

## Synthesis and evaluation of stilbenylbenzoxazole and stilbenylbenzothiazole derivatives for detecting $\beta$ -amyloid fibrils

Ji Hoon Lee,<sup>a,b</sup> Seong Rim Byeon,<sup>a</sup> Soo Jeong Lim,<sup>c</sup> Seung Jun Oh,<sup>c</sup> Dae Hyuk Moon,<sup>c</sup> Kyung Ho Yoo,<sup>a</sup> Bong Young Chung<sup>b,\*</sup> and Dong Jin Kim<sup>a,\*</sup>

<sup>a</sup>Center for Chemoinformatics Research, Korea Institute of Science and Technology,  
PO Box 131, Cheongryang, Seoul 130-650, Republic of Korea

<sup>b</sup>Department of Chemistry, Korea University, Anam-dong, Seongbuk-Gu, Seoul 136-701, Republic of Korea

<sup>c</sup>Asan Medical Center, Department of Nuclear Medicine, 388-1, Pungnap-2-Dong, Songpa-Gu, Seoul 138-736, Republic of Korea

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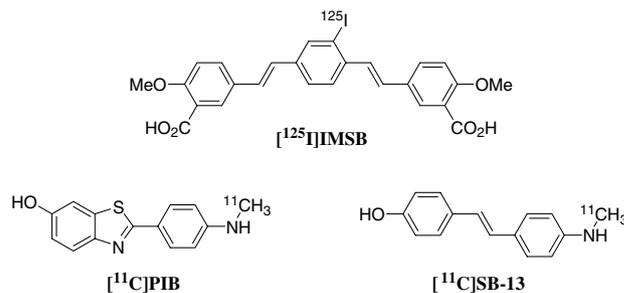
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**Abstract**—This paper describes a novel series of stilbenylbenzoxazole (SBO) and stilbenylbenzothiazole (SBT) derivatives for  $\beta$ -amyloid specific binding probes. These 24 compounds were synthesized and evaluated by competitive binding assay against  $\beta$ -amyloid 1–42 (A $\beta$ 42) aggregates using [<sup>125</sup>I]TZDM. All the derivatives displayed higher binding affinities with  $K_i$  value in the subnanomolar range (0.10–0.74 nM) than Pittsburgh Compound-B (PIB) (0.77 nM). Among these derivatives, **SBT-2**, 5-fluoroethoxy-2-{4-[2-(4-methylaminophenyl)vinyl]phenyl}benzothiazole, showed lowest  $K_i$  value (0.10 nM). In conclusion, the preliminary results suggest that these compounds are implying a possibility as a probe for detection of A $\beta$  fibrils in Alzheimer's disease (AD) patients. © 2007 Elsevier Ltd. All rights reserved.

Alzheimer's disease (AD) is a neurodegenerative disease characterized as progressive memory loss and decrease of cognitive function. In 1907, the first demented patient was identified to have senile plaques (SPs) of  $\beta$ -amyloid protein (A $\beta$ ) aggregates and neurofibrillary tangles (NFTs) formed of highly phosphorylated tau proteins in the post-mortem brain tissue.<sup>1–3</sup> Since then, SPs and NFTs have become the two major pathological hallmarks characteristic of AD and provided the basic for the definitive diagnosis of AD. However, yet the diagnosis of this disease based on neurological observations is often difficult and unreliable. Therefore, an increasing focus on early identification and prevention highlights a need for simpler diagnostic tools and robust biological markers. At present, the A $\beta$ -aggregate-specific radiolabeled imaging agents, using single photon emission computed tomography (SPECT) or positron emission tomography (PET), are needed for early detection or monitoring of the progression and effectiveness of AD treatment.<sup>4–6</sup> A number of groups have studied to develop A $\beta$ -specific binding probes, however those efforts have been limited by low levels of specific binding in

brain regions and poor blood–brain barrier (BBB) penetration.

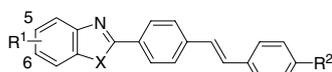
Recently, *N*-methyl-[<sup>11</sup>C]2-(4'-methylaminophenyl)-6-hydroxybenzothiazole ([<sup>11</sup>C]PIB),<sup>7,8</sup> *E,E*-1-iodo-[<sup>125</sup>I]2,5-bis(3-hydroxycarbonyl-4-methoxy)styrylbenzene ([<sup>125</sup>I]-IMSB),<sup>9,10</sup> and [<sup>11</sup>C]4-*N*-methylamino-4'-hydroxystilben ([<sup>11</sup>C]SB-13)<sup>11,12</sup> displayed high binding affinities toward A $\beta$  aggregates. PIB, a modified molecule of thioflavin-T (Th-T), exhibited that neutral benzothiazole–aniline derivatives could bind to amyloid with low nanomolar affinity, enter brains in sufficient amounts for imaging via PET, and clear rapidly from normal brain in animal studies (Fig. 1).



**Figure 1.** Structures of IMSB, PIB, and SB-13.

**Keywords:** Alzheimer's disease;  $\beta$ -Amyloid fibrils; PET imaging.

\* Corresponding authors. Tel.: +82 2 958 5142; fax: +82 2 958 5189; e-mail: dj2991@kist.re.kr



SBO-1~12, SBT-1~12

SBO-1 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH <sub>2</sub>	SBT-1 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH <sub>2</sub>
SBO-2 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )	SBT-2 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )
SBO-3 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>	SBT-3 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>
SBO-4 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH <sub>2</sub>	SBT-4 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH <sub>2</sub>
SBO-5 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )	SBT-5 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )
SBO-6 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>	SBT-6 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>2</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>
SBO-7 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH <sub>2</sub>	SBT-7 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH <sub>2</sub>
SBO-8 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )	SBT-8 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )
SBO-9 : X=O, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>	SBT-9 : X=S, R <sup>1</sup> =5-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>
SBO-10 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH <sub>2</sub>	SBT-10 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH <sub>2</sub>
SBO-11 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )	SBT-11 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =NH(CH <sub>3</sub> )
SBO-12 : X=O, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>	SBT-12 : X=S, R <sup>1</sup> =6-O(CH <sub>2</sub> ) <sub>3</sub> F, R <sup>2</sup> =N(CH <sub>3</sub> ) <sub>2</sub>

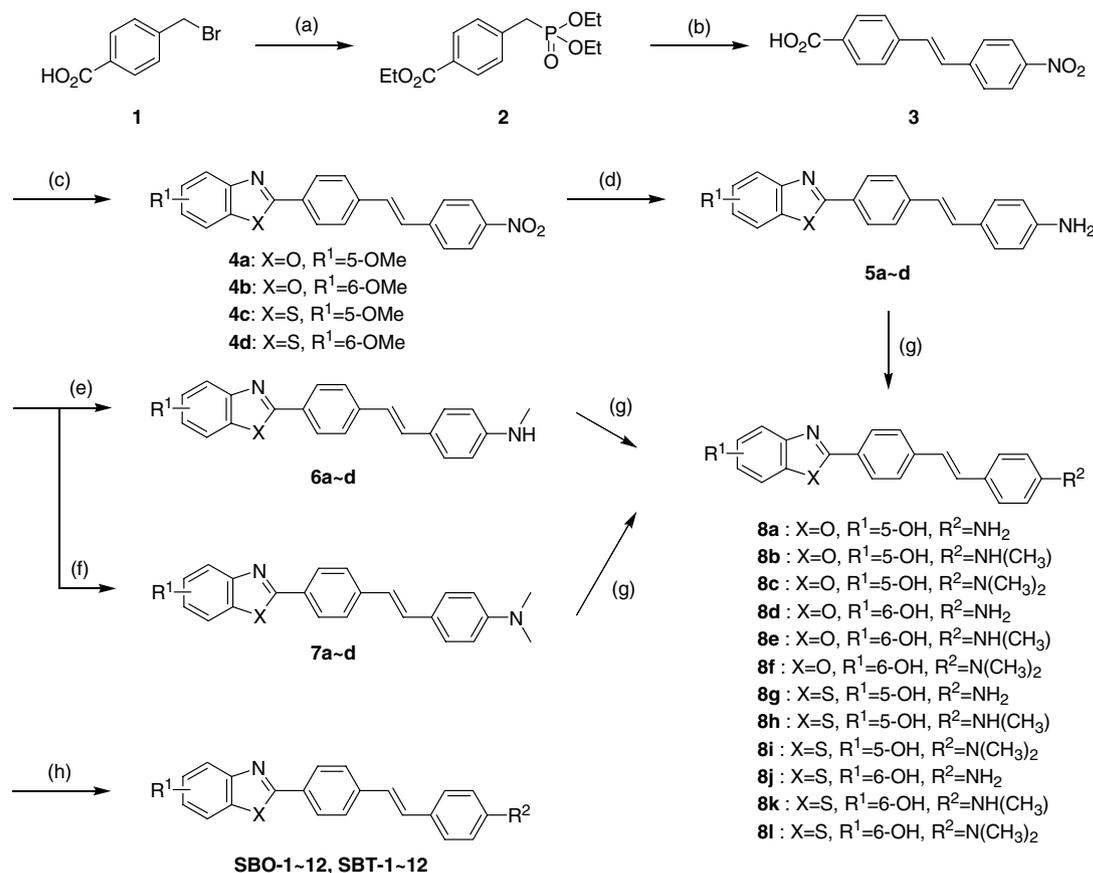
Figure 2. Structures of SBO and SBT derivatives.

However labeling of <sup>11</sup>C radioisotope is limited to short half-life ( $t_{1/2} = 20$  min). SB-13 demonstrated similar binding properties to those of PIB. IMSB showed lower initial brain uptake in normal mice (0.14% ID/organ at 5 min after injection) than radioiodinated Th-T derivatives (0.6–3.5% ID/organ at 2 min), but it displays potent binding affinities for A $\beta$  aggregates.

Our focus was that a sufficient amount of an imaging agent should internalize into the brain to bind to the

target. The agent should have adequate affinity toward the target and show rapid clearance of free and nonspecific bound compounds from the brain. Based on the backbone structures of PIB and SB-13, we have successfully developed highly conjugated SBO and SBT derivatives (Fig. 2). Due to the short half-life of <sup>11</sup>C, to broaden the utility of a PET imaging agent, we have then focused our effort on developing <sup>18</sup>F-labeled imaging agent ( $t_{1/2} = 110$  min). In the beginning, we designed fluoroethyl and fluoropropyl substituted SBO, SBT derivatives. All the synthesized compounds were evaluated by competitive binding assays against A $\beta$  aggregates using [<sup>125</sup>I]TZDM.

The synthesis of SBO and SBT derivatives is outlined in Scheme 1. The first step of synthetic 4-(diethoxyphosphorylmethyl)benzoic acid ethyl ester was achieved with 4-(bromomethyl)benzoic acid and triethylphosphite via Arbuzov reaction.<sup>13</sup> Compound 3 was readily prepared from compound 2 and 4-nitrobenzaldehyde via Horner–Wadsworth–Emmons reaction and hydrolysis. The key step for the formation of the benzoxazole and benzothiazole backbones was accomplished via the intramolecular cyclization reaction<sup>14</sup> between compound 3 and 2-aminophenol or 2-aminothiophenol derivatives.<sup>15</sup> The free amino derivatives, compounds 5a–d were prepared from the nitro compounds 4a–d via reduction



Scheme 1. Synthesis of SBO and SBT derivatives. Reagents and conditions: (a) P(OEt)<sub>3</sub>, 140 °C, 20 h; (b) i)—4-nitrobenzaldehyde, NaH, THF, rt, 2 h; ii)—NaOH, MeOH/H<sub>2</sub>O, reflux, 2 h; (c) i)—thionyl chloride, reflux, 1 h; ii)—2-aminophenol or 2-aminothiophenol derivatives, *N,N*-dimethylaniline, monochlorobenzene, reflux, 1 h; iii)—*p*-TsOH, trichlorobenzene, reflux, 8 h; (d) SnCl<sub>2</sub>, EtOH, reflux, 24 h; (e) *p*-formaldehyde, NaOMe, MeOH/THF, NaBH<sub>4</sub>, reflux, 3 h; (f) *p*-formaldehyde, NaBH<sub>3</sub>CN, AcOH, rt, 12 h; (g) BBr<sub>3</sub>, CH<sub>2</sub>Cl<sub>2</sub>, reflux, 12 h; (h) 1-fluoro-2-tosyloxyethane or 1-fluoro-3-tosyloxypropane, K<sub>2</sub>CO<sub>3</sub>, DMF, 90 °C, 2 h.

**Table 1.**  $K_i$  values of **SBO** and **SBT** derivatives against [ $^{125}$ I]TZDM for binding affinities to A $\beta$ 42 aggregates

Compound	$K_i^a$ (nM)
<b>SBO-1</b>	0.32
<b>SBO-2</b>	0.74
<b>SBO-3</b>	0.44
<b>SBO-4</b>	0.47
<b>SBO-5</b>	0.50
<b>SBO-6</b>	0.45
<b>SBO-7</b>	0.45
<b>SBO-8</b>	0.47
<b>SBO-9</b>	0.45
<b>SBO-10</b>	0.59
<b>SBO-11</b>	0.68
<b>SBO-12</b>	0.46
<b>SBT-1</b>	0.41
<b>SBT-2</b>	0.10
<b>SBT-3</b>	0.35
<b>SBT-4</b>	0.59
<b>SBT-5</b>	0.52
<b>SBT-6</b>	0.57
<b>SBT-7</b>	0.42
<b>SBT-8</b>	0.38
<b>SBT-9</b>	0.49
<b>SBT-10</b>	0.55
<b>SBT-11</b>	0.48
<b>SBT-12</b>	0.12
<b>PIB</b>	0.77

<sup>a</sup>  $K_i$  was calculated by the Cheng–Prusoff equation ( $K_i = IC_{50}/(1 + [L]/K_d)$ )<sup>20</sup> using *Graphpad Prism* software.

with SnCl<sub>2</sub>. Conversion of compounds **5a–d**, to the monomethylamino derivatives, compounds **6a–d**, was achieved via a method previously reported.<sup>16</sup> Compounds **5a–d** were also converted to the dimethylamino derivatives, compounds **7a–d**, via an efficient method with paraformaldehyde, sodium cyanoborohydride, and acetic acid.<sup>17,18</sup> The *O*-methyl group of compounds **5a–d**, **6a–d**, and **7a–d** was removed by reacting with BBr<sub>3</sub> to give compounds **8a–8l**. The desired **SBO** and **SBT** derivatives were prepared from compounds **8a–8l** and 1-fluoro-2-tosyloxyethane or 1-fluoro-3-tosyloxypropane by a nucleophilic substitution reaction.<sup>19</sup>

Specific binding affinities of synthesized compounds to A $\beta$  fibrils were evaluated by an in vitro A $\beta$  fibril binding assay. In vitro competitive binding assay using preformed A $\beta$ 42 aggregates demonstrated that **SBO-1–12**, **SBT-1–12** competed against radioligand such as [ $^{125}$ I]TZDM.<sup>21–23</sup>

The result shown in Table 1 demonstrates that most of the synthesized compounds displayed lower  $K_i$  values ( $K_i = 0.10–0.74$  nM) than PIB compound. In the structure–activity relationship, **SBO** and **SBT** derivatives did not show significant difference of binding affinity. Furthermore, 5-position compounds were slightly better than 6-position compounds. Among them, 5-fluoroethyl substituted **SBT-2**<sup>24</sup> compound exhibited the highest binding affinity.

In conclusion, a series of novel fluoroethyl and fluoro-propyl substituted **SBO**, **SBT** compounds were success-

fully synthesized. These **SBO** and **SBT** derivatives displayed excellent binding affinities to A $\beta$  aggregates. In particular, **SBT-2** exhibited the best binding affinity ( $K_i = 0.10$  nM) implying a possibility as a probe for detection of A $\beta$  fibrils in AD brain. Based on the result, further studies on synthesis and in vivo pharmacokinetics of <sup>18</sup>F-labeled compounds are progressing for the development of AD imaging probe.

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23. We estimated  $K_d$  value (0.13 nM) of [ $^{125}$ I]TZDM for A $\beta$ 42 aggregates. For inhibition studies, the reaction mixture contained 50  $\mu$ L of A $\beta$ 42 aggregates (11.5 nM in the final concentration), 50  $\mu$ L of inhibitors ( $10^{-6}$ – $10^{-12}$  M in DMSO), 50  $\mu$ L of [ $^{125}$ I]TZDM (in 40% EtOH, 0.05 nM in the final concentration), and 10% EtOH in a final volume of 1 mL. Nonspecific binding was defined by adding 2  $\mu$ M Th-T for [ $^{125}$ I]TZDM binding. The mixture was incubated at room temperature for 3 h and the bound and the free radioactivity were separated by a vacuum filtration through Whatman GF/B filters using a Brandel M-24R cell harvester followed by 2 $\times$  3 mL washes of 10% EtOH at room temperature. Filters containing the bound radioligand were counted in a gamma-counter (Cobra-II). The result of inhibition assays was subjected to nonlinear regression analysis using software *Graphpad Prism* by which  $K_i$  values were calculated.
24. Selected data. **SBT-2**:  $^1\text{H}$  NMR (DMSO- $d_6$ , 300 MHz)  $\delta$  2.71 (d,  $J = 4.9$  Hz, 3H), 4.36 (dt,  $J = 4.0$ , 30.3 Hz, 2H), 4.80 (dt,  $J = 4.0$ , 47.9 Hz, 2H), 6.01 (s, NH), 6.56 (d,  $J = 8.4$  Hz, 2H), 7.00 (d,  $J = 16.1$  Hz, 1H), 7.12 (d,  $J = 9.1$  Hz, 1H), 7.26 (d,  $J = 16.5$  Hz, 1H), 7.41 (d,  $J = 8.3$  Hz, 2H), 7.63 (s, 1H), 7.68 (d,  $J = 8.0$  Hz, 2H), 8.01 (d,  $J = 8.2$  Hz, 1H), 8.01 (d,  $J = 8.2$  Hz, 2H);  $^{13}\text{C}$  NMR (DMSO- $d_6$ , 300 MHz)  $\delta$  29.98, 67.85, 81.51, 106.73, 112.11, 115.84, 122.03, 123.19, 124.56, 126.55, 126.85, 127.82, 128.59, 131.17, 131.72, 141.63, 150.66, 155.45, 158.16, 168.87; HRMS  $m/z$  Calcd for  $\text{C}_{24}\text{H}_{22}\text{FN}_2\text{OS}$  (M) $^+$  405.1431. Found: 405.1433.