taken from blood at 2, 5 and 10 min and were deproteinized by mixing with acetonitrile (200 μL). After centrifuging for 5 min at 14,000 rpm, 10 μL of the supernatant layer was analyzed by analytical HPLC using Phenomenex Gemini C18 column (4.6 mm \times 250 mm, 5 μm) with mobile phase consistent of 20 mM NaH_2PO_4 (A)

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1 and acetonitrile (B), a flow rate of 1 mL/min with a gradient as shown below: from 0 to 3
2 min, A 99%, B 1%; from 3 to 10 min, gradient A 99-5%, B 1-95%; from 10 to 15 min,
3 gradient A 5-80%, B 95-20%; from 15 to 18 min, gradient A 80-99%, B 20-1%.

4 *Determination of the partition coefficient (log P)*

5 Log P was assessed by mixing radiotracer [^{18}F]5, [^{18}F]8 or [^{18}F]FMISO with
6 1-octanol and phosphate buffer (0.1 M, pH 7.4) system in a centrifuge tube. The tube was
7 shaken uniformly on a Vortex oscillator (Vortex-Genie 2) for 3 min and then centrifuged
8 at 5000 g for 5 min. Three samples (0.2 mL each) from the 1-octanol and buffer layers
9 were then measured for radioactivity. The partition coefficient was calculated as the
10 mean value of counts per minute in 1-octanol divided by that of the buffer. The
11 measurement was performed for three times, and the final partition coefficient value was
12 expressed as log P .

13 *In vitro cell uptake*

14 Cell uptake studies were evaluated using the murine mammary carcinoma cells
15 EMT6 cell lines, which were purchased from Cancer Hospital Chinese Academy of
16 Medical Sciences, Beijing, China. The cell was maintained (5% CO₂ incubator at 37°C)
17 in RPMI 1640 medium (purchased from Corning) containing 10% fetal bovine serum and
18 1% antibiotics mixture. The cells were dispersed in 20 mL fresh RPMI medium to
19 achieve final concentration of approximately 2×10^6 cells/mL. Aliquots of 10 mL were

1 added into glass vials and incubated at 37°C with gentle magnetic stirring under
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3
4 normoxic (5% CO₂ plus 95% air) or hypoxic (5% CO₂ plus 95% N₂) atmosphere. In
5
6
7 addition, the cells were equilibrated for 60 min in either normoxic or hypoxic conditions,
8
9
10 then the radiotracer ([¹⁸F]FMISO, 2-[¹⁸F]FPA, [¹⁸F]**5** or [¹⁸F]**8**, 0.37 MBq/100 μL) was
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12
13 added to each glass vial and incubated for 30, 60, 120 and 240 min. 1 mL samples were
14
15
16 removed at each time point. From the samples, four aliquots (200 μL) were centrifuged at
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18
19 1500 rpm for 5 min to separate the cells from the supernatant. 90 μL of the supernatant
20
21
22 was removed for counting as A, and 110 μL of residue medium containing cells was
23
24
25 counted as B. The cell uptake was calculated as $C_{in}/C_{out}/10^6$ cells (the uptake in 10⁶ cells),
26
27
28 $C_{in}/C_{out} = (B - A)/A$. The cell viability was detected by trypan blue exclusion assay
29
30
31 during the whole procedure, and the viability of cells was more than 90%. Statistical
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34 analysis was performed using the Student's *t*-test (*n* = 3 at each time point).
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36 *Biodistribution studies*

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40 Biodistribution studies were assessed in BALB/c female mice bearing EMT-6
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43 tumor. 0.1 mL of radiotracer ([¹⁸F]**5** or [¹⁸F]**8**, ~1.11 MBq) was intravenously injected
44
45
46 into each mouse. Five mice for each time were sacrificed at 30, 90, and 120 min
47
48
49 post-injection. The organs or tissues (blood, brain, heart, lung, liver, spleen, kidney,
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52 stomach, bone, muscle, skin, and tumor) were collected, weighed and the corresponding
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55 radio-activities were assayed with a gamma counter. The results were expressed as the
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1 percent uptake of injected dose per gram of tissue (%ID/g) and presented as mean \pm SD.
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7 [18F]FMISO and 2-[18F]FPA were evaluated in the same animal model and used for
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9
10 comparison.

11 *Micro PET/CT imaging*

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15 PET imaging was performed on a Micro PET/CT scanner (Siemens Invenon MM)
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17
18 using BALB/c female mice bearing EMT-6 tumor. [18F]5, [18F]8, [18F]FMISO or
19
20
21 2-[18F]FPA (5.55–11.1 MBq/0.1 mL) was intravenously administered to mice via tail
22
23
24 vein. At 30, 60, 90 and 120 min post injection, mice were anesthetized with 2%
25
26
27 isoflurane inhalation, and fixed on the machine in a prone position. At each time point,
28
29
30 static imaging was obtained with 5 min CT scanning followed by 10 min PET. PET/CT
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32 Image was reconstructed with OSEM3D. Image analysis was carried out using Invenon
33
34
35 Research Workplace software.

36 37 *Statistical Analysis*

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41 Data were presented as mean \pm standard deviation (SD). All statistical tests were
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44 conducted using the IBM SPSS Statistics Version 20.0 for Windows (SPSS, Inc, IBM
45
46
47 Company). The independent samples nonparametric test was used to compare the
48
49
50 difference of 2 quantitative groups. Pearson product-moment correlation coefficient (r)
51
52
53 was used for correlation analysis between continuous variables. A P value of less than
54
55
56 0.05 was considered statistically significant.

1 **Results and discussion**

2 *Synthesis*

3 The radiolabeling precursor **4** and non-radioactive standard [¹⁹F]**5** were prepared
4 by reactions shown in the **Scheme 1**. Starting material **2** was synthesized by N-alkylation
5 of commercially available 2-nitroimidazole. The protecting group OTBDMS of
6 compound **2** was removed by treating with 1% HCl to obtain **3**. The acylation of
7 compound **3** with bromopropionyl bromide and 2-fluoropropionic acid, respectively,
8 produced the radiolabeling precursor **4** and non-radioactive standard [¹⁹F]**5**. The
9 radiolabeling precursor **7** and non-radioactive standard [¹⁹F]**8** were prepared by reactions
10 shown in the **Scheme 2**. Starting material **6** was purchased directly from commercial
11 sources. The acylation of compound **6** with 2-bromopropionyl bromide and
12 2-fluoropropionic acid, respectively, produced the radiolabeling precursor **7** and
13 non-radioactive standard [¹⁹F]**8**. These procedures yielded the desired products after
14 chromatographic isolation. All compounds were characterized by ¹H NMR, ¹³C NMR
15 and HRMS (Compound **2** and **3** were synthesized according to the previously reported
16 methods,⁴³ only ¹H NMR data were included). Results were consistent with proposed
17 structures.

18 *Radiolabeling*

19 *Preparation of [¹⁸F]FMISO*

1 The radiosynthesis of [^{18}F]FMISO was carried out according to the previously
2 reported methods.^{23, 40} [^{18}F]FMISO was synthesized from the precursor NITTP by a
3 nucleophilic substitution fluorination reaction followed by acid hydrolysis of alcohol
4 protecting group. The pure radiotracer of [^{18}F]FMISO was obtained by using a neutral
5 Al_2O_3 cartridge and a Sep-pak C-18 cartridge. The decay-corrected radiochemical yield
6 of [^{18}F]FMISO was $25 \pm 5\%$ ($n = 5$). The preparation took about 60 min. Radio-HPLC
7 and radio-TLC analysis showed that the RCP of [^{18}F]FMISO was more than 95%. The
8 radiochemical identity was confirmed by HPLC (see Supporting information, Figure S1)
9 ([^{18}F]FMISO = 3.9 min, [^{19}F]FMISO = 3.8 min).

10 *Preparation of [^{18}F]5 and [^{18}F]8*

11 [^{18}F]5 and [^{18}F]8 were synthesized from the corresponding bromo precursors 4
12 and 7 by the reactions shown in **Scheme 3**. The bromo precursors, 4 and 7, were reacted
13 with dried [^{18}F]KF/18-crown-6 complex in acetonitrile at 80°C for 10 min. The
14 radiotracers were purified with Oasis HLB cartridge and reformulated in 10%
15 ethanol/saline. The decay-corrected radiochemical yields of [^{18}F]5 was $11 \pm 2\%$ ($n = 5$),
16 and [^{18}F]8 was $13 \pm 2\%$ ($n = 5$). The synthesis time was about 45 min. Radio-HPLC and
17 radio-TLC analysis showed that the RCP of [^{18}F]1 and [^{18}F]2 were more than 95%. The
18 specific activity of [^{18}F]5 and [^{18}F]8 were 30 ± 2 GBq/ μmol ($n = 5$) and 61 ± 8 GBq/ μmol
19 ($n = 5$), respectively. The radiochemical identity was confirmed by HPLC (Supporting
20 information Figure S2 and Figure S3). ([^{18}F]5 = 13.5 min, [^{19}F]5 = 13.4 min; [^{18}F]8 =

1 13.6 min, [^{19}F]**8** = 13.4 min).

2 *Preparation of 2- ^{18}F FPA*

3 The radiosynthesis of 2- ^{18}F FPA was carried out according to the previously
4 reported methods. The decay-corrected radiochemical yields of 2- ^{18}F FPA was $37 \pm$
5 10% (n = 5). The synthesis time was about 60 min. Radio-HPLC analysis showed that the
6 RCP of 2- ^{18}F FPA was more than 95%.

7 *Determination of the partition coefficient (log P)*

8 The partition coefficient (between octanol and 0.1 M phosphate buffer, pH 7.4)
9 was conducted by the method described in experimental section. The log P was
10 calculated shown in Table 1. The log P of [^{18}F]**5** and [^{18}F]**8** were 0.42 and 0.63,
11 comparable to that of [^{18}F]FMISO (0.38). The values for all three agents were statistically
12 similar.

13 *In vitro stability study*

14 After incubating with saline up to 2 h after preparation, the radiochemical purities
15 of [^{18}F]**5** and [^{18}F]**8** were over 95% suggesting their great stability in vitro for further
16 investigation. These two tracers displayed excellent in vitro stability in saline.

17 *In vitro metabolism studies*

18 In vitro stability of these two tracers, [^{18}F]**5** and [^{18}F]**8**, were evaluated in the
19 presence of rat serum. The key difference between saline and rat serum is that in rat

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1 blood the tracers were exposed to various enzymes which might hydrolyze the ester
2 linkage. Measurement of potential radioactive metabolites and the rate of hydrolysis
3 kinetics were carried out after incubating the samples in rat blood at 37°C. The
4 percentages of unchanged [¹⁸F]**5** and [¹⁸F]**8** at different time points was shown in Table 2.
5 The percentage of intact parent compound [¹⁸F]**5** was 9.4% after incubating in rat blood
6 for 2 min, while [¹⁸F]**8** was 15.2%. After incubating for 10 min, both radiotracers [¹⁸F]**5**
7 and [¹⁸F]**8** were very closed to completely hydrolyzed. Furthermore, the radiolabeled
8 metabolite was more polar than the original parent radiotracers, which was likely the
9 expected product, 2-[¹⁸F]FPA, after the cleavage of the ester bond. (See Supporting
10 information Figure S4, Figure S5 and Figure S6)

11 Results of in vitro hydrolysis of [¹⁸F]**5** and [¹⁸F]**8** indicated that the rate of
12 hydrolysis of [¹⁸F]**5** was faster than that [¹⁸F]**8** in rat blood. Due to the existence of ester
13 groups in the radiotracers, it would be reasonable to suspect that esterases in the blood
14 might catalyze the hydrolysis of these two tracers. After the hydrolysis 2-[¹⁸F]FPA was
15 expected to be the major labeled compound in the circulating blood. It was known that
16 2-[¹⁸F]FPA also showed high tumor uptake in tumor models.⁴⁶ Therefore, 2-[¹⁸F]FPA
17 might be a major contributor to the observed uptake in EMT-6 tumor tissue in vivo.

18 *In vitro cell uptake*

19 In vitro cellular uptake of [¹⁸F]**5**, [¹⁸F]**8**, [¹⁸F]FMISO and 2-[¹⁸F]FPA (Figure 2A,

1 2B, 2C and 2D, respectively) in EMT-6 cells under hypoxic and normoxic conditions
2 were determined according to previous reported methods.⁴⁷⁻⁴⁹ This method of in vitro
3 study has been successfully validated in our laboratory in the evaluation of PEG-modified
4 nitroimidazole derivatives.⁵⁰ [¹⁸F]FMISO was used as a gold standard for comparison,
5 while 2-[¹⁸F]FPA as a negative control. As expected, [¹⁸F]FMISO (Figure 2C) showed a
6 significantly greater accumulation in EMT-6 cells after 1 h in hypoxic conditions ($P <$
7 0.01), while the uptakes of 2-[¹⁸F]FPA (Figure 2D) displayed no difference between
8 hypoxic cells and normoxic cells ($P > 0.05$). Under similar hypoxia conditions, cell
9 uptakes of [¹⁸F]**5** and [¹⁸F]**8** (Figure. 2A and 2B, respectively) showed initial increase and
10 follow by a small reduction at 2 h. Similar to that of [¹⁸F]FMISO, both [¹⁸F]**5** and [¹⁸F]**8**
11 showed significantly higher ($P < 0.05$) cellular uptakes under the hypoxia condition than
12 that under the normoxic condition at all time points. In contrast, 2-[¹⁸F]FPA (Figure. 2D)
13 displayed no difference between hypoxic and normoxic conditions. Results in Figure 2
14 both two new radiotracers displayed highly significant hypoxia selectivity in EMT-6
15 cells.

16 *Biodistribution studies*

17 Biodistribution of [¹⁸F]**5**, [¹⁸F]**8**, [¹⁸F]FMISO as well as 2-[¹⁸F]FPA were evaluated
18 in BALB/c mice implanted with EMT-6 tumor, which was commonly used as hypoxia
19 tumor model.⁵¹⁻⁵³ Results of biodistribution expressed as the percentage injected dose per

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1 gram tissue (%ID/g) for tissues of various organs of mice were presented in Tables 3.

2 Biodistribution study showed that [¹⁸F]**5** and [¹⁸F]**8** displayed a high uptake (%ID/g, n =

3 5) in all major organs (Table 3A, 3B and 3C). Specifically, the tumor uptakes of [¹⁸F]**5**

4 were 8.49 ± 0.72 , 8.89 ± 0.42 and 8.69 ± 0.78 %ID/g at 30, 60 and 120 min post-injection,

5 while [¹⁸F]**8** were 8.71 ± 0.81 , 9.03 ± 1.21 , 8.41 ± 0.93 %ID/g. Comparable tumor uptake

6 values were also observed for 2-[¹⁸F]FPA (tumor uptake was 8.61 ± 0.33 , 8.52 ± 0.51 and

7 7.95 ± 0.37 %ID/g at 30, 60 and 120 min post-injection. All three agents, [¹⁸F]**5** and

8 [¹⁸F]**8** and 2-[¹⁸F]FPA showed similar uptake in all major organs and the uptakes at 30,

9 60 and 120 min were remarkably similar. Lipophilicity (Table 1) appeared not to play a

10 role in tumor uptake. Since in vitro studies in the presence of blood showed that [¹⁸F]**5**

11 and [¹⁸F]**8** decomposed to 2-[¹⁸F]FPA via esterase hydrolysis, similar results of

12 biodistribution for these three agents suggested that the biodistribution in vivo might be

13 predominantly determined by the 2-[¹⁸F]FPA. The tumor uptake for [¹⁸F]FMISO was

14 4.41 ± 0.83 , 5.43 ± 0.62 and 3.24 ± 1.58 %ID/g at 30, 60 and 120 min, respectively, using

15 the same mice tumor model. Similar to the results above, at all three time points the

16 tumor uptakes showed no change. The tumor uptake for [¹⁸F]**5** and [¹⁸F]**8** and 2-[¹⁸F]FPA

17 showed noticeable higher tumor uptake (7.9 to 9.0 %ID/g) at all three time points than

18 those for [¹⁸F]FMISO (4.4 to 3.2 %ID/g) ($P < 0.05$); however, the blood levels for [¹⁸F]**5**

19 and [¹⁸F]**8** and 2-[¹⁸F]FPA were also higher leading to lower tumor to blood ratio when

20 compared to that of [¹⁸F]FMISO. Faster in vivo kinetics of [¹⁸F]FMISO also led to lower

1 uptake in retention in all major organs. However, it is likely that the in vivo
2 biodistribution of [^{18}F]**5** and [^{18}F]**8** was determined by a rapid in vivo hydrolysis to
3 possible metabolite, 2- ^{18}F FPA; therefore, the higher and selective hypoxic cell uptake
4 measured by in vitro cell uptake studies (Figure 2) were not observed in the in vivo
5 biodistribution study in EMT-6 mice model.

6 *Micro PET/CT imaging*

7 Using the same EMT-6 tumor-bearing mice micro PET images were acquired at
8 30, 60, 90, 120 min post-injection of [^{18}F]**5**, [^{18}F]**8**, 2- ^{18}F FPA and [^{18}F]FMISO,
9 respectively (Figure 3 and 4). PET images demonstrated that the EMT-6 tumors were
10 clearly visualized using either [^{18}F]**5** or [^{18}F]**8**, and the tumor uptakes for [^{18}F]**5**, [^{18}F]**8**
11 and 2- ^{18}F FPA were very comparable at 120 min post-injection (Figure 4). While
12 [^{18}F]FMISO displayed a lower tumor uptake and less uptake in all other major organs.
13 This is similar to the results of biodistribution study measured by dissection method.

14 Although results of higher tumor uptake in the PET images of [^{18}F]**5** and [^{18}F]**8**,
15 the tumors looked very distinctive (Figure 4); however, the tumor uptake observed
16 appeared to be associated with the metabolite, 2- ^{18}F FPA, which was likely a major
17 contributor in tumor uptake. Additional studies will be needed to see how much of the
18 original imidazole derivatives, if any, have contributed to the in vivo hypoxia tumor
19 uptake observed in the EMT-6 tumor model. The ester linkage may not be a useful linker

1 for 2-[¹⁸F]FPA in developing novel hypoxic targeting agents.

2 It has been reported that 2-[¹⁸F]FPA⁴⁶ accumulated in prostate cancers with high
3 tumor to background ratios, and it may be useful in the clinical diagnosis of prostate
4 cancer in humans. In general, ¹⁸F labeled fluoro-alkyl fatty acids⁵⁴ displayed tumor
5 uptakes. The mechanism(s) of uptake and their relationship with hypoxia conditions has
6 not been reported. Although, 2-[¹⁸F]FPA did not showed preference for in vitro tumor
7 cell uptake under hypoxia condition (Figure 2D). There is a hard lesson to be learned that
8 in vivo metabolism of these nitroimidazole ester derivatives, instead of the tumor hypoxia
9 condition, may be the driving force determining the outcome of in vivo biodistribution.

10 **Conclusions**

11 In summary, two new 2-fluoropropionic acid esters of nitroimidazole,
12 2-fluoropropionic acid 2-(2-nitro-imidazol-1-yl) ethyl ester, **5** and 2-fluoropropionic acid
13 2-(2-methyl-5-nitro-imidazol-1-yl) ethyl ester, **8** ([¹⁸F]**5** and [¹⁸F]**8**) have been
14 synthesized and evaluated as specific PET tracers for hypoxia imaging. In vivo
15 biodistribution results suggested that they were more likely reflecting predominance of in
16 vivo produced metabolite, 2-[¹⁸F]FPA, which formed after an iv injection.

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3 Development Program of China (2016YFC1306300) and Beijing Municipal Science &
4 Technology Commission (Z151100003915116).

5 **Supporting Information**

6 Supporting Information describing the HPLC profiles of [¹⁸F]FMISO, [¹⁸F]**5** and
7 [¹⁸F]**8** for this paper is available in a separate file.

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Table 1. The partition coefficient of [¹⁸F]**5** and [¹⁸F]**8**, compared with [¹⁸F]FMISO. Data were expressed as mean ± SD, n = 3.

Compound	log <i>P</i>
[¹⁸ F] 5	0.42 ± 0.02
[¹⁸ F] 8	0.63 ± 0.03
[¹⁸ F]FMISO	0.38 ± 0.08

Table 2. Percentages of unchanged radiotracers after incubation in rat blood in vitro. Changes of radiotracers were measured by Radio-HPLC. Data were expressed as mean ± SD, n = 3.

Radiotracer	Percentage of unchanged radiotracer (%)		
	2 min	5 min	10 min
[¹⁸ F] 5	9.42 ± 0.12	0.41 ± 0.12	0
[¹⁸ F] 8	15.23 ± 0.96	3.33 ± 0.80	1.84 ± 0.46

Table 3A Biodistribution of [¹⁸F]**5**, [¹⁸F]**8**, [¹⁸F]FMISO and 2-[¹⁸F]FPA in EMT-6 tumor-bearing mice at 30 min after tail vein injection. (%ID/g; mean ± S.D. n = 5)

Tissue	30 min			
	[¹⁸ F] 5	[¹⁸ F] 8	[¹⁸ F]FMISO	2-[¹⁸ F]FPA
Blood	9.45 ± 0.30	8.37 ± 0.75	4.60 ± 0.61	8.29 ± 0.69
Brain	4.85 ± 0.34	5.68 ± 0.33	4.34 ± 0.51	5.98 ± 0.55
Heart	8.10 ± 0.23	9.31 ± 0.77	6.35 ± 0.96	8.64 ± 1.54
Liver	6.95 ± 0.42	6.66 ± 0.52	7.31 ± 0.76	5.98 ± 0.73
Lung	6.99 ± 0.62	7.67 ± 0.43	6.85 ± 0.44	5.47 ± 0.21
Spleen	5.68 ± 0.37	6.18 ± 0.27	4.55 ± 0.59	5.64 ± 0.71
Kidneys	5.21 ± 0.31	5.32 ± 0.20	7.36 ± 0.45	4.87 ± 0.65
Stomach	5.05 ± 0.15	7.53 ± 0.55	5.66 ± 0.90	6.07 ± 1.27
Bone	3.58 ± 0.42	4.95 ± 0.61	3.33 ± 0.70	3.25 ± 0.27
Muscle	5.30 ± 0.27	6.41 ± 0.55	4.53 ± 0.54	6.13 ± 1.47
Skin	3.12 ± 0.24	5.13 ± 0.73	4.44 ± 0.83	5.10 ± 0.52
Tumor	8.49 ± 0.72	8.71 ± 0.81	4.41 ± 0.83	8.61 ± 0.33
Tumor-to-liver	1.18 ± 0.08	1.31 ± 0.09	0.63 ± 0.05	1.59 ± 0.02
Tumor-to-muscle	1.55 ± 0.16	1.38 ± 0.26	1.01 ± 0.14	1.40 ± 0.13

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Table 3B Biodistribution of [¹⁸F]5, [¹⁸F]8, [¹⁸F]FMISO and 2-[¹⁸F]FPA in EMT-6 tumor-bearing mice at 60 min after tail vein injection. (%ID/g; mean ± S.D. n = 5)

		60 min			
Tissue	[¹⁸ F]5	[¹⁸ F]8	[¹⁸ F]FMISO	2-[¹⁸ F]FPA	
Blood	8.69 ± 0.72	8.18 ± 0.77	3.46 ± 0.22	7.95 ± 0.78	
Brain	6.09 ± 0.45	6.09 ± 0.43	3.79 ± 0.26	5.63 ± 0.53	
Heart	8.61 ± 0.87	8.29 ± 0.71	5.61 ± 0.59	8.42 ± 1.09	
Liver	6.57 ± 0.32	6.14 ± 0.65	7.92 ± 0.54	5.71 ± 0.14	
Lung	7.29 ± 0.48	7.41 ± 0.51	5.95 ± 0.34	7.30 ± 0.83	
Spleen	6.17 ± 0.21	5.90 ± 0.69	3.60 ± 0.25	5.67 ± 0.48	
Kidneys	5.55 ± 0.26	5.01 ± 0.51	6.20 ± 0.44	5.11 ± 0.56	
Stomach	6.03 ± 0.38	5.71 ± 0.51	5.31 ± 0.43	5.71 ± 0.37	
Bone	5.54 ± 0.91	6.40 ± 0.81	4.51 ± 0.75	4.70 ± 0.65	
Muscle	5.84 ± 0.38	6.07 ± 0.59	3.80 ± 0.73	7.13 ± 0.92	
Skin	4.14 ± 0.43	5.01 ± 0.69	3.70 ± 0.26	5.37 ± 1.03	
Tumor	8.89 ± 0.42	9.03 ± 1.21	5.43 ± 0.62	8.52 ± 0.51	
Tumor-to-liver	1.35 ± 0.09	1.47 ± 0.14	0.69 ± 0.11	1.49 ± 0.06	
Tumor-to-muscle	1.47 ± 0.18	1.49 ± 0.18	1.50 ± 0.48	1.27 ± 0.22	
Tumor-to-blood	1.03 ± 0.10	1.10 ± 0.07	1.58 ± 0.28	1.12 ± 0.04	

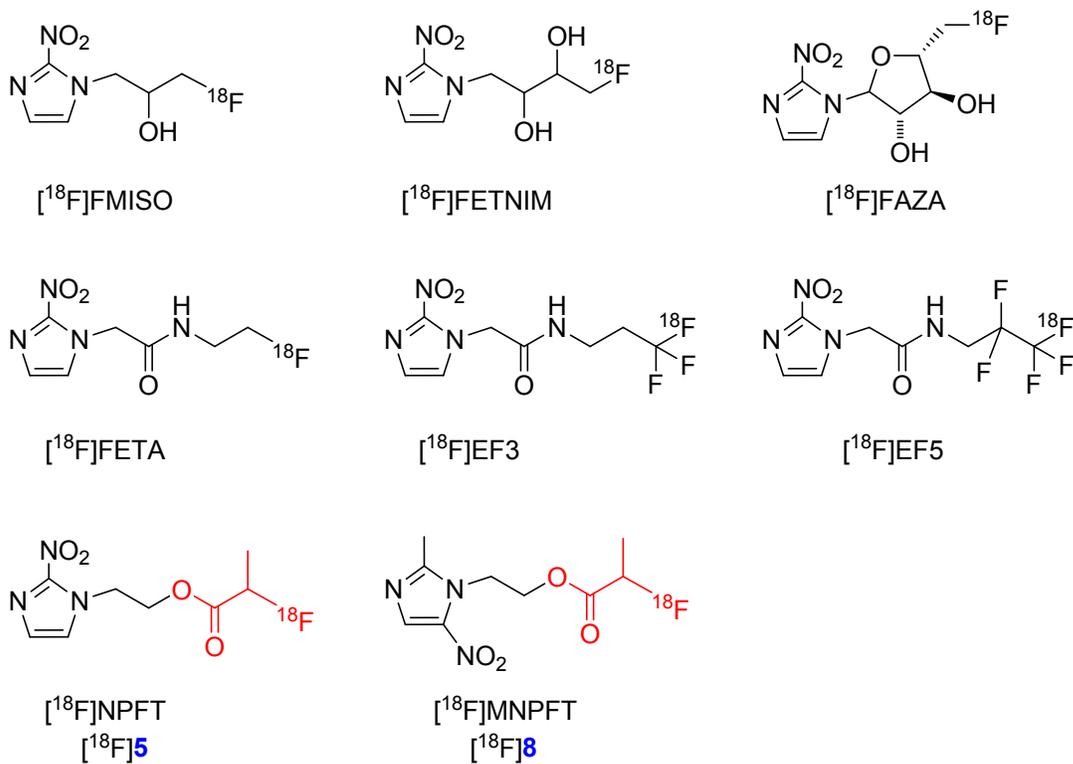
Table 3C Biodistribution of [¹⁸F]5, [¹⁸F]8, [¹⁸F]FMISO and 2-[¹⁸F]FPA in EMT-6 tumor-bearing mice at 120 min after tail vein injection. (%ID/g; mean ± S.D. * n = 5, ** n = 3)

		120 min			
Tissue	[¹⁸ F]5*	[¹⁸ F]8*	[¹⁸ F]FMISO**	2-[¹⁸ F]FPA*	
Blood	8.55 ± 0.45	7.76 ± 0.75	1.13 ± 0.35	7.67 ± 0.67	
Brain	7.46 ± 0.29	5.92 ± 0.72	1.33 ± 0.49	5.30 ± 0.61	
Heart	8.59 ± 0.82	8.33 ± 1.32	2.26 ± 0.76	7.68 ± 0.65	
Liver	6.59 ± 0.37	6.12 ± 0.92	3.85 ± 1.25	5.26 ± 0.14	
Lung	7.89 ± 0.55	7.52 ± 0.81	2.38 ± 0.84	7.34 ± 0.57	
Spleen	6.33 ± 0.41	6.03 ± 0.90	1.28 ± 0.49	5.43 ± 0.38	
Kidneys	5.30 ± 0.24	4.94 ± 0.68	2.33 ± 0.65	4.92 ± 0.49	
Stomach	5.20 ± 0.49	6.91 ± 0.36	2.96 ± 0.80	5.25 ± 0.76	
Bone	8.08 ± 0.18	9.25 ± 0.68	3.65 ± 1.42	8.68 ± 1.88	
Muscle	6.07 ± 0.72	6.11 ± 0.51	2.24 ± 0.72	6.53 ± 0.58	
Skin	4.76 ± 0.63	6.24 ± 0.51	2.20 ± 0.85	6.29 ± 0.64	

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Tumor	8.69 ± 0.78	8.41 ± 0.93	3.24 ± 1.58	7.95 ± 0.37
Tumor-to-liver	1.24 ± 0.03	1.37 ± 0.09	0.82 ± 0.12	1.51 ± 0.03
Tumor-to-muscle	1.23 ± 0.21	1.38 ± 0.07	1.45 ± 0.42	1.23 ± 0.14
Tumor-to-blood	1.00 ± 0.05	1.08 ± 0.05	2.79 ± 0.43	1.08 ± 0.02

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2 **Figure 1.** Various ¹⁸F-labeled PET-tracers based on nitroimidazole structure.

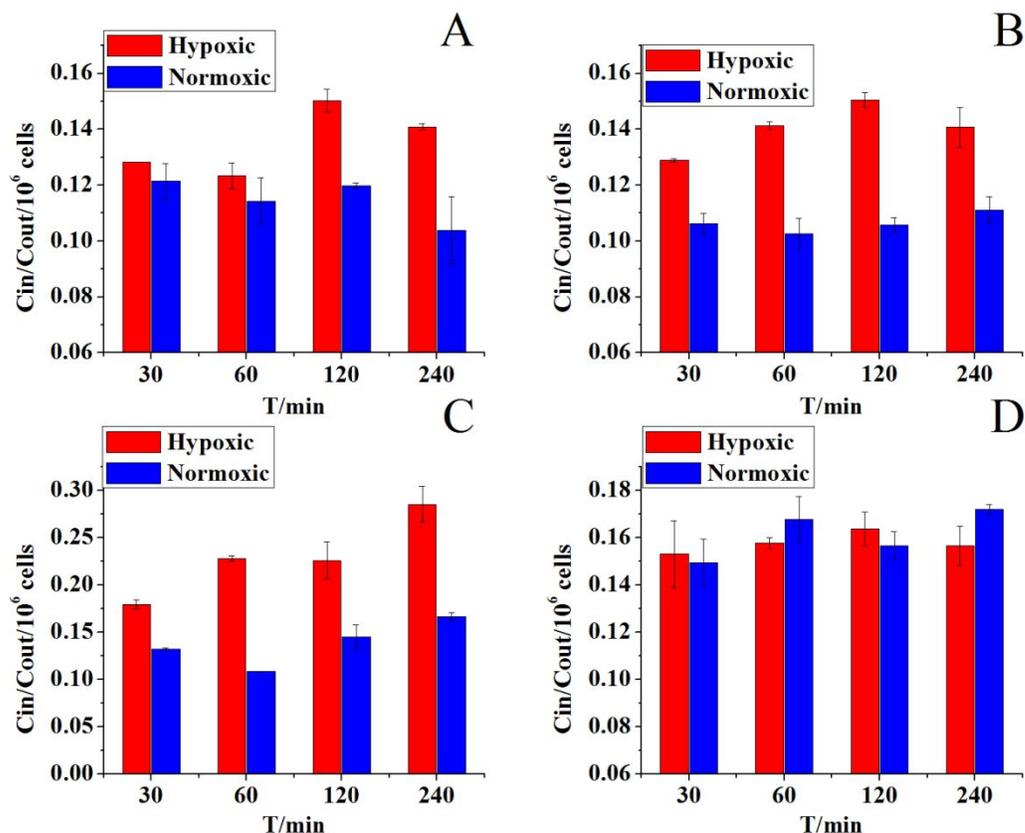
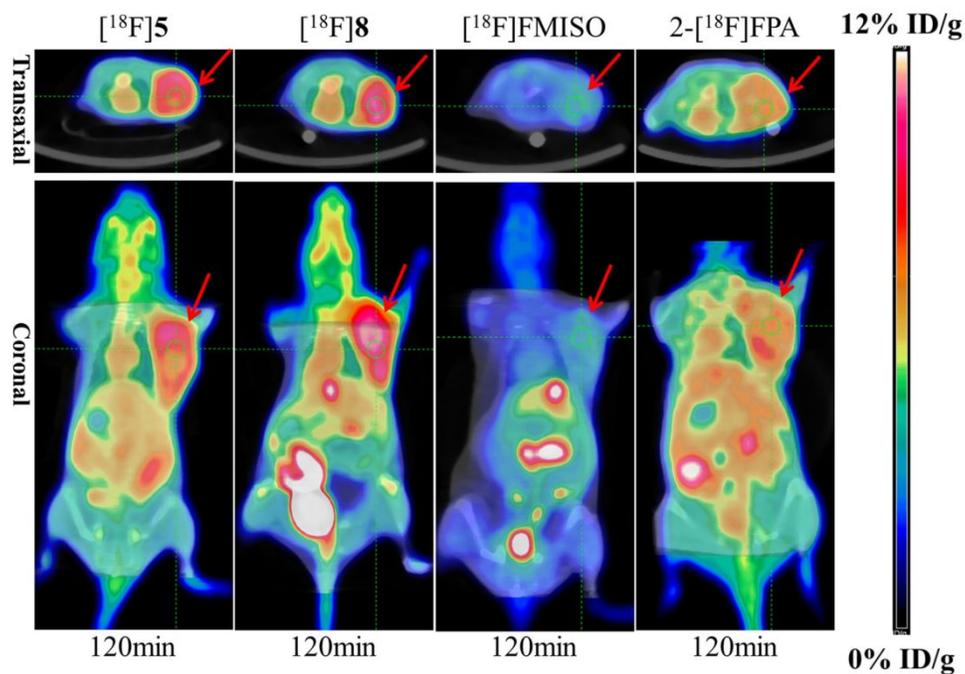
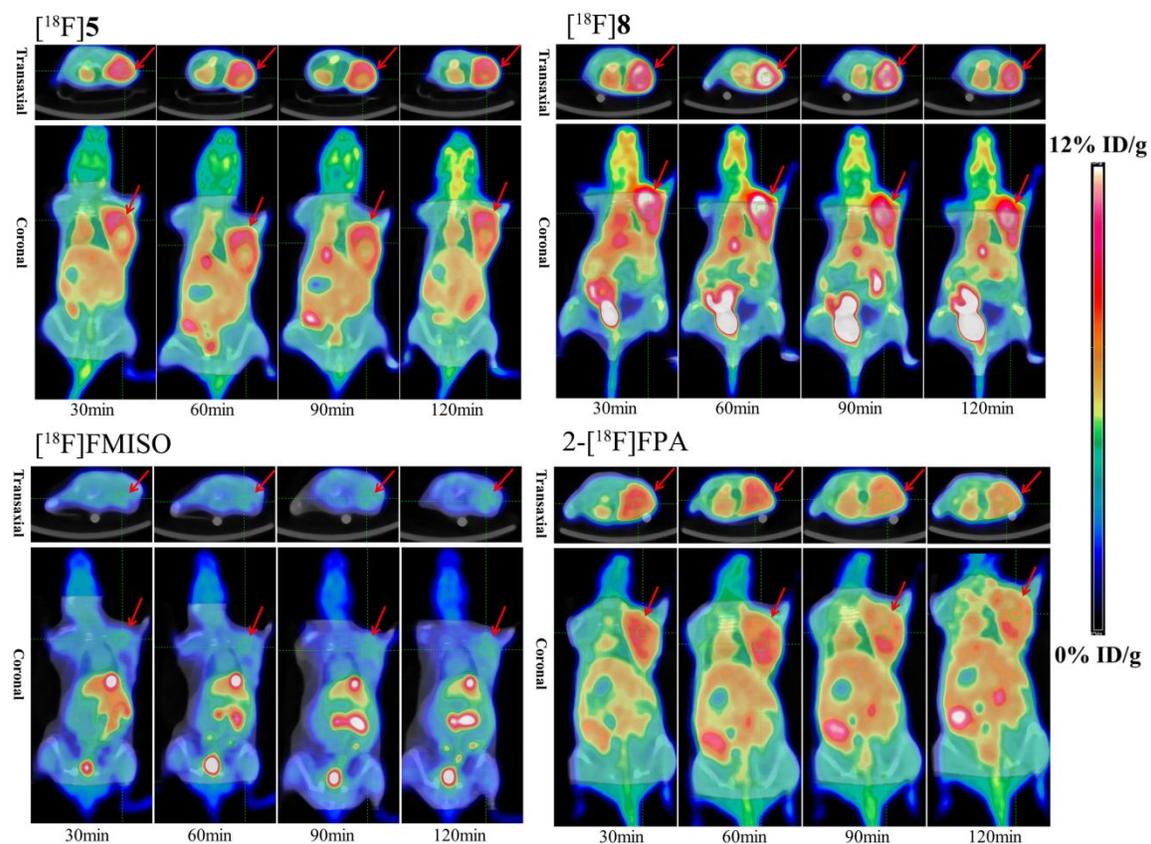


Figure 2. In vitro cell uptake (EMT-6 tumor cells) of [¹⁸F]5* (A), [¹⁸F]8** (B), [¹⁸F]FMISO** (C) and 2-[¹⁸F]FPA*** (D) under hypoxic (5% CO₂ plus 95% N₂) and normoxic (5% CO₂ plus 95% air) conditions after incubation for 30, 60, 120 and 240 min, respectively. Data are expressed as mean ± SD. (n = 3), *P*-values show comparisons of uptake under normoxic and hypoxic conditions (*t*-test): **P* < 0.05, ***P* < 0.01, ****P* > 0.05. In vitro cell uptake study as expected showed that [¹⁸F]5 (A), [¹⁸F]8 (B), [¹⁸F]FMISO (C) displayed highly significant hypoxia selectivity in EMT-6 cell, while 2-[¹⁸F]FPA (D) showed no difference in cell uptake between normoxic and hypoxic conditions.

New PET tracers for imaging hypoxia



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26 **Figure 3.** Transaxial and coronal PET/CT fusion images of $[^{18}\text{F}]5$, $[^{18}\text{F}]8$, $[^{18}\text{F}]FMISO$ and
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29 $2-[^{18}\text{F}]FPA$ at 120 min post-injection (5.55–11.1 MBq/0.1 mL per mouse via the tail vein) in BALB/c
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31 mice bearing EMT-6 tumor. The red arrows represent the location of tumors.
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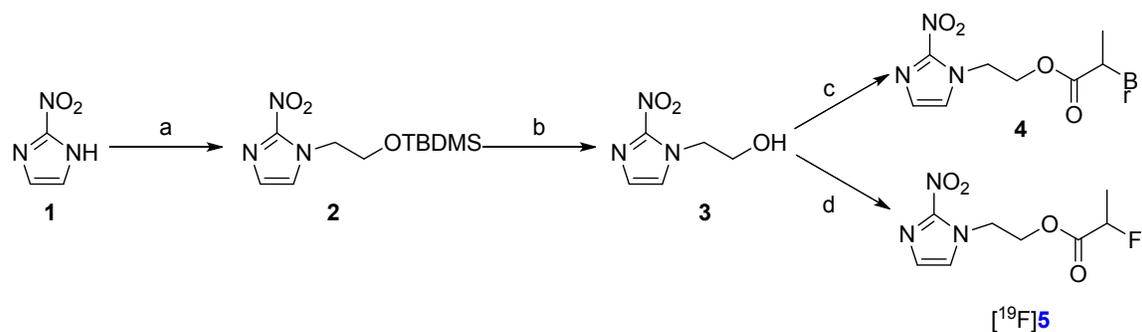


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2 **Figure 4.** Transaxial and coronal PET/CT fusion images of $[^{18}\text{F}]\mathbf{5}$, $[^{18}\text{F}]\mathbf{8}$, $[^{18}\text{F}]\text{FMISO}$ and
 3 $2\text{-}[^{18}\text{F}]\text{FPA}$ at 30, 60, 90 and 120 min post-injection (5.55–11.1 MBq/0.1 mL per mouse via the tail
 4 vein) in BALB/c mice bearing EMT-6 tumor. The red arrows represent the location of tumors.

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6 **Scheme 1. Synthesis of radiolabelling precursor 4 and non-radioactive standard $[^{19}\text{F}]\mathbf{5}$.**



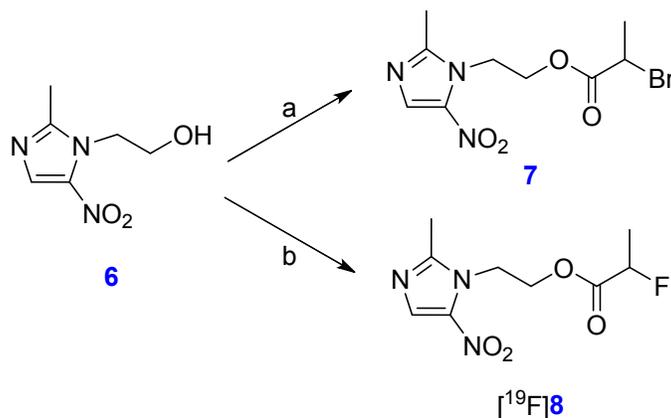
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8 Reagents and conditions: (a) $\text{BrCH}_2\text{CH}_2\text{OTBDMS}$, K_2CO_3 , DMF, 100°C , 4 h; (b) 1% HCl-ethanol,

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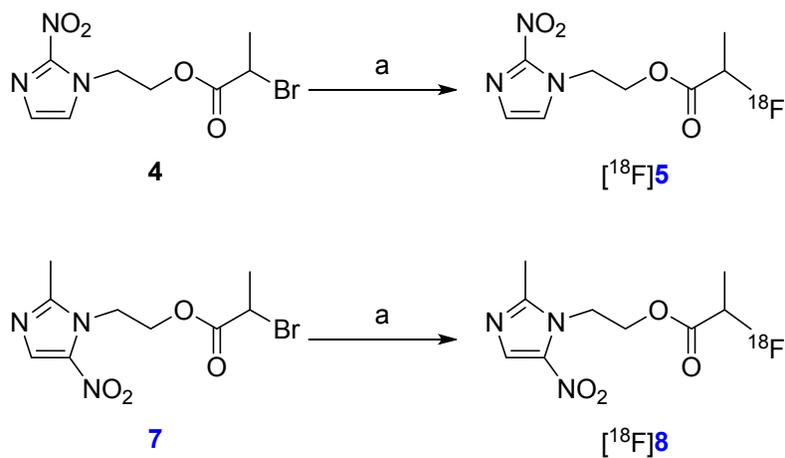
- 1 THF, rt, 3 h; (c) $\text{CH}_3\text{CHBrCBrO}$, Et_3N , DCM, rt, overnight; (d) $\text{FCH}(\text{CH}_3)\text{COOH}$, EDCI, HOBt,
2 DIPEA, DMF, 0°C , 2 h, then rt, overnight.

3 **Scheme 2. Synthesis of radiolabelling precursor 7 and non-radioactive standard [^{19}F]8.**



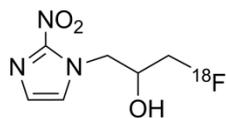
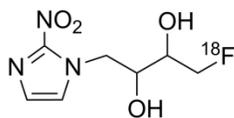
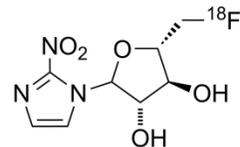
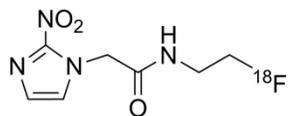
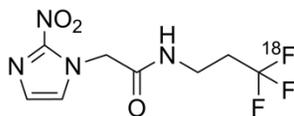
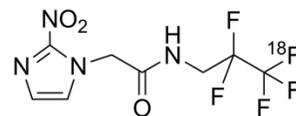
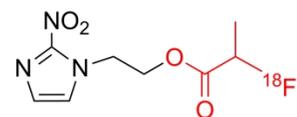
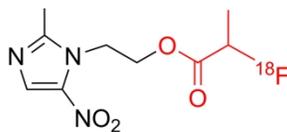
- 5 Reagents and conditions: (a) $\text{CH}_3\text{CHBrCBrO}$, Et_3N , DCM, rt, overnight; (b) $\text{FCH}(\text{CH}_3)\text{COOH}$, EDCI,
6 HOBt, DIPEA, DMF, 0°C , 2 h, then rt, overnight.

7 **Scheme 3. Radiosynthesis of [^{18}F]5 and [^{18}F]8.**

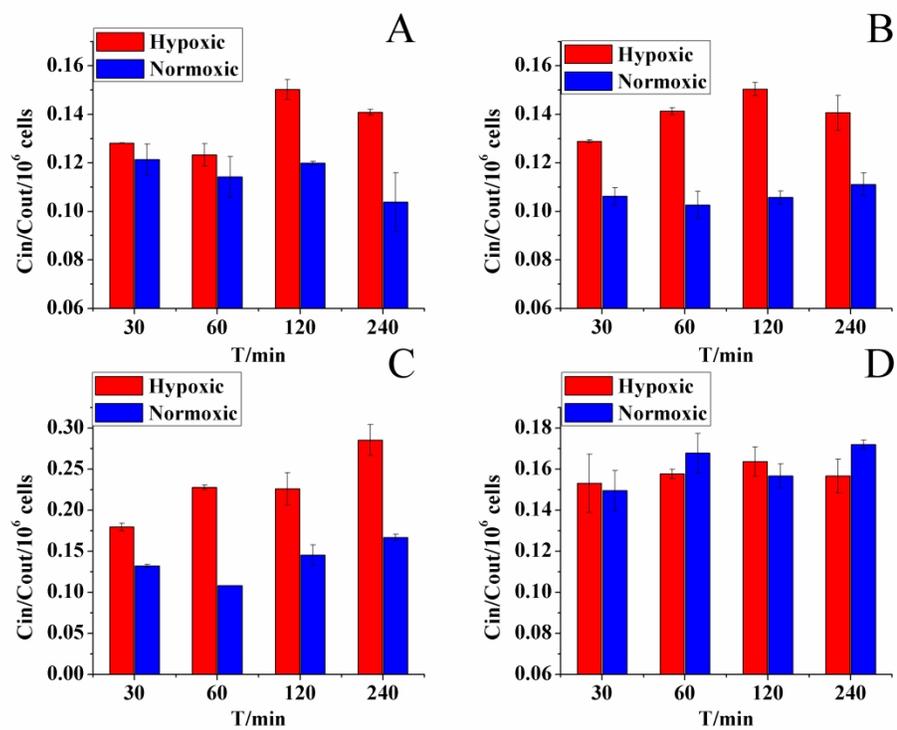


- 9 Reagents and conditions: (a) [^{18}F]KF/18-crown-6, KHCO_3 , acetonitrile, 80°C , 10 min.

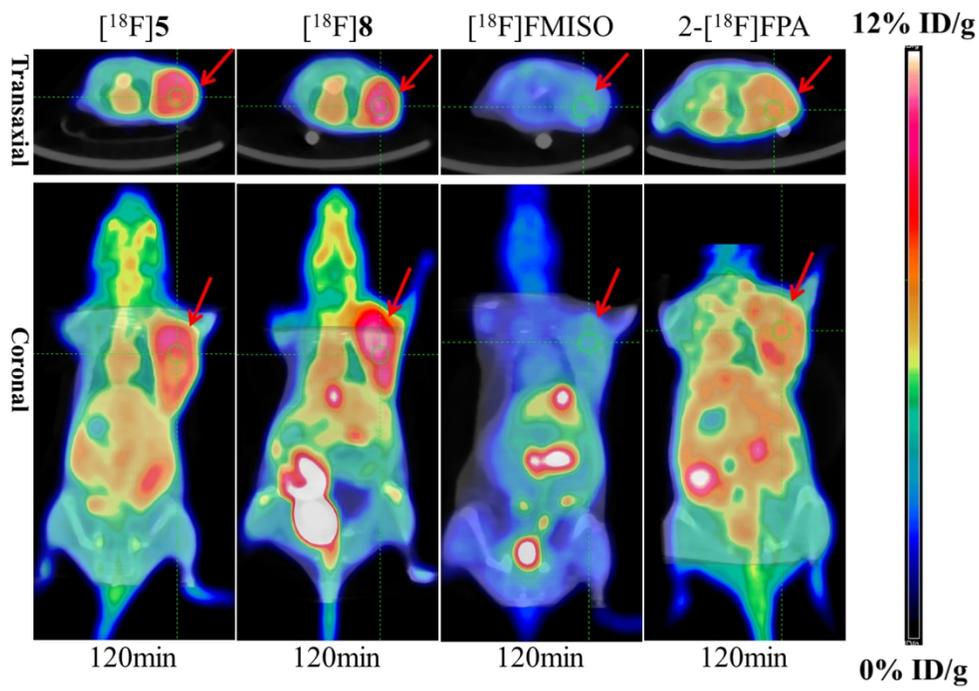
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 $[^{18}\text{F}]$ FMISO $[^{18}\text{F}]$ FETNIM $[^{18}\text{F}]$ FAZA $[^{18}\text{F}]$ FETA $[^{18}\text{F}]$ EF3 $[^{18}\text{F}]$ EF5 $[^{18}\text{F}]$ NPFT
 $[^{18}\text{F}]$ 5 $[^{18}\text{F}]$ MNPFT
 $[^{18}\text{F}]$ 8

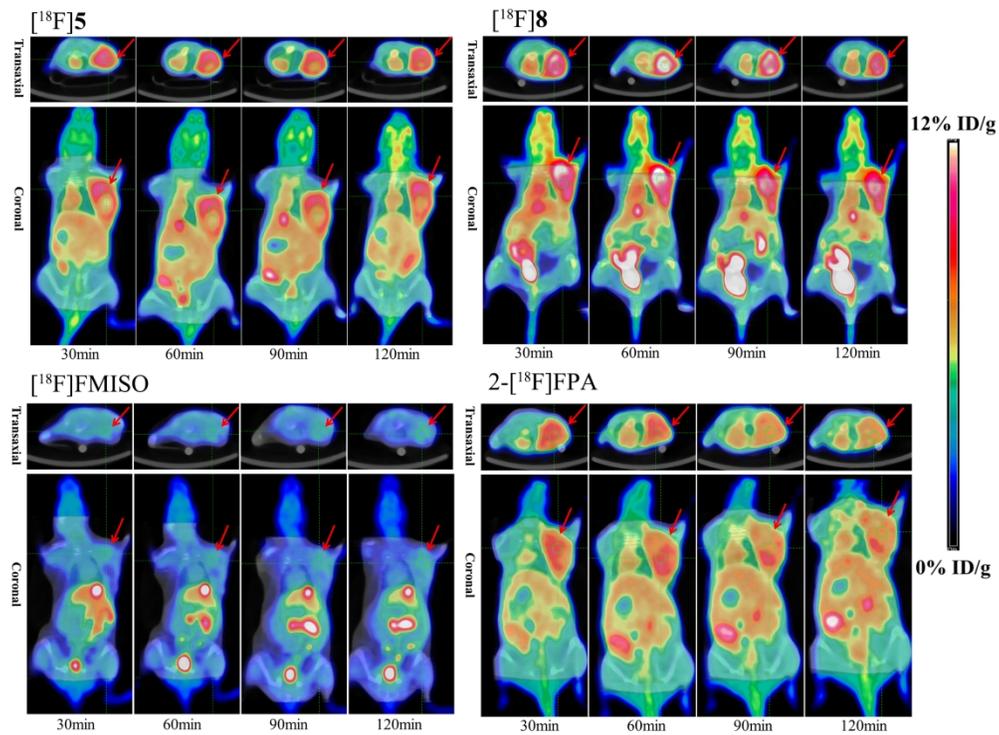
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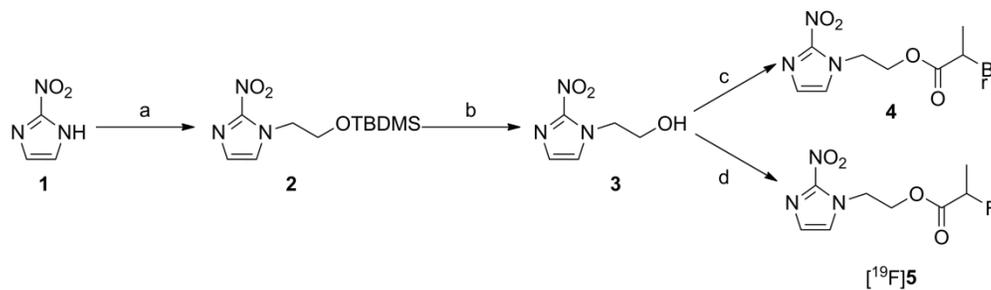
287x220mm (300 x 300 DPI)

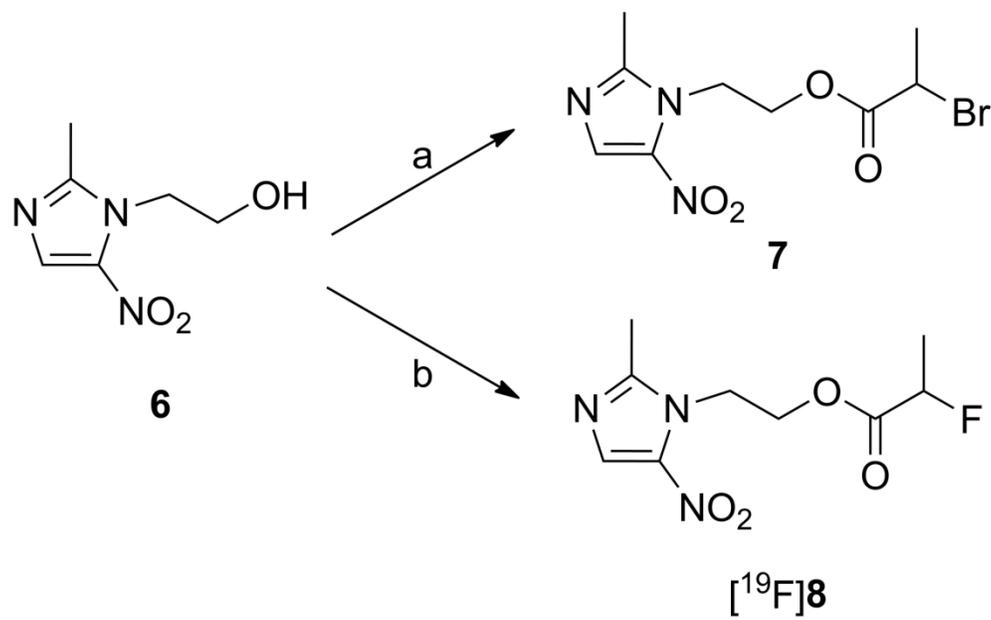


140x99mm (300 x 300 DPI)

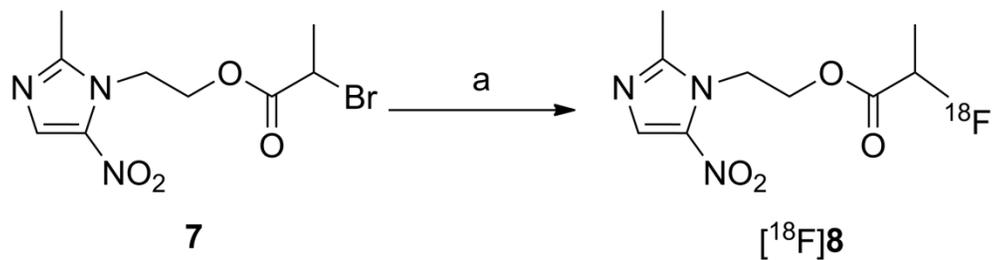
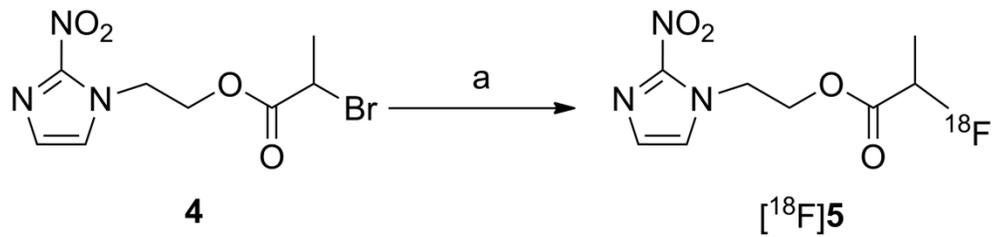


246x183mm (300 x 300 DPI)

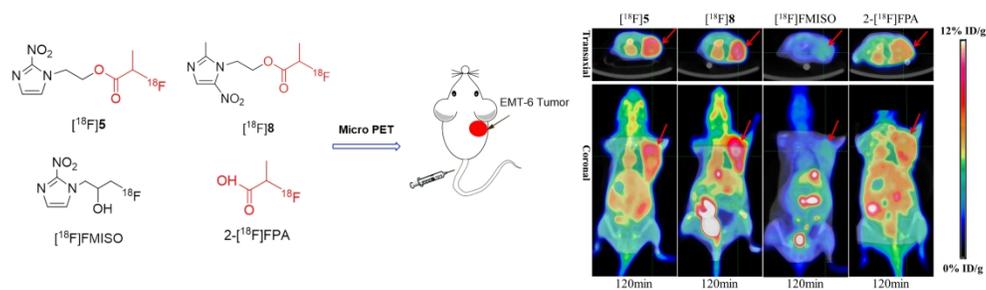




90x56mm (600 x 600 DPI)



104x61mm (600 x 600 DPI)

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