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Short communication

Synthesis of oligo(ethylene glycol) substituted phosphatidylcholines: Secretory PLA₂-targeted precursors of NSAID prodrugs

Renato Rosseto, Joseph Hajdu*

Department of Chemistry and Biochemistry, California State University, 18111 Nordhoff Street, Northridge, CA 91330-8262, USA

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ABSTRACT

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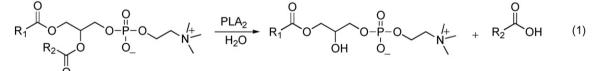
Keywords: Oligo(ethylene glycol) substituted phosphatidylcholines Phospholipase A₂-targeted precursor of prodrugs Non-steroidal anti-inflammmatory drugs Drug delivery methods A series of new phosphatidylcholine analogues with structurally modified *sn*-2-substituents have been prepared. The synthetic compounds include oligo(ethylene glycol) derivatives with chain-terminal pharmacophores that upon catalytic hydrolysis by phospholipase A₂ yielded a series of oligo(ethylene glycol)-conjugates of the respective drugs. The approach here outlined may open a new way to employ OEG derivatives of phospholipids for therapeutic applications as secretory PLA₂-targeted precursors of prodrugs.

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1. Introduction

Phospholipases A_2 (PLA₂'s, EC 3.1.1.4) comprise a large group of intracellular and secreted enzymes that catalyze the hydrolysis of the *sn*-2-ester bond of glycerophospholipids to yield free fatty acids such as arachidonic acid, and lysophospholipids (Burke and Dennis, 2009a, Eq. (1)): proliferation, survival and migration (Rivera and Chun, 2008; Zhao and Natarajan, 2009), while PAF is particularly involved in inflammatory processes (Prescott et al., 2000).

Secreted phospholipases A₂ (sPLA₂'s) are widespread in nature (Six and Dennis, 2000). Early studies have focused on members of the sPLA₂ family isolated from insect and snake venoms; more recently sPLA₂'s have been found in plants, bacteria,



R₁, R₂ = naturally occurring fatty acids

Both products are precursors for signaling molecules with a wide range of biological functions (Burke and Dennis, 2009b). Specifically, arachidonic acid is converted to eicosanoids that have been shown to be involved in immune response, inflammation, pain perception, and sleep regulation (Funk, 2001; Schaloske and Dennis, 2006), while lysophospholipids are precursors of lipid mediators such as lysophosphatidic acid (LPA) and platelet activating factor (PAF). Lysophosphatidic acid has been shown to be involved in cell fungi, viruses, and mammals (Boyanovski and Webb, 2009). The mammalian family of secreted phospholipase A_2 enzymes consists of 12 different members at the present (Rouault et al., 2007). Isolated from the variety of sources, the sPLA₂'s share a series of common structural features. They are small, secreted proteins (14–18 kDa), with a compact structure usually containing 5–8 disulfide bonds (Fuentes et al., 2002). Studies focusing on their mechanism of action have shown that an active site histidine in close proximity to a conserved aspartate are the residues involved in the catalytic reaction, with absolute dependence on Ca²⁺ for activation (Scott et al., 1990).

^{*} Corresponding author. Tel.: +1 818 677 3377; fax: +1 818 677 2912. *E-mail address:* joseph.hajdu@csun.edu (J. Hajdu).

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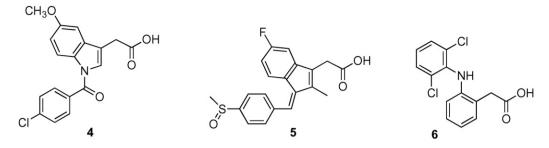


Fig. 1. The structures of NSAIDS's used in the syntheses: indomethacin 4, sulindac 5, and diclofenac 6.

At the present there is a growing interest in elucidation of the in vivo biological functions of mammalian sPLA₂'s, since they have been implicated in a series of physiological and pathophysiological functions including lipid digestion, signal transduction, prostaglandin biosynthesis, cell proliferation, neurosecretion (Burke and Dennis, 2009b), antibacterial defense (Nevalainen et al., 2008), inflammatory diseases (Nevalainen et al., 2000) and cancer (Dong et al., 2006). In this context, secretory phospholipase A₂ enzymes have recently been targets for a therapeutic application, as elevated levels of one subtype, sPLA₂-IIA, were observed in the microenvironment surrounding tumors in human colorectal adenocarcinomas (Abe et al., 1997; Kennedy et al., 1998; Mounier et al., 2008), and in neoplastic prostate tissue (Graff et al., 2001; Menschikowski et al., 2008). The high levels of sPLA₂ in tumors prompted the design of a tumor-activated drug delivery system in the form of sPLA₂ degradable liposomes, transporting conventional therapeutics that were released at the tumor site using sPLA₂ as a tumor-specific trigger (Davidsen et al., 2003).

In this communication we report a new approach to develop $sPLA_2$ -directed therapeutically applicable synthetic phospholipid analogues. We have designed a series of structurally modified phosphatidylcholine analogues incorporating oligoethylene glycol-substituted *sn*-2-ester functions. Relying on the minimum structural requirements for catalytic hydrolysis by the enzyme (Kuipers et al., 1990), including the presence of an essential α -methylene group adjacent to the *sn*-2-ester carbonyl of the substrate, replacement of the hydrocarbon portion of the naturally occurring fatty acid chain with an oligoethylene glycol group appeared to be a promising modification to qualify for catalytic cleavage by sPLA₂ enzymes.

2. Results and discussion

2.1. Design of the synthetic target compounds

In designing the synthetic phospholipid analogues we sought to develop PLA2-directed precursors of oligoethylene glycolconjugated pharmacophores to be released as prodrugs upon catalytic hydrolysis by the enzyme. Specifically, it has been shown recently, that oligoethylene modification of therapeutic agents, much like PEGylation using their high-molecular weight polymeric counterparts (Veronese and Pasut, 2005), greatly improves the pharmacokinetic profiles and targeting of drugs (Marsac et al., 2006). These benefits include: (1) increase in solubility to achieve better bioavailability, (2) resistance to proteolytic degradation, (3) reduction in immunogenicity and antigenicity, and (4) prolonged plasma circulation time (Harris and Chess, 2003; Juillerat-Jeanneret and Schmitt, 2007; Marcus et al., 2008). Furthermore, oligomeric PEG analogues (OEGs) are readily derivatized for site-selective targeting, and they are also amenable to a wide range of structural modification including construction of linear or branched scaffolds (Bowen et al., 2007). To explore the feasibility of the approach we used indomethacin **4**, sulindac **5**, and diclofenac **6**, as these nonsteroidal anti-inflammatory drugs (NSAID) are subject of ongoing biochemical and pharmacological investigation (Fig. 1).

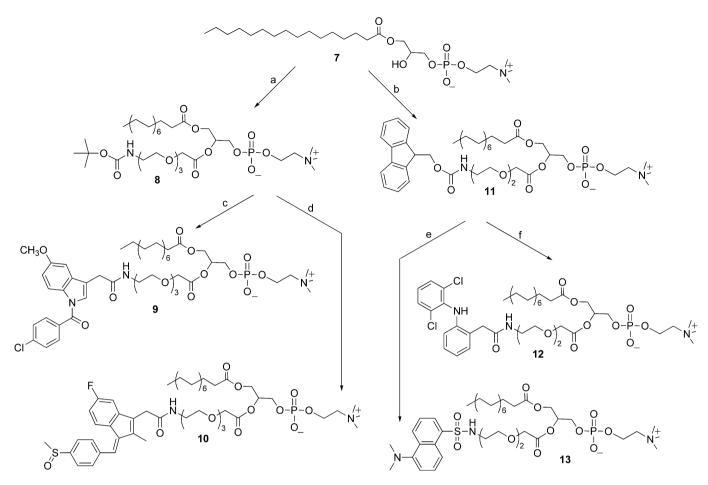
Specifically, in addition to their well-established inhibitory profiles against cyclooxygenases (Prusakiewicz et al., 2004; Felts et al., 2007; Blobaum and Marnett, 2007) non-steroidal antiinflammatory drugs have been found both in epidemiological and clinical studies to reduce the prevalence and severity of Alzheimer's disease (Veld et al., 2001; Gasparini et al., 2004), as inflammation exacerbates the pathology of that disease and other neurodegenerative diseases (Klegeris and McGeer, 2005). However, long-term use of NSAID's is limited by gastrointestinal and renal toxicity of these drugs. Attempts to mitigate the toxic side effects include development of improved delivery systems such as sustained release strategies with the use of prodrugs (Dahan and Hoffman, 2007).

2.2. Syntheses

The synthesis of the target compounds shown in Scheme 1 relied on the following key elements: (1) introduction of the oligoethylene glycol ester at the *sn*-2-position incorporating a chain-terminal protected amino group, (2) activation of the NSAID's by preparation of the corresponding *p*-nitrophenyl esters, and (3) deprotection of the amino group, followed by attachment of the desired antiinflammatory drug. In implementing the synthesis we used a two-prong approach: of the commercially available orthogonally functionalized oligoethylene glycol building blocks we selected OEG-carboxylic acids using both acid-labile *t*-BOC *vs*. base-labile FMOC-protected amino groups to develop the best way for preparation of the target phospholipids.

For acylation of *sn*-1-palmitoyl lysophosphatidylcholine **7** we used the method that we recently developed for acylation of lysophospholipids: (1) increasing the surface of the reaction vessel, where the reaction is believed to take place, by addition of glass beads, and (2) preventing intramolecular acyl migration by keeping the temperature at 25 °C. Thus, we used sonication rather than stirring the reaction mixture and maintained the temperature at 25 °C by cooling the sonicated vessel in a circulatory water bath (Rosseto and Hajdu, 2005). Under these conditions the reactions reached completion in 6-8 h and the products were obtained in good yield, with high regioselectivity. Specifically, reaction of compound 7 with t-BOC protected 11-amino-3,6,9trioxaundecanoic acid with dicyclohexylcarbodiimide (DCC), in the presence of 4-dimethylaminopyridine (DMAP) as catalyst, produced the target compound 8 in 59% yield after purification on silica gel chromatography, while a similar reaction using the base-labile FMOC-protected 8-amino-3,6-dioxaoctanoic acid as acyl donor resulted in formation of compound 11 in 75% yield.

Acid-catalyzed deprotection of the chain-terminal amino group of compound **8** was carried out using 1.0 M anhydrous HCl solution in dioxane at room temperature for 2.5 h, and the resulting amine hydrochloride was isolated from the reaction mixture by freeze-



Scheme 1. Reagents and conditions: (a) (CH₃)₃OCONH(CH₂CH₂O)₃COOH/DCC/DMAP, CHCl₃, 25 °C; (b) FMOC-NH(CH₂CH₂O)₂COOH/DCC/DMAP, CHCl₃, 25 °C; (c) (i) 1.0 M HCl/dioxane, (ii) Et₃N/*p*-nitrophenyl indomethacin, CHCl₃, rt, 3 h; (d) (i) 1.0 M HCl/dioxane, (ii) Et₃N/*p*-nitrophenyl sulindac, CHCl₃, rt, 3 h; (e) (i) DBU/CHCl₃, rt, 1 h, (ii) dansyl chloride/Et₃N, rt, 1 h; (f) (i) DBU/CHCl₃, rt, 1 h, (ii) *p*-nitrophenyl dichlofenac/DMAP, 5 h, rt.

drying. Deprotonation with anhydrous triethylamine, followed by triethylamine catalyzed introduction of the desired pharmacophore *via* the corresponding *p*-nitrophenyl active-ester yielded the NSAID substituted phosphatidylcholines of indomethacin **9** and sulindac **10** in 92% and 97% yields, respectively.

In the second series, the FMOC protecting group of compound **11** was removed by DBU-catalyzed elimination reaction in chloroform at room temperature for 1 h, followed by acylation of the amino group in the same pot, without isolating the intermediate, using the *p*-nitrophenyl ester of diclofenac in the presence of DMAP as catalyst, to obtain the desired phosphatidylcholine **12** in 51% overall yield.

Finally, we have explored the use of the synthetic method here developed for preparation an oligoethylene glycol-substituted phosphatidylcholine analogue **13**, carrying a spectroscopically active reporter group at the *sn*-2-chain-terminal, shown in Scheme 1. Incorporation of fluorescent reporter groups into phospholipid analogues have been shown to be useful for both kinetic studies of lipolytic enzymes, as well as for providing a convenient way for *in vivo* tracking the fate of the carboxylic acid produced on the catalytic hydrolysis by PLA₂ enzymes (Feng et al., 2002).

2.3. Enzymatic hydrolysis

Catalytic hydrolysis of the synthetic phosphatidylcholine analogues **8–13** was carried out with bee-venom phospholipase A_2 , a widely used, readily available representative of the low-molecular weight secretory PLA₂ enzymes (Valentin et al., 2000).

In an assay system (Roodsari et al., 1999) containing Triton X-100-phospholipid mixed micelles, in the presence of catalytically essential Ca^{2+} , each one of the synthetic phosphatidylcholine compounds was completely hydrolyzed by the enzyme, yielding the corresponding lysophosphatidylcholine **7** and the series of oligoethylene substituted long-chain fatty acid analogues, including OEG-conjugated prodrugs of the NSAID's indomethacin, sulindac, and diclofenac (Fig. 2).

2.4. Discussion

The synthesis of the phospholipid analogues here reported provides a new way of employing oligoethylene glycol-substituted phosphatidylcholines as secretory phospholipase A_2 targeted precursors of NSAID prodrugs. Specifically, polyethylene glycol modification (PEGylation) of biomolecules such as proteins, peptides as well as other small-molecular therapeutic agents continues to be a method of growing interest for development of new strategies in drug delivery, diagnostics, and for modification of the physicochemical properties of the compounds. While it has been well established, that PEGylation of a therapeutic agent extends its half-life in circulation, decreases its immunogenicity and antigenicity, and alters the pattern of drug distribution, with the availability of functionalized short-chain oligomers of ethylene glycol (OPE's) new design strategies have become possible. Specifically, OPE's have been shown to be useful not only for improving drug delivery (Warnecke and Kratz, 2003), but also for preparation of membrane biosensors (Chen et al., 2000), and for modula-

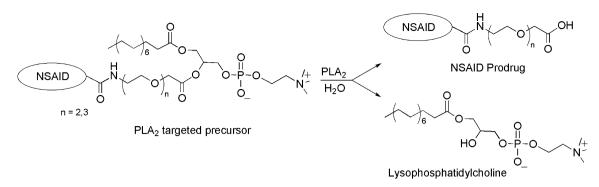


Fig. 2. The concept of using PLA2-targeted phospholipids as precursors of prodrugs.

tion of the physicochemical properties of membrane-targeted lipoproteins (Malolanarasimhan et al., 2007), opening the way toward the design of biomolecule analogues with targeted physical behaviors (Grogan et al., 2005). In addition, branched-chain OPE conjugates of peptides were used to incorporate fluorescent reporter groups to study receptor–ligand interactions, showing retention of the biological potency of the ligand (Bowen et al., 2007).

Preparation and phospholipase A₂ hydrolysis of compounds present a new approach to design of PLA2-targeted oligoethylene glycol conjugates of pharmacophores and other biomolecules. In contrast to earlier applications of PEGylated phospholipid derivatives with polymeric ethylene glycol substituents introduced at the polar headgroup (Zalipsky et al., 1999), the use of structurally well-defined oligoethylene glycol-substituted sn-2-chain here reported, offers improved targeting, flexibility in design of oligomeric linkers, and applicability for introduction of various different therapeutically active pharmacophores as well. Specifically, while NSAID's have been shown to reduce the prevalence and severity of Alzheimer's disease, as well as cyclooxygenasedependent anti-inflammatory and neuroprotecting effects, their long-term use has been limited by the gastrointestinal and renal toxicity exhibited by the drugs (Dahan and Hoffman, 2007). Availability of compounds such as 9, 10, and 12 may lead to development of drug delivery systems relying on sPLA2-targeted release of the respective OEG-prodrug conjugates to circumvent the problem

Finally, the approach of sPLA₂-directed drug delivery systems here illustrated may lead to design of precursors of OEG-prodrugs targeted at tissues with high levels of sPLA₂ enzymes. Significantly, elevated levels of secretory phospholipase A₂'s have been found in a number of tissues under pathological conditions such as prostate and colorectal cancers (Menschikowski et al., 2008; Mounier et al., 2008), atherosclerosis (Bostrom et al., 2007; Kimura-Matsumoto et al., 2008), rheumatoid arthritis, and coronary heart disease (Khuseyinova et al., 2005; Nijmeijer et al., 2008). Thus, the approach here presented may open the way to employ new strategies involving PLA₂-aided tissue specific drug delivery for the development of improved treatments of specific pathological conditions.

3. Experimental procedures

3.1. 1-Palmitoyl-2-(11'-N-t-BOC-amino-3,6,9trioxaundecanoyl)-sn-glycerophosphocholine (**8**)

To a suspension of 1-palmitoyl-2-hydroxy-*sn*-glycero-3-phosphocholine (0.4987 g, 1 mmol) in 25 mL of CHCl₃ were added 11-N-*t*-BOC-amino-3,6,9-trioxaundecanoic acid (0.7011 g, 1.43 mmol), DCC (0.5218 g, 2.5 mmol), DMAP (0.3120 g, 2.5 mmol)

and approximately 1 g of glass beads. The reaction was sonicated for 8 h at 25 °C. The solvent was then evaporated and the residue was purified on silica gel chromatography with CHCl₃/MeOH (4:1) to elute the impurities, followed by CHCl₃/MeOH/H₂O (65:25:4) to isolate the phospholipid. The fractions corresponding to the product were combined and freeze-dried from benzene to give 8 (0.5721 g, 59%) as white solid. IR (CHCl₃): 3342, 1741 br, 1248 cm^{-1} . ¹H NMR (CDCl₃, 200 MHz) δ 0.84 (br t, 3H), 1.22 (br s, 24H), 1.40 (s, 9H), 1.56 (m, 2H), 2.24 (t, 2H, J=7.4 Hz), 3.27 (m, 2H), 3.33 (br s, 9H), 3.42 (t, 2H, J=9.9Hz), 3.65 (s, 4H), 3.67 (m, 4H), 3.75 (m, 2H), 3.88 (m, 2H), 4.13 (m, 2H), 4.30 (m, 4H), 5.03-5.30 (br m, 2H). ¹³C NMR (CDCl₃, 50 MHz) δ 14.03, 22.57, 24.76, 28.35, 29.08, 29.25, 29.44, 31.82, 33.94, 40.24, 54.26, 59.43, 62.51, 63.56, 66.21, 68.26, 70.09, 70.37, 70.69, 71.36, 80.73, 155.91, 169.93, 173.38, ³¹P NMR (CDCl₃, 160 MHz, pyrophosphate ref. ext.) $\delta = 1.28$. R_f (CHCl₃/MeOH/H₂O 65:25:4) 0.41. $[\alpha]_D^{20} + 4.7^\circ$ (c 0.98, CHCl₃/MeOH 4:1). Anal. Calcd for C₃₇H₇₃N₂O₁₃P H₂O 1/3CHCl₃: C, 52.09; H, 9.06; N, 3.25; Found: C, 52.00; H, 8.82; N, 3.39. MS MH+ C₃₇H₇₃N₂O₁₃PH Calcd: 785.4923, Found: 785.4916.

3.2. 1-Palmitoyl-2-(11'-N-indomethacincarboxylamino-3,6,9trioxaundecanoyl)-sn-glycerophosphocholine (**9**)

(i) Indomethacin p-nitrophenyl ester. To a solution of indomethacin (0.5011 g, 1.4 mmol) in 30 mL CHCl₃ were added *p*-nitrophenol (0.2102 g, 1.54 mmol), DCC (0.3203 g, 1.54 mmol) and DMAP (40 mg, 0.3 mmol). The reaction mixture was stirred for 1 h at room temperature. The DCC-urea was then filtered and the filtrate was evaporated to give the *p*-nitrophenyl ester of the drug; $R_f(CHCl_3)$ 0.43, which was suitable for use in the subsequent acylation step without further purification. (ii) Deprotection of the amino group of compound **2**. To a solution of **2** (0.2351 g, 0.24 mmol) in 20 mL 1,4-dioxane was added 4 M HCl (6 mL) in dioxane, and the mixture was stirred for 2.5 h at room temperature. A positive ninhydrin test confirmed the presence of the free amino group in the product near the origin on a TLC plate. The amine hydrochloride was freeze-dried from benzene to give a white solid. (iii) Coupling of the indomethacin active-ester with the chain-terminal amino group. The amine hydrochloride just obtained was dissolved in 10 mL CHCl₃ and the mixture was treated with excess triethylamine (0.3 mL, 2.1 mmol) to adjust the pH of the solution to about 9, followed by addition of indomethacin *p*-nitrophenyl ester (0.3 g, 0.63 mmol). The mixture was kept at room temperature for 3 h, when a negative ninhydrin test indicated that the reaction reached completion. The solution was loaded onto a silica gel column and chromatographed using first CHCl₃/MeOH (4:1), followed by CHCl₃/MeOH/H₂O (65:25:4). The fractions corresponding to the product were combined, evaporated, dispersed in benzene and freeze-dried to give **9** (0.2231 g, 92%) as pale-yellow solid. IR (CHCl₃): 3347, 1740 br, 1690 cm⁻¹; ¹H NMR (CDCl₃, 200 MHz) δ 0.82 (br t, 3H), 1.19 (br s, 24H), 1.50 (m, 2H), 2.21 (t, 2H, J=7.4Hz), 2.31 (s, 3H), 3.28 (br s, 11H), 3.43 (br s, 6H), 3.54 (m, 6H), 3.76 (br s, 5H), 3.94 (m, 2H), 3.98 (m, 3H), 4.53 (m, 3H), 4.81 (br m, 1H), 5.27 (m, 1H), 6.62–6.92 (m, 3H), 7.42 (d, 2H, 8.4Hz), 7.60 (d, 2H, 8.4Hz). ¹³C NMR (CDCl₃, 50 MHz) δ 13.18, 13.93, 22.48, 24.64, 28.95, 29.11, 29.14, 29.31, 29.45, 29.49, 31.70, 31.84, 33.81, 39.06, 54.11, 55.56, 59.22, 62.37, 63.29, 65.99, 68.14, 69.86, 70.13, 70.51, 71.19, 71.32, 101.25, 111.53, 113.22, 114.74, 128.97, 130.46, 130.69, 130.99, 133.56, 135.90, 139.14, 155.91, 168.07, 169.77, 169.95, 173.26. ³¹P NMR (CDCl₃, 160 MHz, pyrophosphate ref. ext.) δ –0.68. R_f (CHCl₃/MeOH/H₂O 65:25:4) 0.54. Anal. Calcd for C₅₁H₇₉ClN₃O₁₄P·1/3·H₂O: C, 59.43; H, 7.79; N, 4.08; Found: C, 59.26; H, 7.80; N, 4.07. MS MH⁺ C₅₁H₇₉ClN₃O₁₄PH Calcd: 1024.5061, Found: 1024.5075. [α]_D²⁰ + 5.8° (c 1.09, CHCl₃/MeOH 4:1).

3.3. 1-Palmitoyl-2-(11'-N-sulindaccarboxylamino-3,6,9trioxaundecanoyl)-sn-glycerophosphocholine (10)

This compound was prepared following the same activation/deprotection/acylation protocol outlined for compound 9. The product **10** was obtained from the *t*-BOC protected precursor **8** in an overall yield of 97%. IR (CHCl₃): 3355, 1739 br cm⁻¹; ¹H NMR (CDCl₃, 200 MHz) δ 0.86 (br t, 3H), 1.23 (br s, 24H), 1.54 (m, 2H), 2.24 (m, 5H), 2.80 (s, 3H), 3.34 (br s, 11H), 3.51 (br s, 8H), 3.65 (m, 6H), 3.83 (m, 2H), 4.04 (m, 2H), 4.17 (m, 2H), 4.34 (m, 2H), 5.28 (m, 1H), 6.51 (br t, 1H), 6.97–7.27 (m, 3H), 7.69 (dd, 4H, J=5.5 Hz and /=8.9 Hz). ¹³C NMR (CDCl₃, 50 MHz) δ 10.54, 14.06, 22.61, 24.76, 29.08, 29.24, 29.28, 29.45, 29.59, 29.63, 31.84, 33.48, 33.93, 39.30, 43.81, 54.37, 59.52, 62.35, 63.76, 66.23, 68.27, 69.59, 69.99, 70.29, 70.66, 71.19, 105.89, 106.36, 110.46, 110.91, 123.47, 123.79, 128.23, 129.62, 130.18, 133.06, 138.40, 139.55, 141.58, 145.42, 146.90, 160.77, 165.66, 169.47, 169.94, 173.40. ³¹P NMR (CDCl₃, 160 MHz, pyrophosphate ref. ext.) δ –1.47. R_f (CHCl₃/MeOH/H₂O 65:25:4) 0.56. Anal. Calcd for C₅₂H₈₀FN₂O₁₃P·3/2·H₂O·1/3CHCl₃: C, 56.81; H, 7.58; N, 2.52; Found: C, 56.92; H, 7.86; N, 2.34. MS MH⁺ C₅₂H₈₀FN₂O₁₃PSH Calcd: 1023.5176, Found: 1023.5147. $[\alpha]_D^{20}$ + 5.7 (c 1.14, CHCl₃/MeOH 4:1).

3.4. 1-Palmitoyl-2-(8'-N-FMOC-amino-3,6-dioxaoctanoyl)sn-glycerophosphocholine (11)

To a suspension of 1-palmitoyl-2-hydroxy-sn-glycero-3phosphocholine (0.4012 g, 0.8 mmol) in 25 mL CHCl₃ were added 8-N-FMOC-amino-3,6-dioxaoctanoic acid (0.3305 g, 0.86 mmol), DCC (0.2482 g, 1.2 mmol), DMAP (0.1504 g, 1.2 mmol) and 1 g of glass beads. The reaction was sonicated for 6 h at 25 °C. The solvent was then evaporated and the residue was purified by silica gel chromatography, first with CHCl₃/MeOH (4:1), followed by CHCl₃/MeOH/H₂O (65:25:4). The fractions of the product were combined and freeze-dried from benzene to yield compound 11 (0.5134 g, 75%) as white solid. IR (CHCl₃): 3330, 1732 br, 1690 cm⁻¹. ¹H NMR (CDCl₃, 200 MHz) δ 0.87 (br t, 3H), 1.24 (br s, 24H), 1.54 (m, 2H), 2.24 (t, 2H, /=7.4Hz), 3.30 (br s, 11H), 3.55-3.75 (br m, 6H), 3.98 (m, 2H), 4.15 (m, 4H), 4.24-4.50 (br m, 6H), 4.67 (m, 1H), 5.28 (m, 1H), 5.86 (m, 1H), 7.25–7.37 (m, 4H), 7.60 (d, 2H, J=7.4 Hz), 7.73 (d, 2H, I = 7.4 Hz).¹³C NMR (CDCl₃, 50 MHz) δ 13.93, 22.48, 24.63, 28.95, 29.11, 29.15, 29.32, 29.46, 31.71, 33.81, 40.60, 47.02, 54.03, 59.27, 62.33, 63.45, 65.97, 66.42, 68.15, 69.79, 70.59, 71.35, 119.75, 124.98, 126.87, 127.48, 141.04, 143.79, 156.42, 169.85, 173.26. Anal. Calcd for C₄₅H₇₁N₂O₁₂P·1/4CHCl₃: C, 60.87; H, 8.04; N, 3.14; Found: C, 60.64; H, 8.26; N, 3.03. MS MH⁺ C₄₅H₇₁N₂O₁₂PH Calcd: 863.4817, Found: 863.4836. ³¹P NMR (CDCl₃, 160 MHz, pyrophosphate ref. ext.) δ –0.85. R_f (CHCl₃/MeOH/H₂O 65:25:4) $0.57. [\alpha]_D^{20} + 5.2^\circ$ (c 0.97, CHCl₃/MeOH 4:1).

3.5. 1-Palmitoyl-2-(8'-N-diclofenaccarboxylamino-3,6-dioxaoctanoyl)-sn-glycerophosphocholine (**12**)

(i) Diclofenac *p*-nitrophenyl ester. To a suspension of diclofenac sodium salt (0.6362 g, 2 mmol) in 50 mL acetone was added Dowex-H⁺ (25 mL). The mixture was stirred for 10 min, and then it was filtered and the filtrate was evaporated to give the corresponding free acid as a white solid. This acid was dissolved in 50 mL $CHCl_3$ and to the solution were added *p*-nitrophenol (0.2546 g, 1.83 mmol), DCC (0.4126 g, 2 mmol) and DMAP (52 mg, 0.43 mmol). The reaction mixture was stirred for 1 h at room temperature. The DCC-urea was removed by filtration, and the solvent was evaporated to give the *p*-nitrophenyl active-ester of diclofenac as a yellow solid; R_f (CHCl₃/EtOAc, 5:1) 0.92. It was suitable to be used for the subsequent acylation step without further purification. (ii) Elimination of the FMOC protecting group of compound 11, and N-acylation at the chain-terminal. To a solution of compound 11 (0.2107 g, 0.24 mmol) in 5 mL CHCl₃ was added DBU (0.1852 g, 1.2 mmol) and the mixture was kept at room temperature for 1 h. To this solution were added diclofenac *p*-nitrophenyl ester (0.4 g, 0.96 mmol), DMAP (42 mg, 0.34 mmol). The reaction was stopped after 5 h, when a ninhydrin test gave negative result on the spot near the origin on the TLC plate. The reaction mixture was loaded directly onto a silica gel column, eluted first with CHCl₃/MeOH (4:1) to remove the impurities followed by CHCl₃/MeOH/H₂O (65:25:4) to elute the pure phospholipid. The fractions corresponding to the product were combined, evaporated, dispersed in benzene and freeze-dried to give 12 (0.1125 g, 51%) as pale-yellow solid. IR (CHCl₃): 3330, 1737 br, 1532 cm⁻¹; ¹H NMR (CDCl₃, 200 MHz) δ 0.86 (br t, 3H), 1.23 (br s, 24H), 1.54 (m, 2H), 2.25 (t, 2H, *I*=7.4Hz), 3.24 (br s, 11H), 3.42 (m, 2H), 3.54 (br m, 6H), 3.73 (m, 4H), 4.04–4.17 (br m, 4H), 4.29 (m, 2H), 4.62 (m, 1H), 5.44 (m, 1H), 6.46 (d, 1H, J=7.5 Hz), 6.85-6.98 (m, 3H), 7.24–7.32 (m, 3H), 8.08 (br s, 1H). ¹³C NMR (CDCl₃, 50 MHz) δ 14.05, 22.61, 24.77, 29.07, 29.27, 29.44, 29.62, 31.84, 33.95, 39.33, 40.37, 54.24, 59.37, 62.41, 63.77, 66.11, 68.31, 69.52, 70.01, 70.71, 71.48, 117.19, 121.06, 123.86, 125.49, 127.45, 128.78, 129.75, 130.67, 137.76, 143.24, 170.20, 172.44, 173.45. ³¹P NMR (CDCl₃. 160 MHz, pyrophosphate ref. ext.) δ –1.28. R_f (CHCl₃/MeOH/H₂O 65:25:4) 0.56. Anal. Calcd for C₄₄H₇₀Cl₂N₃O₁₁P·1/3CHCl₃: C, 55.54; H, 7.39; N, 4.38; Found: C, 55.58; H, 7.61; N, 4.40. MS MH+ $C_{44}H_{70}Cl_2N_3O_{11}PH$ Calcd: 918.4198, Found: 918.4232. [α]_D²⁰ + 4.3° (c 0.87, CHCl₃/MeOH 4:1).

3.6. 1-Palmitoyl-2-(8'-N-[5"-dimethylaminonaphthalene-1"sulfonyl]-amino-3,6-dioxaoctanoyl)-sn-glycerophosphocholine (**13**)

To a solution of compound **11** (0.2115 g, 0.24 mmol) in 5 mL CHCl₃ was added DBU (0.1922 g, 1.2 mmol). The reaction mixture was kept at room temperature for 1 h. To this solution were then added dansyl chloride (0.1295 g, 0.48 mmol) and NEt₃ (0.17 mL, 1.2 mmol), followed by 30 min later a second portion of dansyl chloride (0.1287 g, 0.48 mmol). The reaction was over after 1 h, as shown by a negative ninhydrin test on a TLC plate. The mixture was purified directly by silica gel chromatography using CHCl₃/MeOH (4:1), to remove the impurities, followed by CHCl₃/MeOH/H₂O (65:25:4) to elute the target phospholipid. The fractions corresponding to the product were combined, evaporated, dispersed in benzene and freeze-dried to give compound **13** (0.1028 g, 49%) as a white solid. IR (CHCl₃): 3340, 1742 br cm⁻¹; ¹H NMR (CDCl₃, 200 MHz) δ 0.87 (br t, 3H), 1.24 (br s, 24H), 1.54 (m, 2H), 2.25 (t, 2H, J=7.4 Hz), 2.85 (s, 6H), 2.97 (m, 2H), 3.32 (br s, 11H), 3.42 (m, 4H), 3.57 (m, 2H), 3.83 (m, 2H), 4.15 (br m, 4H), 4.30 (m, 2H), 4.67 (m, 1H), 5.32 (m, 1H), 7.15 (d, 1H, J=7.4Hz), 7.49-7.69 (m, 3H), 8.20 (d, 1H, 7.4 Hz), 8.38 (d, 1H, J=7.4 Hz). ¹³C NMR (CDCl₃, 50 MHz) δ 14.08, 22.64, 24.77, 29.10, 29.27, 29.31, 29.47, 29.66, 31.87, 33.95, 42.73, 45.38, 54.38, 59.65, 62.33, 64.06, 66.21, 68.40, 69.41, 69.99, 70.67, 71.50, 115.23, 119.41, 123.21, 128.26, 128.78, 129.65, 129.94, 135.59, 151.64, 170.24, 173.38. ³¹P NMR (CDCl₃, 160 MHz, pyrophosphate ref. ext.) δ –1.72. R_f (CHCl₃/MeOH/H₂O 65:25:4) 0.40. Anal. Calcd for C₄₂H₇₂N₃O₁₂PS·CHCl₃·C₆H₆: C, 54.92; H, 7.43; N, 3.93; Found: C, 55.27; H, 7.71; N, 3.83. MS MH⁺ C₄₂H₇₂N₃O₁₂PSH Calcd: 874.4667, Found: 874.4602. [α]_D²⁰ + 5.7° (c 1.04, CHCl₃/MeOH 4:1).

3.7. Enzymatic hydrolysis of the synthetic phosphatidylcholine analogues

In a typical experiment, to a sample of phosphatidylcholine 9 (5.0 mg, 5 µmol) was added a solution of 4.1 mL of 0.05 M Tris (pH 8.5) containing 10 mM Triton X-100 and 50 mM CaCl₂. The mixture was vortexed thoroughly, followed by incubation of the resulting dispersion at 40°C in a water bath for 10 min. The mixture was then once again vortexed and used for the phospholipase assay directly. The reaction was initiated by addition of bee-venom phospholipase A_2 (8 µg in 45 µL buffer). The reaction was run at 40 °C for 60 min using a constant temperature water bath, and formation of the products was analyzed by thin layer chromatography. The compounds were visualized on the silica gel plates by UV-absorption, iodine adsorption, and molybdic acid spray. TLC analysis (chloroform/methanol/water 65:25:4) showed complete hydrolysis of phosphatidylcholine 9 (R_f 0.56) yielding 1-palmitoyl-2-lysophosphatidylcholine **7** (R_f 0.17) and the 3,6,9trioxaundecanylamide of indomethacin (R_f 0.90) both identified by respective standards. Under similar assay conditions phosphatidylcholines 10, 12, 13 were also completely hydrolyzed by the enzyme.

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