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In Vivo Chemiluminescent Imaging Agents for Nitroreductase and Tissue Oxygenation

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ABSTRACT: Tissue oxygenation is a driving parameter of the tumor microenvironment and hypoxia can be a prognostic indicator of aggressiveness, metastasis, and poor response to therapy. Here we report a chemiluminescence imaging (CLI) agent based on the oxygen-dependent reduction of a nitroaromatic spiroadamantane 1,2-dioxetane scaffold. Hypoxia ChemiLuminescent Probe 2 (HyCL-2) responds to nitroreductase with ~170-fold increase in luminescence intensity and high selectivity for enzymatic reductase versus other small molecule reductants. HyCL-2 can image exogenous nitroreductase *in vitro* and *in vivo* in living mice and total luminescent intensity is increased by ~5-fold under low oxygen conditions. HyCL-2 is demonstrated to report on tumor oxygenation during oxygen challenge in H1299 lung tumor xenografts grown in a murine model as independently confirmed using multi-spectral optoacoustic tomography (MSOT) imaging of hemoglobin oxygenation.

Introduction

Hypoxia refers to a physiological state of low tissue oxygenation and is a pathogenic characteristic of solid tumors that arises from absent or abnormal vasculature in the tumor microenvironment.¹⁻⁴ Cancer cell populations respond to hypoxia by promoting survival pathways to suppress apoptosis⁵ and initiate angiogenesis,⁶ invasiveness,7 and metastasis.8 A key event initiated by low oxygen levels is the activation of the transcription factor hypoxia inducible factor 1 (HIF1). The HIF1- α subunit remains inactive through oxygen-dependent enzymatic hydroxylation of specific residues.⁹ In the absence of oxygen, however, HIF-1a dimerizes with the HIF-1ß subunit and induces transcription of a host of proteins to support cancer cell survival.¹⁰ Activating prodrugs and imaging agents in a similar oxygen-dependent manner is an attractive strategy for imaging¹¹ and treatment of cancer.¹²⁻¹⁴

Following this idea, the oxygen-dependent reduction of aromatic nitro groups by reductive mammalian enzymes, including xanthine oxidase, NADPH-cytochrome c reductases, and potentially cytosol DT diaphorase, aldehyde oxidase, and lipoyl dehydrogenase, ¹⁵⁻¹⁸ is now a wellestablished method to target drugs, ^{2,12} imaging agents like FMISO,^{11,19-22} and immunohistochemical stains like pimonidazole²³ to hypoxic areas. These targeting strategies have been cross-validated in comparison to other methods for direct measurement of tissue oxygenation including pO₂ electrodes,²⁴ magnetic resonance imaging (MRI) of ¹⁹F-labeled perfluorocarbons,^{25,26} dynamic contrast en-

hanced MRI,^{27,28} tissue²⁹⁻³² or blood³³⁻³⁵ oxygen level dependent (TOLD or BOLD) MRI, MRI-based oxygen imaging (MOXI),³⁶ and multispectral optoacoustic tomography (MSOT) imaging of hemoglobin and oxygenated hemoglobin.³⁷⁻⁴⁰ These techniques offer significant clinical opportunity, but require expensive instrumentation and highly trained experts that increase the cost and lower the throughput of these technologies.

Optical methods can provide a cheaper alternative to MRI and PET imaging methods. In recent years, small molecule fluorescence imaging agents have been developed that take advantage of the reduction of azobenzene, nitrobenzene, nitrofuran, and nitroimidazole functional groups to release a caged fluorescent dye.41-49 Despite progress towards in vivo hypoxia imaging with nearinfrared emitting fluorophores, complications arising from autofluorescence, background, and light scattering remain problematic. Bioluminescent substrates for nitroreductase have been developed and have found application for imaging bacterial infection and cancer cells engineered to express bacterial nitroreductase.⁵⁰⁻⁵² Although they display increased signal to background in comparison to fluorescent probes, these systems require expression or exogenous addition of luciferase and emit light through an oxygen-dependent process, complicating the development of caged luciferin probes for hypoxia imaging.

Considering these outstanding challenges for optical imaging of the tumor microenvironment, we have begun

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to develop chemiluminescent imaging (CLI) agents that can be applied in luciferase-null organisms for imaging a diverse set of parameters.^{53,54} Chemiluminescence results from the formation of an excited state product during an exothermic chemical reaction⁵⁵ and is emerging as a useful preclinical in vivo imaging modality. 56-59 Triggered chemiluminescence emission of spiroadamantane 1,2dioxetanes has been extensively used for clinical assays⁶⁰⁻ ⁶⁵ and analyte sensing⁶⁶⁻⁶⁹ and has been recently demonstrated as an effective in vivo imaging modality for β galactosidase53 and H2S.54 The high-energy 4-membered dioxetane ring can be sterically stabilized by synthetically appending spiroadamantane,^{60,66} fenchyl, ⁷⁰ or other frameworks, allowing for purification, synthetic manipulation, and long term storage. These systems can be designed such that a chosen chemical trigger will initiate an electron transfer cascade that leads to dioxetane ring cleavage. The reaction proceeds through a high-energy transition state that populates the excited state of the product, releasing the energy as light upon relaxation to the ground state.55 This energy can be further transferred to red-shifted dye molecules more suitable for biological imaging.⁷¹⁻⁷⁴ Direct production of light from the energy of a chemical bond offers important advantages over fluorescence imaging by eliminating light excitation of a contrast agent, thereby providing reduced autofluorescence and light scattering. On the basis of these considerations and expanding the toolbox of chemiluminescent imaging methods for nitroreductase and hypoxia, we report the development of a spiroadamantane 1,2-dixoetane-based chemiluminescent platform, Hypoxia ChemiLuminescent Probes 1 and 2 (HyCL-1 and HyCL-2) for imaging tumor oxygenation in living animals.

Experimental section

Spectroscopic Measurements. UV/Vis spectra were acquired on a Beckman-Coulter DU 800 Spectrometer (Beckman Coulter, Inc., Brea, CA). Chemiluminescent responses were acquired using a Hitachi F-7000 Fluorescence Spectrophotometer (Hitachi, Tokyo, Japan) using the luminescence detection module and setting emission wavelength to 545 nm. 889 µL of a 10 mM PBS buffered to pH 7.4, 2 µL of a 5 mM HyCL-1 or HyCL-2 in DMSO, 8 µL of a 50 mM NADH in 0.01 mM NaOH solution, 1.4 µL of nitroreductase from Escherichia coli (NTR, Sigma-Aldrich N9284-1MG) in DI-H₂O (1 mg NTR dissolved in 100 µL DI-H₂O, 10 mg/mL), and 100 µL Emerald II Enhancer (Life Technologies, Carlsbad, CA) were added to an Eppendorf tube and samples were shaken gently to assure mixing. The mixed solution was then transferred to a quartz cuvette (Starna, Atascadero, CA). Time scans were acquired using the time scan module 1 min after adding probes. For the dose-dependent response to nitroreductase, 10 µM HyCL-1 or HyCL-2 were treated with 8 µL of a 50 mM NADH and 0, 0.5, 0.75, 1.0, 1.25, 1.4 µL 10 mg/mL nitroreductase and 20 min (Figure 1, S9) or 120 min (Figure S3) time scans were measured 1 min after adding probes. Selectivity for HyCL-1 and HyCL-2 was measured by monitoring the time-dependent chemiluminescent emission at 545 nm. All assays were performed in 10 mM PBS buffered

to pH 7.4 with 10% Emerald II Enhancer. Further details can be found in the supporting information.

In vitro deoxygenation experiments. 10 mM PBS buffer (pH 7.4) and Emerald II Enhancer were mixed with a ratio of 9 to 1 and N₂, air, or 100% O₂ was bubbled through it for 60 minutes. The solution was then transferred into a capped cuvette by syringe, and HyCL-2, NADH, and nitroreductase were added using a syringe. Time scans were performed 1 min after adding nitroreductase. For deoxygenation experiments, PBS buffer (pH 7.4) and Emerald II Enhancer mixture was deoxygenated by bubbling N, for 60 minutes, and then 889 µL of this deoxygenated mixture was transferred into a capped cuvette by syringe, and later 2 µL of a 5 mM HyCL-2 in DMSO, 8 µL of a 50 mM NADH in 0.01 mM NaOH solution, 1.25 µL of nitroreductase (10 mg/mL) were added into the cuvette using syringe. Time scans were performed 1 min after adding nitroreductase. The control experiment was carried out under ambient conditions without deoxygenation.

In vitro chemiluminescent imaging. Imaging was carried out with a Caliper Xenogen IVIS® Spectrum (Perkin-Elmer, Santa Clara, CA) in black 96-well Costar® plates and all the images were analyzed using Living Image 3.1 software. 1 mM HyCL-2 in DMSO, 2 mg/mL nitroreductase (10 µL from 1 mg NTR/100 uL DI-H₂O diluted to 50 µL by adding 40 µL DI-H2O) and 50 mM NADH in 0.01 mM NaOH solution were prepared prior to imaging. 176.4 µL, 176.1 µL, 175.9 µL, 175.5 µL 175.4 µL and 175.1 µL of 10 mM PBS buffer (pH 7.4) were added into wells from A1 to A6 in sequence, 1.6 µL NADH was pipetted into each well and then different volume of nitroreductase solution (0 µL, 0.25 µL, 0.5 µL, 0.75 µL, 1.0µL, 1.25 µL) were added into each well. 2 µL HyCL-2 was injected into the mixture and 20 µL Emerald II Enhancer was pipetted into each well, and imaging was performed 3.45 minutes after adding reagents into the 96 well plate using an open filter. All images were acquired with f-stop 1, medium binning, auto exposure and the chamber set to 37 °C. The detection limit was determined from the linear plot of NTR concentration versus total photon flux as the amount of nitroreductase required to give a chemiluminescent signal above three times the standard deviation of at least 3 independent experiments with o µg/mL nitroreductase. These provided detection limits of 9.6 ng/mL with measurements taken 30 sec after reagent addition and 1.9 ng/mL with measurements taken 30 min after reagent addition.

General animal protocols. The UT Southwestern Institutional Animal Care and Use Committee approved these investigations under Animal Protocol Number (APN #2009-0150). Hair was removed from area surrounding the tumor using Nair (Church & Dwight Co, Inc, Ewing, NJ), but the skin was left unbroken before injection. Mice were anesthetized and maintained using inhalation of 1.6% isoflurane in 16% oxygen gas.

In vivo CLI of nitroreductase. A stock solution of 5 mM HyCL-2 in DMSO, 1 mg nitroreductase dissolved in 100 μ L DI-H₂O and 50 mM NADH in 0.01 mM NaOH solution were prepared in advance. A 30 μ L aliquot of this

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59 60 solution was taken out from a mixture of 437 μL 10 mM PBS, 4 μL HyCL-2, 8 μL NADH, 1.25 μL NTR and 50 μL Emerald II Enhancer and images were acquired 30 sec after administering subcutaneous injections to anesthetized (1.6% isoflurane) SCID/BALB-C mice. A vehicle control was conducted in the same way except replacing nitroreductase and NADH with H₂O and 0.01 M NaOH, respectively.

In vivo **CLI of hypoxia in tumor xenografts.** A 100 µL solution was taken out from a mixture of 446 µL 10 mM PBS, 50 µL Emerald II Enhancer and 4 µL 5 mM **HyCL-2** and images were acquired immediately and every minute after administering intratumoral injections to H1299 lung tumor xenografts on mice while the animals breathed ambient air. A similar experiment was performed in the same mice, but while breathing 100% oxygen 5 minutes before injection and 1.6% isoflurane and 98.4% oxygen throughout the course of the imaging experiment. These experiments were reproduced on two different mice (n = 2). Tumor sizes were 9.9 mm x 6.4 mm x 5.5 mm and 9.5 mm x 7.6 mm x 6.0 mm.

Multispectral optoacoustic tomography (MSOT). A thin layer of ultrasound coupling gel provided contact with the membrane and the animal holder was placed in the imaging chamber of the MSOT 256-TF device (iThera Medical Gmbh, Munich, Germany). Multi-spectral optoa-coustic tomography (MSOT) imaging was performed in a transaxial section through the center of the tumor using five wavelengths: 715, 730, 760, 800, and 850 nm. Twenty frames per wavelength were acquired and averaged. Initially, the tumor region was imaged while breathing 16% oxygen, which was switched to 100% oxygen. A model-based reconstruction was used prior to multispectral processing to provide relative concentrations of oxyhemoglo-bin and deoxyhemoglobin. These experiments were reproduced on two different mice (n = 2).

Results and Discussion

A spiroadamantane 1,2-dioxetane scaffold was selected for the chemiluminescent-based probe design because it (1) displays instantaneous light production under biologically compatible conditions, (2) does not require the addition of oxidative species like hydrogen peroxide, and (3) the scaffold has demonstrated potential for in vivo imaging.53,54 Our strategy for designing these reaction-based chemiluminescent probes relies on tethering a paranitrobenzyl moiety to a 1,2-dioxetane chemiluminescent scaffold via carbonate or ether linkage (Scheme 1). The nitroaromatic group is sensitive to nitroreductase enzymes and has been frequently used in prodrugs and hypoxia detection. The synthesis of HyCL-1 proceeds from the previously reported phenol 1⁵⁴ by dimethylaminopyridine-catalyzed coupling with the mixed Nhydroxysuccinimidyl carbonate 2 to form the enol ether precursor 3 (Scheme 2). For HyCL-2, the ether linkage of the precursor was prepared by a Mitsunobu reaction⁷⁵ between the phenol 1 and para-nitrobenzyl alcohol 4 to form the enol ether precursor 5 (Scheme 2). Both enol ethers 3 and 5 were subjected to [2+2] cycloaddition with

Scheme 1. Spiroadamantane 1,2-dioxetanes for chemiluminescent nitroreductase (NTR) detection at neutral pH.



Scheme 2. Synthesis of HyCL-1 and HyCL-2.



photogenerated singlet oxygen using rose bengal as a sensitizer to provide **HyCL-1** and **HyCL-2** after purification by silica chromatography. Under hypoxic conditions or in the presence of nitroreductase, the *para*-nitrobenzyl moiety will be reduced, and then chemiluminescent emission will be initiated by self-immolative carbonate or ether cleavage to release the free phenolate bearing the 1,2dioxetane (Scheme 1). The negatively charged phenol unit spontaneously triggers dioxetane cleavage and light emission through a series of electron transfer events.⁷⁶

After obtaining HyCL-1 and HyCL-2, we proceeded to collect their absorption (Figure S1) and emission (Figure S2) spectra and measure their luminescent responses to bacterial nitroreductase in the presence of reduced nicotinamide adenosine dinucleotide (NADH) as a cofactor, a commonly employed model for reductase-activated probes.⁴¹ Nitroreductase-dependent chemiluminescence was first evaluated in PBS (10 mM, pH 7.4) buffer containing 10% Emerald II Enhancer using an F-7000 Hitachi spectrophotometer. The Emerald II Enhancer is a commercial aqueous solution that contains a proprietary cationic polymer and a dye with optical properties similar to fluorescein, with a peak absorption at 505 nm (Figure S1). Treatment of 10 µM of HyCL-1 or HyCL-2 with 14 µg/ml nitroreductase, 0.4 mM NADH, and 10% Emerald II Enhancer resulted in instantaneous and robust luminescent emission with two peaks centered at 455 nm and 545 nm, which correspond to the emission wavelengths of the



Figure 1. Time scans of the chemiluminescent emission at 545 nm from (a) 10 μ M HyCL-1 and (b) 10 μ M HyCL-2 and 0, 2.5, 5, 7.5, 10, 12.5, 14 μ g/mL nitroreductase (NTR) in the presence of 0.4 mM NADH in 10 mM PBS buffer (pH 7.4) containing 10% Emerald II Enhancer.

phenolate and the fluorescein-based Emerald II Enhancer, respectively (Figure S2). This light production increased over a course of 60 minutes (Figure S₃) to provide a ~5fold and ~170-fold luminescence turn-on for HyCL-1 and HyCL-2, respectively (Figure 1). We also found that the chemiluminescent emission enhancement was dosedependent with respect to nitroreductase, demonstrating that both probes could be applied for sensitive nitroreductase detection. A linear response was found between o-14 µg/mL nitroreductase (Figure S4). This dosedependence of light emission is observed immediately, revealing an advantage of using chemiluminescence probes for quick and direct nitroreductase detection without extensive incubation times. Chemiluminescent response data indicated that the ether-linked HyCL-2 displayed a much lower background emission (Figure 1b, red scan) compared with the carbonate linked HyCL-1 (Figure 1a, red scan). The reaction between HyCL-2, NADH, and NTR was analyzed by GC-MS, confirming the generation of 2-adamantanone (Figure S5) and methyl 4chloro-3-hydroxybenzoate (Figure S6), which provided fragmentation patterns that matched the spectra found in the NIST database. A molecular ion at m/z = 121 was also observed that was assigned to 4-methylenecyclohexa-2,5dien-1-one oxime (Figure S7). A high abundance peak at m/z = 123 (aminobenzyl alcohol) was not observed. Taken together these observations are consistent with previous reports that the nitro group is initially reduced to a hydroxylamine,^{52,77} followed by self-immolative cleavage to the chemiluminescent dioxetane phenolate.

We tested the selectivity of **HyCL-1** and **HyCL-2** against other biologically relevant molecules, particularly nucleophilic thiols, which are ubiquitous in physiological systems and involved in various redox cycles. The response



Figure 2. Chemiluminescent responses of (a) 10 μ M HyCL-1 and (b) 10 μ M HyCL-2 to biologically relevant analytes in 10 mM PBS buffer (pH 7.4) containing 10% Emerald II Enhancer. Bars represent chemiluminescent emission at 545 nm and 4, 8, 12, 16, 20 min after addition of reducing agents. Data shown are for 5 mM glutathione, 1 mM cysteine and homocysteine, and 200 μ M for other reducing agents. (1) NTR and NADH; (2) glutathione; (3) L-cysteine; (4) homocysteine; (5) DTT; (6) NTR; (7) NADH; (8) H₂S; (9) citrate; (10) Na₂S₂O₅; (11) L-ascorbic acid; (12) blank.



Figure 3. Integrated chemiluminescent emission in the presence (red bars) and absence (green bars) of oxygen over 20 min of 10 μ M HyCL-2 and 0, 5, 10, and 12.5 μ g mL⁻¹ NTR in 10 mM PBS buffer (pH 7.4) containing 0.4 mM NADH and 10% Emerald II Enhancer (n = 3). Error bars are ±S.D.

of HyCL-1 or HyCL-2 (10 μ M) to 14 μ g/mL nitroreductase and 0.4 mM NADH with 10% Emerald II Enhancer was monitored against other biological species in PBS buffer (10 mM, pH 7.4), by adding 5 mM reduced glutathione (GSH), 1 mM L-cysteine and homocysteine, or 200 μ M H₂S, dithiothreitol (DTT), citrate, sodium metabisulfite, or L-ascorbic acid (Figure 2). We observed that HyCL-1 with a carbonate linker displayed poor selectivity against cellular thiols glutathione, cysteine, homocysteine, and DTT (Figure 2a). On the other hand, HyCL-2 with an ether linker showed excellent selectivity, and none of the other species tested displayed significant increases in luminescence intensity over the blank control (Figure 2b).

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When treated with nitroreductase (14 ug/mL) or NADH (0.4 mM) alone, there was no increase in chemiluminescent emission over a blank control, indicating that both enzyme and cofactor are needed to induce a chemiluminescent response from HyCL-1 and HyCL-2. To better understand the response when treating HyCL-1 with cellular relevant thiol species and decipher the poor selectivity of HyCL-1, this probe was treated with cysteine and the reaction progress was monitored via ¹H NMR (Figure S8). This experiment provided two salient observations: 1. The peak at 5.38 ppm corresponding to the -CH₂- methylene peak para to the nitro group rapidly disappeared within 5 minutes, to be replaced by a new peak at 5.32 ppm; 2. The nitroaromatic peaks at 8.18 ppm and 7.58 ppm persist even after 25 hours of reaction time. The first observation is consistent with displacement of the phenol by the reaction of the thiol with the carbonate functional group, thereby initiating chemiluminescence. The second observation confirms the stability of the nitroaromatic group in the presence of cysteine. Taken together, these observations indicate that the ether linkage provides an improved response and selectivity for HyCL-2 over HyCL-1, making it a sensitive chemiluminescent agent for imaging enzymatic reductase activity without interferences from other biological nucleophiles or small molecule reductants.

After demonstrating that HyCL-2 had the ability to detect enzymatic reductase activity with high sensitivity and selectivity, we moved towards testing its ability for hypoxia detection using an in vitro model. In order to interrogate luminescence response to low oxygen conditions, we deoxygenated a solution of 10 mM PBS (pH 7.4) containing 10% Emerald II Enhancer by bubbling nitrogen gas through the solution for 60 minutes. We then compared the chemiluminescent response of HyCL-2 to nitroreductase under oxygen-free conditions and ambient air conditions (Figure 3). At 5, 10, and 12.5 µg/mL nitroreductase a significant increase in luminescence intensity was observed under low oxygen conditions with up to a 5-fold increase at 12.5 µg/mL nitroreductase. A control experiment consisted of bubbling air through a solution of PBS and Emerald II Enhancer for 60 minutes before probe and enzyme incubation. No significant difference in luminescence emission was observed from the experiment performed under ambient conditions, confirming that the increased response is due to deoxygenation and not from a mechanical effect of the bubbling procedure (Figure S9). Bubbling 100% oxygen through the buffer and Enhancer solution provided a small, but not total, decrease in luminescence versus the air-bubbled conditions (Figure S9). These important experiments demonstrate that the luminescent response of HyCL-2 depends sharply on the presence or absence of dissolved oxygen, a necessary trait for imaging tumor hypoxia.

Having well characterized the *in vitro* spectroscopy, we then proceeded to investigate the ability of **HyCL-2** as a CLI agent for nitroreductase activity at physiological pH using an IVIS Spectrum. An opaque 96-well plate was loaded with 10 μM **HyCL-2**, 0.4 mM NADH and 0, 2.5, 7.5,



Figure 4. Imaging of nitroreductase using **HyCL-2**. (a) Images 30 min after adding 10 μ M **HyCL-2** to 0, 2.5, 5, 7.5, 10, 12.5 μ g/mL NTR in 10 mM PBS buffer (pH 7.4) containing 0.4 mM NADH and 10% Emerald II Enhancer (n = 3 wells). (b) Quantification of total photon flux of the images in (a) (n = 3 wells). Error bars are ±S.D.



Figure 5. *In vivo* nitroreductase imaging. (a) Image of a living SCID/BALB-C mouse 30 s after administering subcutaneous injections of 30 µL of a solution containing 40 µM **HyCL-2**, 14 µg mL⁻¹ NTR, 0.4 mM NADH, and 10% Emerald II Enhancer in 10 mM PBS (pH 7.4). In the vehicle control nitroreductase and NADH were replaced with H₂O and 0.01 M NaOH. (b) Quantification of biological replicates (n = 2 mice). Error bars are high and low values of the two replicates.

10, 12.5 μ g/mL nitroreductase in PBS buffer (pH 7.4) containing 10% Emerald II Enhancer. Imaging light pro-



Figure 6. Images of living H1299 lung tumor xenografts on SCID/BALB-C mice 1.5 min after administering intratumoral injections of 100 μ L 40 μ M **HyCL-2** and 10% Emerald II Enhancer in 10 mM PBS (pH 7.4) while breathing (a) air or (b) 100% oxygen. (c) Quantification of biological replicates (n = 2 mice). Error bars are high and low values of the two replicates.

duction indicated a clear increase in luminescence intensity with increasing nitroreductase concentrations (Figure 4a). The emitted light displayed good linearity with increasing concentrations of nitroreductase (Figure 4b), demonstrating the ability of HyCL-2 to accurately and sensitively image reductase activity, with an estimated detection limit (3σ) between 2–10 ng/mL. Encouraged by the robust chemiluminescent light generated from the multi-well plate experiment, we next tested if light production from HyCL-2 would be sufficient for nitroreductase imaging in living animal tissue. Anesthetized SCID/BALB-C mice were administered subcutaneous injections on their back. On the upper back, a solution of HyCL-2, NADH, nitroreductase, and Emerald II Enhancer was injected (Figure 5a, NTR+NADH), and a vehicle control solution with HyCL-2 and no nitroreductase or NADH was injected on the lower back (Figure 5a, Vehicle). The injected area on the upper back displayed a dramatic increase in chemiluminescent emission compared with the vehicle injection without nitroreductase or NADH on the lower side (Figure 5b). These experiments show that HyCL-2 can function as an *in vivo* CLI agent for nitroreductase activity.

Finally, we interrogated the ability of **HyCL-2** to visualize tissue oxygenation and hypoxia in human tumor xenograft models. H1299 lung tumors were grown subcutaneously on the flanks of SCID/BALB-C mice. Tumor oxygenation was adjusted using an oxygen challenge experiment, where mice breathe either air (21% oxygen) or 100%



Figure 7. Multi-spectral optoacoustic tomography (MSOT) images of a living H1299 bearing SCID/BALB-C mouse while breathing (a) 16% oxygen or (b) 100% oxygen. Scale bars are 3 mm.

oxygen for several minutes prior to and during imaging. A solution of HyCL-2 in PBS buffer (pH 7.4) containing 10% Emerald II Enhancer was injected intratumorally and then imaged using an IVIS Spectra. While breathing air (21% oxygen), high chemiluminescence emission was observed (Figure 6a) that decayed over a period of 10 minutes. After allowing time for the agent to clear, the mice were again injected intratumorally with HyCL-2 in PBS buffer (pH 7.4) containing 10% Emerald II Enhancer, but this time with the mice breathing 100% oxygen. In comparison, breathing 100% oxygen caused an attenuation of the chemiluminescent signal (Figure 6b). This indicates, in agreement with the in vitro experiment described in Figure 3, that HyCL-2 provides increased signal in low oxygenation conditions found in hypoxic tumors. In order to further support this claim, the same mice underwent the oxygen challenge experiment while the levels of hemoglobin (Hb) and oxygen-bound hemoglobin (HbO2) were determined by multi-spectral optoacoustic tomography (MSOT) imaging³⁷ (Figure 7). Magnification of the tumor reveals low total hemoglobin in the tumor center, characteristic of a hypoxic core surrounded by blood vasculature. Comparison of the images of the mouse breathing 16% oxygen (Figure 7a) to the images of the mouse breathing 100% oxygen (Figure 7b) shows a clearly observable increase in HbO₂, consistent with the data collected by chemiluminescent imaging and providing a sec-

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59 60 ondary confirmation. Taken together, these experiments provide a preliminary validation of the CLI agent **HyCL-2** for imaging tumor hypoxia.

Conclusions

We have designed and synthesized two spiroadamantane 1,2-dioxetane chemiluminescent reaction-based imaging probes, **HyCL-1** and **HyCL-2**, that display immediate light emission upon reacting with nitroreductase and NADH at physiological pH. Due to our scaffold optimization, the ether linked chemiluminescent agent **HyCL-2** responds to nitroreductase with ~170-fold increase in luminescence intensity compared to a blank control, largely due to a drastically reduced background of the more hydrolytically stable ether linkage. This ether linkage is also critical to achieving high selectivity, particularly towards abundant biological thiol species. **HyCL-2** has been successively applied for detection of nitroreductase using spectrophotometers, and imaging nitroreductase *in vivo* using an IVIS Spectra instrument.

Studies on the oxygen dependence of the chemiluminescence emission of HyCL-2 in vitro revealed increases in luminescence in the absence of oxygen, a result that was also observed during in vivo oxygen challenge experiments in human H1299 lung tumor xenografts grown on mice. It is unlikely that reductase expression changes within the timeframe of the imaging experiment and the differences in luminescent emission are most likely due to the change in oxygen levels. While the oxygendependence of the probe in vivo is consistent with other nitroaromatic prodrugs and imaging agents,¹¹⁻²³ the oxygen-sensitivity in vitro is striking because the nitroreductase used in this study is generally believed to be oxygeninsensitive.78,79 This suggests a secondary mechanism of oxygen-sensitivity for HyCL-2, potentially the quenching of triplet state products of the chemiluminescent reaction.^{80,81} Tumor hypoxia and changes in oxygenation during the oxygen challenge experiments were independently confirmed by MSOT imaging of hemoglobin and oxygenated hemoglobin as a technique to directly measure in vivo blood oxygen levels. While this application of MSOT is incapable of direct oxygen measurements in central tumor areas with no vasculature, it provides supportive and complementary data to the CLI experiments performed herein.

It should be noted that similar CLI experiments on larger tumors failed to produce consistent results due to decay of light intensity with imaging depth and attempts at imaging hypoxia in cell culture models were complicated by technical challenges with adding chemiluminescence reagents in the absence of oxygen. Future work aims to solve these challenges by developing single component agents with increased light production and nonintensity based readouts that can more accurately report on parameters without the confounding variables of imaging depth and temporal dependence. With these caveats in mind, **HyCL-2** can find application for optical monitoring of tumor oxygenation in well-controlled preclinical experiments. We further anticipate that these studies will contribute towards the generalized development of chemiluminescence as a robust *in vivo* imaging modality.

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The manuscript was written through contributions of all authors. All authors have given approval to the final version of the manuscript.

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Conflict of Interest

The authors declare no competing financial interest.

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Supporting Information

Synthetic procedures, absorption and emission spectra, detailed procedures for selectivity tests, supplementary procedures and figures, and scanned spectra. The Supporting Information is available free of charge on the ACS Publications website. See DOI: 10.1039/b000000x/.

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