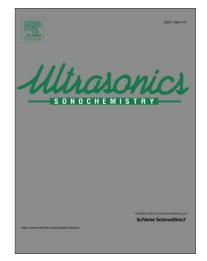
A Simple Sonochemical Assisted Synthesis of Porous $NiMoO_4$ /chitosan Nanocomposite for Electrochemical Sensing of Amlodipine in Pharmaceutical Formulation and Human Serum

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A Simple Sonochemical Assisted Synthesis of Porous NiMoO₄/chitosan Nanocomposite for Electrochemical Sensing of Amlodipine in Pharmaceutical Formulation and Human Serum

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Abstract

In this investigation, a facile sonochemical route has been developed for the preparation of porous nickel molybdate nanosheets/chitosan nanocomposite (NiMoO₄/CHIT) by using ammonium molybdate and nickel(II) acetate tetrahydrate and as nickel and molybdate precursor, respectively (ultrasonic power 60 W/cm² and frequency 20 kHz). The ultrasonic based materials preparation as a fast, convenient and economical approach has been widely used to generate novel nanomaterials. Herein, we report an efficient voltammetric sensor for amlodipine drug by using porous nickel molybdate nanosheets/chitosan nanocomposite (NiMoO₄/CHIT). Its structure and properties were characterized by x-ray diffraction pattern, scanning electron

microscope, transmission electron microscope, elemental analysis and mapping. The electrochemical studies are indicated the NiMoO₄/CHIT modified glassy carbon electrode (GCE) exhibited the good performance towards electrocatalytic sensing of amlodipine drug. Consequently, a linear correlation between the anodic peak current with sensor concentration 0.025 to 373.6 μ M with a detection limit and sensitivity of 4.62 nM and 4.753 μ A. μ M⁻¹.cm⁻², respectively. A voltammetry based drug analysis was found to be high sensitive and reproducible, which able to detect nanomolar concentration. Furthermore, the fabricated electrochemical sensor was applied in drug and biological samples.

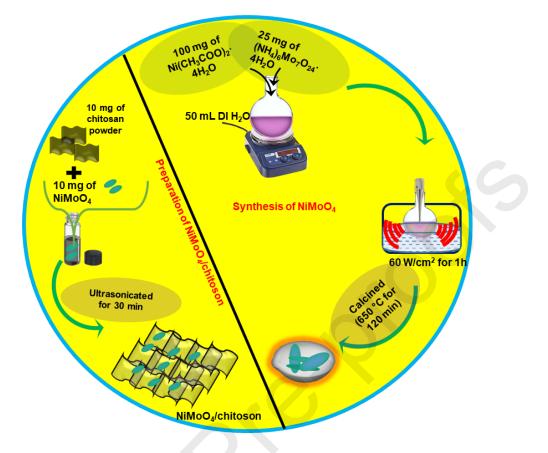
Keywords: Sonochemical synthesis; Bimetal oxide; Electrochemical detection; Drug analysis; Biological samples.

1. Introduction

Amlodipine is a dihydropyridine type drug, which inhibits the several disease such as high blood pressure and coronary artery disease in human and animal [1-4]. So, it has been widely used to treat hypertension; due to its relatively low cost and strong effective [5-7]. However, an excessive intake of amlodipine has side effects in form of abdominal pain, swelling, feeling tired, and nausea [8-11]. Therefore, it is necessary to develop rapid and effective method to determine the level of amlodipine in biological system. So far, HPLC (high performance liquid chromatography) [12], spectrophotometry, GC-TMS (gas chromatography- tandem mass spectrometry) [13, 14], fluorescence sensor [15], capillary zone electrophoresis and electrochemical sensor [16] techniques were used to determine the amlodipine. However, the results in considerable determination of amlodipine sensing in biological samples. Nevertheless,

it has drawbacks on the selectivity, over time consuming and expensive [17, 18]. Recently, electrochemical techniques are provide relatively low cost, facile, easy to operate, good sensitivity and excellent selectivity. Therefore, the fabrication of modified electrodes have been focused more interest in the research and medical development field.

Recently, bimetal oxide is providing exciting new capabilities for research and development in physical and chemical science [10, 19, 20]. In particular, transition series has recently emerged as a promising area in various applications such as supercapacitor [21], photodegradation [22], batteries [23], hydrogen storage [24], electrochemical sensors [25], CO₂ and CO reduction [26]. NiMoO₄ has attracted widespread interests due to the ever-increasing demand for electrocatalytic materials. Here, NiMoO₄ for electrochemical sensor due to their excellent features, including intrinsic properties and electrical conductivity [27]. However, the practical applications of NiMoO₄ in electrochemical sensor are still hinder due to the moderate of sensing ability and stability [28-33]. Hitherto, various electrode materials including conducting biopolymer, carbonaceous materials, and transition metals have been used to develop superior electrocatalytic performances [7, 33-36]. From the past decades, chitosan, a biopolymer has attracted more interest in electrochemical, biocompatible and biodegradable properties [37, 38]. It has been well-established that biomedical applications and generally show higher electrocatalytic activity than other biopolymer materials due its unique features including excellent electrical conductivity, thermal stability, flexibility and large active surface area to anchor and ability to fast electron transfer [17, 39-42]. Therefore, the choice has been made with biopolymer to enhance the performance of nanomaterial in electrochemical sensor.



Scheme 1. Sonochemical synthesis of NiMoO₄/CHIT nanocomposite

Herein, we present our research in developing low-cost, simple and environmental friendly sonochemical-assisted method to prepare NiMoO₄/CHIT for drug sensing. Our study describes the strategies for improving the reproducibility and sensitivity voltammetry method to usability of drug sensing by NiMoO₄/CHIT modified glassy carbon electrode (Scheme 1 and 2). However, literature reports on the application of NiMoO₄/CHIT for electrochemical detection of drug are rare. Herein, we report for a novel and sensitive sensor for the electrochemical detection of amlodipine using NiMoO₄/CHIT nanocomposite modified electrodes, which exhibit remarkable sensitivities and desirable detection limits. In addition, the practicality and feasibility ability of NiMoO₄/CHIT modified glassy carbon electrode toward drug sensor in tablet and human serum samples.

2. Experimental part

2.1. Sonochemical assisted synthesis of NiMoO₄/CHIT

NiMoO₄ nanosheets was synthesized by sonochemical technique [43]. The synthesis, 0.2 g of ammonium molybdate ((NH₄)₆Mo₇O₂₄·4H₂O) and 0.1 g of nickel(II) acetate tetrahydrate (Ni(CH₃COO)₂·4H₂O) were dissolved in 50 ml of deionized water (chemicals and methods are given in supporting information). Then the above solution was heated at 75°C for 30 min under stirring. Then the reaction temperature was increased to 90°C and then treated by ultrasonic irradiation 60 W power and 20 kHz frequency (Misonix S-4000). Finally, the yellow-green product was obtained by washed with deionized water and ethanol and dried. The NiMoO₄/CHIT was prepared by the chitosan biopolymer assisted sonochemical exfoliation of NiMoO₄ nanoparticles was added into 10 mL of chitosan and dispersed in deionized water and directly used for the electrochemical applications.

2.2. Fabrication of NiMoO₄/CHIT/GCE

Prior to modification, the glassy carbon electrode (0.071 cm², Gaoss Union Co. Ltd., China) was polished with 0.05 μ m alumina powder and then the electrode was sonicated in redistilled water for 5 min. After that, the dispersed NiMoO₄/CHIT solution was (eight μ L) drop casting onto the clean surface of glassy carbon electrode. The drop casted glassy carbon electrode was dried out at room temperature and the modified NiMoO₄/CHIT/glassy carbon electrode was used to the further all-electrochemical studies.

3. Results and discussions

3.1. XRD analysis

The XRD pattern of NiMoO₄/CHIT showed several diffraction peaks, which are originate from the (112), (220), (222), (200), (330), (204), (510), (150) and (530) phases of NiMoO₄ nanosheets (figure 1). The phase of NiMoO₄ is similar to its cubic phase structure with JCPDS labeled number of 13-0128 [44, 45]. Hence, the formation of NiMoO₄/CHIT was conformed in the XRD analysis.

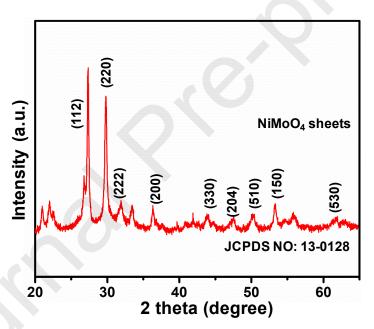


Figure 1. XRD analysis of NiMoO₄/CHIT nanocomposite.

3.2. Structural and morphological studies

Next, the morphological aspect of the nanocomposite was studied by TEM (figure 2A). The micrograph of NiMoO₄ displays mostly nanosheets, while the TEM image of NiMoO₄ is featured with the characteristic sheet-like morphology (figure 2B). However, the SEM image of NiMoO₄/CHIT nanocomposite shows the presence of NiMoO₄ nanosheets well distributed with

CHIT (figure 2C). A good electrostatic-attractive interaction between NiMoO₄ sheets and CHIT are possibly stabilizing them in the nanocomposite form. The EDX spectrum of NiMoO₄/CHIT revealed signals for the expected elements, such as carbon, nitrogen, oxygen, nickel and molybdenum signals (figure S1). The elemental mapping of NiMoO₄ nanosheets displayed the homogeneous distribution of nickel (D), molybdenum (E) and oxygen (F) in the NiMoO₄/CHIT (figure 2D-F).

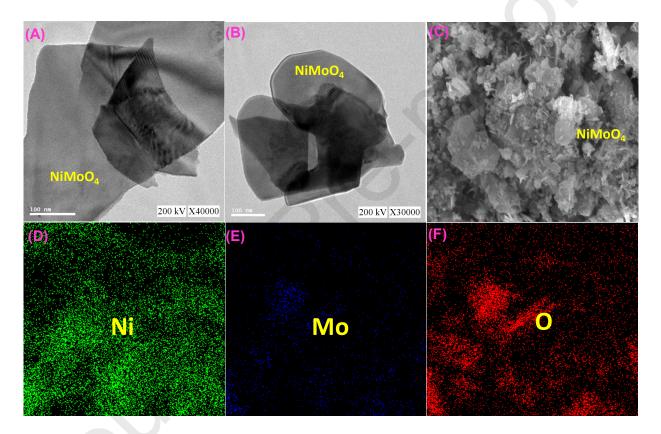


Figure 2. TEM images of NiMoO₄ nanosheets (A-B) and SEM image of NiMoO₄ (C). Elemental mapping analysis of NiMoO₄/CHIT (D-F).

3.3. Electrochemical analysis of amlodipine at NiMoO₄@CHIT modified GCE

Under optimum condition, the electrochemical sensor performance of NiMoO₄/CHIT/GCE and unmodified GCE were analyzed by cyclic voltammetry (CV). The cyclic voltammograms of unmodified GCE (b) and NiMoO₄/CHIT/GCE (c) toward 100 μ M

amlodipine in phosphate buffer (pH = 7.0) are shown in figure 3A. A feeble oxidation peak was observed at potential of 0.83 V at unmodified GCE, indicates the electrode is incapability to catalyze the oxidation reaction of amlodipine drug. The CV of NiMoO₄/CHIT modified GCE exhibited good oxidation peak at lower potential of 0.78 V with high intensity of current. On the other hand, NiMoO₄/CHIT/GCE shows a sharp peak compare to the bare GCE. Notably, the result indicates that NiMoO₄/CHIT/GCE has excellent electrocatalytic and sensing ability towards oxidation of amlodipine drug. The electrochemical oxidation (ECO) of amine group to pyridine position, the reaction is involving with $-2e^-$ and $-2H^+$ process and the mechanism is shown in Scheme 2. Moreover, its irreversible process based on the modified electrode surface. After the electrochemical oxidation, the pyridine position is more stable. Therefore, the reversible reduction process is not possible in pH 7.0. In figure 3A, it indicates that the NiMoO₄/CHIT/GCE has 2.8 folds larger than that at unmodified GCE. Moreover, the superior electrochemical performance of NiMoO₄/CHIT/GCE is due to the excellent synergic effect between NiMoO₄ and CHIT toward amlodipine sensing.

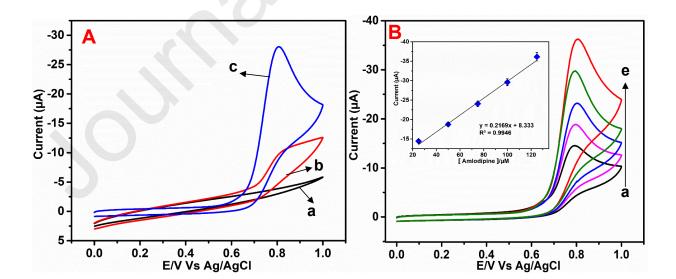
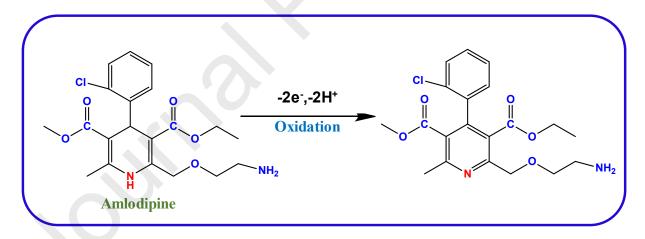


Figure 3. (A) CV responses of NiMoO₄/CHIT (c) modified and unmodified (b) GCE in phosphate buffer (0.05 M; pH 7.0) at 50 mV/s in the presence of 100 μ M amlodipine and the absence of amlodipine (a) (n=3). (B) CVs of oxidation of amlodipine at NiMoO₄/CHIT/GCE for different concentration (25 to 125 μ M) and (inset) the calibration plot of anodic peak current vs. [amlodipine]/ μ M.

In figure 3B, shows the CVs of NiMoO₄/CHIT/GCE towards different concentrations of amlodipine drug. When the concentration of amlodipine drug increase, the peak current is also increases linearly from 25 to 125 μ M without any fouling. In figure 3B, inset shows the plot between peak current and corresponding concentration of amlodipine drug, its exhibits good linearity, thus the NiMoO₄/CHIT nanocomposite modified electrode holds superior electrochemical sensing ability towards drug sensing.



Scheme 2. Systematic mechanism of the electrocatalytic oxidation of amlodipine drug.

3.4. Effect of scan rate and various pHs

The influence of scan rate on NiMoO₄/CHIT/GCE in 0.05 M phosphate buffer at a scan rate of 50 mV/s containing 100 μ M of amlodipine was examined by electrochemical studies,

figure 4A shows the CV results by means of increasing with the scan rate from 20 to 160 mV/s and oxidation peak current density increases and anodic current potential has the ability to shift towards higher positive value, such that the corresponding linear regression equation was acquired to be $I_{pa} = 51.103x + 13.452$ (R² = 0.9909) with excellent linear relationship between scan rate and oxidation peak currents shown in figure 4B. Therefore, these results indicate that the oxidation of amlodipine drug based on NiMoO₄/CHIT/GCE is diffusion-controlled process. Moreover, the electrochemical peak potential was shifted to negative direction when the scan rate was increased which can be attributed to the fast electron transfer process of totally irreversible electrode reaction.

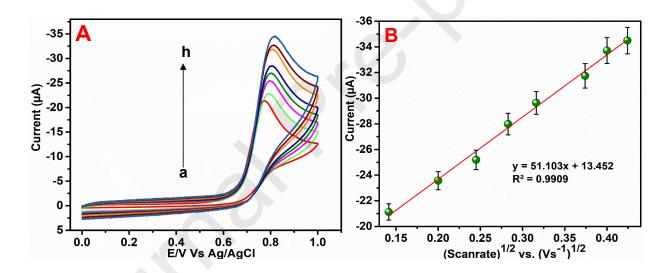


Figure 4. (A) CVs of oxidation of amlodipine at NiMoO₄/CHIT/GCE for different scan rate (20 to 160 mV/s). (B) The calibration plot of anodic peak current vs. square root of the scan rate.

The pH value was optimized by measuring the CV responses of modified electrodes in 100 μ M amlodipine at the scan rate of 50 mV/s. Different ranges of supporting electrolyte was investigated. The phosphate buffer with maximum efficacy on the oxidation peak current response was selected. The effect of 0.05 M phosphate buffer pH on the DPV determination of

amlodipine drug was studied in the range of 3.0 to 11.0. In figure 5A, shows that the pH increasing pH from 3.0 to 11.0, the oxidation peaks potential shifts toward more negative value. The pH 7.0 is high current responses according to figure 5A and B with correlation coefficient of (R^2) 0.9945. Due to pH 7.0 being the normal pH in human and animal biological fluids and the sensitivity of this sensor, pH 7.0 was chosen for use as the supporting electrolyte in all subsequent analytical experiments.

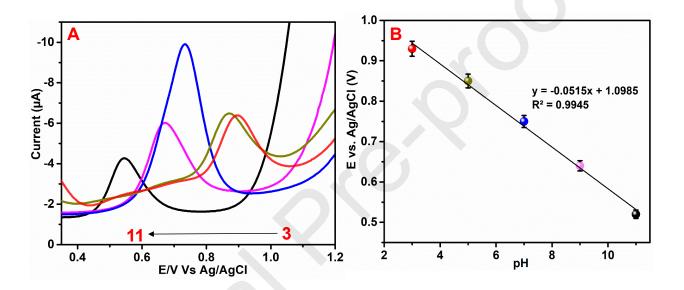


Figure 5. (A) CV responses of 100 μ M of amlodipine in various pH ranging from 3.0 to 11.0 at NiMoO₄/CHIT/GCE (n=3) and (B) calibration plot for anodic peak current/ μ M vs. pH.

3.5. Electrocatalytic determination of amlodipine based on NiMoO₄/CHIT/GCE by DPV

The analytical behavior of NiMoO₄/CHIT/GCE to different additions of amlodipine was investigated also by differential pulse voltammetry (DPV) experiments in 0.05 M phosphate buffer at a scan rate of 50 mV/s (figure 6A). The DPV current response at NiMoO₄/CHIT modified GCE attained for different concentration of amlodipine drug from 0.025 to 373.6 μ M in 0.05 M phosphate buffer at a scan rate of 50 mV/s. The DPV peak responses shown how it is sensitive even at very low concentration (nanomolar). The calibration plot shows that the results

in figure 6B. According to the DPV results, the anodic current intensity is increases linearly towards lower to higher concentration of amlodipine drug. It is evidently seen that the oxidation peaks current of amlodipine increases (0.025 to 373.6 μ M). In figure 6B shows a good linearity between the anodic peak current and concentration of drug with a correlation coefficient (R²) of 0.9941 from the linear regression equation of $I_{pa} = 0.3375x - 0.241$. The limit of detection (LOD) is expressed with $3*S_b/g$ (S_b is the standard deviation of blank sample and g is the slop of the calibration curve). The LOD was obtained 4.62 nM. Furthermore, the sensitivity was evaluated to be 4.753 µA.µM⁻¹.cm⁻². The electrochemical sensor performance of NiMoO₄/CHIT modified GCE was compared with previously reported sensor and results are given in Table 1. The limit of quantification (LOQ) of the enhanced sensor was calculated (24.65 nM) using the equation, LOQ=3*S_b/g. It can be seen that our NiMoO4/CHIT proposed sensor in this work shows improved electrochemical performance of the sensor compared to some of those recently reported electrochemical amlodipine sensors. Compared with conventional electrodes, our modified sensors present several advantages as they are highly versatile, cost-effective, userfriendly, and can be use in on-site detection.

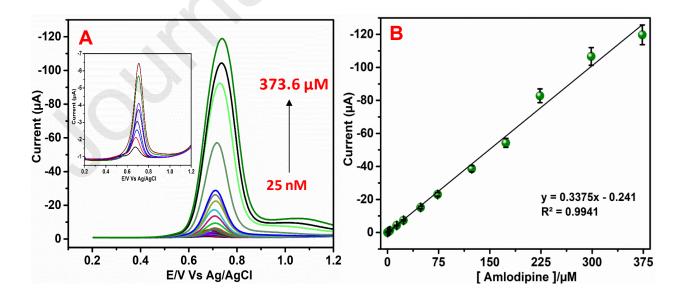


Figure 6. (A) DPV responses of NiMoO₄/CHIT/GCE in phosphate buffer with different concentration of amlodipine. (B) Calibration plot of peak current/ μ A vs. [amlodipine]/ μ M.

Table 1. Comparison between the sensor performance of NiMoO₄/CHIT modified GCE with other previously reported towards amlodipine sensor.

Electrodes	Linear range	Limit of detection	References		
MWCNT/GCE	0.017–0.52 μM	0.009 µM	[46]		
	$0.017 \ 0.02 \ \mu m$	0.000 µ111	[10]		
Carbon nanotubes/GCE	4.3–170 μM	1.7 μM	[47]		
MWCNT/gold electrode	24–34 μM	4.2 μM	[48]		
	2+ 3+ µm	4.2 μινι			
			5403		
boron-doped diamond electrode	6–38 µM	0.07 µM	[49]		
EPPGE	0.005–1 μM	0.001 µM	[50]		
			[6.0]		
CCE	0 1 <i>4</i> 1 M	0.12	[<i>E</i> 1]		
GCE	8.1–41 μM	0.12 µM	[51]		
Fe ₃ O ₄ @SiO ₂ /MWCNT/GCE	0.25–500 μM	0.08 µM	[52]		
	•	•			
Nickel hydroxide/GCE	12.0.167.uM	7 QM	[4]		
NICKEI IIYUIOXIUE/OCE	13.9–167 μM	7.9 µM	[4]		
NiMoO ₄ /CHIT/GCE	0.1 to 374.5 μM	12.74 nM	This work		
	•				
		1			

3.6. Selectivity analysis of amlodipine sensor based on NiMoO₄/CHIT/GCE

To investigate the selectivity of the proposed method, an important parameter for the newly developed electrochemical sensor and the effect of some interfering analyte on the determination of drug was evaluated by DPV method. Selectivity of the NiMoO₄/CHIT modified

electrode to detect amlodipine (ALP) in presence of potential possible interferents such as, dopamine (DA), ascorbic acid (AA), folic acid (FA), uric acid (UA), glucose (Glu), K⁺, Na⁺, Fe²⁺ and H₂O₂ has been studied via DPV method. In figure 7A displays the calibration plot of NiMoO₄/CHIT modified electrode toward 100 μ M of amlodipine and 0.5 mM of aforementioned interfering species. As shown in figure 7A, the electrode quickly responded to the low concentration amounts of amlodipine, while it was not responding to other species even at high concentrations, suggests excellent selectivity of the electrode. The corresponding histogram is also reflect the same observation in a more clear way (Figure 7A). Moreover, figure 7A shows the modified electrode was tested in presence of metal ions (K⁺, Na⁺ and Fe²⁺; 1 mM) and amlodipine concentration was varied in presence of metal ions. The results show that the NiMoO₄/CHIT modified electrode has good selective in presence of metal ions and biological analytes.

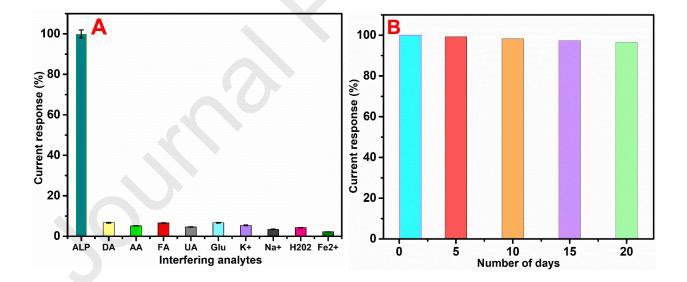


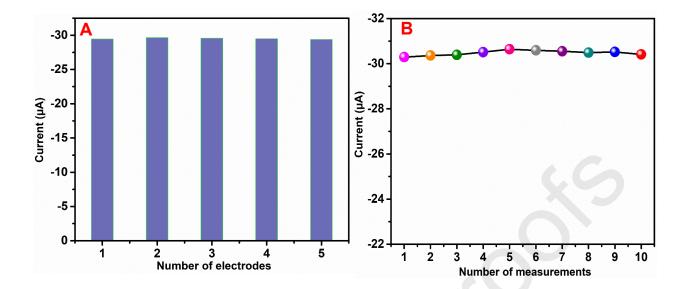
Figure 7. (A) DPVs recorded for amlodipine oxidation in the presence of different interfering compounds (DA-dopamine, AA-ascorbic acid, FA-folic acid, UA-uric acid, Glu-glucose, K⁺,

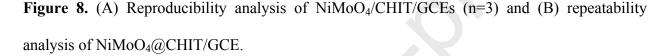
Na⁺, Fe²⁺ and H₂O₂) at NiMoO₄/CHIT/GCE. (B) Stability analysis of NiMoO₄/CHIT/GCE (n=3).

3.7. Reproducibility, repeatability and stability analysis of NiMoO₄/CHIT/GCE

The stability of NiMoO₄/CHIT/GCE was also examined. The DPV experiments were also carried out using the modified electrode once a day under the same operation conditions. In order to ascertain the stability of the proposed electrochemical sensor, the anodic peak current intensity was investigated by DPV for over a period of 20 days at NiMoO₄/CHIT/GCE (figure 7B). The sensor can be kept at room temperature. After 20 days of storage, the obtained peak current response for the modified electrode decreases only by 4.57% from its initial current response. Therefore, the NiMoO₄/CHIT modified sensor retains superior stability as well as excellent applicable electrode material towards the electrochemical oxidation of amlodipine drug.

The reproducibility experiment was analyzed by DPV for four independent NiMoO₄/CHIT modified GCE in 0.05 M phosphate buffer containing 100 μ M of amlodipine drug and its consistent result is shown in figure 8A along with the current response for the oxidation of amlodipine drug is represented as calibration diagram is displayed. The obtained results clearly explained that the developed sensor exhibits outstanding reproducibility with relative standard deviation (RSD) of 3.15%. Besides that, the repeatability test was investigated for identical NiMoO₄/CHIT nanocomposite modified electrode containing 100 μ M of amlodipine drug concentration in PB (pH 7.0) at a scan rate of 50 mV/s, we observed nearly equivalent current response (figure 8B) with less deviation of less than 3.6% for repeated fifteen runs at single NiMoO₄/CHIT modified GCE with RSD of 3.28%. From these studies, it successfully reveals that the good electrochemical sensor possesses predominant performance towards the detection of amlodipine drug.





3.8. Real sample analysis

Practical applicability of the modified electrode was demonstrated in pharmaceutical product and biological samples. Amlodipine tablet samples were collected from a pharmaceutical company and diluted in phosphate buffer pH 7.0. Then, the resulting samples are analyzed by DPV and then known amounts of amlodipine were spiked to prepare stock real sample solution. Afterwards, aliquots (each 5, 25 and 50 μ M) of lab sample and spiked drug samples were injected into the supporting electrolyte. The electrode delivered prompt and stable sensor responses toward each addition of real samples. The amount of amlodipine added, found and recovery are calculated and given in Table 2. They are in the agreeable analytical range, indicating the suitably of the method in analyzing amlodipine in drug samples. The same sets of experiments were carried out using human serum samples in parallel, and the obtained results are given in Table 2. The biological samples were collected from Chang Gung Memorial Hospital.

Samples	Added (µM)	Found (µM)	Recovery (%)	RSD (%)
				(n=3)
Urine	5	4.76	95.2	3.16
	25	23.61	94.44	2.68
	50	47.11	94.22	3.49
amlodipine	5	4.68	93.6	3.28
tablet	25	24.19	96.76	3.62
	50	48.37	96.74	2.94

Table 2. Determination of amlodipine in real sample analysis in biological and pharmaceutical samples

4. Conclusion

In this research, we have synthesized more potential nanosheets like nickel molybdate by simple sonochemical method. A simple, novel and low-cost electrochemical sensor for the rapid determination of amlodipine using NiMoO₄/CHIT nanocomposite was developed. The morphological and surface properties of as-synthesized NiMoO₄/CHIT nanocomposite samples were characterized by XRD pattern, SEM, TEM, EDX and mapping analysis. Furthermore, the NiMoO₄/CHIT/GCE was scrutinized for the electrochemical sensing of amlodipine. Fascinatingly, the developed sensor retains higher electrocatalytic activity with low LOD, LOQ, wide linear range, excellent selectivity, reproducibility and repeatability. Upon considering the above-obtained results, the as-synthesized nanocomposite could be utilized for futurity electrochemical applications including biosensor and practical pharmaceutical analysis.

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Conflict of interest

The authors declare that they have no conflicts of interest to this research work.

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Research highlights

- ➤ A facile and green sonochemical synthesis of NiMoO₄/CHIT nanocomposite
- > The nanocomposite was characterized by SEM, TEM, EDX, XRD and CV
- The obtained NiMoO₄/CHIT NC applied to the electrochemical detection of calcium channel blocker drug (amlodipine)
- The modified sensor has explored high sensitivity and nanomolar detection limit towards amlodipine drug