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Title: Neutrophil Elastase Promotes Linker Cleavage and Paclitaxel Release from an Integrin-Targeted Conjugate

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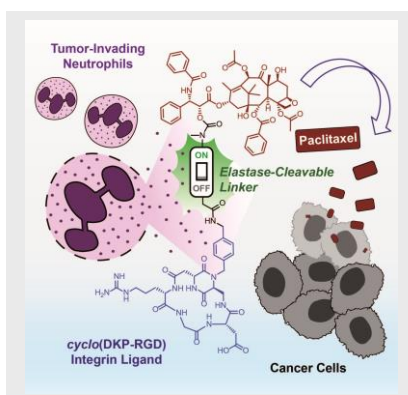
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Key Topic: Tumor Targeting

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Exploiting inflammation in cancer:

A RGD-drug conjugate accumulates on the surface of integrin-expressing human renal cell carcinoma cells and releases paclitaxel upon linker cleavage mediated by neutrophil-secreted elastase.



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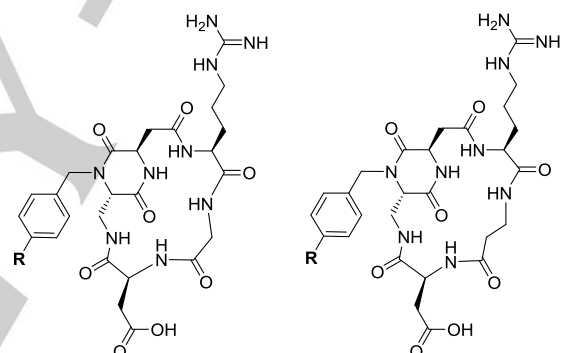
André Raposo Moreira Dias,^[a] Arianna Pina,^[a] Amelia Dean,^[a] Hans-Georg Lerchen,^[b] Michele Caruso,^[c] Fabio Gasparri,^[c] Ivan Fraietta,^[c] Sonia Troiani,^[c] Daniela Arosio,^[d] Laura Belvisi,^[a,d] Luca Pignataro,^[a] Alberto Dal Corso,^[a] and Cesare Gennari^{*,[a,d]}

Abstract: We took advantage of one of the hallmarks of cancers, i.e. the presence of tumor infiltrating cells of the immune system and leukocyte-secreted enzymes, to promote the activation of an anticancer drug at the tumor site. The peptidomimetic integrin ligand *cyclo*(DKP-RGD) was found to accumulate on the surface of $\alpha_v\beta_3$ integrin-expressing human renal cell carcinoma 786-O cells. The ligand was conjugated to the anticancer drug paclitaxel through a Asn-Pro-Val (NPV) tripeptide linker, which is a substrate of neutrophil-secreted elastase. *In vitro* linker cleavage assays and cell antiproliferative experiments demonstrate the efficacy of this tumor-targeting conjugate, opening the way to potential therapeutic applications.

The conjugation of anticancer drugs to specific ligands, capable of selective binding to tumor-associated receptors, represents a widely explored strategy to improve the accumulation of cytotoxic agents at the tumor site, sparing healthy tissues and resulting in better therapeutic outcomes. Antibody-Drug Conjugates (ADCs) represent the first-in-class in this oncology area.^[1] To date, four ADC products have gained marketing authorization (AdcetrisTM, KadcylaTM, MylotargTM and BesponsaTM), while more than 50 are presently under clinical investigation.^[2] Similarly, anticancer agents have also been coupled to small ligands (e.g. peptides/peptidomimetics,^[3] vitamins,^[4] steroids^[5] and enzyme inhibitors^[6]), targeting specific receptors overexpressed by cancer cells. An increasing body of evidences suggests that these so-called Small Molecule-Drug Conjugates (SMDCs)^[7] may accumulate in the tumor mass homogeneously and with high tumor/organ and tumor/blood ratios, potentially showing better anticancer efficacy than conventional cytotoxic agents and ADC products.^[8] In general, these conjugates have been designed to bind the target receptor on the surface of cancer cells and to release the cytotoxic cargo

in intracellular compartments (e.g. lysosomes), upon receptor-mediated internalization and selective cleavage of a linker (e.g. a short peptide sequence or a reducible disulfide bond) connecting the targeting unit to the payload.^[9]

Among the protein antigens that have been explored for tumor targeting applications, integrin $\alpha_v\beta_3$ is a heterodimeric transmembrane receptor overexpressed in a variety of cancer types (such as melanoma, glioblastoma, renal cell carcinoma, and tumors of lung, ovary, breast, prostate and colon), where it is involved in disease progression.^[10] Upon the observation that cyclic peptides bearing the Arg-Gly-Asp (RGD) sequence are potential $\alpha_v\beta_3$ integrin ligands, a large number of RGD-bearing peptides and peptidomimetics have been explored for SMDC development.^[11]



1: R = H
[*cyclo*(DKP-RGD)]
IC₅₀ $\alpha_v\beta_3$ = 4.5 ± 1.1 nM

2: R = CH₂NH-sCy5
[*cyclo*(DKP-RGD)-sCy5]
IC₅₀ $\alpha_v\beta_3$ = 7.8 ± 1.5 nM

3: R = H
[*cyclo*(DKP-RβAD)]
IC₅₀ $\alpha_v\beta_3$ = 1550 ± 226 nM

4: R = CH₂NH-sCy5
[*cyclo*(DKP-RβAD)-sCy5]
IC₅₀ $\alpha_v\beta_3$ = 1200 ± 650 nM

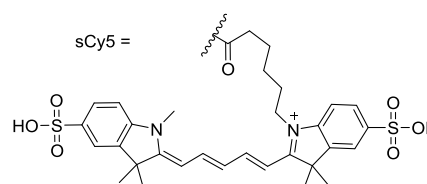


Figure 1. Molecular structure of the $\alpha_v\beta_3$ integrin ligand *cyclo*(DKP-RGD) (1) and its analog *cyclo*(DKP-RβAD) (3), alongside with their relative sulfocyanine5 (sCy5) conjugates *cyclo*(DKP-RGD)-sCy5 (2) and *cyclo*(DKP-RβAD)-sCy5 (4). Data of inhibition of biotinylated vitronectin binding to the $\alpha_v\beta_3$ receptor are shown.

Within this frame, our group synthesized a cyclic peptidomimetic compound bearing the RGD integrin recognition motif and a diketopiperazine (DKP) scaffold, as a low nanomolar $\alpha_v\beta_3$ integrin ligand (compound 1, Figure 1).^[12] The ligand was successfully linked to different cytotoxic payloads (i.e. paclitaxel,^[13] camptothecin^[14] and α -amanitin^[15]) and the resulting conjugates maintained high affinity for the integrin receptor. In line with literature data reporting evidences of internalization of integrin ligands equipped with fluorescent

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Supporting information, including the synthetic procedures, along with the ¹H- and ¹³C-NMR spectra, HPLC and MS data, all procedures for biological and biochemical assays, and the ORCID identification number(s) for the author(s) of this article can be found under: <https://doi.org/10.1002/chem.xxxxxxx>

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dyes,^[16] our *cyclo*(DKP-RGD)-drug conjugates were endowed with suitable linkers for selective payload release in intracellular compartments of the cancer cells. The ability of these SMDs to selectively hit $\alpha_v\beta_3$ -positive cells was quantified through *in vitro* cell antiproliferative assays performed using cancer cell lines expressing the integrin receptor at different levels (i.e. expressing vs. non-expressing cells). To our delight, some of these SMDs proved to be highly selective for the $\alpha_v\beta_3$ -expressing cells,^[17] indicating that **1** effectively recognizes the integrin receptor on the cancer cell membrane. However, the potency of all our conjugates against $\alpha_v\beta_3$ -positive cells proved to be significantly lower (typically one order of magnitude) than that of the free drug. This observation is in contrast with literature data reporting the high potency of internalizing ADCs and SMDs,^[18,19] and it may indicate a suboptimal endocytosis of our ligand-drug conjugates. In order to confirm this hypothesis and evaluate the internalization properties of the *cyclo*(DKP-

RGD) integrin ligand, we labeled it with the near-infrared (NIR) dye sulfo-cyanine5 (sCy5, Figure 1). The ability of the resulting conjugate *cyclo*(DKP-RGD)-sCy5 (**2**) to compete with biotinylated vitronectin for the binding to the isolated $\alpha_v\beta_3$ receptor was measured. The low-nanomolar IC_{50} value obtained confirmed that integrin recognition was not affected by the conjugation with the probe (**2**, Figure 1). Moreover, we devised the preparation of a negative control, possessing almost identical physical-chemical properties, while showing negligible affinity for the receptor. Inspired by the literature,^[20] the Arg-Gly-Asp tripeptide was mutated into a Arg-[β Ala]-Asp sequence, giving rise to the *cyclo*(DKP-R β AD) ligand **3** (Figure 1). In comparison with the parent ligand **1**, the new compound showed a dramatically lower integrin binding affinity (micromolar IC_{50} value) and a similar result was obtained for the fluorescent conjugate *cyclo*(DKP-R β AD)-sCy5 **4** (Figure 1).

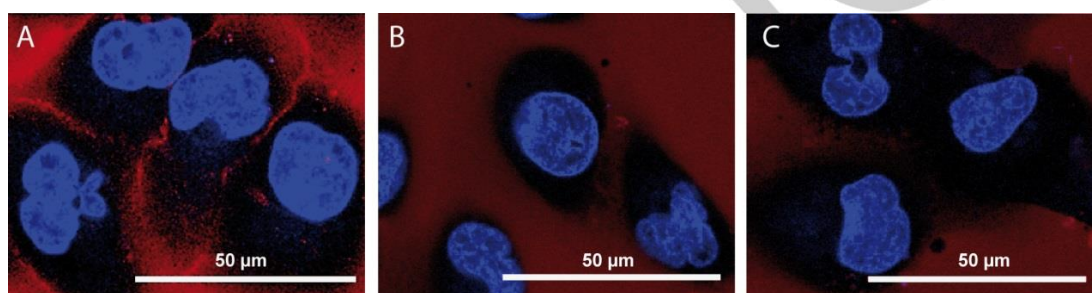


Figure 2. Confocal microscopy images of live $\alpha_v\beta_3$ -expressing human renal cell carcinoma 786-O cells after exposure to conjugates **2** (A), **4** (B) and free sCy5 (C) (1 μ mol/l, exposure time = 2 h). Accumulation at the cell membrane was detected only upon exposure to conjugate **2**. No fluorescent signal was detected in the intracellular compartments for all compounds tested. Blue: Hoechst; Red: NIR dye.

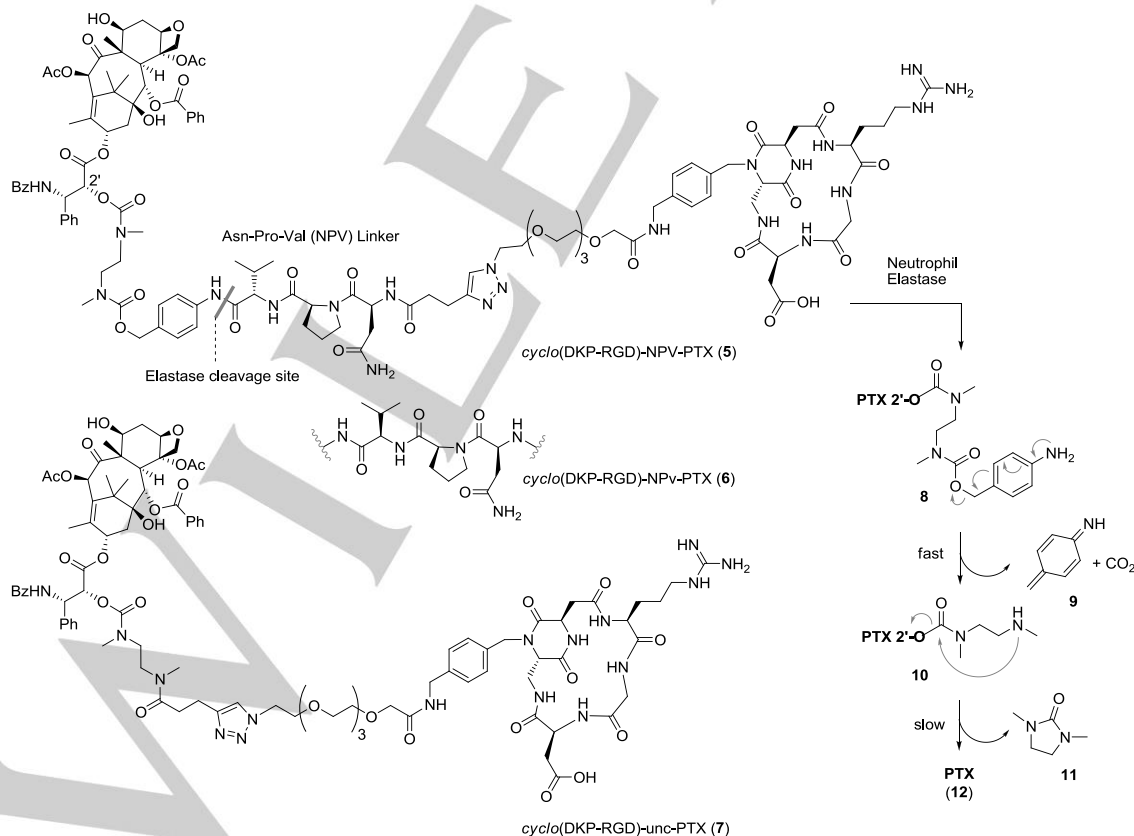


Figure 3. Molecular structures of the $\alpha_v\beta_3$ integrin-targeted conjugate *cyclo*(DKP-RGD)-NPV-PTX (**5**), of its diastereoisomer *cyclo*(DKP-RGD)-NPv-PTX (**6**), whose linker bears D-valine (v), and of the uncleavable conjugate *cyclo*(DKP-RGD)-unc-PTX (**7**). Mechanism of PTX release upon linker cleavage is depicted, consisting in the fast 1,6-elimination of the *p*-aminobenzyl carbamate **8**, followed by amine cyclization in compound **10**, which results in the formation of cyclic urea **11** and free Paclitaxel (**12**).

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Confocal microscopy experiments were carried out with live human cancer cells 786-O (renal cell carcinoma), expressing $\alpha_v\beta_3$ integrin (as detected by Western blot analysis, see Figure S1 in the Supporting Information), in the presence of conjugates **2** and **4**. The uncoupled sulfo-cyanine5 probe was also included in the experiment as additional control. As shown in Figure 2, a fair accumulation of the *cyclo*(DKP-RGD)-sCy5 conjugate (**2**) on the membrane of cancer cells was detected, whereas no significant intracellular uptake was observed. On the other hand, no accumulation of control compounds *cyclo*(DKP-R β AD)-sCy5 (**4**) and free sulfo-cyanine5 was detected neither in intracellular compartments, nor on the cell surface.

Overall, this analysis confirmed that the integrin ligand *cyclo*(DKP-RGD) **1** accumulates on the cell membrane of $\alpha_v\beta_3$ integrin-expressing cancer cells, while is poorly internalized by receptor-mediated endocytosis. This finding may be related to the antagonist behavior of **1**, which has been found to display inhibitory effects on the FAK/Akt integrin activated transduction pathway and on integrin-mediated cell infiltration processes.^[21] The elucidation of the link between the agonist/antagonist behavior of integrin ligands and the receptor-mediated internalization is currently a hot topic in this field.^[22] Interestingly, the importance of conjugate internalization has been recently challenged.^[23] Indeed, ADCs and SMDCs specific to non-internalizing receptors (e.g. collagen IV,^[24] carbonic anhydrase IX,^[25] fibrin^[26] and splice variants of fibronectin^[27] and tenascin-C^[28]) were found to elicit strong antitumor responses *in vivo*, while proving significantly less potent than the parent drug in *in vitro* cell antiproliferative assays.^[29] For these reasons, we envisioned the preparation of a non-internalizing, $\alpha_v\beta_3$ integrin-targeted conjugate, featuring a specific linker for the extracellular release of the payload.

In 2002, researchers at Bayer developed a new SMDC, whose linker consisted in the tripeptide Asn-Pro-Val (NPV), a specific substrate of neutrophil elastase.^[30] The latter is a serine protease stored in azurophilic granules of neutrophils and released into the extracellular space upon infections or inflammation stimuli. High levels of elastase have been reported in primary tumors and metastasis, where it promotes oncogenic signaling and inhibits tumor suppressors. As a result, elevated neutrophil elastase levels correlate with poor prognosis in different types of solid tumors.^[31] To the best of our knowledge, no further investigations of this promising NPV peptide linker have been reported in the literature. For these reasons, we designed an extracellularly-cleavable conjugate (**5**, Figure 3) in which the $\alpha_v\beta_3$ integrin ligand *cyclo*(DKP-RGD) is connected to paclitaxel (PTX) via a self-immolative spacer, the NPV linker and a hydrophilic PEG4 spacer. Two additional conjugates were prepared as negative controls: the *cyclo*(DKP-RGD)-NPV-PTX conjugate (**6**), featuring the non-proteinogenic amino acid [D]-valine, and the *cyclo*(DKP-RGD)-unc-PTX conjugate (**7**), in which the tripeptide moiety is replaced by a proteolytically stable (or "uncleavable") tertiary amide bond. This panel of compounds was designed to gain insights into the specificity of elastase cleavage and the stability of the whole linker system. All synthetic details and analytics are included in the Supporting Information.

The affinity of compounds **5-7** for $\alpha_v\beta_3$ integrin was estimated as described previously and low-nanomolar values were obtained throughout the series (Table 1).

Table 1. Inhibition of biotinylated vitronectin binding to the $\alpha_v\beta_3$ receptor.

Conjugate	Structure	$\alpha_v\beta_3$ IC ₅₀ [nM] ^[a]
5	<i>cyclo</i> (DKP-RGD)-NPV-PTX	12.9 ± 1.4
6	<i>cyclo</i> (DKP-RGD)-NPv-PTX	24.9 ± 2.1
7	<i>cyclo</i> (DKP-RGD)-unc-PTX	5.8 ± 1.2

[a] IC₅₀ values were determined as the concentration of compound required for 50% inhibition of biotinylated vitronectin binding as estimated by GraphPad Prism software. All values are the arithmetic mean ± the standard deviation (SD) of duplicate determinations.

Table 2. Antiproliferative activity of conjugates **5-7** and free PTX in $\alpha_v\beta_3$ -expressing human renal cell carcinoma 786-O cells after 96 h treatment, in the presence (or absence) of elastase from human leukocytes.

Structure	IC ₅₀ [nM] ^[a]	
	Added elastase	
	NO	YES
Paclitaxel (PTX) (12)	35.8 ± 16.7	29.5 ± 7.6
<i>cyclo</i> (DKP-RGD)-NPV-PTX (5)	> 5000	19.6 ± 4.1
<i>cyclo</i> (DKP-RGD)-NPv-PTX (6)	> 5000	> 5000
<i>cyclo</i> (DKP-RGD)-unc-PTX (7)	> 5000	> 5000

[a] IC₅₀ values were determined as the concentration of compound required for 50% inhibition of cell viability in presence or absence of 50 nM elastase (ELANE, 324681, Millipore). Samples were measured in triplicate.

To evaluate the cleavage of the tripeptide linker and the subsequent paclitaxel release in the presence of neutrophil elastase, conjugate **5** was treated with the enzyme in PBS solution at 37 °C, and metabolites were detected by HPLC-MS analysis. The enzymatic cleavage of the tripeptide linker was observed over a 2 h period, resulting in the complete formation of metabolite **10**^[32] (Figure 3), whereas the use of inactivated enzyme did not lead to metabolite formation (Figure S2 in the Supporting Information). The selectivity of linker cleavage was analyzed treating **5** with rat liver-derived lysosome extract, composed by a mixture of proteolytic enzymes. The broad-scope cysteine proteases inhibitor E-64 was used in this experiment to gain insight into the effector enzymes involved in the cleavage. Upon 2 hours exposure to lysosome extract, conjugate **5** was digested only partially (Figure S4 in the Supporting Information), possibly indicating the presence of elastase in the lysosome extract.^[33] This hypothesis was supported by the partial formation of metabolite **10** also in the presence of the E-64 inhibitor, (Figure S4 in the Supporting Information) indicating that cysteine proteases are not responsible for the cleavage of the NPV linker.

Additionally, conjugate **5** was treated with mouse plasma at 37 °C, showing an excellent stability under these conditions (*t*_{1/2} = 35.3 h, Figure S5 in the Supporting Information).

Following the protocol reported by Bayer,^[30] the *in vitro* cell antiproliferative activity of conjugates **5-7** was tested against 786-O cancer cells, in the presence or absence of elastase. Importantly, Western blot analysis showed no significant elastase expression in these cancer cells (see Figure S1 in the Supporting Information). This model assay aimed at evaluating

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the extracellular cleavage of the NPV linker upon activation of neutrophils and release of elastase in the extracellular tumor environment, followed by the PTX internalization into cancer cells by passive diffusion through the cell membrane. In the absence of elastase, conjugates **5-7** did not exhibit a significant cytotoxic activity ($IC_{50} > 5 \mu M$, Table 2), whereas free PTX inhibited cell proliferation at nanomolar concentrations ($IC_{50} = 35.8 \pm 16.7 \text{ nM}$). Interestingly, conjugate **5** displayed a > 250 -fold increased activity ($IC_{50} = 19.6 \pm 4.1 \text{ nM}$) upon addition of elastase (50 nM), and the observed potency was comparable to the one exhibited by free PTX under the same conditions ($IC_{50} = 29.5 \pm 7.6 \text{ nM}$). On the other hand, the presence of elastase did not modify the original cell antiproliferative activity of conjugates **6** and **7**. This result indicates not only that the PTX payload is inactive when it is not released from the targeting vehicle, but also that the use of the natural amino acid [L]-Val at the linker C-terminus is crucial for the recognition of the tripeptide sequence by elastase.

In conclusion, integrin ligands represent promising vehicles for the selective release of anticancer drugs at the tumor site. However, it is still not clear whether different RGD-based ligands may have different effects on the receptor internalization and recycling in cancer cells. Upon the observation that the integrin ligand *cyclo*(DKP-RGD) is not efficiently internalized by $\alpha_v\beta_3$ -expressing cancer cells, we focused on suitable strategies for the delivery of anticancer agents in the extracellular tumor environment. In this work, the peptide sequence NPV, substrate of the serine protease elastase, has been investigated as trigger for the release of paclitaxel from an $\alpha_v\beta_3$ -targeted conjugate. Ideally, the integrin recognition unit would drive the conjugate accumulation at the tumor site, where the pro-inflammatory stimuli result in the recruitment of tumor-infiltrating leukocytes, such as neutrophils. The activation of the latter promotes the release of elastase, which triggers the payload release in the tumor microenvironment. As described elsewhere,^[23] this mode of activation may possess potential therapeutic benefits, since the free payload would diffuse in the tumor mass, and act against a large variety of cells (e.g. antigen-negative cancer cells, endothelial and other cancer-associated host cells) leading to a localized damage. It has been reported that lipophilic payloads are most suited for this strategy, as the membrane permeability would facilitate the cytotoxic activity by the so-called "bystander effect".^[34] Our *in vitro* data indicate that each individual unit of our SMDC (i.e. ligand, linker and drug) may efficiently act according to this ideal mechanism of action. Moreover, the pro-inflammatory environment and the presence of infiltrating cells of the immune system are well-established hallmarks of cancers.^[35] It is therefore conceivable that elastase-activable prodrugs may be therapeutically active against a large variety of tumor types.

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- [32] Compound **10** was synthesized from PTX (see the Supporting Information). The cyclization rate of the ethylenediamine self-immolative spacer in compound **10** was found to be pH dependent: while a half-life of 4.7 h was measured in a DMSO:PBS mixture at pH 7.5 and 37 °C (see Figure S3A in the Supporting Information), no release of free PTX was detected in a DMSO:acetate buffer mixture at pH 5.5 over a 24 h period. The antiproliferative activity of compound **10** was evaluated in $\alpha_5\beta_3$ -expressing human renal cell carcinoma 786-O cells after 110 h treatment, in comparison with free PTX (**12**). Under these experimental conditions, compound **10** proved moderately less potent than PTX (see Figure S3B in the Supporting Information).
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